Kewal K. Jain

The Handbook of Nanomedicine

Third Edition

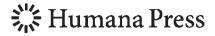
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The Handbook of Nanomedicine

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Kewal K. Jain Jain PharmaBiotech Basel, Switzerland

ISBN 978-1-4939-6965-4 DOI 10.1007/978-1-4939-6966-1

ISBN 978-1-4939-6966-1 (eBook)

Library of Congress Control Number: 2017933292

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Printed on acid-free paper

This Humana Press imprint is published by Springer Nature

The registered company is Springer Science+Business Media LLC

The registered company address is: 233 Spring Street, New York, NY 10013, U.S.A.

Foreword

The Handbook of Nanomedicine provides a thorough guide to this new and very important interdisciplinary area of science and technology. It provides both the basics and a classification system for nanomedicine. Important areas such as nano-arrays, nanofluidics, nanoparticles, nanogenomics, nanoproteomics, nanobiotechnology, nanomolecular diagnostics, and nanopharmaceuticals are evaluated. The role of biotechnology in biological therapies, and in particular oncology, is discussed. Nanodevices in surgery and medicine are also examined. Another important focus of this handbook is the role of nanomedicine in medical specialty areas — particularly in – neurology, cardiology, dermatology, pulmonology, geriatrics, orthopedics, and ophthalmology. Nanomedicine in microbiology, and in regenerative medicine and tissue engineering, is also discussed. In addition, ethical, safety, regulatory educational, and commercialization issues are discussed. Finally, this handbook concludes with an assessment of the future of nanomedicine, which is very bright.

Massachusetts Institute of Technology Cambridge, MA, USA Robert Langer

Preface to the Third Edition

Rapid advances in nanobiotechnology and increasing translation into clinical nanomedicine have necessitated a new edition since the second edition in 2012. The chapter titles have been retained along with some basic information, which still holds, but most of the material has been replaced with new developments. Important classical references were left in, while new ones have been added. Most of the advances have occurred in nanopharmaceuticals, particularly drug delivery using nanobiotechnology. Nanooncology remains the major therapeutic area, although considerable advances have been made in other therapeutic areas. Several new nanobiotechnology-based products have been approved and some are in clinical trials. There is still an ongoing discussion of regulatory issues. Nanobiotechnology continues to play an increasingly important role in personalized medicine. The style of previous editions has been maintained, and the terminology is kept simple for a varied audience consisting of physicians, scientists, and other interested persons.

The author wishes to acknowledge the help and encouragement received from David Casey, publisher's editor, and Patrick J. Marton at Springer during preparation of this book.

Basel, Switzerland

Kewal K. Jain

Preface to the Second Edition

Considerable advances have taken place in nanomedicine since the first edition of the book in 2008. The basic plan of the book has been retained with some reorganization, but most of the material has been updated or replaced with new developments. Important classical references were left in while new ones have been added. Most of the advances have occurred in nanodiagnostics and nanopharmaceuticals, particularly drug delivery using nanobiotechnology. Nanooncology remains the major area of clinical application although considerable advances have been made in other therapeutic areas, particularly nanocardiology and nanoneurology. Several new products have been approved, and clinical applications of nanobiotechnology are progressing. This has required the discussion of some regulatory issues. Combination of diagnosis and therapy is facilitated by nanobiotechnology and fits in with concepts of personalized medicine, which is being increasingly accepted. As with the first edition, requirements of both physicians and scientists have been kept in mind. However, the description is kept simple enough to be understood by any educated lay person.

The author wishes to acknowledge the help and encouragement received from Patrick J. Marton, Senior Editor, Springer Protocols, Humana Press, in completion of the project. David Casey has done an excellent job of editing and organizing this book.

Basel, Switzerland

Kewal K. Jain

Preface to the First Edition

Nanomedicine is application of nanobiotechnology to clinical medicine. However, new technologies do not always enter medical practice directly. Nanobiotechnologies are being used to research the pathomechanism of disease, refine molecular diagnostics, and help in the discovery, development, and delivery of drugs. In some cases, nanoparticles are the nanomedicines. The role is not confined to drugs before devices, and surgical procedures are refined by nanobiotechnology, referred to as nanosurgery.

This handbook covers the broad scope nanomedicine. Starting with the basics, the subject is developed to potential clinical applications many of which are still at an experimental stage. The prefix nano is used liberally and indicates the nanodimension of existing scientific disciples and medical specialties. Two important components of nanomedicine are nanodiagnostics and nanopharmaceuticals and constitute the largest chapters.

Keeping in mind that the readers of the book will include nonmedical scientists, pharmaceutical personnel, as well as physicians, technology descriptions and medical terminology are kept as simple as possible. As a single author book, duplication is avoided. I hope that readers at all levels will find it a concise, comprehensive, and useful source of information.

There is voluminous literature relevant to nanomedicine. Selected references are quoted in the text.

Basel, Switzerland

Kewal K. Jain

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About the Author

Kewal K. Jain is a neurologist/neurosurgeon by training and has been working in the biotechnology/biopharmaceuticals industry for several years. He received graduate training in both Europe and the USA, has held academic positions in several countries, and is a Fellow of the Faculty of Pharmaceutical Medicine of the Royal College of Physicians of UK. Currently he is a consultant at Jain PharmaBiotech. Prof. Jain's 465 publications include 27 books (5 as editor +22 as author) and 50 special reports, which have covered important areas in biotechnology, gene therapy, and biopharmaceuticals. His recent books include Role of Nanobiotechnology in Molecular Diagnostics (2006), Handbook of Nanomedicine (Humana/Springer 2008; Chinese edition, Peking University Press 2011, 2nd ed Springer 2012, 3rd ed 2017), Textbook of Personalized Medicine (Springer 2009; Japanese ed 2012; 2nd ed Springer, 2015), Handbook of Biomarkers (Springer 2010; Chinese edition, Chemical Industry Press 2016), Handbook of Neuroprotection (Springer 2011), Applications of Biotechnology in Cardiovascular Therapeutics (Springer 2011), Applications of Biotechnology in Neurology (Springer 2013), and Applications of Biotechnology in Oncology (Springer 2014). He has edited Drug Delivery Systems, 2nd ed (Springer 2014) and Applied Neurogenomics (Springer 2015).

Abbreviations

AFM	Atomic force microscopy
BBB	Blood-brain barrier
BioMEMS	Biological Micro ElectroMechanical Systems
CNS	Central nervous system
DNA	Deoxyribonucleic acid
DPN	Dip pen nanolithography
ELISA	Enzyme-linked immunosorbent assay
FDA	Food and Drug Administration (USA)
FRET	Fluorescence resonance energy transfer
LNS	Lipid nano-sphere
MEMS	Micro ElectroMechanical Systems
MNP	Magnetic nanoparticle
MRI	Magnetic resonance imaging
NCI	National Cancer Institute (USA)
NIH	National Institutes of Health (USA)
NIR	Near-infrared
NP	Nanoparticle
ODN	Oligodeoxynucleotide
PAMAM	Polyamidoamine (dendrimers)
PCR	Polymerase chain reaction
PEG	Polyethylene glycol
PEI	Polyethylenimine
PLA	Polylactides
PLGA	Poly(lactic-co-glycolic) acid
POC	Point-of-care
QD	Quantum dot
RLS	Resonance light scattering

RNA	Ribonucleic acid
SERS	Surface-enhanced Raman scattering

- Single nucleotide polymorphism Scanning probe microscope SNP
- SPM
- Surface plasmon resonance SPR

Chapter 1 Introduction

Nanomedicine

Nanomedicine is defined as the application of nanobiotechnology to medicine. It is a discipline at the interface of medicine and nanobiotechnology but is not a subspecialty of either of these. Its broad scope covers the use of nanoparticles and nanodevices in healthcare for diagnosis as well as therapeutics. Safety, ethical and regulatory issues are also included. Figure 1.1 shows the relationship of various biotechnologies to nanomedicine.

Basics of Nanobiotechnology

Nanotechnology (Greek word nano means dwarf) is the creation and utilization of materials, devices, and systems through the control of matter on the nanometerlength scale, i.e. at the level of atoms, molecules, and supramolecular structures. Nanotechnology, as defined by the National Nanotechnology Initiative (http://www. nano.gov/), is the understanding and control of matter at dimensions of roughly 1-100 nm, where unique phenomena enable novel applications. Encompassing nanoscale science, engineering and technology, nanotechnology involves imaging, measuring, modeling, and manipulating matter at this length scale. The simplified version of the definition – anything with "one or more external dimensions" between 1 and 100 nm" - is confusing, because nanomaterials can and often do shift shape, e.g. under UV rays, or inside cells, or out in the environment when interacting with other small particles. And particles >100 nm often display nanolike qualities, meaning they act as strangely as the slightly smaller particles do. Some conjugated complex nanoparticles are larger than 100 nm. More than 150 polymers, liposomes, metals, and many other materials, with sizes ranging from 1 to 300 nm, are approved or under investigation as diagnostic and imaging agents, as therapeutics and for enhancing drug delivery,

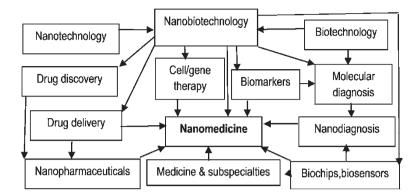


Fig. 1.1 Relationship of various biotechnologies to nanomedicine (© Jain PharmaBiotech)

Object	Dimension
Width of a hair	50,000 nm
Red blood cell	2500 nm
Vesicle in a cell	200 nm
Bacterium	1000 nm
Virus	100 nm
Exosomes (nanovesicles shed by dendritic cells)	65–100 nm
Width of DNA	2.5 nm
Ribosome	2–4 nm
A base pair in human genome	0.4 nm
Proteins	1–20 nm
Amino acid (e.g. tryptophan, the largest)	1.2 nm (longest measurement)
Aspirin molecule	1 nm
An individual atom	0.25 nm

Table 1.1 Dimensions of various objects in nanoscale

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Nanotechnology is the popular term for the construction and utilization of functional structures with at least one characteristic dimension measured in nanometers – a nanometer is one billionth of a meter (10^{-9} m) . This is roughly four times the diameter of an individual atom and the bond between two individual atoms is 0.15 nm long. Proteins are 1–20 nm in size. The definition of 'small', another term used in relation to nanotechnology, depends on the application, but can range from 1 nm to 1 mm. Nano is not the smallest scale; further down the power of ten are angstrom (=0.1 nm), pico, femto, atto and zepto. By weight, the mass of a small virus is about 10 attograms. An attogram is one-thousandth of a femtogram, which is one-thousandth of a picogram, which is one-thousandth of a nanogram. Dimensions of various objects in nanoscale are shown in Table 1.1.

Given the inherent nanoscale functional components of living cells, it was inevitable that nanotechnology will be applied in biotechnology giving rise to the term

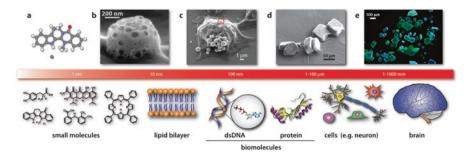


Fig. 1.2 Sizes of biologically entities relevant to the brain. (*Top row* (above scale bar) From *left to right*: (a) X-ray crystal structure of Alzheimer's disease candidate drug, dehydroevodiamine HCl (DHED); (b, c) porous metal oxide microspheres being endocytosed by BV2 microglia cell (close-up and low magnification) SEM images, (d, e) SEM and fluorescence micrograph of DHED microcrystals (DHED is blue-green luminscent). (*Bottom row* below the scale bar) *Left to right*: Small molecules, such as dopamine, minocycline, mefenamic acid, DHED, and heme, are ~1 nm or smaller. The lipid bilayer is a few nanometers thick. Biomolecule such as a microRNA and a protein are only a few nanometers in size. A single cell or neuron is tens or hundreds of microns in size. Size of human brain is tens of centimeters (Reproduced from: Suh et al. (2009), by permission)

nanobiotechnology. A brief introduction will be given to basic nanotechnologies from physics and chemistry, which are now being integrated into molecular biology to advance the field of nanobiotechnology. The aim is to understand the biological processes to improve diagnosis and treatment of diseases. Sizes of biologically entities relevant to the brain are shown in Fig. 1.2.

European Union Definition of Nanomaterials

The European Commission (EU)'s definition of Nanomaterials followed >6 years of scientific consideration of the challenges posed by nanomaterials (European Commission 2011). It is worded as follows:

"nanomaterial is a natural, incidental or manufactured material containing particles, in an unbound state or as an aggregate or as an agglomerate and where, for 50% or more of the particles in the number size distribution, one or more external dimensions is in the size range 1 nm - 100 nm".

The EU document is a milestone as the missing jigsaw piece, ready to slot into publically-driven and government-derived legislation, covering nanomaterial matters from manufacture, labeling and handling, through transport and environmental fate. Main elements of the definition are:

- 1. Counting particles defines nanomaterials: The material is a nanomaterial if >50% of particles have at least one dimension between 1 and 100 nm.
- 2. Alternatively, it is also a nanomaterial if it has a specific surface per unit volume of over 60 m²/cm³.

- 3. There are specific inclusions such as graphene.
- 4. Naturally occurring and incidental materials are included, as well as manufactured particles.
- 5. Aggregates and agglomerates of such particles are included.

No measurement methods are specified; the recommendation is 'best available alternative methods should be applied'. This definition is not regulation; however, its EU provenance informs its authority. The defining of nanomaterials is the cornerstone of any subsequent legislation, and the scientific committee of the EU has determined that number count is at the heart of this definition. The Scientific Committee on Emerging and Newly Identified Health Risks (SCENIHR) publication "Scientific Basis for the Definition of the Term "Nanomaterial", describes in depth the reasoning behind the definition. SCENIHR exhaustively discuss the possible measures and their benefits, and make clear the large areas of ambiguity and difficulty in these judgments. Techniques for measurement of size and distribution of nanoparticles in a sample to comply with EU requirements are described in Chap. 2.

Nanoscale Time and Light

Beyond nanomaterials, nanoscale has been applied to time and light. A nanosecond (ns) is an SI unit of time equal to one billionth of a second (10^{-9}) . Light travels ~29.9 cm (11.8 inches) in 1 ns, leading to designation of ns as a light-foot (actually = ~1.0167 ns).

This time scale is used in telecommunications, pulsed lasers and some areas of electronics. Nanosecond pulsed electric fields (nsPEFs) is a novel non-thermal approach to induce cell apoptosis, and its role in treatment of cancer is described in Chap. 8.

Nanolasers

A nanolaser is a laser (light amplifier by stimulated emission of radiation) that has nanoscale dimensions. This tiny laser can be modulated quickly and, combined with its small footprint, makes it an ideal candidate for on-chip optical computing. The intense optical fields of such a nanolaser also enable the enhancement effect in non-linear optics or surface-enhanced-raman-scattering (SERS), and therefore paves the way toward integrated nanophotonic circuitry. A working room-temperature nanolaser was based on 3D Au bowtie (nanoparticles) and supported by an organic gain material (Suh et al. 2012). The extreme field compression, and thus ultrasmall mode volume, within the bowtie gaps produces laser oscillations at the localized plasmon resonance gap mode of the 3D bowties. Transient absorption measurements confirmed ultrafast resonant energy transfer between photoexcited

dye molecules and gap plasmons on the picosecond time scale. These plasmonic nanolasers are anticipated to be readily integrated into Si-based photonic devices, all optical circuits, and nanoscale biosensors. Use of nanolasers in surgery in is described later in this report.

Relation of Nanobiotechnology to Nanomedicine

Technical achievements in nanotechnology are being applied to improve drug discovery, drug delivery and pharmaceutical manufacturing. A vast range of applications has spawned many new terms, which are defined as they are described in various chapters. Numerous applications in the pharmaceutical industry can also be covered under the term "nanobiopharmaceuticals".

Landmarks in the Evolution of Nanomedicine

Historical landmarks in the evolution of nanomedicine are shown in Table 1.2.

Year	Landmark
1905	Einstein published a paper that estimated the diameter of a sugar molecular as about 1 nm.
1931	Max Knoll and Ernst Ruska discovered electron microscope, which enabled subnanomolar imaging.
1959	Nobel Laureate Richard Feynman gave a lecture entitled 'There's plenty of room at the bottom', at the annual meeting of the American Physical Society He outlined the principle of manipulating individual atoms using larger machines to manufacture increasingly smaller machines (Feynman 1992).
1974	Start of development of molecular electronics by Aviram and Rattner (Hush 2003).
1974	Norio Tanaguchi of Japan coined the word "nanotechnology".
1979	Colloidal gold nanoparticles used as electron-dense probes in electron microscopy and immunocytochemistry (Batten and Hopkins 1979).
1981	Conception of the idea of designing molecular machines analogous to enzymes and ribosomes (Drexler 1981).
1984	The first description the term dendrimer and the method of preparation of poly(amidoamine) dendrimers (Tomalia et al. 1985).
1985	Discovery of bucky balls (fullerenes) by Robert Curl, Richard Smalley and Harold Kroto, which led to the award of Nobel Prize for chemistry in 1996 (Smalley 1985; Curl et al. 1997).
1987	Publication of the visionary book on nanotechnology potential "Engines of Creation" (Drexler 1987).
1987	Cancer targeting with nanoparticles coated with monoclonal antibodies (Douglas et al. 1987).
	(continued)

 Table 1.2
 Historical landmarks in the evolution of nanomedicine

Table 1.2	(continued)
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Year	Landmark
1988	Maturation of the field of supramolecular chemistry relevant to nanotechnology: construction of artificial molecules that interact with each other and are (Lehn 1988). Awarded Nobel prize.
1990	Atoms visualized by the scanning tunneling microscope discovered in 1980's at the IBM Zürich Laboratory (Zürich, Switzerland), which led to award of a Nobel prize (Eigler and Schweizer 1990).
1991	Discovery of carbon nanotubes (Iijima et al. 1992).
1992	Principles of chemistry applied to the bottom-up synthesis of nanomaterials (Ozin 2009)
1994	Nanoparticle-based drug delivery (Kreuter 1994).
1995	FDA approved Doxil, a liposomal formulation of doxorubicin, as an intravenous chemotherapy agent for Kaposi sarcoma. Drug carried by nanosize liposomes is less toxic with targeted delivery.
1997	Founding of the first molecular nanotechnology company - Zyvex Corporation.
1998	First use of nanocrystals as biological labels, which were shown to be superior to existing fluorphores (Bruchez et al. 1998).
1998	Use of DNA-gelatin nanospheres for controlled gene delivery (Truong-Le et al. 1998).
1998	Use of the term "nanomedicine" in publications (Freitas 1998).
2000	Nanotechnology Initiative announced in the US (Roco 2003).
2000	First FDA approval of a product incorporating the NanoCrystal® technology (Elan), solid-dose formulation of the immunosuppressant sirolimus – Rapamune® (Wyeth).
2003	Concept for nanolaser was developed at Georgia State University using nanospheres and nanolens system (Li et al. 2003).
2003	The US Senate passed the Nanotechnology Research & Development Act making the National Nanotechnology Initiative into law and authorized \$3.7 billion over the next 4 years for the program.
2005	FDA approved Abraxane TM , a taxane based on nanotechnology, for the treatment of breast cancer. Nanoparticle form of the drug overcomes insolubility problems encountered with paclitaxel and avoids the use of toxic solvents.
2014	Award of Nobel Prize in Chemistry to one German and two US scientists for discovery of nanoscopy.

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Nanomedicine as a Part of Evolution of Medicine

Medicine is constantly evolving and new technologies are incorporated into the diagnosis and treatment of patients. This process is sometimes slow and there can be a gap of years before new technologies are integrated in medical practice. The reasons for the delay are:

- Establishing the safety and efficacy of innovative treatments is a long process, particularly with clinical trials and regulatory reviews.
- Current generation of physicians are still not well oriented towards biotechnology and conservative elements of the profession may be slow in accepting and learning about nanobiotechnology, which is at the cutting edge of biotechnology.

• High cost of new technologies is a concern for the healthcare providers. Cost-benefit studies are needed to convince the skeptics that some of the new technologies may reduce the overall cost of healthcare.

Molecular medicine, a recognized term, should not be considered a subspecialty of medicine as molecular technologies have an overall impact on the evolution of medicine. Recognition of the usefulness of biotechnology has enabled progress in the concept of personalized medicine, which is also not a branch of medicine but simply indicates a trend in healthcare and the prescription of specific treatments best suited for an individual (Jain 2015). Various nanomachines and other nano-objects that are currently under investigation in medical research and diagnostics will soon find applications in the practice of medicine. Nanobiotechnologies are being used to create and study models of human diseases, e.g. immune disorders. Introduction of nanobiotechnologies in medicine will not create a separate branch of medicine but simply improve diagnosis as well as therapy. Current research is exploring the fabrication of designed nanostructures, nanomotors, microscopic energy sources, and nanocomputers at the molecular scale, along with the means to assemble them into larger systems, economically and in great numbers. Table 1.3 show some of the applications of nanobiotechnology in medicine.

Nanodiagnostics
Extending limits of detection by refining currently available molecular diagnostic technologies
Development of new nanotechnology-based assays
Nanobiosensors
Nanoendoscopy
Nanoimaging
Nanopharmaceuticals
Nanoparticulate formulations of drugs
Nanotechnology-based drug discovery
Nanotechnology-based drug delivery
Regenerative medicine
Use of nanotechnology for tissue engineering
Transplantation medicine
Exosomes from donor dendritic cells for drug-free organ transplants
Nanomedicine relevant to subspecialties
Nanocardiology
Nanodermatology
Nanodentistry
Nanogerontology
Nanohematology
Nanoimmunology
Nanomicrobiology
(continued)

 Table 1.3
 Nanomedicine in the twenty-first century

Nanonephrology

Nanoneurology

Nanooncology

Nanoophthalmology

Nanoorthopedics

Implants

Bioimplantable sensors that bridge the gap between electronic and neurological circuitry Durable rejection-resistant artificial tissues and organs

Implantations of nanocoated stents in coronary arteries to elute drugs and to prevent reocclusion Implantation of nanoelectrodes in the brain for functional neurosurgery

Implantation of nanopumps for drug delivery

Nanosurgery

Minimally invasive surgery: miniaturized nanosensors implanted in catheters to provide real-time data

Nanosurgery by integration of nanoparticles and external energy, nanolasers

Nanorobotic treatments

Vascular surgery by nanorobots introduced into the vascular system

Nanorobots for detection and destruction of cancer

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References

- Batten TF, Hopkins CR. Use of protein A-coated colloidal gold particles for immunoelectronmicroscopic localization of ACTH on ultrathin sections. Histochemistry. 1979;60:317–20.
- Bruchez Jr M, Moronne M, Gin P, Weiss S, Alivisatos AP. Semiconductor nanocrystals as fluorescent biological labels. Science. 1998;281:2013–6.
- Curl RF, Kroto H, Smalley RE. Nobel lectures in chemistry. Rev Mod Phys. 1997;69:691-730.
- Douglas SJ, Davis SS, Illum L. Nanoparticles in drug delivery. Crit Rev Ther Drug Carrier Syst. 1987;3:233–61.
- Drexler KE. Engines of creation, the coming era of nanotechnology. New York: Anchor; 1987.
- Drexler KE. Molecular engineering: an approach to the development of general capabilities for molecular manipulation. Proc Natl Acad Sci U S A. 1981;78:5275–8.
- Eigler DM, Schweizer EK. Positioning single atoms with a scanning tunneling microscope. Nature. 1990;344:524–6.
- European Commission. Recommendation of 18 October 2011 on the definition of nanomaterial. Official Journal of the European Union 2011/696/EU. 2011.; http://eur-lex.europa.eu/ LexUriServ/LexUriServ.do?uri=OJ:L:2011:275:0038:0040:EN:PDF
- Feynman R. There's plenty of room at the bottom: an invitation to enter a new filed of physics. Reprinted in: Crandall BC, Lewis J, editors. Nanotechnology: research and perspectives. Cambridge, MA: The MIT Press; 1992. p. 347–63.
- Freitas Jr RA. Exploratory design in medical nanotechnology: a mechanical artificial red cell. Artif Cells Blood Substit Immobil Biotechnol. 1998;26:411–30.
- Hush NS. An overview of the first half-century of molecular electronics. Ann N Y Acad Sci. 2003;1006:1–20.
- Iijima S, Ajayan PM, Ichihashi T. Growth model for carbon nanotubes. Phys Rev Lett. 1992;69:3100-3.

Jain KK. Textbook of personalized medicine. 2nd ed. New York: Springer; 2015.

- Kreuter J. Drug targeting with nanoparticles. Eur J Drug Metab Pharmacokinet. 1994;19:253-6.
- Lehn JM. Supramolecular chemistry scope and perspectives: molecules, supermolecules, and molecular devices. Ang Chem Int Ed Engl. 1988;27:89–112.
- Li K, Stockman MI, Bergman DJ. Self-similar chain of metal nanospheres as an efficient nanolens. Phys Rev Lett. 2003;91:227402.
- Ozin GA, Arsenault AC, Cademartiri L. Nanochemistry: a chemical approach to nanomaterials. 2nd ed. Cambridge, UK: Royal Society of Chemistry; 2009.
- Roco MC. Nanotechnology: convergence with modern biology and medicine. Curr Opin Biotechnol. 2003;14:337–46.
- Smalley RE. Supersonic cluster beams: an alternative approach to surface science. In: Bartlett RJ, editor. Comparison of Ab initio quantum chemistry with experiments for small molecules. Boston: D. Riedel; 1985.
- Suh WH, et al. Nanotechnology, nanotoxicology, and neuroscience. Prog Neurobiol. 2009;87:133-70.
- Suh JY, Kim CH, Zhou W, et al. Plasmonic bowtie nanolaser arrays. Nano Lett. 2012;12:5769–74.
- Tomalia DA, Baker H, Dewald J, et al. A new class of polymers: starburst-dendritic macromolecules. Polym J. 1985;17:117–32.
- Truong-Le VL, August JT, Leong KW. Controlled gene delivery by DNA-gelatin nanospheres. Hum Gene Ther. 1998;9:1709–17.

Chapter 2 Nanotechnologies

Introduction

This chapter will focus on nanobiotechnologies that are relevant to applications in biomedical research, diagnostics, and medicine. Invention of the microscope revolutionized medicine by enabling the detection of microorganisms and study of histopathology of disease. Microsurgery was a considerable refinement over crude macrosurgery and opened the possibilities of procedure that were either not carried out previously or had high mortality and morbidity. Nanotechnologies, by opening the world beyond microscale, will have a similar impact on medicine and surgery. Various nanobiotechnologies are described in detail in a special report on this topic (Jain 2017). Those relevant to understanding of diseases are described briefly in this chapter.

Classification of Nanobiotechnologies

It is not easy to classify the vast range of nanobiotechnologies. Some just represent motion on a nanoscale but most of them are based on nanoscale structures, which come in a variety of shapes and sizes. A few occur in nature but most are engineered. The word nano is prefixed to just about anything that deals with nanoscale. It is not just biotechnology but many other disciplines such as nanophysics, nanobiology, etc. A simplified classification of basic nanobiotechnologies is shown in Table 2.1. Some technologies such as nanoarrays and nanochips are further developments.

Nanoparticles	
Fluorescent nanoparticles	
Fullerenes	
Gold nanoparticles	
Lipoparticles	
Magnetic nanoparticles	
Nanocrystals	
Nanoparticles assembly into micelles	
Nanoshells	
Paramagnetic and superparamagnetic nanoparticles	
Polymer nanoparticles	
Quantum dots	
Silica nanoparticles	
Nanofibers	
Nanowires	
Carbon nanofibers	
Dendrimers	
Polypropylenimine dendrimers	
Composite nanostructures	
Cochleates	
DNA-nanoparticle conjugates	
Nanoemulsions	
Nanoliposomes	
Nanocapsules enclosing other substances	
Nanoshells	
Nanovesicles	
Nanoconduits	
Nanotubes	
Nanopipettes	
Nanoneedles	
Nanochannels	
Nanopores	
Nanofluidics	
Nanostructured silicon	
Nanoscale motion and manipulation at nanoscale	
Cantilevers	
Femtosecond laser systems	
Nanomanipulation	
Surface plasmon resonance	
Visualization at nanoscale	
Atomic force microscopy	
Magnetic resonance force microscopy and nanoscale MRI	
Multiple single-molecule fluorescence microscopy	

 Table 2.1
 Classification of basic nanomaterials and nanobiotechnologies

(continued)

Table 2.1 ((continued)
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Nanoparticle characterization by Halo™ LM10 technology Nanoscale scanning electron microscopy Near-field scanning optical microscopy Optical Imaging with a Silver Superlens Partial wave spectroscopy Photoactivated localization microscopy Scanning probe microscopy Super-resolution microscopy for in vivo cell imaging Ultra-nanocrystalline diamond Visualizing atoms with high-resolution transmission electron microscopy

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Nanoparticles

Nanoparticles (NPs) form the bulk of nanomaterials. There are two main families of nanoparticles: nanospheres with a homogeneous structure in the whole particle, and nanocapsules, which exhibit a typical core-shell structure. They can be made of different materials, e.g., gold. A NP contains tens to thousands of atoms and exists in a realm that straddles the quantum and the Newtonian. At this size, every particle has new properties that change depending on its size. As matter is shrunk to nanoscale, electronic and other properties change radically. NPs may contain unusual forms of structural disorder that can significantly modify their material properties and thus they cannot just be considered as small pieces of bulk material. Two NPs, both made of pure gold, can exhibit markedly different behavior – different melting temperature, different electrical conductivity, and different color - if one is larger than the other. That creates a new way to control the properties of materials. Instead of changing composition, one can change size. Some applications of nanoparticles take advantage of the fact that more surface area is exposed when material is broken down to smaller sizes. For magnetic NPs, the lack of blemishes produces magnetic fields remarkably strong considering the size of the particles. NPs are also so small that in most of them, the atoms line up in perfect crystals without a single blemish.

Zinc sulfide NPs a mere ten atoms across have a disordered crystal structure that puts them under constant strain, increasing the stiffness of the particles and probably affecting other properties, such as strength and elasticity. In similar semiconducting NPs, such as those made of cadmium selenide, slight differences in size lead to absorption and emission of different wavelengths of light, making them useful as fluorescent tracers. The dominant cause of such properties is quantum mechanical confinement of the electrons in a small package. But the disordered crystal structure now found in nanoparticles could affect light absorption and emission also. X-ray diffraction of single nanoparticles is not yet possible and other methods are used to analyze X-ray diffraction images of nanoparticles to separate the effects of size from those of disordered structure. As a measure of particle size in solution, the Nanotechnology Characterization Laboratory of NCI in the USA uses dynamic light scattering (DLS), during which a laser beam is scattered off the nanoparticle and small fluctuations in the intensity of the scattered light are monitored. DLS is very sensitive to soft molecules such as polymers, proteins, and antibodies because they cause significant frictional drag that the technique detects.

It is beyond the scope of this Handbook to describe all NPs. A few selected NPs relevant to nanomedicine are described briefly in the following pages. Lipoparticles or nanoliposomes will be described under liposomes in Chap. 5 as they play an important role in drug delivery.

Gold Nanoparticles

Mass spectrometry analysis has determined the formula of gold nanocrystal molecules to be Au333(SR)79 (Qian et al. 2012). This metallic nanocrystal molecule exhibits fcc-crystallinity and surface plasmon resonance (SPR) at ~7 to 720 nm. Simulations have revealed that atomic shell largely contributes to the robustness of Au333(SR)79, albeit the number of free electrons is also consistent with electron shell closing based on calculations using a confined free electron model. This work clearly demonstrates that atomically precise nanocrystal molecules are achievable and that the factor of atomic shell closing contributes to their extraordinary stability compared to other sizes.

Ultrashort pulsed laser ablation in liquids represents a powerful tool for the generation of pure gold nanoparticles avoiding chemical precursors and thereby making them useful for biomedical applications. However, there is a concern that their biochemical properties may change because of their properties of accepting electrons, which often adsorb onto the nanoparticles. A study has shown that cotransfection of plasmid DNA and laser-generated gold nanoparticles does not disturb the bioactivity of GFP-HMGB1 fusion protein – either uptake of the vector through the plasma membrane or protein accumulation in the nucleus (Petersen et al. 2009). Thus laser-generated gold nanoparticles provide a good alternative to chemically synthesized nanoparticles for use in biomedical applications.

DNA molecules are attached to gold nanoparticles, which tangle with other specially designed pieces of DNA into clumps that appear blue. The presence of lead causes the connecting DNA to fall apart. That cuts loose the individual gold nanoparticles and changes the color from blue to red. Gold nanoparticles are also used as a connecting point to build biosensors for detection of disease. A common technique for a diagnostic test consists of an antibody attached to a fluorescent molecule. When the antibody attaches to a protein associated with the disease, the fluorescent molecule lights up under ultraviolet light. Instead of a fluorescent molecule, a gold nanoparticle can be attached to the antibody and other molecules such as DNA can be added to the nanoparticle to produce bar codes. Because many copies of the antibodies and DNA can be attached to a single nanoparticle, this approach is much more sensitive and accurate than the fluorescent-molecule tests used currently.

Cubosomes

When surfactants are added to water at high concentrations they self-assemble to form thick fluids called liquid crystals. The most viscous liquid crystal is bicontinuous cubic phase, a unique material that is clear and resembles stiff gelatin. When cubic phase is dispersed into small particles, these nanoparticles are termed cubosomes. Within cubosomes, amphiphilic lipids in definite proportions are organized in 3D as honeycombed structures and divided into internal aqueous channels that can be loaded with biopharmaceuticals (Karami and Hamidi 2016). Methods and compositions for producing lipid-based cubic phase nanoparticles were first discovered in the 1990s. Since then several studies have described properties such as particle size, morphology, and stability of cubic phase dispersions, which can be tuned by composition and processing conditions. Stable particle dispersions with consistent size and structure can be produced by a simple processing scheme comprising a homogenization and heat treatment step. Because of their unique microstructure, they are biologically compatible and capable of controlled release of solubilized active ingredients such as drugs and proteins. As a drug delivery vehicle, high drug payloads, stabilization of peptides or proteins and simple preparation process are also advantages of a cubosome. The ability of cubic phase to incorporate and control release of drugs of varying size and polar characteristics, and biodegradability of lipids make it a versatile drug delivery system for various routes of administration, including oral, topical (or mucosal), transdermal and intravenous. Furthermore, proteins in cubic phase appear to retain their native conformation and bioactivity, and are protected against chemical and physical inactivation.

Fluorescent Nanoparticles

Microwave plasma technique has been used to develop fluorescent nanoparticles. In a second reaction, a layer of organic dye is deposited and the final step is an outer cover of polymer, which protects the nanoparticles from exposure to environments. Each layer has characteristic properties. The size of the particles varies and these are being investigated for applications in molecular diagnostics. Fluorescent nanoparticles can also be used as labels for immunometric assays

Switchable fluorescent silica nanoparticles have been prepared by covalently incorporating a fluorophore and a photochromic compound inside the particle core (May et al. 2012). The fluorescence can be switched reversibly between an on- and off-state via energy transfer. The particles were synthesized using different amounts of the photoswitchable compound (spiropyran) and the fluorophore (rhodamine B) in a size distribution between 98 and 140 nm and were characterized in terms of size, switching properties, and fluorescence efficiency by TEM, and UV\Vis and fluorescence spectroscopy.

Fullerenes

Fullerene technology derives from the discovery in 1985 of Carbon-60, a molecule of 60 carbon atoms that form a hollow sphere 1 nm in diameter. The molecule was named buckyball or fullerene or buckminsterfullerene, because of its similarity to the geodesic dome designed by Buckminster Fuller. Subsequent studies have shown that fullerenes represent a family of related structures containing 20, 40, 60, 70, or 84 carbons. C-60, however, is the most abundant member of this family. Fullerenes are entirely insoluble in water, but suitable functionalization makes the molecules soluble. Initial studies on water-soluble fullerene derivatives led to the discovery of the interaction of organic fullerenes with DNA, proteins, and living cells. Subsequent studies have revealed interesting biological activity aspects of organic fullerenes owing to their photochemistry, radical quenching, and hydrophobicity to form one- to three-dimensional supramolecular complexes. In these areas of research, synthetic organic chemistry has played an important role in the creation of tailor-made molecules.

Upon contact with water, under a variety of conditions, C60 spontaneously forms a stable aggregate with nanoscale dimensions (25–500 nm), termed nano-C60 that are both soluble and toxic to bacteria. This finding challenges conventional wisdom because buckyballs are notoriously insoluble by themselves and most scientists had assumed they would remain insoluble in nature. C60 can be applied to cultured cells without using water-solubilization techniques. Treatment of cells with up to 200 mg/ ml (200 ppm) of C60 does not alter morphology, cytoskeletal organization, and cell cycle dynamics nor does it inhibit cell proliferation. Thus, pristine C60 is non-toxic to the cells, and suggests that fullerene-based nanocarriers may be used for biomedical applications. Fullerenes have important applications in treatment of various diseases such as cancer and as an antioxidant neuroprotective for neurodegenerative disorders in addition to use as contrast agent for brain imaging.

Graphene

Graphene is a monolayer atomic-scale honeycomb lattice of carbon atoms. Its surface area is greater than for carbon nanotubes (CNTs), from ≈ 100 to 1000 m²/g and is the same as activated carbon. 2D crystals provide optoelectronic and photocatalytic properties complementing those of graphene opening several commercial applications (Bonaccorso et al. 2015). Several processes are available for manufacture of graphene quantum dots (QDs). Graphene fibers can be fabricated from chemical vapor deposition grown graphene films. Graphene provides a promising biocompatible scaffold that does not hamper the proliferation of human mesenchymal stem cells and accelerates their specific differentiation into bone cells (Nayak et al. 2011). Honeycomb of hexagonally arranged carbon was termed 3D graphene. Box-shaped graphene nanostructure appear after mechanical cleavage of pyrolytic graphite and is a multilayer system of parallel hollow nanochannels located along the surface and having quadrangular cross-section. The thickness of the channel walls is ~1 nm making nanochannels useful for DNA sequencing. Graphene can be used to create sensitive biosensors. Applications in neurosciences are described in Chap. 9.

Magnetic Nanoparticles

Magnetic nanoparticles (MNPs) are a class of nanoparticle which can be manipulated using magnetic field. The physical and chemical properties of magnetic nanoparticles largely depend on the synthesis method and chemical structure. In most cases, the particles range from 1 to 100 nm in size and may display para- or superparamagnetism. Ferrite nanoparticles are the most used magnetic nanoparticles up to date. Once the ferrite particles reach <128 nm size they become superparamagnetic, which prevents self aggregation because they exhibit their magnetic behavior only when an external magnetic field is applied.

Paramagnetic particles are important tools for cell sorting, protein separation, and single molecule measurements. The particles used in these applications must meet the following requirements: uniform in size, highly paramagnetic, stable in physiological salt buffer, functionizable, and 100–1000 nm in size. They have been used for the detection of model pathogens. Paramagnetic nanoparticles, which are linked to antibodies enable highly specific biological cell separations.

Superparamagnetic iron oxide nanoparticles (SPION) with appropriate surface chemistry have been widely used experimentally for numerous in vivo applications such as magnetic resonance imaging (MRI) contrast enhancement, tissue repair, immunoassay, detoxification of biological fluids, hyperthermia, drug delivery and in cell separation, etc. These applications require that these nanoparticles have high magnetization values and size smaller than 100 nm with overall narrow particle size distribution, so that the particles have uniform physical and chemical properties. In addition, these applications need special surface coating of the magnetic particles, which should be not only nontoxic and biocompatible but also allow a targetable delivery with particle localization in a specific area. Nature of surface coatings of the nanoparticles determines not only the overall size of the colloid but also plays a significant role in biokinetics and biodistribution of nanoparticles in the body. Magnetic nanoparticles can bind to drugs, proteins, enzymes, antibodies, or nucleotides and can be directed to an organ, tissue, or tumor using an external magnetic field or can be heated in alternating magnetic fields for use in hyperthermia. Magnetic labeling of cells provides the ability to monitor their temporal spatial migration in vivo by MRI. Various methods have been used to magnetically label cells using SPIONs. Magnetic tagging of stem cells and other mammalian cells has the potential for guiding future cell-based therapies in humans and for the evaluation of cell-based treatment effects in disease models.

Nanoparticles Assembly into Micelles

Assembly of gold and silver nanoparticle building blocks into larger structures is based on a l method that goes back to one of nature's oldest known chemical innovations, i.e. the self-assembly of lipid membranes that surround every living cell. The method makes use of the hydrophobic effect, a biochemical phenomenon that all living creatures use to create membranes, ultra-thin barriers of fatty acids that form a strong, yet dynamic, sack around the cell, sealing it from the outside world. Cell membranes are one example of a micelle, a strong bilayer covering that is made of two sheets of lipid-based amphiphiles, molecules that have a hydrophilic, end and a hydrophobic end. Like two pieces of cellophane tape being brought together, the hydrophobic sides of the amphiphilic sheets stick to one another, forming the bilayered micelle. All micelles form in three shapes: spheres, cylinders and sack-like vesicles. By varying the length of the polystyrene arm, the solvents used and the size of the gold particles, it is possible to form spheres, vesicles and vary the diameter of their cylinders, some of which grew to well >1000 nm in length. This method may enable creation of a wide variety of useful materials, including potent cancer drugs and more efficient catalysts for the chemical industry.

Nanoshells

Nanoshells are ball-shaped structures measuring ~100 nm and consist of a core of non-conducting glass that is covered by a metallic shell, which is typically gold or silver. Nanoshells possess highly favorable optical and chemical properties for biomedical imaging and therapeutic applications. These particles are also effective substrates for surface-enhanced Raman scattering (SERS) and are easily conjugated to antibodies and other biomolecules. By varying the relative the dimensions of the core and the shell, the optical resonance of these nanoparticles can be precisely and systematically varied over a broad region ranging from the near-UV to the mid-infrared. This range includes the NIR wavelength region where tissue transmissibility peaks, which forms the basis of absorbing nanoshells in NIR thermal therapy of tumors. In addition to spectral tunability, nanoshells offer other advantages over conventional organic dyes including improved optical properties and reduced susceptibility to chemical/thermal denaturation. Furthermore, the same conjugation protocols used to bind biomolecules to gold colloid are easily modified for nanoshells. The core/shell ratio and overall size of a gold nanoshell influences its scattering and absorption properties.

Gold Nanoshells (Spectra Biosciences) possess physical properties similar to gold colloid, in particular a strong optical absorption due to the collective electronic response of the metal to light. The optical absorption of gold colloid yields a brilliant red color, which is very useful in consumer-related medical products such as home pregnancy tests. In contrast, the optical response of Gold Nanoshells depends dramatically on the relative sizes of the nanoparticle core and the thickness of the gold shell. Gold Nanoshells can be made either to absorb or scatter light preferentially by varying the size of the particle relative to the wavelength of the light at their optical resonance. Several potential biomedical applications of nanoshells are under development, including immunoassays, modulated drug delivery, photothermal cancer therapy, and imaging contrast agents.

Plant-Derived Nanoparticles

Naturally occuring nanoparticles in plant cells contain miRNAs, bioactive lipids and proteins, which act as extracellular messengers for cell to cell communication in the same way as exosomes in mammalian cells (Zhang et al. 2016). Plant-derived lipid edible nanoparticles may also be used for efficient drug delivery. Compared to synthetic nanoparticles, plant-derived nanoparticles are easier to scale up for mass production.

Polymer Nanoparticles

Polymer nanoparticles or nanopolymers are single polymer molecule in the nanoscale range. The natural polymer backbone contains oxygen and/or nitrogen. Synthetic polymer backbone can be a composition of carbon, oxygen and/or nitrogen atoms, depending on the chemical nature of monomers employed for polymer synthesis. Synthetic as well as biopolymers are mostly biocompatible, biodegradable and nontoxic. Nanopolymers can be linear or branched. Linear nanopolymers such as polymalic acid carry functional groups distributed over the entire length of the polymer; branched polymers such as dendrimers usually carry them on surface of the molecule. In micelles or other nanoparticles, aggregation restricts accessibility and thus functionality of internally located groups.

Different types of polymer nanoparticles have been designed as drug delivery devices. Biodegradable polymeric nanoparticles are promising drug delivery devices because of their ability to deliver drugs, proteins, peptides and genes as targeting therapeutics to specific organs/tissues. Although several synthetic polymers are available, natural polymers are still popular for drug delivery; these include acacia gum, chitosan, gelatin and albumin. Examples of synthetic biodegradable polymers for controlled release drug delivery are polylactides (PLA), polyglycolides (PLG) and poly(lactide-co-glycolides) or PLGA.

Porous Silicon Nanoparticles

Porous silicon (Psi) is crystalline silicon traversed by nanometer-width pores, providing the material a high surface-to-volume ratio. Production of PSi is based on a top-down approach where the fabrication of size-controlled nanoparticles is usually achieved by mechanical size reduction using ultrasonication or milling nanoparticles Silicon nanoparticles (PSi NPs) vary in size from 25 nm to 1000 nm. (PSi) nanoparticles have unique physicochemical properties making them desirable candidates for drug delivery and other biomedical applications (Santos et al. 2014).

Quantum Dots

Ouantum dots (ODs) are nanoscale crystals of semiconductor material that glow, or fluoresce when excited by a light source such as a laser. OD nanocrystals of cadmium selenide 200–10,000 atoms wide, coated with zinc sulfide. The size of the OD determines the frequency of light emitted when irradiated with low energy light. The ODs were initially found to be unstable and difficult to use in solution. Multicolor optical coding for biological assays has been achieved by embedding different-sized QDs into polymeric microbeads at precisely controlled ratios. Their novel optical properties such as size-tunable emission and simultaneous excitation render these highly luminescent QDs ideal fluorophores for wavelength-andintensity multiplexing. The use of ten intensity levels and six colors could theoretically code one million nucleic acid or protein sequences. Imaging and spectroscopic measurements indicate that the QD-tagged beads are highly uniform and reproducible, vielding bead identification accuracies as high as 99.99% under favorable conditions. DNA hybridization studies demonstrate that the coding and target signals can be simultaneously read at the single-bead level. This spectral coding technology is expected to open new opportunities in gene expression studies, high-throughput screening, and medical diagnostics.

Latex beads filled with several colors of nanoscale semiconductor QDs can serve as unique labels for any number of different probes. When exposed to light, the beads identify themselves and their linked probes by emitting light in a distinct spectrum of colors – a sort of spectral bar code. The shape and size of QDs can be tailored to fluoresce with a specific color. Current dyes used for lighting up protein and DNA fade quickly, but QDs could allow tracking of biological reactions in living cells for days or longer.

QDs can also be placed in a strong magnetic field, which gives an electron on the dot two allowed energy states separated by an energy gap that depends on the strength of the field. The electron can jump the gap by absorbing a photon of precisely that energy, which can be tuned, by altering the field, to correspond with the energy of a far-infrared photon. Once it is excited by absorption of a photon, the electron can leap onto the terminal of a single-electron transistor, where it 'throws the switch' and is detected.

Due to their sheer brightness and high photostability, QDs can act as molecular beacons. When attached to compounds or proteins of interest, QDs enable researchers to track movements within biological media or whole organisms, significantly impacting the way medical professionals study, diagnose and treat diseases. Applications of QDs include the following:

- Life sciences research: tracking proteins in living cells
- · Fluorescence detection: microscopy, biosensors, multi-color flow cytometry
- Molecular diagnostics
- Ex vivo live cell imaging
- In vivo targeting of cells, tissues and tumors with monitoring by PET and MRI
- High throughput screening
- Identification of lymph nodes in live animals by NIR emission during surgery

The new generations of QDs have far-reaching potential for the study of intracellular processes at the single-molecule level, high-resolution cellular imaging, long-term in vivo observation of cell trafficking, tumor targeting, and diagnostics. Best known commercial preparation is QdotTM (Life Technologies).

Synthetic High Density Lipoprotein Nanoparticles

High density lipoprotein nanoparticles (HDL-NPs) are synthesized using a gold nanoparticle template to control conjugate size and ensure a spherical shape (Yang et al. 2013). Like natural HDLs, biomimetic HDL-NPs target scavenger receptor type B-1, a high-affinity HDL receptor expressed by lymphoma cells. Functionally, compared with natural HDL, the gold NP template enables differential manipulation of cellular cholesterol flux in lymphoma cells, promoting cellular cholesterol efflux and limiting cholesterol delivery. This combination of scavenger receptor type B-1 binding and relative cholesterol starvation selectively induces apoptosis. HDL-NPs are biofunctional therapeutic agents, whose mechanism of action is enabled by the presence of a synthetic nanotemplate. HDL-NP treatment of mice bearing B-cell lymphoma xenografts selectively inhibits B-cell lymphoma growth. HDL-NPs have potential applications for other malignancies or diseases of pathologic cholesterol accumulation.

Hybrid Nanoparticles

Hybrid nanoparticles (HNPs) containing two elements have been designed to improve functions of NPs. An example is gold coating of iron oxide nanoparticles (IONPs), which results in particles of increased stability and robustness (Hoskins et al. 2012). Combination of unique properties of iron oxide (magnetic) and gold (surface plasmon resonance) result in a multimodal platform for use as a MRI contrast agent and as a nano-heater. IONPs of core diameter 30 nm and gold coat using the seeding method with a poly(ethylenimine) intermediate layer were synthesized. The final particles were coated in PEG to ensure biocompatibility and increase retention times in vivo. The resulting HNPs possessed a maximal absorbance at 600 nm, and appeared to decrease T2 values in line with clinically used MRI contrast agent Feridex®. HNPs could serve dual functions as MRI contrast agents as well as nano-heaters for therapies such as cellular hyperthermia or thermoresponsive drug delivery.

Bacterial Structures Relevant to Nanobiotechnology

Nanostructures Based on Bacterial Cell Surface Layers

Among the most commonly observed bacterial cell surface structures are monomolecular crystalline arrays of proteinaceous sub units termed S-layers, which are the simplest type of biological membrane developed during evolution. As an important

As a matrix for controlled immobilization of functional molecules
Binding of enzymes for bioanalytical biosensors
Immobilizing monoclonal antibodies for dipstick style immunoassays
Immobilizing antibodies for preparation of microparticles for ELISA
S-layers as carriers for conjugated vaccines
S-layer coated liposomes
Immobilization of functional molecules on S-layer coated liposomes
Entrapping of functional molecules for drug delivery
S-layer coated liposomes with immobilized antigens and haptens for vaccines
Vehicles for producing fusion proteins
Vaccines
Biosensors
Diagnostics
Ching Discourse Discourse

Table 2.2 Applications of S-layers in nanobiotechnology

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component of the bacterial cell envelope, S-layers can fulfill various biological functions and are usually the most abundantly expressed protein species in a cell. S-layer plays an important part in interactions of microbial cell with the environment. S-layers are generally 5–10 mm thick and pores in the protein lattices are of identical size and morphology in the 2–8 nm range. S-layers have applications in nanobiotechnology as shown in Table 2.2.

Bacterial Magnetic Particles

Magnetic bacteria synthesize intracellular magnetosomes that impart a cellular swimming behavior referred to as magnetotaxis. The magnetic structures, magnetosomes, aligned in chains are postulated to function as biological compass needles allowing the bacterium to migrate along redox gradients through the Earth's geomagnetic field lines. Despite the discovery of this unique group of microorganisms several years ago, the mechanisms of magnetic crystal biomineralization have yet to be fully elucidated. A lipid bilayer membrane of approximately 2–4 nm in thickness encapsulates individual magnetosomes (50–100 nm in diameter). Magnetosomes are also referred to as bacterial magnetic particles (BMPs) to distinguish them from artificial magnetic particles (AMPs). The aggregation of BMPs can be easily dispersed in aqueous solutions compared with AMPs because of the enclosing organic membrane.

BMPs have potential applications in the interdisciplinary fields of nanobiotechnology, medicine and environmental management. Through genetic engineering, functional proteins such as enzymes, antibodies, and receptors have been successfully displayed on BMPs, which have been utilized in various biosensors and bio-separation processes. The use of BMPs in immunoassays enables the separation of bound and free analytes by applying a magnetic field. Proteins can be attached covalently to solid supports such as BMPs that prevents desorption of antibodies during an assay. Large scale production of functionally active antibodies or enzymes expressed on BMP membranes can be accomplished.

Carbon Nanotubes

Carbon nanotubes are rolled-up sheets of carbon atoms that appear naturally in soot, and are central to many nanotechnology projects. These nanotubes can go down in diameter to 1 nm, are stronger than any material in the universe and can be any length. These can be used as probes for AFMs that can image individual molecules in both wet and dry environments. This has enormous opportunities for application as conventional structure-based pharmaceutical design is hampered by the lack of high-resolution structural information for most protein-coupled receptors. It is possible to insert DNA into a carbon nanotube. Devices based on the DNA-nanotube combination could eventually be used to make electronics, molecular sensors, devices that sequence DNA electronically, and even gene delivery systems.

Medical Applications of Nanotubes

- Cyclic peptide nanotubes can act as a new type of antibiotic against bacterial pathogens.
- Cyclic peptide nanotubes can be used as artificial ion channels than open and close in response to electrical and chemical stimuli.
- It is easy to chemically functionalize the surfaces of template-synthesized nanotubes, and different functional groups can be attached to the inner versus outer surfaces of the tubes.
- Biomolecules, such as enzymes, antibodies, and DNA chains, can be attached to the nanotube surfaces to make biofunctionalized nanotubes.
- Template-synthesized nanotubes can be used as smart nanophase extraction agents, e.g. to remove drug molecules from solution.
- Template-synthesized nanotube membranes offer new approaches for doing bioseparations, e.g. of drug molecules.
- Nanoscale electromechanical systems (nanotweezers) based on carbon nanotubes have been developed for manipulation and interrogation of nanostructures within a cell.
- · Carbon nanotubes can be used as tips for AFM
- Lumen of a nanotube can carry payloads of drugs
- Nanotubes can be used in biosensors
- Blood-compatible CNTs, with heparin immobilized on the surface, are building blocks for in vivo nanodevices. Activated partial thromboplastin time and thromboelastography studies prove that heparinization can significantly enhance the blood compatibility of nanomaterials.

Studies of electrophoretic transport of ssRNA molecules through 1.5-nm-wide pores of carbon nanotube membranes reveal that RNA entry into the nanotube pores is controlled by conformational dynamics, and exit by hydrophobic attachment of RNA bases to the pores. Differences in RNA conformational flexibility and hydrophobicity result in sequence-dependent rates of translocation, which is a prerequisite for nanoscale separation devices.

The uptake of single-walled carbon nanotubes (SWCNTs) into cells appears to occur through phagocytosis. There are no adverse effects on the cells and the nanotubes retained their unique optical properties suggesting that SWCNTs might be valuable biological imaging agents, in part because SWCNTs fluoresce in the NIR portion of the spectrum, at wavelengths not normally emitted by biological tissues. This may allow light from even a handful of nanotubes to be selectively detected in vivo. Although long term studies on toxicity and biodistribution must be completed before nanotubes can be used in medical tests, but nanotubes are useful as imaging markers in laboratory in vitro studies, particularly in cases where the bleaching, toxicity and degradation of more traditional markers are problematic.

Dendrimers

Dendrimers (dendri – tree, mer – branch) are a novel class of 3D, core-shell nanostructures/nanoparticles with 'onion skin-like' branched layers. Dendrimers can be precisely synthesized for a wide range of applications and specialized chemistry techniques enable precise control over their physical as well as chemical properties. They are constructed generation by generation in a series of controlled steps that increase the number of small branching molecules around a central core molecule. Up to 10 generations can be incorporated into a single dendrimer molecule. The final generation of molecules added to the growing structure makes up the polyvalent surface of the dendrimer (see Fig. 2.1). The core, branching and surface molecules are chosen to give desired properties and functions. The outer generation of each dendrimer has a precise number of functional groups that may act as a monodispersed platform for engineering favorable nanoparticle-drug and nanoparticle-tissue interactions. These features have attracted significant attention in medicine as nanocarriers for traditional small drugs, proteins, DNA/RNA and in some instances as intrinsically active nanoscale drugs.

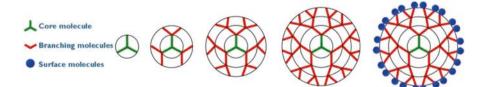


Fig. 2.1 The core, branching and surface molecules of dendrimers (Source: Starpharma Holding Ltd, by permission)

Because of their unique architecture and construction, dendrimers possess inherently valuable physical, chemical and biological properties. These include:

- Precise architecture, size and shape control. Dendrimers branch out in a highly predictable fashion to form amplified 3D structures with highly ordered architectures.
- High uniformity and purity. The proprietary step-wise synthetic process used produces dendrimers with highly uniform sizes (monodispersity) possessing precisely defined surface functionality and very low impurity levels.
- High loading capacity. Internal cavities intrinsic to dendrimer structures can be used to carry and store a wide range of metals, organic, or inorganic molecules.
- High shear resistance. Through their 3D structure dendrimers have a high resistance to shear forces and solution conditions.
- Low toxicity. Most dendrimer systems display very low cytotoxicity levels.
- Low immunogenicity when injected or used topically.

Properties

The surface properties of dendrimers may be manipulated by appropriate 'capping' reagents on the outermost generation. In this way, dendrimers can be readily decorated to yield a novel range of functional properties. These include:

- Polyvalency The outer shell of each dendrimer can be manipulated to contain numerous reactive groups. Each of these reactive sites has the potential to interact with a target entity, often resulting in polyvalent interactions.
- Flexible charge and solubility properties Through use of appropriate capping groups on the dendrimer exterior, the charge and solubility of dendrimers can be readily manipulated.
- Flexible binding properties By using appropriate capping groups on the dendrimer exterior, dendrimers can be designed to exhibit strong affinity for specific targets.
- Transfection Dendrimers can move through cell boundaries and transport genetic materials into cell interiors.

Applications

Dendrimers, with their highly customizable properties, are basic building blocks with the promise of enabling specific nanostructures to be built to meet existing needs and solve evolving problems. Dendrimer research and development is currently making an impact on a broad range of fields as shown by exponential growth in the number of dendrimer-based publications. Dendrimer-based drugs, as well as diagnostic and imaging agents, are emerging as promising candidates for many nanomedicine applications. While the potential applications of dendrimers are unlimited, some of their current uses relevant to nanomedicine are shown in Table 2.3.

Diagnostics
Sensors
Imaging contrast agents
Drug delivery
Improved delivery of existing drugs
Improved solubility of existing drugs
Drug development
Polyvalent dendrimers interacting simultaneously with multiple drug targets
Development of new pharmaceuticals with novel activities
Improving pharmacological activity of existing drugs
Improving bioavailability of existing drugs
Therapeutics
Antimicrobial agents
Chemotherapy
Prevention of scar tissue formation after surgery
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Table 2.3 Potential applications of dendrimers in nanomedicine

Advances in understanding of the role of molecular weight and architecture on the in vivo behavior of dendrimers, together with recent progress in the design of biodegradable chemistries, has enabled the application of dendrimers as antiviral drugs, tissue repair scaffolds, targeted carriers of chemotherapeutics and optical oxygen sensors. Examples of pharmaceutical products based on dendrimers are:

- VivaGel SPL7013 (Starpharma Pty Ltd), dendrimer-based topical treatment of bacterial vaginosis is in phase III clinical trials (NCT01577537).
- DEPTM-Docetaxel (DTX-SPL8783, Starpharma/AstraZeneca), a dendrimerbased conjugate, is in a phase I clinical trial for advanced or metastatic cancer.

A potential application of dendrimer-based complexes is for in vivo real-time imaging, and combination of diagnosis with treatment leading to personalized treatment of various diseases. Before such products can reach the market, however, the field must not only address the cost of manufacture and quality control of pharmaceutical-grade materials, but also assess the long-term human and environmental health consequences of dendrimer exposure in vivo.

DNA Nanostructures

DNA is a material that can be readily used for the programmed self-assembly of wireframe, 2D or 3D nanostructures due to the predictability of base pairing. DNA can self-assemble into nanoscale shapes and small bioactive molecules such as dyes, nanoparticles or proteins can be attached with site-specificity to DNA nanostructures

through ligands, antibodies, aptamers or recombinant genetic techniques. Advantages of DNA nanostructure are (Smith et al. 2013):

- · Biocompatibility
- Increased stability against degradation in a variety of biological media compared with ssDNA or dsDNA.
- Further protection against the body's immune response can be provided by the addition of encapsulating PEG or lipid shells.
- Nanoscale structures and frames from DNA show a lack of toxicity to cells and initiate a generally low immune response.

Targeted delivery of molecular therapeutics can be achieved by carriers that have been successfully constructed from DNA material, which can selectively deliver material such as siRNA, the anticancer drugs or signaling molecules to target cells in vivo. DNA-based structures are suitable carriers for immunostimulating nucleotide sequences, which can act as adjuvants for inducing long-term immunity in vaccination. Besides therapeutic applications, DNA nanostructures can be used in diagnostics. Nanopores constructed by the DNA origami method can be used for the detection and sequence-specific recognition of DNA molecules.

Potential Applications of DNA Octahedron

DNA octahedron is a single strand of DNA that spontaneously folds into a highly rigid, nanoscale octahedron that is several million times smaller than the length of a standard ruler and about the size of several other common biological structures, such as a small virus or a cellular ribosome. The octahedron consists of 12 edges, six vertices, and eight triangular faces. The structure is about 22 nm in diameter. Making the octahedron from a single strand was a breakthrough. Because of this, the structure can be amplified with the standard tools of molecular biology and can easily be cloned, replicated, amplified, evolved, and adapted for various applications. This process also has the potential to be scaled up so that large amounts of uniform DNA nanomaterials can be produced. These octahedra are potential building blocks for new tools for basic biomedical science. With these we have biological control, and not just synthetic chemical control, over the production of rigid, wire frame DNA objects.

Because all 12 edges of the octahedral structures have unique sequences, they are versatile molecular building blocks that could potentially be used to self-assemble complex higher-order structures. Possible applications include using these octahedra as artificial compartments into which proteins or other molecules could be inserted, something like a virus in reverse – DNA is on the outside and proteins on the inside. In nature, viruses are self-assembling nanostructures that typically have proteins on the outside and DNA or RNA on the inside. The DNA octahedra could possibly form scaffolds that host proteins for the purposes of x-ray crystallography, which depends on growing well-ordered crystals, composed of arrays of molecules.

Nanowires

The manipulation of photons in structures smaller than the wavelength of light is central to the development of nanoscale integrated photonic systems for computing, communications, and sensing. Assembly of small groups of freestanding, chemically synthesized nanoribbons and nanowires into model structures illustrates how light is exchanged between subwavelength cavities made of three different semiconductors. With simple coupling schemes, lasing nanowires can launch coherent pulses of light through ribbon waveguides that are up to a millimeter in length. Also, interwire coupling losses are low enough to allow light to propagate across several right-angle bends in a grid of crossed ribbons. Nanoribbons function efficiently as waveguides in liquid media and provide a unique means for probing molecules in solution or in proximity to the waveguide surface. These results lay the groundwork for photonic devices based on assemblies of active and passive nanowire elements. There are potential applications of nanowire waveguides in microfluidics and biology. Some nanowire-based nanobiosensors are in development.

Nanopores

Nanopores are tiny structures that occur in the cell in nature for specific functions. At the molecular level, specific shapes are created that enable specific chemical tasks to be completed. For examples, some toxic proteins such as alpha hemolysin can embed themselves into cell membranes and induce lethal permeability changes there due to its central pore. The translocation of polymers across nanometer scale apertures in cell membranes is a common phenomenon in biological systems. The first proposed application was DNA sequencing by measuring the size of nanopore, application of an electric potential across the membrane and waiting for DNA to migrate through the pore to enable one to measure the difference between bases in the sequence (see Chap. 3). Protein engineering has been applied to ion channels and pores and protein as well as non-protein can be constructed. Potential applications of engineered nanopores are:

- Tools in basic cell biology
- · Molecular diagnostics: sequencing
- Drug delivery
- · Cryoprotection and desiccation of cells
- · Components of nanodevices and nanomachines
- Nanomedicine

Nanoporous Silica Aerogel

Nanoporous silica aerogels have been used in nanotechnology devices such as aerogel nanoporous insulation blankets. Silica aerogel substrate enables stable formation of lipid bilayers that are expected to mimic real cell membranes. Typical bilayers are 5 nm in thickness and the silica beads in aerogel are approximately 10–25 nm in diameter. Silica aerogels have a unique structure and chemistry that allow for the transformation of nano-sized liposomes into continuous, surface-spanning lipid bilayers. These lipid bilayers adsorb to the aerogel surface and exhibit the characteristic lateral mobility of real cell membranes. The high (98%) porosity of aerogel substrates creates an underlying "water-well" embedded in the aerogel pore structure that allows these membrane molecules to carry out normal biological activities including transport across the membrane. This porosity could potentially accommodate the movement of membrane proteins or other membrane-extruding molecules.

This aerogel is an improvement over conventional substrates for synthetic biomembranes as it is porous, thus minimizing non-physiological interaction between membrane proteins and a hard substrate surface. This prevents the proteins from becoming immobilized, denatured and eventually losing their biological functions. Applications of lipid bilayers are:

- Model biological membranes for research
- Biosensors and lab-on-chip devices (microfluidic systems, analyte detector, etc.)
- Bio-actuating devices
- Arrays for use in screening arrays of compounds for membrane-associated drug targets. Lipid bilayer system has been used in immunological screening for drug targets.
- Display libraries of compounds
- Patterned lipid bilayers can be used for tissue culture and engineering (micro-patterns of lipid membranes direct discriminative attachment or growth of living cells)

Advantages of aerogel biomembrane are:

- · Best able to mimic the lateral mobility of molecules in real cell membranes
- Enable membrane transport studies due to liquid permeability of aerogels
- Both sides of supported membranes are accessible compared to only one side in conventional solid support
- Can be used to design functional membranes for different applications by incorporating organic, inorganic, polymeric and/or biologically active components into the aerogel structures
- Non-physiological interaction of the membrane-associated components with the underlying support (compared to glass)
- · Membranes on the aerogel maintain stability for weeks

Nanostructured Silicon

Silicon has been used for implants in the human body for several years. Following nanostructuring, silicon can be rendered biocompatible and biodegradable. BioSiliconTM (pSiMedica Ltd) contains nano-sized pores measuring 100 nm. The "silicon skeleton" between the pores comprises tens of silicon atoms in width. Initial applications are in drug delivery. The kinetics of drug release from BioSiliconTM can be controlled by adjusting the physical properties of the matrix, including modifying the pore size. Other potential applications include nanospheres for targeted systemic and pulmonary drug delivery. Nanostructured silicon, as multilayered mirrors, can be used for subcutaneous implants for diagnostics. Nanostructures can be used as prostheses to improve adhesion to bone tissue.

Nanoparticle Conjugates

DNA-Nanoparticle Conjugates

DNA-DNA hybridization has been exploited in the assembly of nanostructures including biosensors, and DNA scaffolds. Many of these applications involve the use of DNA oligonucleotides tethered to gold nanoparticles or nanoparticles may be hybridized with one another. Two types of DNA-nanoparticle conjugates have been developed for these purposes. Both types entail the coupling of oligonucleotides through terminal thiol groups to colloidal gold particles. In one case, the oligonucleotides form the entire monolayer coating the particles, whereas in the other case, the oligonucleotides are incorporated in a phosphine monolayer, and particles containing discrete numbers of oligonucleotides are separated by gel electrophoresis. A minimal length of 50 residues is required, both for separation by electrophoresis and hybridization with complementary DNA sequences. These limitations of shorter oligonucleotides are attributed to interaction between the DNA and the gold. In a new technique, glutathione monolayerprotected gold clusters were reacted with 19- or 20-residue thiolated oligonucleotides and the resulting DNA-nanoparticle conjugates can be separated based on the number of bound oligonucleotides by gel electrophoresis and assembled with one another by DNA-DNA hybridization. This approach overcomes previous limitations of DNAnanoparticle synthesis and yields conjugates that are precisely defined with respect to both gold and nucleic acid content.

Networks of Gold Nanoparticles and Bacteriophage

Biological molecular assemblies are excellent models for the development of nanoengineered systems with desirable biomedical properties. A biologically active molecular network consists of bacteriophage (phage) directly assembled with gold (Au) nanoparticles and termed Au-phage. When the phage is engineered so that each phage particle displays a peptide, such networks preserve the cell surface receptor binding and internalization attributes of the displayed peptide. The spontaneous organization of these targeted networks can be manipulated further by incorporation of imidazole (Au-phage-imid), which induces changes in fractal structure and near-infrared optical properties. The networks can be used as labels for enhanced fluorescence and dark-field microscopy, surface-enhanced Raman scattering detection, and near-infrared photon-to-heat conversion. Together, the physical and biological features within these targeted networks offer convenient multifunctional integration within a single entity with potential for nanotechnology-based biomedical applications such as biological sensors and cell-targeting agents.

Carboxymethyl chitosan capped gold nanoparticles (CMC-AuNPs) are used as plasmonic probes and are synthesized by a simple one pot wet chemical method. The conjugation of carboxymethyl chitosan-linked AuNPs with T7 virions enables simple, selective and sensitive colorimetric biosensing of viruses (Kannan et al. 2014). This method is low cost.

This genetically programmable nanoparticle with a biologically compatible metal acts as a nanoshuttle that can target specific locations in the body. For example, it could potentially locate damaged areas on arteries that have been caused by heart disease, and then deliver stem cells to the site that can build new blood vessels. It may be able to locate specific tumors, which could then be treated by either heating the gold particles with laser light and/or using the nanoparticles to selectively deliver a drug to destroy the cancer.

Protein-Nanoparticle Combination

Proteins come in many handy shapes and sizes, which make them major players in biological systems. Chaperonins are ring-shaped proteins found in all living organisms where they play an essential role in stabilizing proteins and facilitating protein folding. A chaperonin can be adapted for technological applications by coaxing it to combine with individual luminescent semiconductor nanoparticles. In bacteria, this chaperonin protein takes in and re-folds denatured proteins to return them to their original useful shapes. This ability would make the proteins good candidates for drug carriers.

Cadmium sulfite nanoparticles emit light so long as they are isolated from each other; encasing the nanoparticles in the protein keeps the tiny particles apart. The biological fuel molecule ATP releases the nanoparticles from the protein tubes, freeing the particles to clump together, which quenches the light. The protein-nanoparticle combination could be used to detect ATP. This blend of nanotechnology and molecular biology could lead to new bioresponsive electronic nanodevices and biosensors very different from the artificial molecular systems currently available. By adding selective binding sites to the solvent-exposed regions of the chaperonin, the protein-nanoparticle bioconjugate becomes a sensor for specific targets (Xie et al. 2009).

Polymer Nanofibers

Polymer nanofibers, with diameters in the nanometer range, possess larger surface areas per unit mass and permit easier addition of surface functionalities compared with polymer microfibers. Research on polymer nanofibers, nanofiber mats, and their applications has seen a remarkable growth over the last few years. Among various methods of manufacture, electrospinning has been used to convert a large variety of polymers into nanofibers and may be the only process that has the potential for mass production. Although measurement of mechanical properties such as tensile modulus, strength, and elongation is difficult because of the small diameters of the fibers, these properties are crucial for the proper use of nanofiber mats. Owing to their high surface area, functionalized polymer nanofibers will find broad applications as drug delivery carriers, biosensors, and molecular filtration membranes in future.

Virus-Like Particles

Virus-like particles (VLPs), noninfectious viruses without genetic material, have evolved to become an accepted technology and some VLP-based vaccines are currently used as commercial medical products, and other VLP-based products are at different stages of clinical development. VLPs have advantages as gene therapy tools and as nanomaterials. VLPs can be used as nano-scaffolds for enzyme selection as well as patterning, phage therapy, raw material processing, and single molecule enzyme kinetics studies (Cardinale et al. 2012). Analysis of published data shows that at least 110 VLPs have been constructed from viruses belonging to 35 different families (Zeltins 2013). Novavax Inc's VLP technology uses recombinant protein technology to imitate the structure of a virus to provide protection without the risk of infection or disease. Virion proteins can self-assemble into VLPs when over-expressed in certain cells.

Measurement of Nanoparticle Size and Distribution

Number weighted nanoparticle (NP) size distribution in a sample is not only important for basic research but is also required under European Union regulations that apply for researchers and industry alike. A representative number of NPs are typically counted by use of a transmission electron microscope (TEM) in which a beam of electrons probes an ultra-thin specimen and interact with the sample as they pass through leading to a "shadow image" of the specimen. Sample preparation generally requires the complete removal of the suspending liquid leading to aggregation of NPs which makes it difficult both to count them and to determine if the particles were already aggregated beforehand. This renders automatic counting systems useless as well, leaving researchers with the huge task of interpreting images manually.

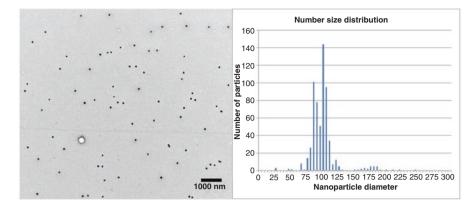


Fig. 2.2 Imaging and size distribution of nanoparticles with TEM (Source: Adolphe Merkle Institute (University of Freiburg, Switzerland), by permission)

To prevent artifacts from sample preparation and simplify interpretation, researchers at the Adolphe Merkle Institute (University of Fribourg, Switzerland) have devised a straightforward protocol for prevention of the onset of drying artifacts, thereby enabling the preservation of in situ colloidal features of NPs during sample preparation for TEM (Michen et al. 2015). This is achieved by adding bovine serum albumin, a macromolecular agent, to the suspension to stabilize nanoparticles and prevent aggregation. Both research- and economically-relevant particles with high polydispersity and/or shape anisotropy are easily characterized following this approach, which allows for rapid and quantitative classification in terms of dimensionality and size as shown in Fig. 2.2.

Scientists at Center for Environmental Nanoscience and Risk (University of South Carolina, USA) have presented a validated quantitative sampling technique for atomic force microscopy (AFM) that overcomes the drawbacks of conventional preparation of NP samples and allows full recovery and representativeness of the NPs under consideration by forcing the NPs into the substrate via ultracentrifugation and strongly attaches the NPs to the substrate by surface functionalization of the substrate or by adding cations to the NP suspension (Baalousha et al. 2014). The high efficiency of the analysis is demonstrated by the uniformity of the NP distribution on the substrate (that is low variability between the number of NPs counted on different images on different areas of the substrate), the high recovery of the NPs up to 71%) and the good correlation between the mass and number concentrations. This validated quantitative sampling technique enables the use of the full capabilities of microscopy tools to quantitatively and accurately determine the number size distribution and number concentration of NPs at environmentally relevant low concentrations (i.e. 0.34-100 ppb). This approach is of high environmental relevance and can be applied widely in environmental nanotoxicology for accurately measuring the number size distribution of NPs.

Nanomaterials for Biolabeling

Nanomaterials are suitable for biolabeling. Nanoparticles usually form the core in nanobiomaterials. However, to interact with biological target, a biological or molecular coating or layer acting as an interface needs to be attached to the nanoparticle. Coatings that make the nanoparticles biocompatible include antibodies, biopolymers or monolayers of small molecules. A nanobiomaterial may be in the form of nanovesicle surrounded by a membrane or a layer. The shape is more often spherical but cylindrical, plate-like and other shapes are possible. The size and size distribution might be important in some cases, for example if penetration through a pore structure of a cellular membrane is required. The size is critical when quantum-sized effects are used to control material properties. A tight control of the average particle size and a narrow distribution of sizes allow creating very efficient fluorescent probes that emit narrow light in a very wide range of wavelengths. This helps with creating biomarkers with many and well distinguished colors. The core itself might have several layers and be multifunctional. For example, combining magnetic and luminescent layers one can both detect and manipulate the particles.

The core particle is often protected by several monolayers of inert material, for example silica. Organic molecules that are adsorbed or chemisorbed on the surface of the particle are also used for this purpose. The same layer might act as a biocompatible material. However, more often an additional layer of linker molecules is required that has reactive groups at both ends. One group is aimed at attaching the linker to the nanoparticle surface and the other is used to bind various biocompatible substances such as antibodies depending on the function required by the application.

Efforts are being made to improve the performance of immunoassays and immunosensors by incorporating different kinds of nanostructures. Most of the studies focus on artificial, particulate marker systems, both organic and inorganic. Inorganic nanoparticle labels based on noble metals, semiconductor QDs and nanoshells appear to be the most versatile systems for these bioanalytical applications of nanophotonics. The underlying detection procedures are more commonly based on optical techniques. These include nanoparticle applications generating signals as diverse as static and time-resolved luminescence, one- and two-photon absorption, Raman and Rayleigh scattering as well as surface plasmon resonance and others. All efforts are aimed at achieving one or more of the following goals:

- Lowering of detection limits (if possible, down to single-molecule level)
- Parallel integration of multiple signals (multiplexing)
- Signal amplification by several orders of magnitude

Potential benefits of using nanoparticles and nanodevices include an expanded range of label multiplexing. Different types of fluorescent nanoparticles and other nanostructures have been promoted as alternatives for the fluorescent organic dyes that are traditionally used in biotechnology. These include QDs, dye-doped polymer and silica nanoparticles (Dosev et al. 2008). Various nanomaterials for biolabeling are shown in Table 2.4.

	Lable 2.4 Nanomaterials for biolabeling	
Label/reporter	Characteristics	Function/applications
Dendrimer /silver nanocompsites	Water-soluble, biocompatible, fluorescent and 3–7 nm diameter stable nanoparticles.	Biomarkers for in vitro cell labeling
Electrogenerated chemiluminescence	Tris(2,2'-bipyridy1)ruthenium(II) molecular labels.	Nanoscale bioassay
Europium(III)-chelate- doped nanoparticles	Combined with selection of high affinity monoclonal antibodies coated on label particles and microtitration wells.	The sensitivity for virus particle detection is improved compared to immunofluorometric assays
Fluorescent color-changing dyes	3-hydroxychromone derivatives that exhibit 2 fluorescence bands resulting from excited-state intramolecular proton transfer reaction.	Biosensors
Fluorescent lanthanide nanorods	Retain their fluorescent properties after internalization into cells.	Multiplexed imaging of molecular targets in living cells
Luminescent core/shell nanohybrid	Luminescent rare earth ions in a nanosized Gd203 core (3.5 nm) and FTTC molecules entrapped within in a polysiloxane shell (2.5–10 nm).	Two different luminescence emissions: (1) FITC under standard illumination; (2) Tb ³⁺ under high-energy source giving highly photostable luminescence
Magnetic nanotags (MNTs)	Alternative to fluorescent labels in biomolecular detection assays	Multiplex protein detection of cancer biomarkers at low concentrations
Nanogold® labels (Nanoprobe Inc)	Unlike nanogold particles, gold labels are uncharged molecules, which are cross-linked to specific sites on biomolecules.	Nanogold@ labels have a range and versatility, which is not available with colloidal nanogold particles.
Nanophosphors	Nanophosphors contains embedded lanthanide ions, like europium or terbium	Nanophosphor signals hardly fade and can also be used for multiplex testing.
Plasmon resonant nanoparticles	Scatter light with tremendous efficiency	Ultrabright nanosized labels for biological applications, replacing other labeling methods such as fluorescence.
QD end-labeling	Multicolor fluorescence microscopy using conjugated QDs	Detection of single DNA molecules.
SERS (Surface-enhanced Raman Scattering)- based nanotags	A metal nanoparticle where each type of tag exploits the Raman spectrum of a different small molecule and SERS bands are 1/50th the width of fluorescent bands.	Enables greater multiplexed analyte quantification than other fluorescence-based quantitation tags.
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 Table 2.4
 Nanomaterials for biolabeling

DNA Nanotags

Bright fluorescent dye molecules can be integrated with DNA nanostructure to make nanosized fluorescent labels – DNA nanotags, which improve the sensitivity for fluorescence-based imaging and medical diagnostics. DNA nanotags are useful for detecting rare cancer cells within tissue biopsies. In addition, they offer the opportunity to perform multicolor experiments. This feature is extremely useful for imaging applications because the multiple colors can be seen simultaneously, requiring only one experiment using one laser and one fluorescence-imaging machine. Fluorescent DNA nanotags have been used in a rolling circle amplification immunoassay based as a versatile fluorescence assay platform for highly sensitive proteins detection (Xue et al. 2012).

Fluorescent Lanthanide Nanorods

Inorganic fluorescent lanthanide (europium and terbium) orthophosphate nanorods can be used as a novel fluorescent label in cell biology. These nanorods, synthesized by the microwave technique, retain their fluorescent properties after internalization into human umbilical vein endothelial cells or renal carcinoma cells. The cellular internalization of these nanorods and their fluorescence properties have been characterized by fluorescence spectroscopy, differential interference contrast microscopy, confocal microscopy, and transmission electron microscopy. Nanorods are nontoxic up to concentrations of 50 ug/ml. Nanorods can be used for the detection of cancer at an early stage and functionalized nanorods are potential vehicles for drug delivery.

Magnetic Nanotags

Magnetic nanotags (MNTs) are a promising alternative to fluorescent labels in biomolecular detection assays, because minute quantities of MNTs can be detected with inexpensive sensors. Probe sensors are functionalized with capture antibodies specific to the chosen analyte. During analyte incubation, the probe sensors capture a fraction of the analyte molecules. A biotinylated linker antibody is subsequently incubated and binds to the captured analyte, providing binding sites for the streptavidin-coated MNTs, which are incubated further. The nanotag binding signal, which saturates at an analyte concentration-dependent level, is used to quantify the analyte concentration. However, translation of this technique into easy-to-use and multilplexed protein assays, which are highly sought after in molecular diagnostics such as cancer diagnosis and personalized medicine, has been challenging. Multiplex protein detection of potential cancer biomarkers has been demonstrated at subpicomolar concentration levels (Osterfeld et al. 2008). With the addition of nanotag amplification, the analytic sensitivity extends into the low femtomolar concentration range. The multianalyte ability, sensitivity, scalability, and ease of use of the MNT-based protein assay technology make it a strong contender for versatile and portable molecular diagnostics in both research and clinical settings. A hand-held, portable biosensor platform for quantitative biomarker measurement combines MNP tags with giant magnetoresistive spin-valve sensors, to achieve highly sensitive (picomolar) and specific biomarker detection in >20 min (Hall et al. 2010). This platform can detect multiple biomarkers simultaneously in a single assay at point-of-care (POC) to provide a low-cost diagnostic tool for multiple applications.

Molecular Computational Identification

Molecular computational identification, based on molecular logic and computation, has been applied on nanoscale. Examples of populations that need encoding in the microscopic world are cells in diagnostics or beads in combinatorial chemistry. Taking advantage of the small size (about 1 nm) and large 'on/off' output ratios of molecular logic gates and using the great variety of logic types, input chemical combinations, switching thresholds and even gate arrays in addition to colors, unique identifiers have been produced for small polymer beads (about 100 μ m) used for synthesis of combinatorial libraries. Many millions of distinguishable tags become available. This method should be extensible to far smaller objects, with the only requirement being a 'wash and watch' protocol. The basis of this approach is converting molecular science into technology concerning analog sensors and digital logic devices. The integration of molecular logic gates into small arrays has been a growth area in recent years (de Silva 2011).

Nanophosphor Labels

Nanostructures based on inorganic phosphors (nanophosphors) are a new emerging class of materials with unique properties that make them very attractive for labeling. The molecular lattice of phosphors contains individual embedded lanthanide ions, like europium or terbium. The crystal lattice or sometimes "activator ions" such as cerium ions used especially for this purpose – absorbs the stimulating light and transfers the energy to the lanthanide ions, which are the true source of fluorescence. The color emitted depends mainly on the lanthanide ions used. Terbium, for example, gives off a yellowish green color, while europium produces a red fluorescence. As shown by the "microparticles" in fluorescent lights, the cycle of stimulation and emission can be endlessly repeated, which means that the dye never fades.

Bayer scientists are developing nanophosphors, which many of the advantages of QDs and fewer disadvantages such as high cost and heavy metals content that may not be environmentally friendly. Nanophosphor signals hardly fade and can also be

used for multiplex testing. And the major advantage they have over QDs is that the wavelength of their emitted light does not depend on particle size but on the type of lanthanide ions used. For this reason, their particle size, which is also no more than 10 nm, does not need to be monitored so precisely. Because of this, the manufacturing process is simpler and less expensive. Moreover, most ions of lanthanides, also called rare earths, are considered less harmful to the environment, and this facilitates their manufacture and disposal.

Background fluorescence from biological components of cells, makes it difficult to interpret the signal, e.g. the positive result of a diagnostic test for cancer. Nanophosphors can get around this problem because for many types of nanophosphor, the life span of the fluorescence i.e. the time between stimulation and emission extends to several milliseconds. Accordingly, when the nanophosphor is exposed to a brief impulse of light, the background fluorescence disappears before the test result is displayed. This considerably enhances the sensitivity of the fluorescent marker in its various applications. Another important advantage of the nanophosphor system, particularly where medical diagnostics are concerned, is its ability to transfer fluorescent energy to a closely related dye. This allows biochemical reactions, like the coupling between antibodies, to be detected without the need for any additional procedures. Therefore, the relevant antibodies in the patient's sample can be detected immediately after the dye has been added to the test solution.

Before the nanophosphors can be used to track down certain segments of DNA, for example in cancer tests, they themselves need to be attached to suitable DNA segments. It is always a major challenge to achieve stable coupling of small organic molecules or larger biomolecules with unique, inorganic nanoparticles. The particles must be painstakingly adapted to the properties of the organic molecules and prevented from lumping together themselves in the process. If this can be done successfully, it will meet the demanding challenges of medical diagnostics in the future.

Photoluminescence imaging in vitro and in vivo has been shown by use of near infrared to near infrared (NIR-to-NIR) up-conversion in nanophosphors. This NIRto-NIR up-conversion process provides deeper light penetration into biological specimen and results in high contrast optical imaging due to absence of an autofluorescence background and decreased light scattering. Fluoride nanocrystals (20-30 nm size) co-doped with Tm³⁺ and Yb³⁺, have been synthesized and characterized by TEM, XRD, and photoluminescence spectroscopy (Nyk et al. 2009). In vitro cellular uptake was demonstrated with no apparent cytotoxicity. Subsequent animal imaging studies were performed using Balb-c mice injected intravenously with up-converting nanophosphors, demonstrating the high contrast PL imaging in vivo by photoluminescence spectroscopy. Lanthanide doped nanocrystals, have also been used for imaging of cells and some deep tissues in animals. Polyethyleneimine (PEI) coated NaYF4:Yb,Er nanoparticles produce very strong upconversion fluorescence when excited at 980 nm by a NIR laser, which is resistant to photo-bleaching, and non-toxic to bone marrow stem cells (Chatterjee et al. 2008). The nanoparticles delivered into some cell lines or injected intradermally and intramuscularly into some tissues either near the body surface or deep in the body of rats showed visible fluorescence, when exposed to a 980 nm NIR laser.

Organic Nanoparticles as Biolabels

The use of organic nonpolymeric nanoparticles as biolabels was not considered to be promising or have any advantage over established metallic or polymeric probes. Problems include quenching of fluorescence in organic dye crystals, colloidal stability and solubility in aqueous environments but some of these can be circumvented. Labels have been constructed by milling and suspending a fluorogenic hydrophobic precursor, fluorescein diacetate, in sodium dodecyl sulfate (SDS). Thus, a negative surface charge is introduced, rendering the particles (500 nm) colloidally stable and minimizing leakage of fluorescein diacetate molecules into surrounding water. Now it has been shown that the polyelectrolyte multilayer architechture is not vital for the operability of this assay format. Instead of SDS and multilayers the adsorption of only one layer of an amphiphilic polymeric detergent, e.g. an alkylated poly(ethylene imine), is sufficient to stabilize the system and to provide an interface for the antibody attachment. This is the basis of a technology "ImmunoSuperNova®" (invented by 8sens.biognostic AG, Germany). In this the reaction of the analyte molecule with the capture antibody is followed by an incubation step with the antibody-nanoparticle conjugate, which serves as detector. After some washing steps an organic release solvent is added, dissolving the particle and converting fluorescein diacetate into fluorescein.

Quantum Dots as Labels

The unique optical properties of QDs make them appealing as in vivo and in vitro fluorophores in a variety of biological investigations, in which traditional fluorescent labels based on organic molecules fall short of providing long-term stability and simultaneous detection of multiple signals. The ability to make QDs water soluble and target them to specific biomolecules has led to promising applications in cellular labeling, deep-tissue imaging, assay labeling and as efficient fluorescence resonance energy transfer donors.

DNA molecules attached to QD surface can be detect by fluorescence microscopy. The position and orientation of individual DNA molecules can be inferred with good efficiency from the QD fluorescence signals alone. This is achieved by selecting QD pairs that have the distance and direction expected for the combed DNA molecules. Direct observation of single DNA molecules in the absence of DNA staining agents opens new possibilities in the study of DNA-protein interactions. This approach can be applied for the use of QDs for nucleic acid detection and analysis. CdSe QDs can also be used as labels for sensitive immunoassay of cancer biomarker proteins by electrogenerated chemiluminescence. This strategy has been successfully used as a simple, cost-effective, specific, and potential method to detect α -fetoprotein in practical samples (Liu et al. 2011). In contrast to a QD that is selectively introduced as a label, an integrated QD is one that is present in a system throughout

a bioanalysis, and has a simultaneous role in transduction and as a scaffold for biorecognition. The modulation of QD luminescence provides the opportunity for the transduction of these events via fluorescence resonance energy transfer (FRET), bioluminescence resonance energy transfer (BRET), charge transfer quenching, and electrochemiluminescence (Algar et al. 2010).

SERS Nanotags

Surface enhanced Raman scattering (SERS) nanotags (Oxonica Inc) are silica-coated gold nanoparticles that are active at the glass-metal interface, and are optically detectable tags. Each type of tag exploits the Raman spectrum of a different small molecule and SERS bands are 1/50th the width of fluorescent bands. These enable more multiplexing than current fluorescence-based quantitation tags. The spectral intensity of SERS-based tags is linearly proportional to the number of particles allowing them to be used for multiplexed analyte quantification. Because they are coated with glass, attachment to biomolecules is straightforward. They can be detected with low-cost instrumentation. The particles can be interrogated in the near-IR, enabling detection in blood and other tissues. Another advantage of these particles is that they are stable and are resistant to photodegradation. Nanoplex Biotags can measure up to 20 biomarkers in a single test without interference from biological matrices such as whole blood. SERS nanotags are also useful for POC diagnostics. There is a great potential for multiplexed imaging in living subjects in cases in which several targeted SERS probes could offer better detection of multiple biomarkers associated with a specific disease (Zavaleta et al. 2009). The primary limitation of Raman imaging for tissue penetration in humans is also faced by other optical techniques. Over the last several years, Raman spectroscopy imaging has advanced significantly and many critical proof-of-principle experiments have been successfully carried out. It is expected that imaging with Raman spectroscopy will continue to be a dynamic research field over the next decade (Zhang et al. 2010).

Silica Nanoparticles for Labeling Antibodies

Luminescent silicon dioxide nanoparticles with size of 50 nm containing rhodamine (R-SiO2) have been synthesized by sol-gel method. These particles can emit intense and stable room temperature phosphorescence signals. At room temperature, a phosphorescent immunoassay can be used for the determination of human IgG using an antibody labeled with the nanoparticles containing binary luminescent molecules. This method is sensitive, accurate and precise. Lissamine rhodamine B sulfonylchloride and other dyes can be covalently bound to and contained in spherical silica nanoparticles (30–80 nm). Compared to organic molecular markers these fluorophore hybrid silica particles exhibit superior photostability and detection

sensitivity, e.g., for detecting trace levels of hepatitis B surface. Dye-doped fluorescent silica nanoparticles are highly efficient labels for glycans and applied to detect bacteria by imaging as well as to study carbohydrate-lectin interactions on a lectin microarray (Wang et al. 2011).

Silver Nanoparticle Labels

Silver (Ag) nanoparticles have unique plasmon-resonant optical scattering properties that are useful for nanomedical applications as signal enhancers, optical sensors, and biomarkers. Sensitive electrochemical DNA hybridization detection assay uses Ag nanoparticles as oligonucleotide labeling tags. The assay relies on the hybridization of the target DNA with the Ag nanoparticle-oligonucleotide DNA probe, followed by the release of the Ag metal atoms anchored on the hybrids by oxidative metal dissolution and the indirect determination of the solubilized Ag ions by anodic stripping voltammetry. Liquid electrode plasma-atomic emission spectrometry requires no plasma gas and no high-power source, which makes it suitable for onsite portable analysis, can be used for protein sensing studies employing Ag nanoparticle labeling. Human chorionic gonadotropin (hCG) was used as a model target protein, and the immunoreaction in which hCG is sandwiched between two antibodies, one of which is immobilized on the microwell and the second is labeled with Ag nanoparticles, was performed (Tung et al. 2012). hCG was analyzed in the range from 10 pg/mL to 1 ng/mL. This detection method has a wide variety of promising applications in metal-nanoparticle-labeled biomolecule detection.

Micro- and Nano-electromechanical Systems

The rapid pace of miniaturization in the semiconductor industry has resulted in faster and more powerful computing and instrumentation, which have begun to revolutionize medical diagnosis and therapy. Some of the instrumentation used for nanotechnology is an extension of MEMS (Micro ElectroMechanical Systems), which refers to a key enabling technology used to produce micro-fabricated sensors and systems. The potential mass application of MEMS lies in the fact that miniature components are batch fabricated using the manufacturing techniques developed in the semiconductor microelectronics industry enabling miniaturized, low-cost, high-performance and integrated electromechanical systems. The "science of miniaturization" is a much more appropriate name than MEMS and it involves a good understanding of scaling laws, different manufacturing methods and materials that are being applied in nanotechnology.

MEMS devices currently range in size from one to hundreds of micrometers and can be as simple as the singly supported cantilever beams used in AFM or as complicated as a video projector with thousands of electronically controllable microscopic mirrors. NEMS devices exist correspondingly in the nanometer realm – nano-electromechanical systems (NEMS). The concept of using externally controllable MEMS devices to measure and manipulate biological matter (BioMEMS) on the cellular and subcellular levels has attracted much attention recently. This is because initial work has shown the ability to detect single base pair mismatches of DNA and to quantifiably detect antigens using cantilever systems. In addition is the ability to controllably grab and manipulate individual cells and subsequently release them unharmed.

Surface nanomachining, combines the processing methods of MEMS with the tools of electron beam nanofabrication to create 3D nanostructures that move (and thus can do new types of things). Ultra-short pulsed-laser radiation, e.g. using femtolasers, is an effective tool for controlled material processing and surface nano/ micro-modification because of minimal thermal and mechanical damage. Surface nanomachining has potential applications in nanobiotechnology.

BioMEMS

Because BioMEMS involves the interface of MEMS with biological environments, the biological components are crucially important. To date, they have mainly been nucleic acids, antibodies and receptors that are involved in passive aspects of detection and measurement. These molecules retain their biological activity following chemical attachment to the surfaces of MEMS structures (most commonly, thiol groups to gold) and their interactions are monitored through mechanical (deflection of a cantilever), electrical (change in voltage or current in the sensor) or optical (surface plasmon resonance) measurements. The biological components are in the nanometer range or smaller; therefore, the size of these systems is limited by the minimum feature sizes achievable using the fabrication techniques of the inorganic structures, currently 100 nm–1 µm. Commercially available products resulting from further miniaturization could be problematic because of the expanding cost and complexity of optical lithography equipment and the inherent slowness of electron beam techniques. In addition to size limitations, the effects of friction have plagued multiple moving parts in inorganic MEMS, limiting device speeds and useful lifetimes.

Microarrays and Nanoarrays

Arrays consist of orderly arrangements of samples, which, in the case of biochips, may be cDNAs, oligonucleotides, or even proteins. Macroarraying (or gridding) is a macroscopic scheme of organizing colonies or DNA into arrays on large nylon filters ready for screening by hybridization. In microarrays, however, the sample spot sizes are usually less than 200 microns in diameter and require microscopic analysis. Microarrays have sample or ligand molecules (e.g. antibodies) at fixed locations on the chip while microfluidics involves the transport of material, samples, and/or reagents on the chip.

Microarrays provide a powerful way to analyze the expression of thousands of genes simultaneously. Genomic arrays are an important tool in medical diagnostic and pharmaceutical research. They have an impact on all phases of the drug discovery process from target identification through differential gene expression, identification and screening of small molecule candidates, to toxicogenomic studies for drug safety. To meet the increasing needs, the density and information content of the microarrays is being improved. One approach is fabrication of chips with smaller, more closely packed features – ultrahigh density arrays, which will yield:

- High information content by reduction of feature size from 200 µm to 50 nm
- Reduction in sample size
- · Improved assay sensitivity

Nanoarrays are the next stage in the evolution of miniaturization of microarrays. Whereas microarrays are prepared by robotic spotting or optical lithography, limiting the smallest size to several microns, nanoarrays require further developments in lithography strategies. Technologies available include the following:

- Electron beam lithography
- Dip-pen nanolithography
- Scanning probe lithography
- Finely focused ion beam lithography
- Nano-imprint lithography

Dip Pen Nanolithography for Nanoarrays

Dip Pen NanolithographyTM (DPNTM), developed by Mirkin Lab at Northwestern University, uses the tip of an AFM to write molecular "inks" directly on a surface. Biomolecules such as proteins and viruses can be positioned on surfaces to form nanoarrays that retain their biological activity. DPN is schematically shown in Fig. 2.3.

Advantages of DPN are as follows:

<u>Ultrahigh resolution</u>. DPN is capable of producing structures with line widths of less than 15 nm. This is compared to photolithography, which supports features of no less than 65 nm line width, and slower e-beam and laser lithography systems, which support features of 15 nm line width.

<u>Flexibility</u>. Direct fabrication is possible with many substances, from biomolecules to metals.

<u>Accuracy</u>. By leveraging existing highly accurate atomic force microscopy technology, DPN utilizes the best possible means for determining exactly where features are being placed on the substrate. This allows for the integration of multiple component nanostructures and for immediate inspection and characterization of fabricated structures.

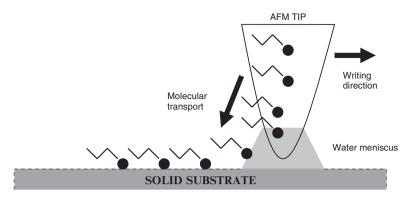


Fig. 2.3 Schematic representation of Dip Pen Nanolithography (DPN). A water meniscus forms between the atomic force microscope (AFM) tip coated with oligonucleotide (ODN) and the Au substrate. The size of the meniscus, which is controlled by relative humidity, affects the ODN transport rate, the effective tip-substrate contact area, and DPN resolution (© Jain PharmaBiotech)

<u>Low capital cost.</u> Techniques such as e-beam lithography that approach DPN-scale resolution are considerably more expensive to purchase, operate and maintain.

<u>Ease of use</u>. DPN systems may be operated by non-specialized personnel with minimal training. Further, DPN may be performed under normal ambient laboratory conditions with humidity control.

<u>Speed</u>. 100-nm spots can be deposited with a single DPN pen in less than a second. DPN can be used to fabricate arrays of a single molecule with more than 100,000 spots over 100×100 microns in less than an hour.

Applications of Dip-Pen Nanolithography

Multiple-allergen testing for high throughput and high sensitivity requires the development of miniaturized immunoassays that can be performed with minute amounts of test analyte that are usually available. Construction of such miniaturized biochips containing arrays of test allergens needs application of a technique able to deposit molecules at high resolution and speed while preserving its functionality. DPN is an ideal technique to create such biologically active surfaces, and it has already been successfully applied for the direct, nanoscale deposition of functional proteins, as well as for the fabrication of biochemical templates for selective adsorption. It has potential applications for detection of allergen-specific immunoglobin E (IgE) antibodies and for mast cell activation profiling (Sekula-Neuner et al. 2012).

Protein Nanoarrays

High-throughput protein arrays allow the miniaturized and parallel analysis of large numbers of diagnostic biomarkers in complex samples. This capability can be enhanced by nanotechnology. DPN technique has been extended to protein arrays with features as small as 45 nm and immunoproteins as well as enzymes can be deposited. Selective binding of antibodies to protein nanoarrays can be detected without the use of labels by monitoring small (5–15 nm) topographical height increases in AFM images.

Miniaturized microarrays, 'mesoarrays', created by DPN with protein spots 400× smaller by area compared to conventional microarrays, were used to probe the ERK2-KSR binding event of the Ras/Raf/MEK/ERK signaling pathway at a physical scale below that previously reported (Thompson et al. 2011). This study serves as a first step towards an approach that can be used for analysis of proteins at a concentration level comparable to that found in the cellular environment.

Single-Molecule Protein Arrays

The ability placeme individual protein molecules on surfaces could enable advances in many areas ranging from the development of nanoscale biomolecular devices to fundamental studies in cell biology. An approach that combines scanning probe block copolymer lithography with site-selective immobilization strategies has been used to create arrays of proteins down to the single-molecule level with arbitrary pattern control (Chai et al. 2011). Scanning probe block copolymer lithography was used to synthesize individual sub-10-nm single crystal gold nanoparticles to act as scaffolds for the adsorption of functionalized alkylthiol monolayers for facilitating the immobilization of specific proteins. The number of protein molecules that adsorb onto the nanoparticles depends on particle size; when the particle size approaches the dimensions of a protein molecule, each particle can support a single protein. This was demonstrated with both gold nanoparticle and QD labeling coupled with TEM imaging. The immobilized proteins remain bioactive, as demonstrated by enzymatic assays and antigen-antibody binding experiments.

Microfluidics and Nanofluidics

Microfluidics is the handling and dealing with small quantities (e.g. microliters, nanoliters or even picoliters) of fluids flowing in channels the size of a human hair (~50 microns thick) even narrower. Fluids in this environment show very different properties than in the macro world. This new field of technology was enabled by advances in microfabrication – the etching of silicon to create very small features. Microfluidics is one of the most important innovations of biochip technology. Typical dimensions of microfluidic chips are 1–50 cm² and have channels 5–100 microns. Usual volumes are 0.01–10 microliters but can be less. Microfluidics is the link between microarrays and nanoarrays as we reduce the dimensions and volumes.

Microfluidics is the underlying principle of lab-on-a-chip devices, which carry out complex analyses, while reducing sample and chemical consumption, decreasing waste and improving precision and efficiency. The idea is to be able to squirt a very small sample into the chip, push a button and the chip will do all the work, delivering a report at the end. Microfluidics allows the reduction in size with a corresponding increase in the throughput of handling, processing and analyzing the sample. Other advantages of microfluidics include increased reaction rates, enhanced detection sensitivity and control of adverse events.

Drawbacks and limitations of microfluidics and designing of microfluidic chips include the following:

- · Difficulties in microfluidic connections
- · Because of laminar flows, mixing can only be performed by diffusion
- Large capillary forces
- Clogging
- Possible evaporation and drying up of the sample

Applications of microfluidics include the following:

- DNA analysis
- Protein analysis
- · Gene expression and differential display analysis
- Biochemical analysis

Nanotechnology on a Chip

Nanotechnology on a chip is a new paradigm for total chemical analysis systems. The ability to make chemical and biological information much cheaper and easier to obtain is expected to fundamentally change healthcare, food safety and law enforcement. Lab-on-a-chip technology involves micro-total analysis systems that are distinguished from simple sensors because they conduct a complete analysis; a raw mixture of chemicals goes in and an answer comes out. Sandia National Laboratories is developing a hand-held Lab-on-a-chip that will analyze for air-borne chemical warfare agents and liquid-based explosives agents. This development project brings together an interdisciplinary team with areas of expertise including microfabrication, chemical sensing, microfluidics, and bioinformatics. Although nanotechnology plays an important role in current efforts, miniaturized versions of conventional architecture and components such as valves, pipes, pumps, separation columns, are patterned after their macroscopic counterparts. Nanotechnology will provide the ability to build materials with switchable molecular functions could provide completely new approaches to valves, pumps, chemical separations, and detection. For example, fluid streams could be directed by controlling surface energy without the need for a predetermined architecture of physical channels. Switchable molecular membranes and the like could replace mechanical valves. By eliminating the need for complex fluidic networks and micro-scale components used in current approaches, a fundamentally new approach will allow greater function in much smaller, lower power total chemical analysis systems.

A new scheme for the detection of molecular interactions based on optical readout of nanoparticle labels has been developed. Capture DNA probes can be arrayed on a glass chip and incubated with nanoparticle-labeled target DNA probes, containing a complementary sequence. Binding are monitored by optical means, using reflected and transmitted light for the detection of surface-bound nanoparticles. Control experiments significant Influence of nonspecific binding on the observed contrast can be excluded. Distribution of nanoparticles on the chip surface can be demonstrated by scanning force microscopy.

BioForce Nanosciences has taken the technology of the microarray to the next level by creating the "nanoarray," an ultra-miniaturized version of the traditional microarray that can measure interactions between individual molecules down to resolutions of as little as 1 nm. Here, 400 nanoarray spots can be placed in the same area as a traditional microarray spot Nanoarrays are the next evolutionary step in the miniaturization of bioaffinity tests for proteins, nucleic acids, and receptor-ligand pairs. On a BioForce NanoArrayT, as many as 1500 different samples can be queried in the same area now needed for just one domain on a traditional microarray.

Microfluidic Chips for Nanoliter Volumes

Nanoliter implies extreme reduction in quantity of fluid analyte in a microchip. The use of the word "nano" in nanoliter (nL) is in a different dimension than in nanoparticle, which is in nanometer (nm) scale. Chemical compounds within individual nanoliter droplets of fluid can be microarrayed on to glass slides at 400 spots/cm². Using aerosol deposition, subsequent reagents and water can be metered into each reaction center to rapidly assemble diverse multicomponent reactions without cross contamination or the need for surface linkage. Such techniques enable the kinetic profiling of protease mixtures, protease-substrate interactions, and high-throughput screening reactions. From one printing run that consumes <1 nanomole of each compound, large combinatorial libraries can be subjected to numerous separation-free homogeneous assays at volumes much smaller than current high-throughput methods. The rapid assembly of thousands of nanoliter reactions per slide using a small biological sample represents a new functional proteomics format implemented with standard microarraying and spot-analysis tools.

Use of Nanotechnology in Microfluidics

Use of nanotechnology in microfluidics is called nanofluidics. Because nanofluidics enables the manipulation of confined ions and electrolytes on nanoscale, it has applications in nanosensors and nanochips for study of subcellular structures.

2D Nanofluidics

The remarkable electronic properties of graphene and related 2D materials result from the confinement of electrons within the material. Similarly, the interstitial space between 2D materials enables the 2D confinement of ions and electrolytes and alters their transport. Several 2D sheets can be obtained by exfoliation of natural layered materials, and an exfoliation-reconstruction strategy can convert powders of layered materials into continuous, robust bulk forms in which lamellar nanochannels occupy a substantial fraction of volume amounting up to several tens of percent (Koltonow and Huang 2016).

Construction of Nanofluidic Channels

Techniques such as nanoimprinting are used to construct large arrays of nanoscale grooves with efficiency and speed. Such grooves can be sealed with similar ease, to form nanofluidic channels. Laser-assisted direct imprint techniques enable the construction of millions of enclosed nanofluidic channels side by side on a single substrate, which is ideal for such parallel processing. By sputter-depositing silicon dioxide at an angle onto an array of prefabricated nanochannels imprinted into the surface of a biopolymer substrate, not only is an effective and uniform seal formed over the entire array, but the channels are further narrowed to 10 nm, from an initial width of 55 nm. This process could be easily used for narrowing and sealing micro-and nano-fluidic structures formed by other patterning techniques. By minimizing the hollow space in such structures, it could help surpass existing limitations in the spatial resolution of these techniques.

A chip-scale maze for combing out strands of DNA and inserting them into nanoscale channels was made using standard, inexpensive lithographic techniques. Their 'gradient nanostructure' might be used to isolate and stretch DNA molecules for analysis, e.g. to look for bound proteins such as transcription factors along the strand. Such molecules would be obscured in normal solution because DNA, like any other linear polymer, collapses into a random coil as a featureless blob. The strands can, in principle, be straightened by feeding them into channels just a few tens of nanometers wide, using nanofluidic techniques.

Restriction mapping with endonucleases is a central method in molecular biology. Restriction mapping of DNA molecules cab be performed using restriction endonucleases in nanochannels with diameters of 100–200 nm. It is based on the measurement of fragment lengths after digestion, while possibly maintaining the respective order. The location of the restriction reaction within the device is controlled by electrophoresis and diffusion of Mg²⁺ and EDTA. It is possible to measure the positions of restriction sites with precision using single DNA molecules with a resolution of 1.5 kbp within 1 minute.

A review of nanofluidic systems reveals that these are divided into two large categories: top-down and bottom-up methods. The technology in the region of 1-10 nm is lacking and potentially can be covered by using the pulsed-laser deposition method as a controlled way for thin film deposition (thickness of a few nanometers) and further structuring by the top-down method.

The benefits of operating in the nanoliter space include reduction of solvent, waste disposal costs, and human exposure by factors of 1000×. New routine liquid handling capabilities include a purported 10x increase in MALDI sensitivity for analysis of proteins in proteomics work as demonstrated by various products such as nanoliter syringes based on induction-based fluidics technology that uses electric fields to launch liquids to targets.

Nanoscale Flow Visualization

Most of the microscale flow visualization methods evolved from methods developed originally for macroscale flow. It is unlikely, however, that developed microscale flow visualization methods will be translated to nanoscale flows in a similar manner. Resolving nanoscale features with visible light presents a fundamental challenge. Although point-detection scanning methods have the potential to increase the flow measurement resolution on the microscale, spatial resolution is ultimately limited by the optical probe volume (length scale on the order of 100 nm), which, in turn, is limited by the wavelength of light employed. Optical spatially resolved flow measurements in nanochannels are difficult to visualize. There is a need for refinement of microscale flow visualization methods and the development of direct flow measurement methods for nanoflows.

Moving (Levitation) of Nanofluidic Drops with Physical Forces

The manipulation of droplets/particles that are isolated (levitated in gas/vacuum) from laboratory samples containing chemicals, cells, bacteria or viruses, is important both for basic research in physics, chemistry, biology, biochemistry, and colloidal science and for applications in nanotechnology and microfluidics. Various optical, electrostatic, electromagnetic and acoustic methods are used for levitation.

Microfluidic drops can be moved with light – the lotus effect. On a super-rough surface, when light shines on one side of a drop, the surface changes, the molecules switch and the drop moves. This technology has potential applications in drug screening as it can be used for quickly analyzing and screening small amounts of biological materials. Called digital microfluidics, this approach enables one to quickly move small drops around by shining light on them. Hundreds of screens could be done on only one surface. The molecules, e.g. protein traces, do not interfere with movements of the drops because the surfaces are hydrophobic and the molecules have little contact with the surface.

The size of diamagnetic levitation devices can be reduced by using micron scale permanent magnets to create a magnetic micromanipulation chip, which operates with femtodroplets levitated in air. The droplets used are one billion times smaller in volume than has been demonstrated by conventional methods. The levitated particles can be positioned with up to 300 nm accuracy and precisely rotated and assembled. Using this lab-on-a-chip it might be possible to do the same thing with numerous fluids, chemicals and even red blood cells, bacteria and viruses.

Electrochemical Nanofluid Injection

The ability to manipulate ultrasmall volumes of liquids is required in such diverse fields as cell biology, microfluidics, capillary chromatography, and nanolithography. In cell biology, it is often necessary to inject materials of high molecular weight such as DNA and proteins into living cells because their membranes are impermeable to such molecules. Currently used techniques for microinjection are limited by the relatively large injector size and poor control of the amount of injected material. An electrochemical attosyringe forcontrol of the fluid motion enables dispensing of attoliter-to-picoliter (10^{-18} to 10^{-12} liter) volumes of either aqueous or nonaqueous solutions. By changing the voltage applied across the liquid/liquid interface, one can produce a sufficient force to draw solution inside a nanopipette and then inject it into an immobilized biological cell. A high success rate has been achieved for injections of fluorescent dyes into human cells in culture. The injection of femtoliterrange volumes can be monitored by video microscopy, and current/resistance-based approaches can be used to control injections from very small pipettes. Other potential applications of the electrochemical syringe include fluid dispensing in nanolithography and pumping in nanofluidic systems.

Nanofluidics on Nanopatterned Surfaces

A very thin layer of liquid behaves on a "nanopatterned" silicon surface, i.e. a surface etched with an ordered array of cavities, each only 20 nm deep. Watching how a liquid adsorbs on a nanopatterned surface is one way to study the basic properties of liquids that are confined in extremely tiny amounts within nanoscale structures. Understanding these properties will help in developing many useful fluid-based nanotechnologies. This work could help improve the "lab on a chip". Currently, the knowledge about the microscopic behavior of liquids on solid surfaces, known as "wetting" phenomena, is predominately based on measurements taken using structureless, flat surfaces. In those cases, the behavior of the liquid is based on the strength of attractive molecule-molecule forces known as "van der Waals interactions." But for a surface that contains a regular pattern of cavities, the shape of the surface influences how the liquid will fill those cavities. Analysis of the X-ray data reveals that a liquid layer builds up inside each nanocavity at a faster rate than on a flat surface of the same material. The wetting properties of the surface are considerably enhanced by the nanopatterning.

Nano-Interface in a Microfluidic Chip

There are emerging experimental and conceptual platforms for probing living cells with nanotechnology-based tools in a microfluidic chip. Considerable advances have been made in measuring nanoscale mechanical, biochemical, and electrical interactions at the interface between biomaterials and living cells. By merging the fields of microfluidics, electrokinetics, and cell biology, microchips can create tiny, mobile laboratories. The challenge for the future of designing a nano-interface in a microfluidic chip to probe a living cell lies in seamlessly integrating techniques into a robust and versatile, yet reliable, platform. Potential benefits of nanosystems on a microchip result from real-time detection of numerous events in parallel. In addition to early detection of cell-level dysfunctions, these systems will enable broad screening that encompasses not just many toxic stimuli and disease processes but also population subgroups. This will facilitate the development of personalized medicine. To reach this goal requires advancing the knowledge base of cellular and subcellular functions, perhaps by designing nanosystems that operate in the tissue milieu.

Nanofluidic Channels for Study of DNA

Nanofluidic channels enable molecular biologists to spot the association and dissociation of proteins on fluorescently labeled DNA. The simple system could even help researchers visualize induced tertiary structures such as loops, which push conventional optical or magnetic stretching methods to the limit. This silicon dioxideglass nanochannel system, also referred to as nanoslit requires no externally applied forces or fields. To unravel the molecules, one places a drop of solution containing DNA at one end of the nanochannel. Capillary action then draws the liquid into channels measuring 2-10 µm wide and 100 nm deep. After 1 min, a drop of buffer solution is added at the other end of the channel to equalize the pressure in the device and stop the flow. In channels of 100 nm depth or less, DNA molecules spontaneously adopt an extended state adjacent to the channel wall. The nanochannel geometry, however, physically confines polymer molecules to two spatial dimensions. Further reduction in configuration results in spontaneous axial stretching of molecules and appears to be electrostatically mediated. The physics for stretching a DNA molecule is built into the structure of the device. Fabrication of the channels and mass production of the unit is easy. Devices are made by first patterning a silicon substrate using laser lithography and then forming parallel channels 100 nm deep by either reactive ion etching in plasma or wet etching in HF. Cover glass is used to seal the channels from above.

Visualization and Manipulation on Nanoscale

3D Single-Molecule Microscopy with Nanoscale Accuracy

The localization of single fluorescent molecules enables the imaging of molecular structure and dynamics with subdiffraction precision and can be extended to 3D using point spread function (PSF) engineering. Previous calibration techniques for super-resolution microscopy were not sufficiently accurate for 3D measurements of single molecules. The new calibration method uses a nanohole array to correct for

optical distortions. Nanoscale accuracy of localization throughout a 3D singlemolecule microscope's field of view has now been achieved using regularly spaced subdiffraction apertures filled with fluorescent dyes, which reveal field-dependent aberrations as large as 50–100 nm and show that they can be corrected to <25 nm over an extended 3D focal volume (von Diezmann et al. 2015). This technique can be applied for 2 engineered PSFs, the double-helix PSF and the astigmatic PSF. These results are expected to be broadly applicable to 3D single-molecule tracking and superresolution methods demanding high accuracy. This technique is being used it to study protein localization in bacteria that measure only 2 μ in length. With the 3D calibration technique, it is possible to accurately measure and track key signaling proteins in nanodomains that are only 150–200 nm in size. Tracking how molecules move, form shapes and interact within the body's cells and neurons offers a powerful new view of key biological processes such as signaling, cell division and neuron communication, which impact people's health and susceptibility to disease.

4Pi Microscope

The most prominent restrictions of fluorescence microscopy are the limited resolution and the finite signal. Established conventional, confocal, and multiphoton microscopes resolve at best approximately 200 nm in the focal plane and only 500 nm in depth.

4Pi microscope (Leica Microsystems) uses a special phase- and wavefrontcorrected double-objective imaging system linked to a confocal scanner to enable 4 to 7-fold increased axial resolution over confocal and two photon microscope. Even in living specimens, axial sections of ~100 nm are obtained. The system maintains all advantages of fast scanning, Acousto-Optical Beam Splitting (AOBS®) and Spectral Detection of the Leica TCS SP2 AOBS for routine operation. The first marked leap in resolution in commercial 3D fluorescence microscopy opens new dimensions for research in cell and developmental biology. Co-localization studies of immunolabeled microtubules and mitochondria demonstrate the feasibility of 4Pi microscopy for routine biological measurements; particularly, to visualize the 3D entanglement of the two networks with unprecedented detail.

Atomic Force Microscopy

AFM Basics

In its most basic form, atomic force microscopy (AFM) images topography by precisely scanning a probe across the sample to "feel" the contours of the surface. The interaction between the needle and the surface is measured and an image is

reconstructed from the data collected in this manner. With AFM, it is possible it is possible to reach an extremely high resolution. Because it can be applied under standard conditions in an aqueous environment, any significant perturbation of the sample can be avoided. In contrast to light microscopy and scanning electron microscopy, AFM provides the most optimal means to investigate the surface structures in three dimensions, with resolutions as high as 0.1–0.2 nm.

A key element of the AFM is its microscopic force sensor, or cantilever. The cantilever is usually formed by one or more beams of silicon or silicon nitride that is 100 to 500 microns long and about 0.5 to 5 microns thick. Mounted on the end of the cantilever is a sharp tip that is used to sense a force between the sample and tip. For normal topographic imaging, the probe tip is brought into continuous or intermittent contact with the sample and raster-scanned over the surface.

Advantages of AFM

In addition to its superior resolution and routine three-dimensional measurement capability, AFM offers several other clear advantages over traditional microscopy techniques. For example, scanning and transmission electron microscopy (SEM, TEM) image biologically inactive, dehydrated samples and generally require extensive sample preparation such as staining or metal coating. AFM eliminates these requirements and, in many cases, allows direct observation of native specimens and ongoing processes under native or near-native conditions.

Further adding to its uniqueness, the AFM can directly measure nanoscale interactive forces, e.g. ligand-receptor binding. Samples can be examined in ambient air or biological fluids without the cost and inconvenience of vacuum equipment. Sample preparation is minimal and allows the use of standard techniques for optical microscopy. The MultiMode AFM provides maximal resolution while the BioScope AFM integrates the best of optical and atomic force microscopy to help life scientists explore new frontiers.

The ability of the AFM to create 3D micrographs with resolution down to the nanometer and Angstrom scales has made it an essential tool for imaging surfaces in applications ranging from semiconductor processing to cell biology. In addition to this topographical imaging, however, the AFM can also probe nanomechanical and other fundamental properties of sample surfaces, including their local adhesive or elastic (compliance) properties.

Microscopic adhesion affects a huge variety of events, from the behavior of paints and glues, ceramics and composite materials, to DNA replication and the action of drugs in the human body. Elastic properties are similarly important, often affecting the structural and dynamic behavior of systems from composite materials to blood cells. AFM offers a new tool to study these important parameters on the micron to nanometer scale using a technique that measures forces on the AFM probe tip as it approaches and retracts from a surface.

AFM as Nanorobot

An AFM-based nanorobot has been introduced for biological studies (Xie et al. 2011). Using the AFM tip as an end effector, the AFM can be modified into a nanorobot that can manipulate biological objects at the single-molecule level. By functionalizing the AFM tip with specific antibodies, the nanorobot can identify specific types of receptors on the cell membrane. It is like the fluorescent optical microscopy but with higher resolution. By locally updating the AFM image based on interaction force information and objects' model during nanomanipulation, real-time visual feedback is obtained through the augmented reality interface. The development of the AFM-based nanorobotic system enables us to conduct in situ imaging, sensing, and manipulation simultaneously at the nanometer scale (e.g. protein and DNA levels). The AFM-based nanorobotic system offers several advantages and capabilities for studying structure-function relationships of biological specimens. Therefore, many biomedical applications can be achieved by the AFM-based nanorobotic system.

Force Sensing Integrated Readout and Active Tip

Force sensing Integrated Readout and Active Tip (FIRAT) is an extremely sensitive AFM technology that is capable of high-speed imaging 100 times faster than current AFM technology. Current AFM scans surfaces with a thin cantilever with a sharp tip at the end. An optical beam is bounced off the cantilever tip to measure the deflection of the cantilever as the sharp tip moves over the surface and interacts with the material being analyzed. FIRAT works a bit like a cross between a pogo stick and a microphone. In one version of the probe, the membrane with a sharp tip moves toward the sample and just before it touches, it is pulled by attractive forces. Much like a microphone diaphragm picks up sound vibrations, the FIRAT membrane starts taking sensory readings well before it touches the sample. And when the tip hits the surface, the elasticity and stiffness of the surface determines how hard the material pushes back against the tip. So rather than just capturing a topography scan of the sample, FIRAT can pick up a wide variety of other material properties.

FIRAT can capture additional measurements not possible before with AFM, including parallel molecular assays for drug screening and discovery, as well as material property imaging. This research breakthrough could prove invaluable for many types of nano-research, including translating into movies of molecular interactions in real time. FIRAT might eventually replace AFM.

Cantilever Technology

Cantilevers (Concentris) transform a chemical reaction into a mechanical motion on the nanometer scale. Measurements of a cantilever are: length 500 μ m, width 100 μ m, thickness 25–500 μ m and deflection 10 nm. This motion can be measured directly by

deflecting a light beam from the cantilever surface. Concentris uses an array of parallel VCSELs (Vertical Cavity Surface Emitting Lasers) as stable, robust and proven light source. A state-of-the-art position sensitive detector is employed as detection device.

The static mode is used to obtain information about presence of certain target molecules in the sample substance. The surface stress caused by the adsorption of these molecules results in minute deflections of the cantilever. This deflection directly correlates with the concentration of the target substance. The dynamic mode allows quantitative analysis of mass loads in the sub-picogram area. As molecules get adsorbed, minimal shifts in the resonance frequency of an oscillating cantilever can be measured and associated to reference data of the target substance. Both modes can also be operated simultaneously.

The controlled deposition of functional layers is the key to converting nanomechanical cantilevers into chemical or biochemical sensors. Inkjet printing as a rapid and general method to coat cantilever arrays efficiently with various sensor layers. Selfassembled monolayers of alkanethiols are deposited on selected Au-coated cantilevers and rendered them sensitive to ion concentrations or pH in liquids. The detection of gene fragments is achieved with cantilever sensors coated with thiol-linked singlestranded DNA oligomers on Au. A selective etch protocol proves the uniformity of the monolayer coatings at a microscopic level. A chemical gas sensor is fabricated by printing thin layers of different polymers from dilute solutions onto cantilevers. The inkjet method is easy to use, faster and more versatile than coating via microcapillaries or the use of pipettes. In addition, it is scalable to large arrays and can coat arbitrary structures in non-contact. The applications of cantilever technology, Cantosens (Concentris) are listed in Table 2.5 and discussed further in Chap. 3.

Further research continues at academic laboratories to develop nanoscale cantilevers, which would be smaller than the wavelength of light and make laser detection more difficult. When these devices are developed, they could be incorporated into AFMs, which are currently designed for standard size cantilevers.

AFM cantilevers have been actuated using a micro-heater at the bottom and integrated with deflection sensor as well as micro-actuator for imaging of soft biological samples in fluid (Fantner et al. 2009). Influence of the water was investigated on the cantilever dynamics, the actuation and the sensing mechanisms, as well as the crosstalk between sensing and actuation. Successful imaging of yeast cells in water using the integrated sensor and actuator shows the potential of the combination of this actuation and sensing method. This constitutes a major step towards the automation and miniaturization required to establish AFM in routine biomedical diagnostics and in vivo applications.

CytoViva® Microscope System

Specifically designed to support research in nanotechnology and infectious disease, the CytoViva Microscope System (CytoViva Inc) employs a proprietary darkfieldbased optical illumination technology, which dramatically improves contrast and signal-to-noise ratio. This transmitted-light illumination system enables scientists to

Table 2.5 Applications of cantilever technology
Basic Research
Study of chemical reactions or host-guest interactions on surfaces
Nano-calorimetry
Medical diagnostics
Parallel and label-free detection of disease biomarkers, e.g. serum proteins or autoantibodies.
Fast, label-free recognition of specific DNA sequences (SNPs, oncogenes, genotyping)
Detection of microorganisms and antimicrobial susceptibility
Drug discovery and life sciences research
Label-free biochemical assays and investigation of biomolecular interactions
Multiplexed assays.
Process and quality control
Process monitoring.
Purity analysis
Food analysis
Detection of trace contaminations, e.g. antibiotics, hormones, pesticides.
Detection of microorganisms.
Identification and quality control
Environmental monitoring/public health
Detection of heavy metal ions, pesticides, air pollutants.
Water analysis
Fragrance and flavor analysis
Using neural networks to analyze cantilever sensor array signals can identify and characterize complex chemical mixtures ("electronic nose" or "tongue").
Security devices
Detection of potentially hazardous chemicals and microorganisms
Work place security
© Jain PharmaBiotech

observe a wide range of nanomaterials quickly and easily, without any special preparation. In addition, live cells and pathogens can also be viewed at a level of detail not possible with traditional optical imaging techniques such as phase contrast or differential interference contrast. When using the CytoViva Dual Mode Fluorescence system, researchers can also observe the interactions between fluorescently labeled nanoparticles or bacteria and live unlabeled cells. This unique capability can eliminate the need to create computer enhanced overlay images, which require two different illumination methods and advanced software programs. Finally, when combined with the CytoViva Hyperspectral Imaging system, this high contrast microscopy method enables researchers to secure spectral data from these images.

Fluorescence Resonance Energy Transfer

Fluorescence Resonance Energy Transfer (FRET) is a process by which energy that would normally be emitted as a photon from an excited fluorophore can be directly transferred to a second fluorophore to excite one of its electrons. This, on decay, then

generates an even longer wavelength photon. The extent of FRET is critically dependent on the distance between the two fluorophores as well as their spectral overlap. Thus, FRET is a powerful reporter of the separation of the two fluorophores. FRET is a simple but effective tool for measurements of protein-protein interactions. It is one of the few techniques that can give dynamic information about the nanometer-range proximity between molecules, as opposed to simply the subcellular co-localization that is provided by fluorescence microscopy.

Fluorescence by Unbound Excitation from Luminescence

Fluorescence by unbound excitation from luminescence (FUEL) is a phenomenon that exploits radiating luminescence to excite nearby fluorophores by epifluorescence (Dragavon et al. 2012). This study showed that photons from bioluminescent bacteria radiate over mesoscopic distances and induce a red-shifted fluorescent emission from appropriate fluorophores in a manner distinct from bioluminescence resonance energy transfer (BRET). FUEL helps to overcome a common difficulty due to the presence of blue-green absorbers such as hemoglobin that interferes with in vivo excitation of nanoparticles using luminescent bacteria, which produce biological chemiluminescence typically centered on 490 nm. Characterization of FUEL, both in vitro and in vivo, demonstrates how the resulting blue-to-red wavelength shift is both necessary and sufficient to yield contrast enhancement revealing mesoscopic proximity of luminescent and fluorescent probes in the context of living biological tissues. The results of this study suggest FUEL is an important and overlooked component of BRET phenomena, potentially altering the empirical, quantitative, and experimental interpretation.

Magnetic Resonance Force Microscopy and Nanoscale MRI

IBM has been working over a decade to develop nanoscale magnetic resonance imaging technology called magnetic resonance force microscopy (MRFM). The central feature of MRFM is a silicon 'microcantilever' that looks like a miniature diving board and is 1000 times thinner than a human hair. It vibrates at a frequency of about 5000 times a second, and a tiny but powerful magnetic particle attached to the tip attracts or repels individual electrons. The company claimed a breakthrough in nanoscale MRI by directly detecting for the first time a faint magnetic signal from single electrons buried inside solid samples. MRFM has been combined with 3D image reconstruction to achieve MRI with resolution <10 nm (Degen et al. 2009). The image reconstruction converts measured magnetic force data into a 3D map of nuclear spin density, taking advantage of the unique characteristics of the "resonant slice" that is projected outward from a nanoscale magnetic tip. The basic principles are demonstrated by imaging the 1H spin density within individual tobacco mosaic virus particles sitting on a nm-thick layer of adsorbed hydrocarbons. This result,

which represents a 100 million-fold improvement in volume resolution over conventional MRI, demonstrates the potential of MRFM as a tool for 3D, elementally selective imaging on the nanometer scale.

With further progress in resolution and sample preparation, force-detected MRI techniques could have significant impact on the imaging of nanoscale biological structures, even down to the scale of individual molecules. Achieving resolution of 1 nm appears to be realistic because the current apparatus operates almost a factor of 10 away from the best demonstrated force sensitivities and field gradients. Even with a resolution >1 nm, MRFM may enable the basic structure of large molecular assemblies to be elucidated. MRFM image contrast can be enhanced beyond the basic spin-density information by using techniques like that developed for clinical MRI and NMR spectroscopy. Such contrast may include selective isotopic labeling, selective imaging of different chemical species, relaxation-weighted imaging, and spectroscopic imaging that reflects the local chemical environment.

The development represents a major milestone in the creation of a microscope that can make 3D images of molecules with atomic resolution. Such a device could have a major impact on the study of materials, ranging from proteins and pharmaceuticals to integrated circuits for which a detailed understanding of the atomic structure is essential. The ability to image the detailed atomic structure of proteins directly would also aid the development of new drugs. This new capability should ultimately lead to fundamental advances in nanotechnology and biology.

Multiple Single-Molecule Fluorescence Microscopy

Fitting the image of a single molecule to the point spread function of an optical system greatly improves the precision with which single molecules can be located. In nanometer-localized multiple single-molecule (NALMS) fluorescence microscopy, short duplex DNA strands are used as nanoscale "rulers" for validation. Nanometer accuracy of this microscope has been demonstrated for 2–5 single molecules within a diffraction-limited area. NALMS microscopy will greatly facilitate single-molecule study of biological systems because it covers the gap between fluorescence resonance energy transfer-based (<10 nm) and diffraction-limited microscopy (>100 nm) measurements of the distance between two fluorophores. NALMS microscopy has been applied to DNA mapping with <10-nm resolution.

Near-Field Scanning Optical Microscopy

Near-field scanning optical microscopy (NSOM) was the first technique that has overcome the limits of light microscopy by about one order of magnitude. Typically, the resolution range below 100 nm is accessed for biological applications. Using appropriately designed scanning probes allows for obtaining an extremely small near-field light excitation volume (some tens of nanometers in diameter). Because of the reduction of background illumination, high contrast imaging becomes feasible for light transmission and fluorescence microscopy. The height of the scanning probe is controlled by atomic force interactions between the specimen surface and the probe tip. The control signal can be used to produce a topographic (nonoptical) image that can be acquired simultaneously.

Scattering near-field microscopy (s-SNOM) can determine infrared "fingerprint" spectra of individual poly(methyl methacrylate) nanobeads and viruses as small as 18 nm. Amplitude and phase spectra are found surprisingly strong, even at a probed volume of only 10^{-20} liter, and robust regarding particle size and substrate. This makes infrared spectroscopic s-SNOM a versatile tool for chemical and protein-secondary-structure identification.

Nano-sized Light Source for Single Cell Endoscopy

A nano-sized light source can emit coherent light across the visible spectrum. Among the potential applications of this nano-sized light source are single cell endoscopy and other forms of subwavelength bio-imaging, integrated circuitry for nanophotonic technology, and new advanced methods of cyber cryptography. Working with individual nanowires, scientists have developed the first electrode-free, continuously tunable coherent visible light source that's compatible with physiological environments. Nanowires with diameters as small as 20 nm and aspect ratios of >100 can be trapped and transported in 3D, enabling the construction of nanowire architectures that may function as active photonic devices. It is possible to trap and manipulate single nanowires with optical tweezers, a critical capability not only for bio-imaging but also for wiring together nanophotonic circuitry. This nanowire light source is like a tiny flashlight that can scan across a living cell, enabling visualization of the cell, and at the same time, mechanically interacting with it.

Nanoparticle Characterization by Nanosight LM10 Technology

Nanosight LM10 (Malvern NanoSight) is based on the laser illumination of a specially designed optical element on to which sample is simply placed manually or allowed to flow across the surface. This is the first nanoparticle characterization tool, specifically designed for liquid phase sizing of individual nanoparticles, with the use of a conventional light microscope. Particles as small as 20 nm have been successfully visualized by this method, and each particle seen as an individual point of light moving under Brownian motion within the liquid. The intensity of light scattered by a particle varies as the 6th power of its radius. By doubling the diameter of the particle, 64-fold more light is scattered by the particle. This has significant implications for the early and simple detection of aggregation, flocculation and dimerization of particulates at the nanometer scale.

Molecular diagnostics
Detection of viral particles
DNA analysis
Mycoplasma detection in animal cell culture
Contaminant monitoring
Drug delivery
Drug carriers
Monitoring drug efficacy in body fluids
Biofilm production and implants
Nanoparticles
Environmental
Biodefence
Airborne contaminants such as asbestos particles
Medical
Clinical diagnosis of viral diseases, e.g. cerebrospinal fluid
Cancer cell detection, e.g. metastases
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 Table 2.6
 Applications of optical nanoscopy

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Use of a shorter wavelength laser source capable of exciting fluorescent labels enables specific components within the sample to be distinguished from nonspecific background particles. The image can be analyzed by suitable software allowing changes in individual particle position to be followed furnishing real time information about particle diffusion and particle-to-particle interactions. In the fluorescence mode, correlation techniques can be used to derive information by use of the technique known as fluorescence correlation spectroscopy. Nanosight LM10 is supported by software.

The laser source need only be a few mW in power and can be delivered to the optical device via fiber optic connection or the laser diode can be coupled directly to the edge of the optical element. The optical element can be manufactured in optical quality plastic or in glass or silica. The optical element need only be a few mm square and 2-5 mm in depth.

Larger volumes of sample containing dilute concentrations of particles of interest can be analyzed by being configured within a flow cell. Fabrication of the optical element is by industry standard metal coating techniques such as those found in the electronics and optical devices industries. Applications relevant to nanobiotechnology are shown in Table 2.6.

Nanoscale Scanning Electron Microscopy

Pharmaceutical enterprises require a range of imaging products that provide high quality information, allowing them to reach their own targets on technology, productivity, and ultimately profitability. With the increasing expectations upon drug delivery systems for efficient and controlled delivery of the active material there is a matching need for accurate information on these mechanisms. One of the most effective instruments in this area is a scanning electron microscope (SEM) from Carl Zeiss that has a unique ability to provide high resolution images of a specimen under investigation. One example of its application of EVO® EP instrument (Carl Zeiss) in manufacture of aspirin. The interaction of water with soluble aspirin demonstrates the mechanisms by which tablets lose mechanical strength and stability and hence release the active material. This process can be observed in real-time in the SEM by introducing water vapor into the chamber at sufficiently high pressures that liquid water is condensed onto the specimen. During the wetting phase the particle absorbs water and fragments. During the drying phase the reverse processes can be followed in detail. The latest product from Carl Zeiss, ULTRA 55 field emission SEM features a totally new "Complete Detection System", which enables simultaneous surface, compositional and crystallographic imaging down to the nanometer level with high signal contrast and unsurpassed clarity.

Use of SEM to Reconstruct 3D Tissue Nanostructure

3D structural information is important in biological research. Excellent methods are available to obtain structures of molecules at atomic, organelles at electron microscopic, and of tissue at light-microscopic resolution. However, there is a need to reconstruct 3D tissue structure with a nanoscale resolution to identify small organelles such as synaptic vesicles. Such 3D data are essential to understand cellular networks that need to be completely reconstructed throughout a substantial spatial volume, particularly in the nervous system. Datasets meeting these requirements can be obtained by automated block-face imaging combined with serial sectioning inside the chamber of a SEM. Backscattering contrast is used to visualize the heavy-metal staining of tissue prepared using techniques that are routine for TEM. The resolution is sufficient to trace even the thinnest axons and to identify synapses. Stacks of several hundred sections, 50–70 nm thick, have been obtained at a lateral position jitter of typically under 10 nm. This opens the possibility of automatically obtaining the electron-microscope-level 3D datasets needed to completely reconstruct the neuronal circuits.

Optical Imaging with a Silver Superlens

A superlens has been created using a thin film of silver as the lens and ultraviolet light that can overcome a limitation in physics that has historically constrained the resolution of optical images. The superlens has been used to record the images of an array of nanowires at a resolution of about 60 nm, whereas current optical microscopes can only make out details down to 400 nm. This work has an impact on the development of detailed biomedical imaging. With current optical microscopes,

scientists can only make out relatively large structures within a cell, such as its nucleus and mitochondria. With a superlens, optical microscopes could reveal the movements of individual proteins traveling along the microtubules that make up a cell's skeleton. SEM and AFM are now used to capture detail down to a few nanometers. However, such microscopes create images by scanning objects point by point, which means they are typically limited to non-living samples, and image capture times can take up to several minutes. Optical microscopes can capture an entire frame with a single snapshot in a fraction of a second, opening up nanoscale imaging to living materials, which can help biologists better understand cell structure and function in real time, and ultimately help in the development of new drugs to treat human diseases.

Partial Wave Spectroscopy

An optical microscopy technique, partial wave spectroscopy (PWS), is capable of quantifying statistical properties of cell structure at the nanoscale. PWS has been used to show for the first time the increase in the disorder strength of the nanoscale architecture not only in tumor cells but also in the microscopically normal-appearing cells outside of the tumor. Although genetic and epigenetic alterations have been previously observed in the field of carcinogenesis, these cells were considered morphologically normal. PWS can show organ-wide alteration in cell nanoarchitecture. This seems to be a general event in carcinogenesis, which is supported by data in three types of cancer: colon, pancreatic, and lung. These results have important implications in that PWS can be used as a new method to identify patients harboring malignant or premalignant tumors by interrogating easily accessible tissue sites distant from the location of the lesion. Once optimized, PWS could be used to detect cell abnormalities early and help physicians assess who might be at risk for developing cancer. Like a pap smear of the cervix, a simple brushing of cells is all that is needed to get the specimen required for testing. PWS can look inside the cell and see those critical building blocks, which include proteins, nucleosomes and intracellular membranes, and detect changes to this nanoarchitecture. Conventional microscopy cannot do this, and other techniques that can (to some degree) are expensive and complex. PWS is simple, inexpensive and minimally invasive.

Photoactivated Localization Microscopy

Photoactivated localization microscopy (PALM) enables scientists peering inside cells to discern individual proteins at nanometer ~2 to 25 nm resolution. The basic concepts behind this technology are simple: The researchers label the molecules they want to study with a photoactivatable probe, and then expose those molecules to a small amount of violet light. The light activates fluorescence in a small

percentage of molecules, and the microscope captures an image of those that are turned on until they bleach. The process is repeated approximately 10,000 times, with each repetition capturing the position of a different subset of molecules. When a final image is created that includes the center of each individual molecule, it has a resolution previously only achievable with an electron microscope. Unlike electron microscopy, however, the new technique allows for more flexibility in labeling molecules of interest. The method is demonstrated in thin sections by imaging specific target proteins in lysosomes and mitochondria, and in fixed, whole cells by imaging vinculin at focal adhesions, actin within a lamellipodium, and the distribution of the retroviral protein Gag at the plasma membrane. A great feature of PALM is that is can be readily used with electron microscopy, which produces a detailed image of very small structures, but not proteins, in cells. By correlating a PALM image showing protein distribution with an electron microscope image showing cell structure of the same sample, it becomes possible to understand how molecules are individually distributed in a cellular structure at the molecular scale. Correlative PALM unites the advantages of light and electron microscopy, producing a revolutionary new approach for looking at the cell in molecular detail. As the PALM technology advances, it may prove to be a key factor in unlocking at the molecular level secrets of intracellular dynamics that are unattainable by other methods. However, the time needed to collect the thousands of single molecule images that go into each PALM picture is cumbersome. With the camera snapping one to two pictures each second, it can take 2-12 h to image a single sample. Activating more molecules per frame would reduce the number images that must be collected, and making the molecules brighter would reduce the time needed to take each image. Either would help to speed the PALM process. The technique is still undergoing refinements with an aim to developing a practical tool for use by biologists.

Scanning Probe Microscopy

The scanning probe microscope (SPM) system is an important tool for non-intrusive interrogation of biomolecular systems in vitro. Its special features are that it retains complete functionality in a biocompatible fluid environment and can track the dynamics of cellular and molecular processes in real time and real space at nm resolution, as an imaging tool, and with pN force-sensing/imposing resolution, as an interaction tool. The capability may have relevance as a test bed for monitoring cellular response to environmental stimuli and pharmaceutical intervention. Best known contributions of SPM are towards explanatory and predictive descriptions of biomolecular interactions at surfaces and interfaces, and there are some attempts to reconfigure the SPM platform for demonstration of novel biodevice applications. SPM enables high resolution without any of the drawbacks of electron microscopy, which can damage sensitive molecules by electrons. SPM enables investigation of biomolecules in fluid environments under physiological conditions and is useful for study of biology on nanoscale.

Scanning ion conductance microscopy is part of the larger family of SPM. It was specially designed for the submicrometer resolution scanning of soft non-conductive materials that are bathed in electrolyte solution. It consists of an electrically charged glass micro- or nanopipette probe filled with electrolyte lowered toward the surface of the sample (which is non-conducting for ions) in an oppositely charged bath of electrolyte. As the tip of the micropipette approaches the sample, the ion conductance and therefore current decreases since the gap through which ions can flow, is reduced in size. It is a suitable tool for imaging surfaces of living cells in a contact-free manner and enables tracing of the outlines of entire cell soma and detection of changes in cellular shape and volume. It can also be used to quantitatively observe cellular structures such as cell processes of living cells and cell soma of motile cells within hours.

Single-Molecule Photon Localization Microscopy

Visualization of nanoscale intracellular structures formed by nucleic acids, such as chromatin, in undisturbed state is important for an understanding of biological processes. Conventional superresolution techniques for visualization of subdiffractional macromolecular structures formed by nucleic acids require labeling, which may disturb cell function, and alter the molecular processes that are to be studied. A photoswitching process of native nucleotides has been investigated and subdiffraction-resolution imaging of cellular structures using intrinsic contrast from unmodified DNA based on the principle of single-molecule photon localization microscopy (PLM) has been demonstrated (Dong et al. 2016). With a demonstrated sub–20-nm resolution, DNA-PLM provides an ideal technique to visualize the spatial organization of single or groups of nucleosomes and quantitatively estimate the nucleosome occupancy level of DNA in unstained chromosomes and nuclei. This study opens a new way for label-free superresolution nanoscopic imaging of macromolecular structures with nucleotide topologies and will contribute to the development of new DNA-based contrast agents for superresolution imaging.

STED Microscopy

The novel stimulated emission depletion (STED) microscopy technique is a process that provides super resolution by selectively deactivating fluorophores to enhance the imaging in that area. Because of its targeted on/off switching of fluorescence, STED is not hampered by a diffraction-limited resolution barrier. STED microscopy can therefore provide much sharper images, permitting nanoscale visualization by sequential imaging of individual labeled biomolecules, which should allow previous findings to be re-investigated and provide novel information. STED makes nanoscale materials and components of the cell accessible for fluorescence-based investigations. With multicolor superresolution imaging, even the interactions between biological and engineered nanostructures can be studied in detail. A review has highlighted promising applications of STED microscopy and their impact on unresolved issues in biomedical science (Blom and Brismar 2014).

A substantial advantage of STED microscopy over other super-resolution methods is that images can be acquired in real-time without any post-processing. However, imaging speed and photodamage are two major concerns for STED imaging of whole cells. A new microscopy method termed Bessel-Beam STED (or BB-STED) has been proposed that overcomes both these limitations of conventional STED microscopy (Zhang et al. 2014). In the proposed method, rather than exciting a single STED spot in the sample, an entire line of the sample is illuminated. This line-scanning technique dramatically increases the speed of STED. In addition, plane-illumination by scanning of the line across the focal plane of a detection objective limits the light to a thin layer of the sample and thus significantly reduces photobleaching and photodamage above and below the focal plane compared to epi-illumination. STED power required to break the diffraction limit has been calculated using the organic dye Atto647N as an example.

Super-Resolution Microscopy for in Vivo Cell Imaging

Normal microscopes enable visualization of cell contents that are >200 nm in size but would be unable to detect very small molecules such as insulin, which is about 10 nm in size. Super-resolution microscopy enables nanoscale observation of cells in vivo. Super-resolution microscopy comprises a variety of new approaches such as Structured Illumination (3D-SIM), Localization Microscopy (PALM, STORM), Stimulated Emission Depletion (STED), and RESOLFT nanoscopy that have been developed to surpass the limits of conventional optical microscopes. These methods allow precise visualization and measurement of features that are below the diffraction limit. In vivo study of cells provides invaluable information for study of pathomechanism of disease at cell level and for cell-based drug discovery. Electron microscopes have similar resolution to a super-resolution microscope, but they do not allow observation of cells in vivo. Exploration of cellular functions at nanoscale enables a better understanding of the processes that occur in a dysfunctional cell. Super-resolution microscopes have been used to study how the HIV virus penetrates cells and provide information for developing new drugs.

3D-Sim

3D-SIM (Applied Precision Inc./GE Healthcare) projects a structured light pattern onto the sample. The illumination pattern interacts with the fluorescent probes in the sample to generate interference patterns know as moiré fringes. By modulating the illumination pattern, collecting and reconstructing the subsequent images, superresolution images with double the lateral and axial resolution are obtained.

Nanomicroscopy for Live Cell Tomography

NanoLive's Cell Explorer's technology enables determination of how light propagates through the cell. Thus, one can measure the cell's physical properties, ie, the refractive index. The result is quantitative cell tomography without any invasion or sample preparation. Non-invasive optical nanoscopy can achieve a lateral resolution of 90 nm by using a holographic detection scheme and complex deconvolution (Cotte et al. 2013). The authors recorded holograms from different illumination directions on the sample plane and observed subwavelength tomographic variations of the specimen. Nanoscale apertures serve to calibrate the tomographic reconstruction and to characterize the imaging system by means of the coherent transfer function. This gives rise to realistic inverse filtering and guarantees true complex field reconstruction. These observations were utilized for nanoscopic porous cell diatoms, for the direct study of bacteria and for a time-lapse approach to explore the dynamics of living neurones. Applications of this technology, which is commercially available, will enable discoveries on living cells and study of diseases as well as effects of drugs at cell level. It will be useful for recording cellular uptake as well as localization of metal nanoparticles and assessments of cell exposure to nanoparticles.

RESOLFT Nanoscopy

The super-resolution microscopy called RESOLFT relying on fluorophore switching between long-lived states stands out by its coordinate-targeted sequential sample interrogation using low light levels. Although RESOLFT has been shown to discern nanostructures in living cells, the reversibly photoswitchable green fluorescent protein (rsEGFP) employed in these experiments was switched rather slowly and recording lasted tens of minutes. Scientists at the Max Planck Institute (MPI) for Biophysical Chemistry in Germany have reported the generation of rsEGFP2 providing faster switching and the use of this protein to demonstrate 25-250 times faster recordings (Grotjohann et al. 2012). They mutated only a few amino acids to produce an EGFP that switches more quickly than previous iterations and showed that the new fluorophore lasts longer, resisting "photofatigue" that wears out fluorescent proteins and leaves them stuck in one state after too many rounds of excitation. The ability to excite fluorophores at lower energy levels and switch quickly between on/off states should allow extremely high resolution imaging of dynamic processes in live cells without risk of damage. MPI's Stefan Hell along with two American scientists – Eric Betzig from the Howard Hughes Medical Institute's Janelia Farm, and Stanford University's William Moerner - were awarded the 2014 Nobel Prize for Chemistry for the development of super-resolved fluorescence microscopy or nanoscopy. Betzig and Moerner, working separately, came up with single-molecule microscopy that relies on turn on and off the fluorescence of individual molecules while an area is scanned multiple times to make a composite picture. The researchers have been applying their approaches to examine brain synapses, proteins involved in Huntington's disease, and cell division in embryos.

Ultra-nanocrystalline Diamond

A common problem in AFM is the deterioration of the tip apex as surfaces are scanned. To overcome this problem, an ultrananocrystalline diamond (UNCD) was used to fabricate a hard, low-wear probe for contact-mode writing techniques such as dip pen nanolithography. Diamond, the hardest known material, is probably the optimal tip material for many applications. In addition to hardness, diamond is stiff, biocompatible and wear resistant. Diamond tips with radii down to 30 nm were obtained through growth of UNCD films followed by selective etching of the silicon template substrate. The probes were monolithically integrated with diamond cantilevers and subsequently integrated into a chip body obtained by metal electroforming. The probes were characterized in terms of their mechanical properties, wear, and atomic force microscopy imaging capabilities. The developed probes performed exceptionally well in DPN molecular writing/imaging mode. Furthermore, the integration of UNCD films with appropriate substrates and the use of directed microfabrication techniques are particularly suitable for fabrication of one- and two-dimensional arrays of probes that can be used for massive parallel fabrication of nanostructures by the dip pen nanolithography method. The technology can be employed for a variety of AFM scanning modes, from regular surface scanning in air or fluids to conductive AFM. It can also be employed as a nanofabrication tool. Examples include nanopatterning of biomolecules (for sequencing, synthesis and drug discovery) and scanning probe electrochemistry (scanning electrode imaging, localized electrochemical etching or deposition of materials and nanovoltametry). Potential markets include those industries where it is pivotal to preserve the performance of the tips or that require two-dimensional arrays for high throughput in which the cost of manufacturing is such that minimum possible tip wear is paramount. These include the chemical and biological sensor industry where high throughput and spatial resolution are important.

Visualizing Atoms with High-Resolution Transmission Electron Microscopy

The characterization of nanostructures down to the atomic scale is essential to understand some physical properties. Such a characterization is possible today using direct imaging methods such as aberration-corrected high-resolution transmission electron microscopy (HRTEM), when iteratively backed by advanced modeling produced by theoretical structure calculations and image calculations. Aberration-corrected HRTEM is therefore extremely useful for investigating low-dimensional structures, such as inorganic fullerene-like particles and inorganic nanotubes. The atomic arrangement in these nanostructures can lead to new insights into the growth mechanism or physical properties, where imminent commercial applications are unfolding. HRTEM study combined with modeling reveals new information regarding the chirality of the different shells and provides a better understanding of their growth mechanism. The next frontier will be seeing atoms in 3D.

Surface Plasmon Resonance

Surface plasmon resonance (SPR) is an optical-electrical phenomenon involving the interaction of light with the electrons of a metal. Light is coupled into the surface plasmon by means of either a prism or a grating on the metal surface. Depending on the thickness of a molecular layer at the metal surface, the SPR phenomenon results in a graded reduction in intensity of the reflected light. The optical-electronic basis of SPR is the transfer of the energy carried by photons of light to a group of electrons (a plasmon) at the surface of a metal.

In Biacore systems (Fig. 2.4), SPR arises when light is reflected under certain conditions from a conducting film at the interface between two media of different refractive index. The media are the sample and the glass of the sensor chip, and the conducting film is a thin layer of gold on the chip surface. SPR causes a reduction in the intensity of reflected light at a specific angle of reflection (the SPR angle). When molecules in the sample bind to the sensor surface, the concentration and therefore the refractive index at the surface changes and an SPR response is detected. Plotting the response against time during an interaction provides a quantitative measure of the progress of the interaction. This plot is called a sensorgram.

Biomedical applications take advantage of the exquisite sensitivity of SPR to the refractive index of the medium next to the metal surface, which makes it possible to measure accurately the adsorption of molecules on the metal surface and their eventual interactions with specific ligands. Applications of this technique include the following:

- · Measurement in real-time of the kinetics of ligand-receptor interactions
- · Screening of lead compounds in the pharmaceutical industry
- Measurement of DNA hybridization
- Enzyme-substrate interactions
- · Polyclonal antibody characterization
- · Protein conformation studies
- Label-free immunoassays.

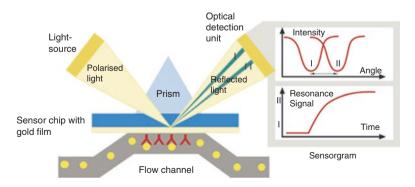


Fig. 2.4 Surface plasmon resonance (SPR) technology

Nanotechnology and Phototherapy

Phototherapy can be used in two completely different but complementary therapeutic applications. While low level laser (or light) therapy uses red or near-infrared light alone to reduce inflammation, pain and stimulate tissue repair and regeneration, photodynamic therapy (PDT) uses the combination of light plus non-toxic dyes (called photosensitizers) to produce reactive oxygen species that can kill infectious microorganisms and cancer cells or destroy unwanted tissue (neo-vascularization in the choroid, atherosclerotic plaques in the arteries). Nanotechnology has opened a new front of advancement in the field of phototherapy and has provided hope for the development of nanoscale drug delivery platforms for effective destruction of pathological cells and to promote repair and regeneration. Despite the well-known beneficial effects of phototherapy and nanomaterials in producing the killing of unwanted cells and promoting repair and regeneration, there are few reports that combine all three elements, i.e. phototherapy, nanotechnology and, tissue repair and regeneration (Gupta et al. 2013).

References

- Algar WR, Tavares AJ, Krull UJ. Beyond labels: a review of the application of quantum dots as integrated components of assays, bioprobes, and biosensors utilizing optical transduction. Anal Chim Acta. 2010;673:1–25.
- Baalousha M, Prasad A, Lead JR. Quantitative measurement of the nanoparticle size and number concentration from liquid suspensions by atomic force microscopy. Environ Sci Process Impacts. 2014;16:1338–47.
- Blom H, Brismar H. STED microscopy: increased resolution for medical research? J Int Med. 2014;276:560–78.
- Bonaccorso F, Colombo L, Yu G, et al. 2D materials. Graphene, related two-dimensional crystals, and hybrid systems for energy conversion and storage. Science. 2015;347:1246501.
- Cardinale D, Carette N, Michon T. Virus scaffolds as enzyme nano-carriers. Trends Biotechnol. 2012;30:369–76.
- Chai J, Wong LS, Giam L, Mirkin CA. Single-molecule protein arrays enabled by scanning probe block copolymer lithography. Proc Natl Acad Sci U S A. 2011;108:19521–5.
- Chatterjee DK, Rufaihah AJ, Zhang Y. Upconversion fluorescence imaging of cells and small animals using lanthanide doped nanocrystals. Biomaterials. 2008;29:937–43.
- Cotte Y, Toy F, Jourdain P, et al. Marker-free phase nanoscopy. Nat Photonics. 2013;7:113-7.
- de Silva AP. Molecular logic gate arrays. Chem Asian J. 2011;6:750–66.
- Degen CL, Poggio M, Mamin HJ, et al. Nanoscale magnetic resonance imaging. Proc Natl Acad Sci U S A. 2009;106:1313–7.
- Dong B, Almassalha LM, Stypula-Cyrus Y, et al. Superresolution intrinsic fluorescence imaging of chromatin utilizing native, unmodified nucleic acids for contrast. Proc Natl Acad Sci U S A. 2016;113:9716–21.
- Dosev D, Nichkova M, Kennedy IM. Inorganic lanthanide nanophosphors in biotechnology. J Nanosci Nanotechnol. 2008;8:1052–67.
- Dragavon J, Blazquez S, Rekiki A, et al. In vivo excitation of nanoparticles using luminescent bacteria. Proc Natl Acad Sci U S A. 2012;109:8890–5.
- Fantner GE, Schumann W, Barbero RJ, et al. Use of self-actuating and self-sensing cantilevers for imaging biological samples in fluid. Nanotechnology. 2009;20:434003.

- Grotjohann T, Testa I, Reuss M, et al. rsEGFP2 enables fast RESOLFT nanoscopy of living cells. elife. 2012;1:e00248.
- Gupta A, Avci P, Sadasivam M, et al. Shining light on nanotechnology to help repair and regeneration. Biotechnol Adv. 2013;31:607–31.
- Hall DA, Wang SX, Murmann B, Gaster RS. Portable biomarker detection with magnetic nanotags. Conf Proc (Midwest Symp Circuits Syst). 2010 (August 3):1779–82.
- Hoskins C, Min Y, Gueorguieva M, et al. Hybrid gold-iron oxide nanoparticles as a multifunctional platform for biomedical application. J Nanobiotechnol. 2012;10:27.
- Jain KK. Nanobiotechnology: applications, markets and companies. Basel: Jain PharmaBiotech Publications; 2017.
- Kannan P, Los M, Los JM, Niedziolka-Jonsson J. T7 bacteriophage induced changes of gold nanoparticle morphology: biopolymer capped gold nanoparticles as versatile probes for sensitive plasmonic biosensors. Analyst. 2014;139:3563–71.
- Karami Z, Hamidi M. Cubosomes: remarkable drug delivery potential. Drug Discov Today. 2016;21:789–801.
- Koltonow AR, Huang J. Two-dimensional nanofluidics. Science. 2016;351:1395-6.
- Liu Q, Han M, Bao J, et al. CdSe quantum dots as labels for sensitive immunoassay of cancer biomarker proteins by electrogenerated chemiluminescence. Analyst. 2011;136:5197–203.
- May F, Peter M, Hütten A, et al. Synthesis and characterization of photoswitchable fluorescent SiO(2) nanoparticles. Chemistry. 2012;18:814–21.
- Michen B, Geers C, Vanhecke D, et al. Avoiding drying-artifacts in transmission electron microscopy: characterizing the size and colloidal state of nanoparticles. Sci Rep. 2015;5:9793.
- Nayak TR, Andersen H, Makam VS, et al. Graphene for controlled and accelerated osteogenic differentiation of human mesenchymal stem cells. ACS Nano. 2011;5:4670–8.
- Nyk M, Kumar R, Ohulchanskyy TY, et al. High contrast in vitro and in vivo photoluminescence bioimaging using near infrared to near infrared up-conversion in Tm(3+) and Yb(3+) doped fluoride nanophosphors. Nano Lett. 2009;8:3834–8.
- Osterfeld SJ, Yu H, Gaster RS, et al. Multiplex protein assays based on real-time magnetic nanotag sensing. Proc Natl Acad Sci U S A. 2008;105:20637–40.
- Petersen S, Soller JT, Wagner S, et al. Co-transfection of plasmid DNA and laser-generated gold nanoparticles does not disturb the bioactivity of GFP-HMGB1 fusion protein. J Nanobiotechnol. 2009;7:6. doi:10.1186/1477-3155-7-6.
- Qian H, Zhu Y, Jin R. Atomically precise gold nanocrystal molecules with surface plasmon resonance. Proc Natl Acad Sci U S A. 2012;109:696–700.
- Santos HA, Mäkilä E, Airaksinen AJ, et al. Porous silicon nanoparticles for nanomedicine: preparation and biomedical applications. Nanomedicine (Lond). 2014;9:535–54.
- Sekula-Neuner S, Maier J, Oppong E, et al. Allergen arrays for antibody screening and immune cell activation profiling generated by parallel lipid dip-pen nanolithography. Small. 2012;8:585–91.
- Smith D, Schüller V, Engst C, et al. Nucleic acid nanostructures for biomedical applications. Nanomedicine (Lond). 2013;8:105–21.
- Thompson DG, McKenna EO, Pitt A, Graham D. Microscale mesoarrays created by dip-pen nanolithography for screening of protein-protein interactions. Biosens Bioelectron. 2011;26: 4667–73.
- Tung NH, Chikae M, Ukita Y, et al. Sensing technique of silver nanoparticles as labels for immunoassay using liquid electrode plasma atomic emission spectrometry. Anal Chem. 2012;84: 1210–3.
- von Diezmann A, Lee MY, Lew MD, Moerner WE. Correcting field-dependent aberrations with nanoscale accuracy in three-dimensional single-molecule localization microscopy. Optica. 2015;2(11):985–93.
- Wang X, Ramström O, Yan M. Dye-doped silica nanoparticles as efficient labels for glycans. Chem Commun (Camb). 2011;47:4261–3.
- Xie H, Li YF, Kagawa HK, et al. An intrinsically fluorescent recognition ligand scaffold based on chaperonin protein and semiconductor quantum-dot conjugates. Small. 2009;5:1036–42.

- Xie Y, Akada M, Hill JP, et al. Real time self-assembly and reassembly of molecular nanowires of trigeminal amphiphile porphyrins. Chem Commun (Camb). 2011;47:2285–7.
- Xue Q, Wang L, Jiang W. A versatile platform for highly sensitive detection of protein: DNA enriching magnetic nanoparticles based rolling circle amplification immunoassay. Chem Commun (Camb). 2012;48:3930–2.
- Yang S, Damiano MG, Zhang H, et al. Biomimetic, synthetic HDL nanostructures for lymphoma. Proc Natl Acad Sci U S A. 2013;110:2511–6.
- Zavaleta CL, Smith BR, Walton I, et al. Multiplexed imaging of surface enhanced Raman scattering nanotags in living mice using noninvasive Raman spectroscopy. Proc Natl Acad Sci U S A. 2009;106:13511–6.
- Zeltins A. Construction and characterization of virus-like particles: a review. Mol Biotechnol. 2013;53:92–107.
- Zhang M, Viennois E, Xu C, Merlin D. Plant derived edible nanoparticles as a new therapeutic approach against diseases. Tissue Barriers. 2016;4:e1134415.
- Zhang P, Goodwin PM, Werner JH. Fast, super resolution imaging via Bessel-beam stimulated emission depletion microscopy. Opt Express. 2014;22:12398–409.
- Zhang Y, Hong H, Cai W. Imaging with Raman spectroscopy. Curr Pharm Biotechnol. 2010; 11:654–61.

Chapter 3 Nanotechnologies for Basic Research Relevant to Medicine

Introduction

Life sciences are the testing ground for many new biotechnologies for applications in medicine. Nanobiotechnology is a good example. Despite the remarkable speed of development of nanoscience, relatively little is known about the interaction of nanoscale objects with living systems. Much of the research in life sciences is directly relevant to applications described in the following chapters. Because of this overlap some of the applications are indicated in this chapter and some of the research in life sciences is described along with applications. Important areas of research in life sciences where nanotechnologies are applied and that are relevant to applications in health sciences are:

- Role of nanotechnology in biological research
- Genomics and proteomics
- Gene sequencing
- Bioinformatics
- Assays

Nanotechnology and Biology

Investigative methods of nanotechnology have made inroads into uncovering fundamental biological processes, including self-assembly, cellular processes, and systems biology (such as neural systems). Key advances have been made in the ability to make measurements at the subcellular level and in understanding the cell as a highly organized, self-repairing, self-replicating, information-rich molecular machine. Single-molecule measurements are shedding light on the dynamics and mechanistic properties of molecular biomachines, both in vivo and in vitro, allowing the direct investigation of molecular motors, enzyme reactions, protein dynamics, DNA transcription and cell signaling. It has also been possible to measure the chemical composition within a single cell in vivo. Micro total analysis systems, using molecular manipulation on nanoscale, offer the potential for highly efficient, simultaneous analysis of several biologically important molecules in genomic, proteomic and metabolic studies.

The physical sciences offer tools for synthesis and fabrication of devices for measuring the characteristics of cells and sub-cellular components, and of materials useful in cell and molecular biology; biology offers a window into the most sophisticated collection of functional nanostructures that exists. Particles made of semiconductors at the nanoscale are already used in the electronic and information technology industries. For example, the active part of a single transistor on a Pentium silicon chip is a few tenths of a nanometer in size. The semiconductor laser used to read digital information on a CD or DVD has an active layer of similar dimensions. Creating the ability to import such electronic functions into the cell and meshing them with biological functions could open tremendous new possibilities, both for basic biological sciences and for medical and therapeutic applications. For QDs are used by life science researchers as tiny beacons or biomarkers, allowing them to easily see individual genes, nucleic acids, proteins or small molecules.

NanoSystems Biology

Systems biology is defined as the biology of dynamic interacting networks. It is also referred to as pathway, network, or integrative biology. An analysis of the structure and dynamics of network of interacting elements provides insights that are not obvious from analysis of the isolated components of the system. Proteomics plays an important role in systems biology because most biological systems involve proteins. Systems biology is providing new challenges for advancing science and technology. Analyses of pathways may provide new insight into the understanding of disease processes, developing more efficient biomarkers and understanding mechanisms of action of drugs.

NanoSystems biology is the application of nanobiotechnology, microfluidics, and molecular imaging methods, in the study of systems biology. It will play an important role in understanding biology of disease by:

- · Providing refined tools for the study of proteomics
- Nanotechnology provides real-time single particle tracing in living cells.
- Nanotechnology will facilitate dissecting of signaling pathways.

The goal of NanoSystems Biology is to develop a suite of nanotechnology tools – ranging from integrated microfluidics to nanoelectronics to nanomechanical devices – that will enable a large-scale, systems-biology driven, multiparameter analysis within a clinical setting – i.e. every patient, every visit. Such an analysis constitutes an 'informative diagnosis' of disease. Nanobiosensors are currently being developed for cancer biomarkers for early detection of the disease.

Nanobiology and the Cell

It is perhaps superfluous to use the term 'nanobiology' because cell is the smallest unit alive. Molecules in the cell are organized in nanometer scale dimensions. Visualizing the dynamic change in these molecules and studying the function of cells is one of the challenges in nanobiology. A single molecule is the ultimate nanostructure. Single molecule microscopy and spectroscopy are some of the techniques used to study single molecules.

The objective is to gain a detailed knowledge about biochemical processes occurring locally in the cell nucleus, which is a prerequisite for a comprehensive understanding of genome function. The combination of a resolution range of a few nanometers, high penetrating power, analytical sensitivity, and compatibility with wet specimens allows x-ray microscopy and scanning x-ray microscopy of whole cells. The spatial resolution of 20 nm reached up to now is much better than that of current conventional light microscopes. To further our understanding of chromosome biology and nuclear function, it is essential to develop techniques that enable the measurement of structures inside the living cell with a spatial resolution down to the scale of 10 nm.

The ability to work with an individual cell using nanotechnology is very promising and there are already several research groups working on this. The single cell is an ideal sensor for detecting various chemical and biochemical processes, and the genetic manipulation of cells could be better done through mechanical rather than biochemical means.

Using a water droplet as a sort of nanoscale test tube, analysis and experimentation has been done at unprecedented tiny scales (Chiu 2010). The microfluidic device captures a single cell, or even a small subcellular structure called an organelle, within a droplet. The device has water in one channel and oil in an adjoining channel. The target is placed at the interface between the oil and water so the target is encapsulated as the water droplet is formed. It then employs a powerful laser microscope to study the contents and examine chemical processes, and a laser beam is used to manipulate the cell or even just a few molecules, combining them with other molecules to form new substances. This nanoscale laboratory enables one to do an experiment in the droplet on one cell or even a few molecules. The new approach makes it easier to get a wide range of information about a cell and to study structure and form simultaneously.

Biosensing of Cellular Responses

Cells represent the minimum functional and integrating communicable unit of living systems. Cultured cells both transduce and transmit a variety of chemical and physical signals, i.e., production of specific substances and proteins, throughout their life cycle within specific tissues and organs. Such cellular responses might be usefully employed as parameters to obtain chemical information for both pharmaceutical

and chemical safety, and drug efficacy profiles in vitro as a screening tool. However, such cellular signals are very weak and not easily detected with conventional analytical methods. By using micro- and nanobiotechnology methods integrated on-chip, a higher sensitivity and signal amplification has been developed for cellular biosensing. Nanotechnology is rapidly evolving to open new combinations of methods with improved technical performance, helping to resolve challenging bioanalytical problems including sensitivity, signal resolution and specificity by interfacing these technologies in small volumes to confirm specific cellular signals. Integration of cell signals in both rapid time and small space, and importantly, between different cell populations (communication and systems modeling) will permit many more valuable measurements of the dynamic aspects of cell responses to various chosen stimuli and their feedback. This represents the future for cell-based biosensing.

Genetically encoded nanosensors have been developed to monitor glutamate levels inside and at the surface of living cells using the fluorescent indicator protein for glutamate (FLIPE), which consists of the glutamate/aspartate binding protein ybeJ from *Escherichia coli* fused to two variants of the green fluorescent protein. Such sensors respond to extracellular glutamate with a reversible concentration-dependent decrease in FRET efficiency. FLIPE nanosensors can be used for real-time monitoring of glutamate metabolism in living cells, in tissues, or in intact organisms, providing tools for studying metabolism or for drug discovery.

Single cell imaging of sodium dynamics has been limited due to the narrow selection of fluorescent sodium indicators that are available currently. Fluorescent nanosensors that measure sodium in real-time have been used for the detection of spatially defined sodium activity during action potentials in cells. They are reversible and are completely selective over other cations such as potassium that were used to image sodium previously. The use of the nanosensors in vitro has been validated by determining drug-induced activation in heterologous cells transfected with the voltage-gated sodium channel NaV1.7. Spatial information of sodium concentrations during action potentials will provide insight at the cellular level on the role of sodium and how slight changes in sodium channel function can affect the entirety of an action potential. Regulation of sodium flux across the cell membrane plays a vital role in the generation of action potentials and regulation of sodium channel function has been implicated in diseases such as epilepsy, long QT syndrome, and heart failure.

Control of T Cell Signaling Activity

The immunological synapse is a specialized cell-cell junction that is defined by large-scale spatial patterns of receptors and signaling molecules yet remains largely enigmatic in terms of formation and function. The marriage of inorganic nanotechnology with organic molecules and cells enables the scientists to go inside a living cell and physically move around its signaling molecules with molecular precision.

Supported bilayer membranes and nanometer-scale structures fabricated onto the underlying substrate have been used to directly control T cell signaling activity. Analysis of the resulting alternatively patterned synapses reveals a causal relation between the radial position of T cell receptors (TCRs) and signaling activity, with prolonged signaling from TCR microclusters that had been mechanically trapped in the peripheral regions of the synapse. These results are consistent with a model of the synapse in which spatial translocation of TCRs represents a direct mechanism of signal regulation.

Measuring Mass of Single Cells

A silicon cantilever mass sensor has been used to measure the mass of single cells with high accuracy (Park et al. 2008). HeLa cells were injected into microfluidic channels were subsequently captured on the cantilevers and then cultured in a microfluidic environment. The resonant frequencies of the cantilevers were measured. The mass of a single HeLa cell was extracted from the resonance frequency shift of the cantilever and was found to be close to the mass value calculated from the cell density from the literature and the cell volume obtained from confocal microscopy. This technique could enable development of inexpensive, portable diagnostic devices and might also offer a unique glimpse into how cells change as they undergo cell division. Unlike conventional methods, this technique allows cells to remain in fluid while they are being measured, opening a new realm of possible applications. In addition to weighing cells, the technology can be used to "weigh nanoparticles or sub-monolayers of biomolecules with a resolution in solution that is six orders of magnitude more sensitive than commercial mass sensor methods. One application is mass-based flow cytometry, a way to weigh and count specific cells.

Nanostructures Involved in Endocytosis

Electron microscopy has been used to uncover new structures, 40 nm in size, which are involved in the very first step of particle and nutrient uptake into cells. Cells require a constant flux of nutrients and other chemicals for survival and it is vitally important to understand how these materials reach the inside of the cell. Endocytosis, the process of regulated uptake by the cell, is vitally important as it occurs continuously and a cell virtually consumes its entire covering every 30 min. Endocytosis can be hijacked by viruses to enter the cell and so understanding this process can provide avenues to stop some viral infections. In addition, endocytosis can be used to deliver drugs into cells. The discovery of this pathway presents unexplored avenues for the development of new drugs to fight certain viral infections, as well as opening new possibilities for gene therapy.

Clathrin-mediated endocytosis (CME) plays a fundamental role in many cellular activities including receptor down-regulation, nutrient uptake and maintenance of

signal transmission across nerve cell junctions. Disturbances in CME are implicated in cancer and neurodegenerative diseases. Live cell imaging and a novel fluorescence assay have been used to visualize the formation of clathrin-coated vesicles at single clathrin-coated pits (CCP) with a time resolution of seconds. This reveals how proteins linked to the actin, a part of the molecular motor, are transported to sites of coated pit. Disturbing actin polymerization with the toxin latrunculin B, a toxin found in Red Sea sponge, drastically reduces the efficiency of membrane scission and affects many aspects of CCP dynamics. The novel assay used in this study can be applied for drug screening. It has been shown that particles in the size range of tens to hundreds of nanometers can enter or exit cells via wrapping even in the absence of clathrin or caveolin coats, and an optimal particles size exists for the smallest wrapping time.

Nanoparticles for In Vivo Study of Cells

Nanoparticles (NPs) can be used as probes for characterizing cellular events both in vitro and in vivo, e.g., they are used for in situ visualization of molecular biomarkers on the cell surface to monitor cellular behaviors in real time (Liu et al. 2016). The clinically relevant probes can be functionalized to engage cellular receptors and trigger internalization. AuNPs have been widely used as cellular probes and their surface-enhanced Raman spectroscopy-based imaging enables localized cellular biochemical analysis. The adhesion and uptake of NPs are largely influenced by their surface modification. For example, negative surface charged AuNPs have higher cell internalization ability than negative ones in nonphagocytic cells, while uptake extent of negatively charged AuNPs was similar with that of the positively charged AuNPs when in phagocytic cells.

Nanotechnology-Based Live-Cell Single Molecule Assays

Advances in nanotechnology are being harnessed to analyze individual cells. Many enzymatic reactions in the cell are coupled, i.e. the product of one enzyme is passed on for use by the nearest enzyme to form a complex network, which functions somewhat like an assembly line. In these networks, proper functioning and control is provided by both space and time parameters. Many traditional techniques for analysis require "fixing" cell samples prior to analysis. This process often destroys the precise intracellular architecture governing the network. Thus, the rate of a biochemical reaction occurring in a test tube could be quite different from that observed for the same reaction inside a cell. DNA, mRNA and some proteins exist in low numbers within cells, making them difficult to detect because they often remain hidden among all the other molecules. Measuring gene and protein expression levels may involve detecting a single molecule when an individual cell is used as the reaction vessel.

Quantum Dots for Stem Cell Labeling

Mesenchymal stem cells (MSCs) can differentiate into bone, -cartilage, adipose, and muscle cells. Adult MSCs are being investigated because of their potential to be used for cell-based transplantation. Methods for tracking MSCs in vivo are limited, limiting long-term functional studies of transplanted cells. Quantum dots (QDs), which are resistant to chemical and metabolic degradation, are an alternative to organic dyes and fluorescent proteins for labeling and tracking stem cells in vitro as well as in vivo. A technique to label MSCs with QDs and demonstrate intracellular QD distribution in the labeled MSCs with laser scanning confocal fluorescent microscopy has been described (Collins et al. 2012). This could provide an innovative tool for noninvasive in vivo imaging of stem cell therapy.

Quantum Dot/Antibody Conjugates for In Vivo Cytometric Imaging

In vivo cytometric imaging requires novel stable fluorophore conjugates that have an appropriate size for prolonged circulation and diffusion with no nonspecific binding to cells/serum while binding to cells of interest with high specificity. This can be achieved by use of biocompatible conjugates measuring ~15 nm in hydrodynamic diameter, which were developed by coupling whole monoclonal antibodies (MAbs) to QDs coated with norbornene-displaying polyimidazole ligands using tetrazine-norbornene cycloaddition (Han et al. 2015). These QD-MAb immunoconstructs were used for in vivo single-cell labeling in bone marrow. The intravital imaging studies using a chronic calvarial bone window showed that QD-MAb conjugates diffuse into the entire bone marrow and efficiently label single cells belonging to rare populations of hematopoietic stem and progenitor cells. This in vivo cytometric technique may be useful in a wide range of structural and functional imaging to study the interactions between cells and between a cell and its environment in intact and diseased tissues.

Quantum Dots for Study of Apoptosis

Apoptosis (programmed cell death) is characterized by multiple biochemical and morphological changes in different organelles, including nuclei, mitochondria and lysosomes. It is the dynamics of the spatio-temporal changes in the signaling and morphological adaptations which will ultimately determine the 'shape' and fate of the cell. 3D reconstruction of nuclei and intracellular lipid peroxidation in cells exposed to oxidative stress induced by QDs enables a study of this process. This approach is also applicable more generally to investigating changes in organelle morphology in response to therapeutic interventions, stressful stimuli and internalized nanoparticles. Moreover, the approach provides quantitative data for such changes, which will help us to better integrate compartmentalization of subcellular events and to link morphological and biochemical changes with physiological outcomes.

Ribosome as a Brownian Nanomachine

A Brownian machine, a tiny device buffeted by the random motions of molecules in the environment, can exploit these thermal motions for many of the conformational changes in its work cycle. Such machines are now thought to be ubiquitous, with the ribosome, a molecular machine responsible for protein synthesis, increasingly regarded as a prototype. An analytical approach has been used for determining the free-energy landscape and the continuous trajectories of molecular machines from several snapshots obtained by cryogenic electron microscopy (Dashti et al. 2014). The authors demonstrated this approach in the context of experimental images of a large ensemble of nontranslating ribosomes purified from yeast cells. The freeenergy landscape is seen to contain a closed path of low energy, along which the ribosome exhibits conformational changes known to be associated with the elongation cycle. This approach enables model-free quantitative analysis of the degrees of freedom and the energy landscape underlying continuous conformational changes in nanomachines, including those important for biological function.

Single Cell Injection by Nanolasers

The problem with previous methods of single-cell injection by nanolasers was low cell viability and low efficacy. To refine this procedure, transient membrane permeabilization of single living bovine aortic endothelial cells (BAEC) was studied as an effect of the incident laser intensity focused femtosecond (1 billionth of 1 millionth of a second) near-infrared laser pulses that created a pore or opening in the cellular wall of living cells and encouraged the cell to take in different molecules (Peng et al. 2007). The rate of dye uptake by the cells was analyzed using time-lapse imaging. Membrane permeabilization occurs for laser intensities higher than 4.0×1012 W/cm². For laser intensity above 3.3×1013 W/cm² the cell disintegrates. Within these two limits the rate of dye uptake increases logarithmically with increasing laser intensity. This functional dependence is explained by considering the Gaussian intensity distribution across the laser focal spot. Cell membrane permeabilization is explained by the creation of plasma within the laser focal spot. The physical understanding of the relationship between dye uptake, pore characteristics, and laser intensity allows control of the concentrations of molecules delivered into cells through the control of pore characteristics. The findings could serve as a set of guidelines for future research that requires precise microinjection of live single cells. The technique will enable researchers to use unprecedented precision to microinject cells or even perform nanosurgery on cells.

Study of Complex Biological Systems

Nanotechnology holds great promise for the analysis of complex processes inside living cells. It is anticipated to provide new tools to study the responses of different naturally occurring and genetically altered cell types and extend the approaches for monitoring cell behavior and activity in embryos, differentiated tissues, and organs as well as physiological systems. In addition to biological sensors that will be able to measure single molecule behavior, nanodevices are presently being developed that can be used to relocate various components inside the cell nucleus. This will allow different regions in the nucleus to be probed and manipulated to study various processes, such as their permissiveness for transcription. This will likely open direct approaches for investigating structure-function relationships by perturbing the local organization of the genome and determining its effect on function. A most promising method for nanomanipulation in living cells is the use of magnetic nanoparticles that are microinjected into the nucleus of living cells. Such particles can be functionalized by the covalent attachment of selected molecules, e.g., specific proteins. Recently developed magnetic tweezers, in combination with high-resolution microscopy, would allow one to move such nanoparticles at will inside living cells, thereby changing local genome structure. Nanoprobes in the nucleus could be used to monitor changes in chromosome arrangement associated with changes in gene expression.

The study of complex biological systems requires methods to perturb the system in complex yet controlled ways to elucidate mechanisms and dynamic interactions, and to recreate in vivo conditions in flexible in vitro set-ups. Nanotechnologies have been applied to the study of complex biological systems and provide advantages in these two areas. They are particularly useful for controlling the chemical and mechanical microenvironments of cells is a set of techniques called soft lithography, whereby elastomeric materials are used to transfer and generate micro- and nanoscale patterns. Examples of some of the capabilities of soft lithography include the use of elastomeric stamps to generate micropatterns of protein and the use of elastomeric channels to localize chemicals with subcellular spatial resolutions. These nanotechnologies combined with mathematical modeling will considerably improve our understandings of cellular and subcellular physiology.

Tissue-Engineering for Studying Effects of Nanoparticles on Cells

Tissue-engineered constructs have been investigated as a platform for providing doses of nanoparticles over different exposure periods to cells within a 3D environment that can be tuned to mimic in vivo conditions (Mansfield et al. 2014). Uptake of QDs by model neural cells was first investigated in a high-dose exposure scenario, resulting in a strong concentration-dependent uptake of carboxyl-functionalized QDs. PEG hydrogel scaffolds with varying mesh sizes were then investigated for their ability to support cell survival and proliferation. Cells were co-encapsulated with carboxyl-functionalized PEG-coated QDs at a lower dose than is typical for monolayer cultures. Although the QDs leach from the hydrogel within 24 h, they are also incorporated by cells within the scaffold, enabling the use of these constructs in future studies of cell behavior and function. Thus, hydrogel tissue scaffolds can be a "powerful bridge" between current laboratory in vitro tests and in vivo tests that use animal models. The scaffold does not require exposing cells to nanoparticles in doses that exceed normal exposure levels, providing a more

representative scenario for evaluating biological effects. In addition, the scaffolds will enable studies of how these interactions evolve over time and of how the physical features of nanoparticles may change.

Molecular Motors

A molecular-level machine may be defined as an assembly of several molecules that are designed to perform movements. Molecular self-assembly is an important route toward the construction of artificial molecular-level devices. These devices are characterized by the energy source, the nature of the movement, the way it may be controlled, its repeatability, its purpose, and the time scale of the nanometer-scaled conformational changes. They play an important role in cell function.

A remarkable little rotary motor located at the base of every flagellum of *E. coli* bacteria, which spins to propel the organism, is being studied. This remarkable device is driven by proton gradients, has its own shaft seals through the cell membrane, can achieve ~50% efficiency, and can spin bidirectionally up to a couple thousand rpm. A microrotary motor, composed of a 20- μ m-diameter silicon dioxide rotor driven on a silicon track by the gliding bacterium *Mycoplasma mobile*, is fueled by glucose and inherits some of the properties normally attributed to living systems.

Every cell in the body has "a dynamic city plan" comprised of molecular highways, construction crews, street signs, cars, fuel and exhaust. Maintenance of this highly organized structure is fundamental to the development and function of all cells and much of it can be understood by figuring out how the functional units in the cell, molecular motors or biological nanomachines, do the work to keep cells orderly. Their function depends on catalytic activity of their constituent proteins. The miniature motor that drives our cells is the enzyme ATP synthase that converts food or light into ATP, the energy currency of the cell. Spinning at several thousand revolutions per minute, the detailed internal workings of the tiny motor are tough to decipher high-speed imaging has been used to snap freeze-frames of the spinning shaft. Linear micromotors that move the cell, voltage-gated ion channels, DNA replication complexes and countless other structures are quite complex and their functions are still not well understood. Lasers, detectors, and optics have been used to study how two protein machines, myosin and kinesin, move about in vitro. The results show how multiple motors compete for activity on their protein scaffolds. Kinesin and another motor, dynein, operate in large groups to produce more than ten times the speed that is expected from a single molecule. Use of a technique called Fluorescence Imaging with One Nanometer Accuracy (FIONA), which has a spatial resolution of 1.5 nm, show that myosin V, kinesin, and myosin VI, all move in handover-hand fashion. Further studies with FIONA have shown that average step size is ~8 nm for both dynein and kinesin, which work together rather than against each other in vivo, producing up to ten times the in vitro speed.

One of the unknowns about dynein is that the molecular site where chemical energy is initially released from ATP is very far away from where the mechanical force occurs and how the mechanical force was transmitted over a large distance. A variety of modeling techniques that allow resolution at the level of atoms, has enabled identified of a flexible, spring-like "coiled-coil" region within dynein, which couples the motor protein to the distant ATP site. It allows a very rapid transduction of chemical energy into mechanical energy. Conversion to mechanical energy allows dynein to transport cellular structures such as mitochondria that perform specific jobs such as energy generation, protein production and cell maintenance. Dynein also helps force apart chromosomes during cell division. Although the research offers no immediate application to human disease, the authors noted that mutations of dynein have been implicated in some neurodegenerative and kidney disorders. Disruption of dynein's interaction with a regulator protein causes defects in nerve cell transmission and mimics the symptoms of patients with amyotrophic lateral sclerosis.

Proteins that function as molecular motors are surprisingly flexible as well as agile, and can navigate obstacles within the cell. These properties could lead to better ways to treat motor neuron diseases such as amyotrophic lateral sclerosis. Using a specially-constructed microscope that enables observation of the action of one macromolecule at a time, reveals that a protein motor can move back and forth along a microtubule – a molecular track – rather than in one direction. The proteins in this motor, dynein and dynactin, are the "long-distance truckers" of the cell: working together, they are responsible for transporting cellular cargo from the periphery of a cell toward its nucleus. Mutation in dynactin leads to degeneration of motor neurons, the hallmark of motor neuron disease. A mutation decreases the efficiency of the dynein-dynactin motor in "taking out the trash" of the cell, and thus leads to the accumulation of misfolded proteins in the cell, which may in turn lead to the degeneration of the neuron.

Another type of molecular motor provides the rigidity needed by the tiny sensors in the inner ear to respond to sound. This motor creates the proper amount of tension in the sensors and anchors itself to maintain that tension. A motor able to create structural changes by taking up slack in proteins and clamping down so that they remain in a rigid position may help explain many intricacies of cellular organization, such as how chromosomes line up and separate during cell division. Molecular motors called myosins are proteins that carry out cellular motion by attaching to and "walking" along fibers of actin. The interaction of actin and myosin is the mechanism behind cell actions such as muscle contractions, the pinching of two daughter cells from a mother cell during division and the hauling of cargo molecules around in a cell. Of the various types of myosin molecules, myosin VI is responsible for setting the tension for stereocilia - actin-filled rods on the sound-sensing hair cells of the inner ear. A defect in myosin VI results in deafness. Although it was known that myosin moves along actin fibers, it had never previously been demonstrated how myosin could function as an anchor or a clamp. Optical tweezers, a focused laser that allows the manipulation of microscopic beads, enables observation of a single molecule and how it behaves, but there are very few proteins in biology that have been analyzed and understood down to this level. Such studies to provide an understanding of the biological nanostructures would be stimulating for nanobiotechnology.

Designers of nanomachines can learn much from nanobiology as many nanostructures in biology can be used as tools in nanobiotechnology.

Biological molecular motors have several unique advantages over artificial motors, including efficient conversion of chemical energy into mechanical work and the potential for self-assembly into larger structures, as is seen in muscle sarcomeres and bacterial and eukaryotic flagella. The development of an appropriate interface between such biological materials and synthetic devices should enable us to realize useful hybrid micromachines. When the scientists discover how to design and mass-produce molecular motors artificially, it will be a major stride in the era of nanotechnology.

Nanomotor Made of Nucleic Acids

Although protein machines are abundant in biology, it has recently been proposed that nucleic acids could also act as nanomolecular machines in model systems. Several types of movements have been described with DNA machines: extension-contraction movement, rotation and "scissors-like" opening and closing. The simple and robust device described is composed of a single 21-base oligonucleotide and relies on a duplex-quadruplex equilibrium that may be fueled by the sequential addition of DNA single strands, generating a DNA duplex as a by-product. The interconversion between two well-defined topological states induces a 5-nm two-stroke, linear motor-type movement, which is detected by fluorescence resonance energy transfer spectroscopy. This system could be used to obtain precise control of movements on the nanometer scale.

Nucleic acids are increasingly used to build nanometer-scale structures that may be used in future nanotechnology devices. There are two key goals in this area: to perform controlled mechanical movements, and to produce complex structures from simple molecular building blocks. Several areas, such as error correction and scaledup self-assembly, require special attention if the potential of nucleic acid-based nanotechnology is to be fulfilled.

A DNA nanomechanical device enables the positional synthesis of products whose sequences are determined by the state of the device. Such a machine can emulate the translational capabilities of the ribosome. Ribosomes are miniature biological machines that weld together amino acids to form the enzymes that modulate body chemistry and the structural materials, like collagen. DNA was twisted and bent to build a structure that is approximately 110 nm long, 30 and 2 nm thick, roughly the same size as a ribosome, though not as complex. The DNA machine can swivel into four geometric positions and can be locked into any one of them by another fragment of DNA, which provides the instructions. Locking the machine into position dials in the sequence of very short DNA strands that it recognizes and positions for welding. The welding itself is performed by an enzyme that links DNA molecules. In the absence of the machine, this enzyme would create many different combinations of DNA strands; in its presence, only a single, preprogrammed combination results. The device has potential applications that include designer polymer synthesis, encryption of information, and use as a variable-input device for DNA-based computation.

phi29 DNA Packaging Nanomotor

The condensation of bacteriophage (a virus that infects bacteria) phi29 genomic DNA into its preformed procapsid requires the DNA packaging motor, which is the strongest known biological motor. The virus uses the motor to package DNA and move it into the capsid, a shell made of proteins, as part of the viral reproduction process. The packaging motor is an intricate ring-shaped protein/RNA complex, and its function requires an RNA component called packaging RNA (pRNA). Current structural information on pRNA is limited, which hinders studies of motor function. Site-directed spin labeling has been used to map the conformation of a pRNA 3-way junction that bridges binding sites for the motor ATPase and the procapsid (Zhang et al. 2012). The studies were carried out on a pRNA dimer, which is the simplest ring-shaped pRNA complex and serves as a functional intermediate during motor assembly. The studies establish a new method for mapping global structures of complex RNA molecules, and provide information on pRNA conformation that aids investigations of phi29 packaging motor and developments of pRNA-based nano-medicine and nanomaterial.

The controllable DNA-packaging nanomotor has been constructed and is driven by synthetic ATP-binding pRNA monomers. When fed a supply of ATP fuel, the RNA strands kick against the axle in succession, much like pistons in a combustion engine. This phenomenon explains how RNA powers viral assembly. The nanomotor can stuff DNA into a protein shell and can be turned on and off. The motor components form regular arrays, which have potential applications in medicine and nanotechnology. Fusing pRNA with receptor-binding RNA aptamer, folate, short interfering RNA (siRNA), ribozyme, or another chemical group does not disturb dimer formation or interfere with the function of the inserted moieties. The motor pRNA can deliver siRNA, ribozyme or other therapeutic molecules to specific cells and destroy them. This has been demonstrated in various cancer cells as well as in cells infected with hepatitis B virus. The use of such a nanomotor/pRNA/siRNA complex could extend the short half-life of therapeutic small molecules in vivo and overcome the delivery problems of molecules larger than 100 nm.

The nanoscale size range of phi29 motor is ideal for delivery inside the body. Anything smaller would be filtered out through the kidneys too quickly to be effective, and larger molecules would not be able to enter cells. The nanomotor can be attached to a lipid sheet, cell membrane and liposome, which would take the place of the capsid into which the phi29 biological motor pumps DNA. The nanomotor, once embedded into the outer wall of the liposome or cell membrane, would pump DNA, drugs or other therapeutic molecules into the liposome pocket's open space, or directly into the cell through a controlled mechanism. The long-term goal is to place thousands of nanomotors in an array assembled on a porous surface, such as silicon, and to have them function for use in biosensing. Nanomotors are being studied further for potential use in the diagnosis and treatment of diseases such as cancer, AIDS, hepatitis B and influenza. Nanomotors will be used to package and deliver therapeutic DNA or RNA to disease-causing cells. The aim is to create a medical tool using a device that mimics a natural biological structure. This biomimetic tool will be a hybrid of natural biological structures and synthetic structures that will operate on the nanoscale.

Light-Activated Ion Channel Molecular Machines

Light-regulated molecular machines, such as the SPARK (synthetic photoisomerizable azobenzeneregulated K^+) channels may also have applications in nanobiotechnology. A molecular tether that attaches to the ion channel can change its shape when exposed to different wavelengths of light. The tether's long form will block the channel, but its short form will leave the channel open. When open, these channels allow positively charged ions to flow out of the neuron, which silences its activity. These engineered channels improve on previous attempts to selectively manipulate activity in a set of neurons and can used for rapid, reversible and precise silencing of neural firing. This new technique has potential applications in dissecting neural circuits and controlling activity downstream from sites of neural damage or degeneration

Application of AFM for Biomolecular Imaging

AFM has become a well-established technique for imaging single biomolecules under physiological conditions. The exceptionally high spatial resolution and signal-to-noise ratio of the AFM enables the substructure of individual molecules to be observed. In contrast to other methods, specimens prepared for AFM remain in a plastic state, which enables direct observation of the dynamic molecular response, creating unique opportunities for studying the structure–function relationships of proteins and their functionally relevant assemblies.

The combination of single-molecule imaging with other techniques to monitor topographical, biochemical and physical parameters simultaneously is a powerful, interesting and unique application of AFM. This correlation of biochemical and physical information can provide new insights into fundamental biological processes. Several different approaches for obtaining multiple parameters during AFM imaging have been developed, including AFM in combination with optical microscopy, patch clamp electrophysiology and ion-conductance pipettes. Used as a sensor, the AFM tip can also probe the charges of biological surfaces immersed in a buffer solution. So far, such approaches have successfully characterized protein interactions but in the future they could be applied to imaging and detecting multiple parameters on a single molecule simultaneously.

AFM has been used to study and characterize gene complexes composed of plasmid DNA and cationic lipids. Surface morphology of spherical complexes with diameters of approximately 200–300 nm can be examined. However, AFM technique does not enable any conclusions to be drawn regarding the architecture of the inner core of the lipoplex as only the morphology of the surface structures can be obtained reliably.

One of the critical limitations of AFM is its inability to recognize the specific chemical composition of a molecule. AFM uses a tiny, highly sensitive probe that, when pulled across the surface of a sample, maps its topography down to the nanometer scale. Until recently, it could not identify exactly what the proteins on its map as all proteins look the same in an AFM image. A solution to this limitation is use of an even tinier polymer thread that attached antibodies designed to bind to individual proteins to the tip of the AFM probe. When the antibody binds to the target protein, it creates a variance in the microscope's reading. This is a technique for identifying any antigen in a complex sample on the nanometer scale and has applicability that goes far beyond sorting out AFM images. It could be used to read arrays on the nanometer scale to enable mapping of the entire interaction potential landscape between a receptor and a ligand.

Future Insights into Biomolecular Processes by AFM

AFM has become a well-established technique for imaging individual macromolecules at a spatial resolution of <1 nm. The next step will be to establish new AFM methods to investigate structure-function relationships among the variety of molecular machines. Such results will provide insights into how such machines work at the molecular level, and drive the understanding of common principles that govern them. The next challenge will be to study the behavior of individual molecular machines in heterogeneous assemblies, and to understand how different machines form small functional entities. Here, again, AFM promises to be an important tool as it enables individual molecules to be imaged at sufficient resolution for their behavior within macromolecular complexes to be characterized.

4Pi Microscopy to Study DNA Double-Strand Breaks

DNA double-strand breaks caused by cellular exposure to genotoxic agents or produced by inherent metabolic processes initiate a rapid and highly coordinated series of molecular events resulting in DNA damage signaling and repair. Phosphorylation of histone (a spools around which DNA is wound) H2AX to form gamma-H2AX is one of the earliest of these events and is important for coordination of signaling and repair activities. An intriguing aspect of H2AX phosphorylation is that gamma-H2AX spreads a limited distance up to 1-2 Mbp from the site of a DNA break in mammalian cells. Generally light microscopy has limited resolution. By manipulating how light waves behave, however, biophysicists are expanding the limits of light microscopy, and one of the latest advances - the 4Pi microscope - provides neverbefore-seen views of cellular components, including structures within the nucleus. 4Pi microscopy has been used to visualize endogenous nuclear proteins. These observations suggest that H2AX is not distributed randomly throughout bulk chromatin, rather it exists in distinct clusters that themselves are uniformly distributed within the nuclear volume. These data support a model in which the size and distribution of H2AX clusters define the boundaries of gamma-H2AX spreading and may provide a platform for the immediate and robust response observed after DNA damage. 4Pi microscopy allows researchers to see the response in 3D, at resolutions down to 100 nm. Therefore, the role of the physical structures in various processes within the nucleus can now be visualized.

Nanoscale DNA Imaging

DNA nanotechnology has developed powerful techniques for the construction of precisely defined molecular structures and machines, and nanoscale imaging methods have always been crucial for their experimental characterization (Jungmann et al. 2012). While initially AFM was the most widely employed imaging method for DNA-based molecular structures, a variety of other techniques have been adopted by researchers in the field, i.e. electron microscopy (EM), super-resolution fluorescence microscopy, and high-speed AFM. EM is now typically applied for the characterization of compact nano-objects and 3D DNA origami structures, which is a powerful technique for the assembly of almost arbitrarily shaped nanoscale objects, because it not only offers better resolution than AFM but can also be used for 3D reconstruction from single-particle analysis. Although the small size of DNA nanostructures had previously precluded the application of fluorescence microscopic methods, the development of super-resolution microscopy has facilitated the application of fast and powerful optical methods in DNA nanotechnology. Particularly, observation of dynamic processes associated with DNA nanoassemblies, e.g. molecular walkers and machines, requires imaging techniques that are both fast and enable observation under native conditions. For this, single-molecule fluorescence techniques and high-speed AFM are beginning to play an increasingly important role.

Multi-isotope Imaging Mass Spectrometry

Secondary-ion mass spectrometry (SIMS) is an important tool for investigating isotopic composition in the chemical and materials sciences, but its use in biology has been limited by technical considerations. Multi-isotope imaging mass spectrometry (MIMS), which combines a new generation of SIMS instrument with sophisticated ion optics, labeling with stable isotopes, and quantitative image-analysis software, was developed to study biological materials. A beam of ions is used to bombard the surface atoms of the biological samples, and a fraction of the atoms are emitted and ionized. These "secondary ions" can then be manipulated with ion optics - in the way lenses and prisms manipulate visible light – to create an atomic mass image of the sample. The new instrument enables the production of mass images of high lateral resolution (down to 33 nm), as well as the counting or imaging of several isotopes simultaneously. As MIMS can distinguish between ions of very similar mass, it enables the precise and reproducible measurement of isotope ratios, and thus of the levels of enrichment in specific isotopic labels, within volumes of less than a cubic micrometer. The sensitivity of MIMS is at least 1000 times that of 14C autoradiography. The depth resolution can be smaller than 1 nm because only a few atomic layers are needed to create an atomic mass image.

MIMS can generate quantitative, 3D images of proteins, DNA, RNA, sugar and fatty acids at a subcellular level in tissue sections or cells and follow the fate of these

molecules when they go into cells, where they go, and how quickly they are replaced. The method does not need staining or use of radioactive labeling. Instead, it is possible to use stable isotopes to track molecules. MIMS has been to image unlabeled mammalian cultured cells and tissue sections; to analyze fatty-acid transport in adjpocyte lipid droplets using 13C-oleic acid; to examine nitrogen fixation in bacteria using 15N gaseous nitrogen; to measure levels of protein renewal in the cochlea and in postischemic kidney cells using 15N-leucine; to study DNA and RNA co-distribution and uridine incorporation in the nucleolus using 15N-uridine and 81Br of bromodeoxyuridine or 14C-thymidine; to reveal domains in cultured endothelial cells using the native isotopes 12C, 16O, 14N and 31P; and to track a few 15N-labeled donor spleen cells in the lymph nodes of the host mouse, suggesting that MIMS may be highly useful in immunology and cancer research. MIMS makes it possible for the first time to both image and quantify molecules labeled with stable or radioactive isotopes within subcellular compartments, suggesting that MIMS may have applications in tracking stem cells and in understanding why some organ transplants are rejected.

Applications of Biomolecular Computing in Life Sciences

Early biomolecular computer research focused on laboratory-scale, human-operated computers for complex computational problems. Now simple molecular-scale autonomous programmable computers have been shown to enable both input and output information in molecular form. Such computers, using biological molecules as input data and biologically active molecules as outputs, could produce a system for 'logical' control of biological processes. An autonomous biomolecular computer can, at least in vitro, logically analyze the levels of mRNA species, and in response produce a molecule capable of affecting levels of gene expression. This approach might be applied in vivo to biochemical sensing, genetic engineering and even medical diagnosis and treatment. Such computers have been programmed to identify and analyze mRNA of disease-related genes associated with models of small-cell lung cancer and prostate cancer, and to produce a single-stranded DNA molecule modeled after an anticancer drug. To have therapeutic value, such computers must be installed inside cells and protected from cellular defense mechanisms once they get there.

Using computer modeling, six phases of high-density nano-ice are predicted to form within CNTs at high pressure. High-density nano-ice self-assembled within smaller-diameter CNT exhibits a double-walled helical structure where the outer wall consists of four double-stranded helixes, which resemble a DNA double helix with the inner wall as a quadruple-stranded helix. This finding has major implications for study of the protein structures that cause diseases such as Alzheimer's and bovine spongiform encephalopathy.

Molecular systems based on DNA computing and strand displacement circuitry can exhibit autonomous brain-like behaviors. Using a simple DNA gate architecture that allows experimental scale-up of multilayer digital circuits, arbitrary linear threshold circuits were transformed into DNA strand displacement cascades that function as small neural networks (Qian et al. 2011). Four fully connected artificial neurons, after training in silico, were demonstrated to remember four ssDNA patterns and recall the most similar one when presented with an incomplete pattern. These results suggest that DNA strand displacement cascades could be used to endow autonomous chemical systems with the capability of recognizing patterns of molecular events, making decisions and responding to the environment.

Bacteria for Construction of Nanomachines

Single-molecule and super-resolution fluorescence imaging provide powerful tools for the biochemical, structural and functional characterization of cells as biological nanomachines. Data obtained from single bacterial cells have been used successfully to make tiny bio-electronic circuits. Microbes can serve as templates for fabricating nanoscale structures and might obviate the need for the tedious and time-consuming construction of devices at the smallest scale. This may also form the basis for a new class of biosensors for real-time detection of dangerous biological agents, including anthrax and other microbial pathogens.

Exploiting the complex topography of the bacterial cell surface and microbial interactions with antibodies, more complex nanoscale structures can be constructed because of the natural ability of cells to dock with different kinds of molecules. This would be easier than the painstaking manipulation of individual nanosized components, such as the microscopic wires and tubes that comprise the raw materials of nanotechnology. Bacteria can be considered as nature's nanowires that can be easily grown and manipulated. One can attach microscopic gold particles to the shell of the bacterium, making it more like a nanoscale gold wire. The ability to capture and analyze individual microbes might make it easier for scientists to retrieve specified cells from a complex mixture and have applications in cell therapy.

Natural Nanocomposites

Natural materials such as bone and tooth are nanocomposites of proteins and minerals with superior strength. Nanocomposites in nature exhibit a generic mechanical structure in which the nanometer size of mineral particles is selected to ensure optimum strength and maximum tolerance of flaws. The widely-used engineering concept of stress concentration at flaws is no longer valid for nanomaterial design. Natural nanocomposites can be used as a guide to enhance the properties of artificial nanocomposite materials, which eventually could excel compared to their biological counterparts.

Nanotechnology in Biological Research

Invention of the scanning tunneling microscope has opened new realms in study of biology. A whole family of scanning probe instruments has been developed, extending biological to the scale of atoms and molecules. Such instruments are especially useful for imaging of biomolecular structures because they can produce topographic images with submolecular resolution in aqueous environments. Instruments with increased imaging rates, lower probe-specimen force interactions, and probe configurations not constrained to planar surfaces are being developed, with the goal of imaging processes at the single-molecule level-not only at surfaces but also within 3D volumes. New development in nanotechnology are facilitating the study of biological processes at nanoscale and providing an understanding of many life processes that are relevant to healthcare. Single molecule nanobiology can be used as a tool for understanding the working principles of biological nanosystems in live cells.

AFM has been extensively used not only to image nanometer-sized biological samples but also to measure their mechanical properties by using the force curve mode of the instrument. The presence of specific receptors on the living cell surface has been mapped by this method. The force to break the co-operative 3D structure of globular proteins or to separate a double stranded DNA into single strands has been measured. Extension of the method for harvesting functional molecules from the cytosol or the cell surface for biochemical analysis has been reported. There is a need for the development of biochemical nano-analysis based on AFM technology.

Near infrared (NIR) laser microscopy enables optical micromanipulation, piconewton force determination, and sensitive fluorescence studies by laser tweezers. Fluorescence images with high spatial and temporal resolution of living cells and tissues can be obtained via non-resonant fluorophore excitation with multiphoton NIR laser scanning microscopes. Furthermore, NIR femtosecond laser pulses at can be used to realize non-invasive contact-free surgery of nanometer-sized structures within living cells and tissues. These novel versatile NIR laser-based tools can be used for the determination of motility forces, coenzyme and chlorophyll imaging, 3D multigene detection, noninvasive optical sectioning of tissues (optical biopsy), functional protein imaging, and nanosurgery of chromosomes.

QDs for Biological Research

QDs are used in a variety of assays such as immunohistochemistry, flow cytometry, Western blotting and plate-based assays. QDs have been used to study mechanism of protein trafficking. The early stages of receptor tyrosine kinases (RTKs)-dependent signaling in living cells have been imaged using continuous confocal laser scanning microscopy and flow cytometry. Epidermal growth factor (EGF)-QDs are highly specific and potent in the binding and activation of the EGF receptor (erbB1), being rapidly internalized into endosomes that exhibit active trafficking and extensive fusion. It is expected that QD-ligands will find widespread use in basic research and biotechnological developments. A coating for inorganic particles at the nanoscale may be able to disguise QDs as proteins. This process enables particles to function as probes that can penetrate the cell and light up individual proteins inside, and create the potential for application in a wide range of drug development, diagnostic tools and medications.

The organic coatings – short chains of peptides – can be used to disguise QDs, quantum rods and quantum wires so effectively that the cells mistake them for proteins, even when the coatings are used on particles that are inorganic and possibly even toxic. These peptide coatings trick the live cell into thinking that the nanoparticles are benign, protein-like entities. Therefore, one can use these coated particles to track the proteins in a live cell and conduct a range of studies at the molecular level. Using the new coatings, the UCLA team has been able to solubilize and introduce into the cell different color quantum dots that can all be excited by a single blue light source. The color encoding method is like encoding of information that is sent down an optical fiber, called wavelength division multiplexing. The peptide coating technology could, in principle, color encode biology itself, by painting different proteins in the cell with different-color quantum dots. The scientists are developing methods to attach QDs of specific colors to the different proteins on cells' surface and inside cells. By painting a subset of proteins in the cell with different color QDs, one can follow the molecular circuitry, the dynamic rearrangement of circuit nodes and the molecular interactions. In addition to the capacity to paint and observe many different proteins with separate colors, quantum dots can be used for the ultimate detection sensitivity: observing a single molecule. Until now, tracking and following a single protein in the cell has been extremely difficult.

By observing with a fluorescence microscope and high-sensitivity imaging cameras, researchers can track a single protein tagged with a fluorescent QD inside a living cell in 3D and within a few nanometers of accuracy. This process is, in some ways, the molecular equivalent of using the global positioning system to track a single person anywhere on earth. Researchers can use optical methods to track several different proteins tagged with different-color QDs, measure the distances between them and use those findings to better understand the molecular interactions inside the cell.

Particles disguised with the peptide coatings can enter a cell without affecting its basic functioning. Since the peptide-coated QDs are small, they have easy and rapid entry through the cell membrane. In addition, since multiple peptides of various lengths and functions could be deposited on the same single QD, it would be feasible to create smart probes with multiple functions.

This work on coatings was inspired by nature. Some plants and bacteria cells evolved unique capabilities to block toxic heavy-metal ions as a strategy to clean up the toxic environment in which they grow. These organisms synthesize peptides, called phytochelatins that reduce the number of toxic-free ions by strongly binding to inorganic nanoparticles made of the sequestered toxic salts and other products.

The peptide coating bridges the inorganic chemistry world with the organic world on the nanometer scale. These coatings will be used to provide electrical

contact between nanoscale inorganic electronic devices and functional proteins, which would lead to the evolution of novel and powerful 'smart drugs,' 'smart enzymes,' 'smart catalysts,' 'protein switches' and many other functional hybrids of inorganic-organic substances. It might enable the creation of a hybrid nanoparticle that could be specifically targeted to identify and destroy cancer cells in the body.

Molecular Biology and Nanotechnology

Structural DNA Nanotechnology

DNA is an ideal molecule for building nanometer-scale structures. Strands of DNA interact in the most programmable way. Their enormous variability provides ample scope for designing molecules. DNA scaffolds could hold guest molecules in orderly arrays for crystallography. Nanometer-scale DNA machines can function by having part of their structure change from one DNA conformation to another. These movements can be controlled by chemical means or by special DNA strands.

Structural DNA nanotechnology uses the basic chemical units of DNA – C, T, A, or G – to self-fold into several different building blocks that can further self-assemble into patterned structures. Unusual DNA motifs can be combined by specific structurally well-defined cohesive interactions (primarily sticky ends) to produce target materials with predictable 3D structures. This effort has generated DNA polyhedral catenanes, robust nanomechanical devices, and a variety of periodic arrays in 2D. This is a good example of artificial nanostructures that can be replicated using the machineries in live cells. The system has been used to produce specific patterns on the mesoscale through designing and combining specific DNA strands, which are then examined by AFM. The combination of these constructions with other chemical components is expected to contribute to the development of nanoelectronics, nanorobotics, and smart materials (Seeman 2007).

Three different structurally robust end states can be obtained in one system, all resulting from the addition of different set strands to a single floppy intermediate as an extension of the PX-JX2 DNA device (Chakraborty et al. 2008). The three states are related to each other by three different motions, a twofold rotation, a translation of $\approx 2.1-2.5$ nm, and a twofold screw rotation, which combines these two motions. The transitions were demonstrated by gel electrophoresis, by FRET, and by AFM.

Many new tertiary interactions are being discovered and some of these are being used for generating new nucleic acid-based materials. These may ultimately lead to a new generation of capabilities for structural nucleic acid nanotechnology. As more knowledge is gained about the metabolism of DNA, new motifs may be discovered that are currently exploited by living systems and that can be used by the materials sciences to generate new materials. Structural nucleic acid nanotechnology is in its infancy, but it seems to be capable of remarkable versatility in the organization of matter on the nanoscale. Despite the dramatic evolution of DNA nanotechnology, a versatile method that replicates artificial DNA nanostructures with complex secondary structures remains an appealing target. Previous success in replicating DNA nanostructures enzymatically in vitro suggests that a possible solution could be cloning these nanostructures by using viruses. A system has been reported where ssDNA nanostructure is inserted into a phagemid, a virus-like particle that infects a bacteria cell (Lin et al. 2008). Once inside the cell, the phagemid uses the cell just like a photocopier machine to reproduce millions of copies of the DNA. By theoretically starting with just a single phagemid infection, and a single milliliter of cultured cells, the cells can churn out trillions of the DNA junction nanostructures. The DNA nanostructures produced in the cells were found to fold correctly, just like the previously built test tube structures. The simplicity, efficiency, and fidelity of nature are fully reflected in this system. UV-induced psoralen cross-linking is used to probe the secondary structure of the inserted junction in infected cells. These data suggest the possible formation of the immobile four-arm junction in vivo.

Another future goal is incorporation of DNA devices into nanorobotics. Nanoelectronic components, such as metallic nanoparticles or carbon nanotubes, will need to be combined with DNA molecules in compatible systems. It may be possible to have DNA-based replicating machines in a few decades.

RNA Nanotechnology

RNA has an important role in nanoscale fabrication due to its amazing diversity of function and structure. RNA molecules can be designed and manipulated with a level of simplicity characteristic of DNA while possessing versatility in structure and function similar to that of proteins. RNA helicases are a large family of molecular motors that utilize nucleoside triphosphates to unwind RNA duplexes and to remodel RNA protein complexes. These enzymes have a potential application in controlling conformational changes in nanoassemblies that contain RNA.

Assembly and folding principles of natural RNA can be used to build potentially useful artificial structures at the nanoscale. Reliable prediction and design of the 3D structure of artificial RNA building blocks has been achieved to generate molecular jigsaw puzzle units called tectosquares, which can be programmed with control over their geometry, topology, directionality, and addressability to algorithmically self-assemble into a variety of complex nanoscopic fabrics with predefined periodic and aperiodic patterns and finite dimensions. Such studies emphasize the modular and hierarchical characteristics of RNA by showing that small RNA structural motifs can code the precise topology of large molecular architectures. They demonstrate that fully addressable materials based on RNA can be synthesized and provides insights into self-assembly processes involving large populations of RNA molecules.

The ability of RNA to fold into a variety of rigid structural motifs can provide potential modules for supramolecular engineering. Nano-grids may eventually be used as a starting point to generate nanochips, nanocircuits and nanocrystals with potential applications in nanotechnology and materials science. Healthcare applications include the development of medical implants, regeneration of organs and nanodiag-nostics. The most recent development in exploration of RNA nanoparticles is for pathogen detection, drug/gene delivery, and therapeutic application.

A conference on RNA Nanotechnology concluded (Shukla et al. 2011):

- Applications and the impact of RNA nanotechnology in the assembly and delivery of siRNAs, pRNA, therapeutic ribozymes, RNA aptamers, and riboswitches are becoming a reality.
- RNA nanotechnology is already making a significant impact in drug delivery and therapeutics as many siRNA-based products are in the pipeline for potential treatment of viral infections, liver cancer, and Huntington's disease.
- Collaborative endeavors between academia, government, and industry are likely required to advance RNA nanotechnology into a practical tool for drug discovery and delivery in the future.

Genetically Engineered Proteins for Nanobiotechnology

With the development of nanoscale engineering in physical sciences and the advances in molecular biology, it is possible to combine genetic tools with synthetic nanoscale constructs to create a novel method. Peptides/proteins can now be genetically engineered to specifically bind to selected inorganic compounds for applications in nanobiotechnology. These genetically engineered proteins for inorganics (GEPIs) can be used in the assembly of functional nanostructures. Based on the three fundamental principles – molecular recognition, self-assembly and DNA manipulation – GEPI has been used successfully in nanotechnology.

Organization and immobilization of inorganic nanoparticles in 2D or 3D is fundamental to the use of nanoscale effects. It would be desirable to use GEPIs that specifically recognize inorganics for nanoparticle assembly. An advantage of this approach is that GEPI can be genetically or synthetically fused to other functional biomolecular units or ligands to produce multifunctional molecular entities. Proteins may be useful in the production of tailored nanostructures and the recognition activity of the protein could provide an ability to control the particle distribution, and particle preparation conditions could allow size control.

Self-assembled GEPI monolayers could open new avenues for designing and engineering novel surfaces for a wide variety of nano- and biotechnology applications, e.g. a GEPI recognizing and assembling on the surface of a therapeutic device could be fused to a human protein to enhance biocompatibility, or used for drug delivery through colloidal inorganic particles. Coupled with a molecular motor, a GEPI may provide a critical step towards creating dynamic nanostructures. Ultimately, using nanopatterned multimetallic or multisemiconducting particles and localized surface plasmon effects, several different GEPI molecules could serve as specific linkers in creating nanoscale platforms for rapid development of nanoarrays for proteomics. Based on the insights achieved through these studies in the coming decade, and following the lead of molecular biology, a roadmap could be developed in which GEPI could be used as a versatile molecular linker and open new avenues in the self-assembly of molecular systems in nanobiotechnology.

Single Molecule Studies

3D Single-Molecular Imaging by Coherent X-Ray Diffraction Imaging

Coherent X-ray diffraction imaging is a rapidly advancing form of microscopy: diffraction patterns, measured using the latest third-generation synchrotron radiation sources, can be inverted to obtain full 3D images of the interior density within nanocrystals. 3D imaging of a nanocrystal, obtained by inversion of the coherent X-ray diffraction, shows the expected faceted morphology, but in addition reveals a real-space phase that is consistent with the 3D evolution of a deformation field. Measuring and inverting diffraction patterns from nanocrystals represent a vital step towards the goal of atomic resolution single-molecule imaging that is a major justification for development of X-ray freeelectron lasers. It may be applied to determine the structure of single protein molecules placed in the femtosecond beam of a free-electron laser.

Nanoscale NMR for Imaging Single Molecules

Traditional MRI prevents visualization of anything much smaller than millimeterswide structures. An atomic-scale sensor is needed to detect just a few protons, such as those of a single molecule. Extension of nuclear magnetic resonance (NMR) to nanoscale samples has been a longstanding challenge because of the insensitivity of conventional detection methods. Use of diamonds for this purpose has been explored but a perfect diamond, made entirely of carbon atoms covalently bonded to each other, has no free electrons and therefore no magnetic properties. However, a miniscule diamond flaw consisting of difference of just two atoms, termed near-surface nitrogenvacancy (NV) center, confers unique magnetic properties and has been used as a sensor to detect proton NMR in an organic sample located external to the diamond (Mamin et al. 2013). Using a combination of electron spin echoes and proton spin manipulation, the authors showed that the NV center senses the nanotesla field fluctuations from the protons, enabling both time-domain and spectroscopic NMR measurements on the nanometer scale. This approach relies on a single electron to detect perturbation in molecular magnetic fields that can provide clues about structures of proteins and other molecules without resorting to time-consuming and technically exacting X-ray crystallography. Eventually, the researchers will need to bring the NV center even closer to the surface and its target nuclei to get nanoscale resolution of complex molecules. But doing so without interfering with its properties will be a serious challenge, because the magnetic fields of extraneous nuclei such as water molecules on the diamond's surface can influence the NV center as well.

Optical Trapping and Single-Molecule Fluorescence

Two of the mainstay techniques in single-molecule research are optical trapping and single-molecule fluorescence. Previous attempts to combine these techniques in a single experiment and on a single macromolecule of interest have met with little success, because the light intensity within an optical trap is more than ten orders of magnitude greater than the light emitted by a single fluorophore. Instead, the two techniques have been employed sequentially, or spatially separated by distances of several micrometers within the sample, imposing experimental restrictions that limit the utility of the combined method. Instrument capable of true, simultaneous, spatially coincident optical trapping and single-molecule fluorescence have been developed opening the door to many types of experiment that employ optical traps to supply controlled external loads while fluorescent molecules report concurrent information about macromolecular structure. The combination of these two biophysical techniques in a single assay offers a powerful tool for studying molecular systems by allowing direct correlations to be made between nanoscale structural changes.

Study of Molecular Assembly of Single Molecules in Living Cells

In living cells, the 3D architecture of molecular assemblies, such as chromosomes, lipid bilayers, and the cytoskeleton, is regulated through the interaction among their component molecules. Monitoring the position and orientation of constituent molecules is important for understanding the mechanisms that govern the structure and function of these assemblies. An instantaneous fluorescence polarization microscope simultaneously images position and orientation of fluorophores in living cells with single-molecule sensitivity and time resolution of 100 ms (Mehta et al. 2016). Image acquisition and analysis methods were used to track single particles that interact with higher-order assemblies of molecules. Fluctuations in position and orientation of molecules were tracked from the level of an ensemble of fluorophores down to single fluorophores. This system was tested in vitro using fluorescently labeled DNA and F-actin, in which the ensemble orientation of polarized fluorescence is known. Tracked the orientation of sparsely labeled F-actin network at the leading edge of migrating human keratinocytes revealed the anisotropic distribution of actin filaments relative to the local retrograde flow of the F-actin network. Data indicate that septin-GFP molecules undergo positional fluctuations within \sim 350 nm of the binding site and angular fluctuations within \sim 30° of the central orientation of the bundle. By reporting position and orientation of molecules while they form dynamic higher-order structures, this approach provides insights into how micrometer-scale assemblies emerge from nanoscale molecules in living cells.

Nanochemistry

Nanochemistry involves the utilization of a chemical synthesis approach to make new materials with at least one physical dimension straddling the molecular (nanoscale) and macroscopic world. In practice, nanochemistry deals with the production and the reactions of nanoparticles and their compounds.

A new generation of spectroscopic dyes is gradually becoming available to biological researchers, from an unexpected source: materials chemists who study the synthesis and properties of nano-sized inorganic objects. Research into tailoring the optical properties, surface chemistry and biocompatibility of metallic and semiconductor nanoparticles is fulfilling the promise of these nanostructures as customizable substitutes for organic molecular probes. Chemists have reported synthetic routes towards semiconductor 'quantum dots' for fluorescent tagging, metal nanoparticles with extraordinarily high extinction coefficients for labeling in colorimetric and surface plasmon resonance assays and elongated 'nanorods' for measuring anisotropy. Nanoparticles are also providing alternatives to organic and organometallic probes for other (non-optical) biological applications, such as paramagnetic particles for magnetic resonance contrast imaging and metal particles for thermal probing of specific biomolecular interactions. The chemical synthesis of most of these nanostructures is typically achieved with just one reaction, involving a chemical transformation of a precursor source of inorganic material followed by a nanocrystallization process in the same vessel. Fine control over synthetic conditions is responsible for the reproducible range of novel properties these materials exhibit. As a result, nanostructured biological probes are easier to make and might eventually be less expensive to buy than organic dyes. In addition, the specific photochemical reactions that cause organic probes to photobleach or crosslink nonspecifically with biological samples are far less common for inorganic nanostructures. Admittedly, there are still limitations to using nanostructures as biological probes. Nanoparticles are significantly larger than molecular dyes and a bound nanostructure might sterically block access to the active sites of a biomolecule or affect its diffusion. In addition, the bioconjugation chemistry of some nanomaterials is still not fully refined. Nevertheless, the control that synthetic chemists have demonstrated over the structure and properties of nanoparticle materials is impressive, and naturally points towards their biological applications.

Nanoscale pH Meter

An all-optical nanoshell coated with pH-sensitive molecules that functions as a standalone, nanoscale pH meter can monitor its local environment through the pH-dependent surface-enhanced Raman scattering (SERS) spectra of the adsorbate molecules (Bishnoi et al. 2006). The complex spectral output is reduced to a simple

device characteristic by application of a locally linear manifold approximation algorithm. This approach represents the first method of measuring accurate pH changes inside living tissue and cells, including tumors, in real-time.

Nanolaser Applications in Life Sciences

A nanolaser is a tiny laser which emits a coherent beam of light through the vibration of a single electron, rather than the space-consuming optical pumping process of a traditional laser. The nanolasers were developed by growing semiconductor nanowires. The line widths, wavelengths, and power dependence of the nanowire emission characterize the nanowires as active optical cavities. Current leading solidstate lasers, often made of gallium arsenide or gallium nitride, are made of multilayer thin films and measure several micrometers in size. The nanowire laser is 1000 times smaller, allowing localized optical illumination. It can be tuned to emit light of different wavelengths from the infrared to the deep ultraviolet by simply changing the diameter or composition of the nanowire.

One of the smallest lasers ever made, nanowire nanolaser, is too small to be seen even with the aid of the most powerful optical microscope. The nanowire nanolasers are pure crystals of zinc oxide that grow vertically in aligned arrays like the bristles on a brush. These crystal nanowires range from 2 to 10 microns in length, depending upon how long the growth process proceeds. The nanowire nanolaser, which emits flashes of ultraviolet light, measures just less than 100 nm. The individual ZnO nanowires have uniform diameters ranging from 10 to 300 nm. Under optical excitation, each individual ZnO nanowire serves as a Fabry-Perot optical cavity, and together they form a well-ordered nanowire ultraviolet laser array.

It is the small area of illumination that holds near-term potential for the nanolaser. Near-term products could include ultrahigh resolution photolithography for next-generation microchips, as well as laser-powered biochips. Other potential applications for the nanolaser include high-density information storage, highdefinition displays, photonics, optocommunications and chemical analysis on microchips. Nanolaser spectroscopy has also been used to study very small biological structures. This technology has also been applied for biphotonic detection of cancer in single cells (see Chap. 4).

Nanoelectroporation

Whereas cells precisely control the passage of substances in and out of their membranes, efforts to transport materials into cells in human employ clumsier techniques, which often damage cells and provide little control, if any, over the material delivered. In nanoelectroporation paired microchannels are connected by a nanochannel through which materials can move into cells and might help solve this problem (Boukany et al. 2011).

Nucleic acids are usually introduced into cells by bulk electroporation, in which suspended cells and reagents are placed together in a vessel, and an electric field is applied to increase the permeability of the cell membrane. The technique is simple, but it also destroys many cells and leaves many untransfected. Another technique, microfluidics-based electroporation, positions cells next to small openings that focus electric fields on only a small section of the cell membrane, which results in lower rates of cell death and higher rates of transfection, but it does not allow control over how much material is delivered. The new device enables electroporation on nanometer scale. Not only is the electric field applied to an area one-hundredth the size of those used in microfluidic-based methods, the volume of material delivered to cells can be precisely controlled through the duration and number of electric pulses. Bulk electroporation does not allow investigation of effects of dose levels. Microinjection can deliver precise dose levels, but this method works best with large cells, which are less easily damaged by the injection needle. A method enabling precisely controlled transfection for small cells would overcome this limitation.

This device described is made of a series of paired microchannels, each connected by an even tinier nanochannel with a diameter of about 90 nm. This nanochannel is made by laying gold-coated DNA strands into a low-viscosity resin into which microchannels have been stamped, and then etching out the strands' impression. Cells are placed in one microchannel and the transfection material in the other. A voltage pulse creates a tiny pore in the cell membrane through which a precise amount of material can be driven.

The device was tested by transfecting cells with 18-mer oligonucleotides attached to a fluorescent marker as well as with an RNA-based molecular beacon (a probe designed to fluoresce upon hybridization to a target RNA or DNA molecule). Dose control was demonstrated by transfecting cancer cells with varying levels of a siRNA targeting a protein that inhibits apoptosis, demonstrating that varying dose levels affected cell viability. The technique also enabled controlled delivery of specified numbers of quantum dots and large DNA molecules into cells. With other forms of electroporation, nanoparticles tend to get stuck in the cell membrane, but nanochannel electroporation allows the particles to reach interior of cells. The device also works with large nucleic acids (larger than 4,000,000 Daltons, or about 6.6 kilobases), which are difficult to transfect using existing methods.

Currently, only a handful of cells can be transfected at a time with the nanochannel electroporation device because cells are loaded into the microchannel using optical tweezers. However, work is in progress on a second-generation device that would allow parallel transfection of 100,000 cells. The device can be used for studying fundamental biological problems but the most important applications will be for modifying cells in gene therapy and reprogramming them. Current techniques can result in overdosing and other transfection-caused toxicity, but a precisely controlled high dose delivered to the precursor cells can be successful with low chance of forming cancerous cells.

Nanomanipulation

AFM enables the imaging and manipulation of biological systems at the nanometer scale. Examples include the following:

- · Extraction of chromosomal DNA for genetic analysis
- Disruption of antibody antigen bonds
- Dissection of biological membranes
- Nanodissection of protein complexes
- · Controlled modulation of protein conformations

Nanomanipulation by Combination of AFM and Other Devices

An instrument constructed by combining an objective-type total internal reflection fluorescence microscope with an AFM can detect and confirm the result of cellular level manipulations made with the AFM, partly through the detection system of the highly sensitive fluorescence microscope. In this combination, manipulations are now possible from the nanometer to the micrometer scales and the fluorescence detection system is sensitive enough even for localizing single molecules.

Nanomanipulation and nanoextraction on a scale close to and beyond the resolution limit of light microscopy is needed for many modern applications in biological research. For the manipulation of biological specimens, a combined microscope enabling ultraviolet (UV) microbeam laser manipulation together with manipulation by an AFM has been used. In a one-step procedure, human metaphase chromosomes can be dissected optically by the UV-laser ablation and mechanically by AFM manipulation. With both methods, sub-400-nm cuts is achieved routinely. Thus, the AFM is an indispensable tool for in situ quality control of nanomanipulation.

Design of a compact nanomanipulator that can be operated inside the sample chamber of a SEM for biological sample manipulation is based on that of AFM (Iwata et al. 2011). A self-sensitive cantilever is used to realize the compact body. Using this system, the scientists accomplished nanodissection of biological samples as well as AFM imaging under SEM observation. They then fabricated the surface of a rat renal glomerulus by scan-scratching and succeeded in making a small hole on the wall of a blood capillary. As a result of this, it was possible to observe the internal structure of the capillary, which had been hidden beneath the surface wall. Furthermore, using two AFM units on the sample stage of the SEM, they successfully dissected the lens fiber cells taken from a rat eye in a multi-probe operation using the two cantilevers. This system is expected to become a very useful tool for micro- and nanometer-scale anatomical manipulations.

Surgery on Living Cells Using AFM with Nanoneedles

Operations on living cells can be performed at nanoscale resolution using AFM and a modified AFM tip. The AFM tips are sharpened to ultrathin needles of 200–300 nm in diameter using focused ion beam etching. Force-distance curves obtained by AFM using the needles indicate that the needles penetrate the cell membrane following indentation to a depth of $1-2 \mu m$. The increase of force during the indentation process is consistent with application of the Hertz model. A 3D image generated by laser scanning confocal microscopy directly reveals that the needle penetrates both the cellular and nuclear membranes to reach the nucleus. This technique enables the extended application of AFM to analyses and surgery of living cells.

A nanoknife, fabricated from a commercial AFM cantilever by focused-ion-beam etching technique, has been proposed for single-cell cutting (Shen et al. 2011). The material identification of the nanoknife was determined using the energy dispersion spectrometry method. The buffering beam was used to measure the cutting force based on its deformation. The spring constant of the beam was calibrated based on a referenced cantilever by using a nanomanipulation approach. The cutting force and the sample slice angle for various nanoknives were evaluated. It was shown that the compression to the cell can be reduced when using the nanoknife with a small edge angle 5° . Consequently, the nanoknife was capable for in situ single-cell cutting tasks.

Optoelectronic Tweezers

The ability to easily manipulate cells has many applications, e.g. isolation and study of circulating fetal cells in a mother's blood sample to sort out abnormally shaped organisms from healthy ones. This sorting process is usually painstakingly done by hand. A technician finds the cell of interest under a microscope and literally cuts out the piece of glass where the cell is located, taking care not to harm the sample. The conventional manipulation techniques – including optical tweezers, electrokinetic forces, magnetic tweezers, acoustic traps and hydrodynamic flows – cannot achieve high resolution and high throughput at the same time. Optical tweezers offer high resolution for trapping single particles, but have a limited manipulation area owing to tight focusing requirements; on the other hand, electrokinetic forces and other mechanisms provide high throughput, but lack the flexibility or the spatial resolution necessary for controlling individual cells.

Optical image-driven dielectrophoresis enables high-resolution patterning of electric fields on a photoconductive surface for manipulating single particles. Such optoelectronic tweezers (OETs) can produce instant microfluidic circuits without the need for sophisticated microfabrication techniques. With direct optical imaging control, multiple manipulation functions are combined to achieve complex, multi-step manipulation protocols. Microscopic polystyrene particles suspended in a liquid are sandwiched between a piece of glass and the photoconductive material. Wherever light hits the photosensitive material, it behaves like a conducting electrode, while areas not exposed to light behave like a non-conducting insulator. Once a light source is removed, the photosensitive material returns to normal. Depending upon the properties of the particles or cells being studied, they are either attracted to or repelled by the electric field generated by the OET. It requires 100,000 times less optical intensity than optical tweezers. Parallel manipulation of 15,000 particle traps can be done on a $1.3 \times 1.0 \text{ mm}^2$ area. The researchers are now studying ways to combine this technology with computer pattern recognition so that the sorting process could be automated. A program could be designed to separate cells by size, luminescence, texture, fluorescent tags and basically any characteristic that can be distinguished visually.

By combining the manipulation capabilities of OET with other relevant biological techniques (such as cell lysis and electroporation), it is possible to realize a true parallel, single-cell diagnostic and stimulation tool. The usefulness of the OET device has been demonstrated by integrating it onto single-chip systems capable of performing in situ, electrode-based electroporation/lysis, individual cell, light-induced lysis, and light-induced electroporation.

Optical Manipulation of Nanoparticles

Mechanical pumps do not scale down well for moving objects at the nanoscale. Optofluidics uses the pressure of light to move and manipulate biological molecules. A beam of light can trap and move particles as small as 75 nm in diameter, including DNA molecules. This is possible because of the paradoxical dual nature of light, which is a stream of particles called photons that can exert a force, or as waves of expanding and contracting electric and magnetic fields. If light is confined to a waveguide narrower than its wavelength, the wave overflows and can exert a force beyond the guide. In a slot waveguide, two parallel silicon bars 60 nm apart, serve as two parallel wave guides (Yang et al. 2009). Light waves traveling along each guide expand beyond its boundaries, but because the parallel guides are so close together, the waves overlap and most of the energy is concentrated in the slot. In addition to creating a more intense beam, this structure allows a beam of light to be channeled through air or water. This device will help to bridge the gap between optical manipulation and nanofluidics. A tiny biological sample could be carried through microscopic channels for processing. This would enable portable, fastacting detectors for disease organisms or food-borne pathogens and other tests that now take hours or days. Further development could make it possible to separate DNA molecules by length for rapid DNA sequencing.

Manipulation of DNA Sequence by Use of Nanoparticles as Laser Light Antennas

Optical techniques have been developed for the parallel manipulation of nanoscale structures with molecular resolution. Bioconjugated metal nanoparticles are positioned at the location of interest, such as certain DNA sequences along metaphase chromosomes,

prior to pulsed laser light irradiation of the whole sample. Nanoparticles are designed to absorb the introduced energy highly efficiently, thus acting as nanoantenna. As result of the interaction, structural changes of the sample with subwavelength dimensions and nanoscale precision are observed at the location of the particles. The process leading to the nanolocalized destruction is caused by particle ablation as well as thermal damage of the surrounding material. The procedure is highly parallel and can be potentially multiplexed by addressing several different sequences (such as genes). Potential applications are in DNA analysis such as DNA fingerprinting or mutation analysis as well as single-molecule manipulation.

Nanomanipulation of Single Molecule

The development of nanomanipulation techniques has given investigators the ability to manipulate single biomolecules in the order of nanometers and to record mechanical events of biomolecules at the single molecule level. The techniques can elucidate the mechanism of molecular motors by directly monitoring the unitary process of the mechanical work and the energy conversion processes by combining these techniques with the single molecule imaging techniques. The results strongly suggest that the sliding movement of the actomyosin motor is driven by Brownian movement. Other studies have reported data that are more consistent with the lever arm model. These methods and imaging techniques enable monitoring of the behavior of biomolecules at work and can be applied to other molecular machines.

By monitoring the end-to-end extension of a mechanically stretched, supercoiled, single DNA molecule, it is possible to directly observe the change in extension associated with unwinding of approximately one turn of promoter DNA by RNA polymerase. This approach has been used to quantify the extent of unwinding and compaction, the kinetics of unwinding and compaction, and effects of supercoiling, sequence, and nucleotides. The approach should permit analysis of other nucleic-acid-processing factors that cause changes in DNA twist and/or DNA compaction.

Fluorescence-Force Spectroscopy

Despite the recent advances in single-molecule manipulation techniques, purely mechanical approaches cannot detect subtle conformational changes in the biologically important regime of weak forces. A hybrid scheme combining force and fluorescence has enabled the examination of the effect of subpiconewton forces on the nanometer scale motion of the Holliday junction (HJ) at 100-hertz bandwidth (Hohng et al. 2007). The HJ is a four-stranded DNA structure that forms during homologous recombination, e.g. when damaged DNA is repaired. To better understand the mechanisms and functions of proteins that interact with the HJ, researchers must first understand the structural and dynamic properties of the junction itself.

But purely mechanical measurement techniques cannot detect the tiny changes that occur in biomolecules in the regime of weak forces. Mechanical interrogation of the HJ in three different directions helped elucidate the structures of the transient species populated during its conformational changes. This method combines the exquisite force control of an optical trap and the precise measurement capabilities of single-molecule fluorescence resonance energy transfer for mapping 2D reaction landscapes at low forces. It is readily applicable to other nucleic acid systems and their interactions with proteins and enzymes.

Nanomanipulation for Study of Mechanism of Anticancer Drugs

Using single-molecule nanomanipulation by magnetic tweezers, investigators have shown that anticancer drug topotecan, a camptothecin, kills cancer cells by preventing the enzyme DNA topoisomerase I, from uncoiling double-stranded DNA in those cells (Koster et al. 2007). The DNA becomes locked in tight twists, called supercoils, which bulge out from the side of the over-wound DNA molecule. If these supercoils accumulate and persist while the cell is trying to separate the two strands of DNA to make exact copies of the chromosomes during cell division, the cells will die. In vivo experiments in the budding yeast verified the resulting prediction that positive supercoils would accumulate during transcription and replication resulting from camptothecin poisoning of topoisomerase I. Based on the results of these studies, the supercoil theory was developed to explain camptothecins' cytotoxic effect, which could help in the clinical development of these agents.

Nanotechnology in Genomic Research

Studies in genetics, genomics, and cell biology have provided a foundation on which to build an understanding of genome biology. Extending this knowledge will require merging these approaches with additional disciplines and new technologies such as nanotechnology.

Nanotechnology for Separation of DNA Fragments

Nanotechnology has been used to carry out separations of a wide range of DNA fragments with high speed and high resolution during microchip electrophoresis. Optimal pressure conditions and concentrations of packed nanospheres are important for achieving improved DNA separations.

Electrophoretic transport of ions and macromolecules within long, thin nanochannels is being studied. Electrophoresis in nanochannels is a method to exploit coupling of disparate physical forces at the nanoscale in microfluidic devices for fast and accurate electrophoresis and chromatography. Potential application of nanochannel electrophoresis is improvements in DNA separation and sequencing. Conventional methods of DNA electrophoresis make use of either a gel or a concentrated solution of hydrophilic polymers as a separating medium in which DNA molecules migrate in the presence of an electric field. Gel-less separation of DNA via nanochannel electrophoresis, for example, might offer a significant reduction in both cost and time across a wide range of basic research, medical, and forensics applications. In order to achieve this it is important at this stage to develop a fundamental understanding of how each phenomenon is regulated, and to observe how the coupling of these affects separations. There is need to experimentally probe the dynamics of electrophoretic separations in nanochannels to expand the currently limited knowledge base.

Nanotechnology-Based DNA Sequencing

An efficient, nanoliter-scale microfabricated bioprocessor can be used to integrate all three Sanger sequencing steps: thermal cycling, sample purification, and capillary electrophoresis. Lab-on-a-chip-level integration enables complete Sanger sequencing from only 1 fmol of DNA template. The performance of a miniaturized DNA sequencer provides a benchmark for predicting the ultimate cost and efficiency limits of Sanger sequencing.

A method for the single-molecule detection of specific DNA sequences involves hybridization of double-stranded DNA (dsDNA) with peptide nucleic acid (PNA) and threading the DNA through 4–5 nm pores in a silicon nitride membrane (Singer et al. 2010). The membrane is then placed between two small fluid chambers and an electric current is applied across the membrane using a pair of silver electrodes. This current causes individual DNA molecules to move through the pore, unraveling as they enter the pore. When the matched DNA-PNA sequence passes through the pore, it produces a marked change in the electrical current passing between the two electrodes, which is easily distinguished from unaltered ssDNA, i.e. DNA not duplexed with the PNA probe. The device can analyze one DNA molecule per second. This high-throughput, long-read length method can be used to identify key sequences embedded in individual DNA molecules, without the need for amplification or fluorescent/radio labeling. The concept of nanopore-based sequencing is shown in Fig. 3.1.

Many of the technical hurdles preventing the use of nanopores in DNA sequencing (slowing transit though the pore, aligning bases properly for reading, designing the proper-sized nanopore) have been largely addressed. Scientists at the Technische Universität München in Germany have used nanoscale cover plates to convert

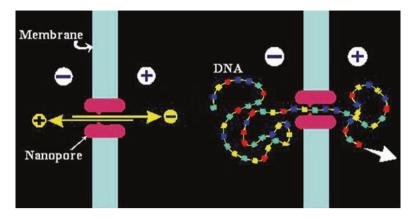


Fig. 3.1 Concept of nanopore-based sequencing. When a current is applied across the membrane, charged biomolecules migrate through the pores. As each nucleotide passes through the nanopore, an electric signature is produced that characterizes it because the size of the nanopore allows only a single nucleic acid strand to pass through it at one time

nanopores in solid-state membranes into versatile devices for label-free molecular sensing and the custom apertures in the nanoplates can be chemically addressed for sequence-specific detection of DNA (Wei et al. 2012). This is called "DNA origami", i.e. the art of programming strands of DNA to fold into custom-designed structures with specified chemical properties. Different chemical components beyond DNA could be attached to the appropriate site on a DNA nanoplate.

Nanopore-based sequencers, as the fourth-generation DNA sequencing technology, have the potential to quickly and reliably sequence the entire human genome for less than \$1000, and possibly for even less than \$100 (Feng et al. 2015). The single-molecule techniques used by this technology enables further study of the interaction between DNA and protein, as well as between protein and protein. Nanopore analysis opens a new door to molecular biology investigation at the single-molecule level, but a limitation is the requirement of precise, high-speed DNA detection beyond the spatial and temporal resolutions of existing optical and electrical technologies. Therefore, main challenges are single base recognition and slowing down the rate of DNA velocity. Nevertheless, nanopore technology will have a considerable impact on DNA sequencing and molecular diagnostics for personalized medicine.

Graphene, because of its unique structure and properties, provides opportunities for the development of a new sequencing technology. In recent years, a wide range of creative ideas for graphene sequencers have been theoretically proposed and the first experimental demonstrations have begun to appear. There are several approaches using graphene nanodevices for DNA sequencing, which involve passage of DNA through graphene nanopores, nanogaps, and nanoribbons (Heerema and Dekker 2016).

Role of Nanobiotechnology in Identifying Single Nucleotide Polymorphisms

Genetic analysis based on single nucleotide polymorphisms (SNPs) has the potential to enable identification of genes associated with disease susceptibility, to facilitate improved understanding and diagnosis of those diseases, and should ultimately contribute to the provision of new therapies. To achieve this end, new technology platforms are required that can increase genotyping throughput, while simultaneously reducing costs by as much as two orders of magnitude. Development of a variety of genotyping platforms with the potential to resolve this dilemma is already well advanced through research in the field of nanobiotechnology. Novel approaches to DNA extraction and amplification have reduced the times required for these processes to seconds. Microfluidic devices enable polymorphism detection through very rapid fragment separation using capillary electrophoresis and high-performance liquid chromatography, together with mixing and transport of reagents and biomolecules in integrated systems. The potential for application of established microelectronic fabrication processes to genetic analyses systems has been demonstrated (e.g. photolithography-based in situ synthesis of oligonucleotides on microarrays). Innovative application of state-of-the-art photonics and integrated circuitry are leading to improved detection capabilities. The diversity of genotyping applications envisaged in the future, ranging from the very high-throughput requirements for drug discovery through to rapid and cheap near-patient genotype analysis, suggests that several SNP genotyping platforms will be necessary to optimally address the different niches.

Nanobiotechnology for Study of Mitochondria

While autosomal nuclear DNA genes are confined to the nucleus, limited to two copies per cell, the mitochondrial DNA (mtDNA) genes are distributed throughout the cytoplasm and are present in numerous copies per cell. The mtDNA molecule is relatively small containing 16,569 nucleotide pairs. Mutations of mtDNA are responsible for several human diseases, e.g. neurological diseases. Mitochondrial diseases are often underdiagnosed and therapies are inadequate. Nanobiotechnology has been applied to study of mitochondria.

Nanomaterials for the Study of Mitochondria

Some of the nanomaterials for study of mitochondrial nanobiotechnology are shown in Table 3.1.

Nanomaterial	Modification	Application
Biosomes	Self-assembly of mitochoondriotropic bols amphiphile (DQAsomes)	Selective delivery of DNA to mitochondria to enable mitochondrial gene therapy
Liposomes	Mitochondria-specific ligands with hydrophobic anchor to form mitochondria-targeted liposomes	Mitochondrial-specific drug delivery
Nanoparticles	Mitochondria-specific ligands with linker to form mitochondria-targeted nanoparticles	Selective accumulation in mitochondria to probe or manipulate mitochondrial function
Quantum dots	Mitochondria-specific ligands with linker to form mitochondria-targeted quantum dots	To study the function and morphology of mitochondria

Table 3.1 Nanomaterials for the study of mitochondria

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Study of Mitochondria with Nanolaser Spectroscopy

Because mitochondria are so small, averaging a few hundred nanometers, scientists have been unable to study them in vitro with the necessary precision. Nanolaser spectroscopy is useful for the study of mitochondria. Isolated mitochondria can be studied by nanolaser spectroscopy to assess the optical density of an individual mitochondrion. This measurement uniquely reflects the mitochondrion size and biomolecular composition. As such, the optical density is a powerful parameter that rapidly interrogates the biomolecular state of single cells and mitochondria. In normal cells, mitochondria are highly organized within the cytoplasm and highly scattering, yielding a correlated signal, whereas in cancer cells, mitochondria are more chaotically organized and scattered (Gourley and McDonald 2007). These differences correlate with important bioenergetic disturbances that are hallmarks of many types of cancer. These optical methods may be useful for detecting cancer at an early stage.

Nanoproteomics

Nanoproteomics – application of nanobiotechnology to proteomics – improves on most current protocols including protein purification/display and automated identification schemes that yield unacceptably low recoveries with reduced sensitivity and speed while requiring more starting material. Low abundant proteins and proteins that can only be isolated from limited source material (e.g. biopsies) can be subjected to nanoscale protein analysis – nanocapture of specific proteins and complexes, and optimization of all subsequent sample handling steps leading to

mass analysis of peptide fragments. This is a focused approach, also termed targeted proteomics, and involves examination of subsets of the proteome, e.g., those proteins that are either specifically modified, or bind to a DNA sequence, or exist as members of higher order complexes, or any combination thereof. Some nanoproteomic technologies are described here briefly.

Biochips for Nanoscale Proteomics

Protein Biochips Based on Fluorescence Planar Wave Guide Technology

The fluorescence planar wave guide (PWG) technology has demonstrated exceptional performance in terms of sensitivity, making it a viable method for detection in chipbased microarrays. Thin film PWGs as used in ZeptoMARK protein microarrays consist of a 150-300 nm thin film of a material with high refractive index, which is deposited on a transparent support with lower refractive index (e.g., glass or polymer). A parallel laser light beam is coupled into the waveguiding film by a diffractive grating, which is etched or embossed into the substrate. The light propagates within this film and creates a strong evanescent field perpendicular to the direction of propagation into the adjacent medium. It has been shown that the intensity of this evanescent field can be enhanced dramatically by increasing the refractive index of the waveguiding layer and equally by decreasing the layer thickness. Compared to confocal excitation the field intensity close to the surface can be increased by a factor of up to 100. The field strength decays exponentially with the distance from the waveguide surface, and its penetration depth is limited to about 400 nm. This effect can be utilized to selectively excite only fluorophores located at or near the surface of the waveguide. By taking advantage of the high field intensity and the confinement of this field close to the waveguide PWG technology combines highly selective fluorescence detection with highest sensitivity.

For bioanalytical applications, specific capture probes or recognition elements for the analyte of interest are immobilized on the waveguide surface. The presence of the analyte in a sample applied to a PWG chip is detected using fluorescent reporter molecules attached to the analyte or one of its binding partners in the assay. Upon fluorescence excitation by the evanescent field, excitation and detection of fluorophores is restricted to the sensing surface, whilst signals from unbound molecules in the bulk solution are not detected. The result is a significant increase in the signal/noise ratio compared to conventional optical detection methods.

A variety of proteins can be immobilized on PWG microarrays as selective recognition elements for the investigation of specific ligand-protein interactions such as antigen-antibody, protein-protein and protein-DNA interactions. Protein microarrays based on PWG allow the simultaneous, qualitative and quantitative analysis of protein interactions with high sensitivity in a massively parallel manner. This method enables cost-effective determination of efficacy of drug candidates in a vast number of preclinical study samples.

Nanofilter Array Chip

Microfabricated nanofilter array chips can size-fractionate protein complexes and small DNA molecules based on the Ogston sieving mechanism, which is the earliest and simplest model of the sieving action of gels. The gel is assumed to be a static sieve. Depending on the solid phase material used and its concentration, the gel will have a particular distribution of pore sizes around a mean and a particular thickness of the matrix fibers. Nanofilter arrays with a gap size of 40–180 nm have been fabricated and characterized. Millions of pores can be spread across a microchip the size of a thumbnail. The proteins move through deep and shallow regions that act together to form energy barriers, which separate proteins by size. The smaller proteins go through quickly, followed by increasingly larger proteins, with the largest passing through last. To date, the Ogston sieving model has been used to explain gel electrophoresis, even though no one has been able to unequivocally confirm this model in gel-based experiments. The performance of the current one-dimensional sieves matches the speed of one-dimensional gels, but it can be improved greatly. The sieves could potentially be used to replace 2D gels in the process of discovering disease biomarkers.

Dynamic Reassembly of Peptides

Nanofiber structures of some peptides and proteins as biological materials are being studied including their molecular mechanism of self-assembly and reassembly. Nanofiber scaffold can be sonicated into smaller fragments and the mechanism of reassembly has been studied by AFM. These sonicated fragments not only quickly reassemble into nanofibers that are indistinguishable from the original material, but their reassembly also correlates with the rheological analyses showing an increase of scaffold rigidity as a function of nanofiber length. The disassembly and reassembly processes were repeated several times and, each time, the reassembly reaches the original length. This reassembly process is important for the construction of new scaffolds for 3D cell culture, tissue repair, and regenerative medicine.

High-Field Asymmetric Waveform Ion Mobility Mass Spectrometry

An ion mobility technology – high-field asymmetric waveform ion mobility mass spectrometry (FAIMS) – has been introduced as online ion selection methods compatible with electrospray ionization (ESI). FAIMS uses ion separation to improve detection limits of peptide ions when used in conjunction with electrospray and nanoelectrospray MS. This facilitates the identification of low-abundance peptide ions

often present at ppm levels in complex proteolytic digests and expand the sensitivity and selectivity of nanoLC–MS analyses in global and targeted proteomics approaches. This functionality likely will play an important role in drug discovery and biomarker programs for monitoring of disease progression and drug efficacy.

In nanoelectrospray ionization (nanoESI) techniques, the hydrophilic character of the emitters generally produces large bases for the Taylor cones, thereby generating relatively large droplet sizes and consequently reduced sensitivity. To minimize this wetting effect in nanoESI, a model hydrophobic polymer (an acrylic paint) was coated at the tip of commercial polyaniline (PANI)-coated emitters, and their performance was compared with that of unmodified PANI emitters using oxytocin and neuropeptide Y solutions. In experiments with oxytocin, the hydrophobic emitter produced higher signal intensities as well as higher signal-to-noise ratios than those from the unmodified PANI emitter. In addition, the hydrophobic emitter showed reusability and a slightly wider linear dynamic range than that from the unmodified PANI emitter (Choi and Wood 2007). In the case of neuropeptide Y, the hydrophobic emitter also enabled an approximately 350-fold overall increase in sensitivity than the unmodified PANI. The enhanced performance of the hydrophobic emitter clearly indicates potential for further increases in nanoESI sensitivity using emitters with tailored hydrophobic overcoatings.

Manipulation of Redox Systems by Nanotechnology

Redox proteins and enzymes carry out many key biological reactions, the underlying process of which is electron transfer. Protein-mediated electron transfer plays a key role in cellular processes such as respiration and photosynthesis. Redox proteins are attractive targets for nanobiotechnology because many can be detected both electrochemically and optically; they can perform specific reactions; they are capable of self-assembly; and their dimensions are in the nanoscale. There are several examples of novel approaches where redox proteins are "wired up" in efficient electron-transfer chains, are "assembled" in artificial multidomain structures and are "linked" to surfaces in nanodevices for biosensing and nanobiotechnological applications. Redox proteins present advantages for applications in electronic devices and biological tools because their intrinsic dimensions are in nanoscale and they are capable of self-assembly.

Multi Photon Detection

A new detection technique called Multi Photon Detection (MPD) is in development at BioTrace Inc. and enables quantitation of sub-zeptomole amounts of proteins. It will be used for diagnostic proteomics, particularly for cytokines and other low abundance proteins. BioTrace is developing supersensitive protein biochips to

Nanoflow Liquid Chromatography

The use of liquid chromatography (LC) in analytical chemistry is well established but relatively low sensitivity associated with conventional LC makes it unsuitable for the analysis of certain biological samples. Furthermore, the flow rates at which it is operated are not compatible with the use of specific detectors, such as electrospray ionization mass spectrometers. Therefore, due to the analytical demands of biological samples, miniaturized LC techniques were developed to allow for the analysis of samples with greater sensitivity than that afforded by conventional LC. In nanoflow LC (nanoLC) chromatographic separations are performed using flow rates in the range of low nanoliter per minute, which result in high analytical sensitivity due to the large concentration efficiency afforded by this type of chromatography. NanoLC, in combination to tandem mass spectrometry, was first used to analyze peptides and as an alternative to other mass spectrometric methods to identify gel-separated proteins. Gel-free analytical approaches based on LC and nanoLC separations have been developed, which are allowing proteomics to be performed in faster and more comprehensive manner than by using strategies based on the classical 2D gel electrophoresis approaches.

Protein identification using nanoflow liquid chromatography-mass spectrometry (MS)-MS (LC-MS-MS) provides reliable sequencing information for low femtomole level of protein digests. However, this task is more challenging for subfemtomole peptide levels.

Nanoparticle-Protein Interactions

Due to their small size, nanoparticles have distinct properties compared with the bulk form of the same materials. In a biological fluid, proteins associate with nanoparticles, and the amount and presentation of the proteins on the surface of the particles leads to an in vivo response. Proteins compete for the nanoparticle "surface," leading to a protein "corona" that largely defines the biological identity of the particle. Thus, knowledge of rates, affinities, and stoichiometries of protein association with, and dissociation from, nanoparticles is important for understanding the nature of the particle surface seen by the functional machinery of cells. Several approaches have been developed to study these parameters and apply them to plasma and simple model systems. A series of copolymer nanoparticles are used with variation of size and composition (hydrophobicity). Isothermal titration calorimetry is suitable for studying the affinity and stoichiometry of protein binding to nanoparticles. The rates of protein association and dissociation are determined using surface plasmon resonance technology with nanoparticles that are thiol-linked to gold, and through size exclusion chromatography of protein–nanoparticle mixtures. This method is less perturbing than centrifugation, and is developed into a systematic methodology to isolate nanoparticle-associated proteins. The kinetic and equilibrium binding properties depend on protein identity as well as particle surface characteristics and size.

Nanopore-Based Protein Sequencing

Nanopore-based DNA sequencing is well on its way to becoming a practical technique. Such an approach could also be adapted to sequence proteins. Before a bench-top protein sequencer can be made, however, several methodological challenges must be overcome. Two of these challenges have been addressed: how to unfold the protein to allow it to go through the pore; and how to ensure that it goes through the pore processively and unidirectionally (Nivala et al. 2013). The researchers created a system using the α -hemolysin pore with the unfoldase ClpX positioned on the trans side of the pore. They designed a polyanionic tag (for the protein of interest) that is captured and threaded through the pore when a voltage is applied; ClpX then recognizes a targeting motif on the C terminus of the tag and, fueled by ATP hydrolysis, unfolds and pulls the protein of interest through the pore.

Nanopores for Phosphoprotein Analysis

Nanopore technology has been used to demonstrate single-molecule, site-specific detection of protein phosphorylation with protein (Rosen et al. 2014). A model protein, thioredoxin, was phosphorylated at two adjacent sites. Analysis of the ionic current amplitude and noise, as the protein unfolds and moves through an α -hemolysin pore, enables the distinction between unphosphorylated, monophosphorylated and diphosphorylated variants. These results provide a step toward nanopore proteomics.

Nanoproteomics for Study of Misfolded Proteins

Misfolding and self-assembly of proteins in nano-aggregates of different sizes and morphologies (nano-ensembles, primarily nanofilaments and nano-rings) is a complex phenomenon that can be facilitated, impeded, or prevented, by interactions with various intracellular metabolites, intracellular nanomachines controlling protein folding and interactions with other proteins. A fundamental understanding of molecular processes leading to misfolding and self-aggregation of proteins involved in various neurodegenerative diseases will provide critical information to help identify appropriate therapeutic routes to control these processes. An elevated propensity of misfolded protein conformation in solution to aggregate with the formation of various morphologies impedes the use of traditional physical chemical approaches for studies of misfolded conformations of proteins. In an alternative approach, the protein molecules are tethered to surfaces to prevent aggregation and AFM force spectroscopy is used to probe the interaction between protein molecules depending on their conformations. It reveals that formation of filamentous aggregates is facilitated at pH values corresponding to the maximum of rupture forces. A novel surface chemistry was developed for anchoring of A β peptides at their N-terminal moieties. The use of a site-specific immobilization procedure enables measurement of the rupture of A β -A β contacts at single molecule level. The rupture of these contacts is accompanied by the extension of the peptide chain detected by a characteristic elasto-mechanical component of the force-distance curves. Nanomechanical studies have potential applications for an understanding of the mechanisms of development of protein misfolding diseases such as Alzheimer's disease.

Nanotube Electronic Biosensor for Proteomics

Single-walled carbon nanotubes can be used as a platform for investigating surfaceprotein and protein-protein binding and developing highly specific electronic biomolecule detectors. Nonspecific binding on nanotubes, a phenomenon found with a wide range of proteins, is overcome by immobilization of polyethylene oxide chains. A general approach is then advanced to enable the selective recognition and binding of target proteins by conjugation of their specific receptors to polyethylene oxide-functionalized nanotubes. These arrays are attractive because no labeling is required and all aspects of the assay can be carried out in solution phase. This scheme, combined with the sensitivity of nanotube electronic devices, enables highly specific electronic sensors for detecting clinically important biomolecules such as antibodies associated with human autoimmune diseases. These arrays are attractive because no labeling is required and all aspects of the assay can be carried out in solution phase. Interfacing novel nanomaterials with biological systems could therefore lead to important applications in disease diagnosis, proteomics, and nanobiotechnology in general.

Protein Nanocrystallography

Application of nanotechnology to structural proteomics can produce and characterize diffracting, stable and radiation-resistant crystals of miniscule dimensions. Protein microcrystals obtained by nanotechnology-based protein thin-film template crystallization, as well as groundbreaking technology, such as AFM, nanogravimetry and synchrotron microfocus, have enabled protein nanocrystallography to be defined as a unique technology capable of forming and characterizing stable protein microcrystals down to atomic resolution. A new route from art to science and technology has, therefore, been opened in protein crystallography, and it could be used to unravel the mysteries of many systems that remain unsolved.

Previous studies of symmetry preferences in protein crystals suggest that symmetric proteins, such as homodimers, might crystallize more readily on average than asymmetric, monomeric proteins. Proteins that are naturally monomeric can be made homodimeric artificially by forming disulfide bonds between individual cysteine residues introduced by mutagenesis. Furthermore, by creating a variety of single-cysteine mutants, a series of distinct synthetic dimers can be generated for a given protein of interest, with each expected to gain advantage from its added symmetry and to exhibit a crystallization behavior distinct from the other constructs.

Protein Engineering on Nanoscale

Nanowires for Protein Engineering

When folded into their native structures, proteins in biological systems function as nanostructured machines. Although proteins provide many valuable properties, poor physical stability and poor electrical characteristics have prevented their direct use in electrical circuits. By contrast, some polypeptides tend to aggregate into other well-ordered structures, namely amyloid fibrils. Such well-ordered protein fibrils are attractive materials for nanobiotechnology because they self-associate through noncovalent bonds under controlled conditions. Self-assembling amyloid protein fibers have been used to construct nanowire elements. Such applications will potentially become one of the next trends in protein engineering and nanobiotechnology. Complex circuit schematics could be generated with these fibers, initiated by patterned surface modifications such as lithography, growth in flows or magnetic field gradients, alignment by electrical fields, active patterning with optical tweezers, dielectrophoresis and 3D patterning using hydrogels or microfluidic channels. When these fibers are placed across gold electrodes, additional metal can be deposited by highly specific chemical enhancement of the colloidal gold by reductive deposition of metallic silver and gold from salts. The resulting silver and gold wires are ~100 nm wide. These biotemplated metal wires demonstrate the conductive properties of a solid metal wire, such as low resistance and ohmic behavior. By use of such materials it should be possible to harness the extraordinary diversity and specificity of protein functions to nanoscale electrical circuitry. There is a great opportunity to expand further the potential interconnections in these circuits by exploiting the natural diversity and strength of protein-protein interactions.

A Nanoscale Mechanism for Protein Engineering

Proteins are switched on and off in living cells by a mechanism called allosteric control; proteins are regulated by other molecules that bind to their surface, inducing a change of conformation, or distortion in the shape, of the protein, making the

protein either active or inactive. An artificial nanoscale mechanism of allosteric control is based on mechanical tension by chemically stringing a short piece of DNA around the protein and controlling the stiffness by inserting a molecular spring on the protein. The protein can be switched on and off by changing the stiffness of the DNA. Gluing together of two disparate pieces of the cell's molecular machinery, a protein and a piece of DNA, creates a spring-loaded protein which can be turned on and off. This approach to protein engineering can lead to a new generation of targeted "smart" drugs that are active only in cells where a certain gene is expressed, or a certain DNA sequence is present. Such drugs would have reduced side effects. Another application for the new molecules is as amplified molecular probes. Currently it is difficult for scientists to study a single live cell and find what gene it is expressing, but with an amplified molecular probe, one could inject the probe into a single cell and detect that the cell is expressing a specific gene. An amplified molecular probe would make it possible to study the individuality of cells, with applications in stem cell research and early detection of disease.

Role of Nanoparticles in Self-Assembly of Proteins

In their physical dimensions, surface chemistry, and degree of anisotropic interactions in solution, CdTe nanoparticles are like proteins. How to direct and control the self-assembly of nanoparticles is a fundamental question in nanotechnology. Nanocrystals in a fluid can be induced to assemble into free-floating sheets the same way some protein structures form in living organisms. The sheets, which can appear colored under UV illumination from bright green to dark red depending on the nanoparticle size, are made from cadmium telluride crystals, a material used in solar cells. Computer simulation and concurrent experiments have demonstrated that the dipole moment, small positive charge, and directional hydrophobic attraction are the driving forces for the self-organization process. This establishes an important connection between two basic building blocks in biology and nanotechnology, i.e., proteins and nanoparticles, which is important for assembling materials from the bottom up for applications ranging from drug delivery to energy.

Role of Nanotechnology in Peptide Engineering

Several types of self-assembling peptide systems have been developed, e.g., peptide nanotubes and nanovesicles. These self-assembling peptide systems are simple, versatile and easy to produce and represent a significant advance in the molecular engineering. Protein design studies using coiled coils have illustrated the potential of engineering simple peptides to self-associate into polymers and networks. Although basic aspects of self-assembly in protein systems have been demonstrated, it remains a major challenge to create materials whose large-scale structures are well determined from design of local protein-protein interactions. A helical peptide has been designed by using phased hydrophobic interactions to drive assembly into nanofilaments and nanofibrils. In this structure, the nanostructures designed are characterized by

biophysical methods such as dynamic light scattering and AFM to study their behavior on surfaces. The assembly of such structures can be predictably regulated by using various environmental factors such as pH and specifically designed "capping" peptides. This ability to regulate self-assembly is a critical feature in creating smart peptide biomaterials.

QD-Protein nanoassembly

An intein-based method for site-specific conjugation of QDs to target proteins in vivo has been described, which enables the covalent conjugation of any nanostructure and/or nanodevice to any protein and thus the targeting of such material to any intracellular compartment or signaling complex within the cells of the developing embryo (Charalambous et al. 2009). In vivo intein-splicing produces fully functional conjugates that can be monitored in real time within live embryos. Use of Near Infra Red (NIR)-emitting QDs allows monitoring of QD-conjugates within the embryo at depths where enhanced green fluorescent protein is undetectable demonstrating the advantages of QD's for this type of experiment.

Single Cell Nanoprobe for Studying Gene Expression of Individual Cells

The localization of specific mRNA generates cell polarity by controlling the translation sites of specific proteins. Although most of these events depend on differences in gene expression, no method is available to examine time dependent gene expression of individual living cells. In situ hybridization (ISH) is a powerful and useful method for detecting the localization of mRNAs, but it does not allow a time dependent analysis of mRNA expression in single living cells because the cells need to be fixed for mRNA detection. To overcome these issues, the extraction of biomolecules such as mRNAs, proteins, and lipids from living cells should be performed without severe damage to the cells. A single cell nanoprobe (SCN) method to examine gene expression of individual living cells is available by using AFM without killing the cells. The SCN method has been compared with ISH (Uehara et al. 2007). Spatial beta-actin mRNA expression in single living cells was examined first, with the SCN method, and then the same cells were subjected to ISH for beta-actin mRNA. In the SCN method, quantity of beta-actin mRNA was analyzed by quantitative PCR and in ISH intensity of ISH was used as a parameter of concentration of beta-actin mRNA. The results showed that intensity of ISH as well as quantity of beta-actin mRNA detected by the SCN method is higher. Thus, SCN is a suitable and reliable method to examine mRNAs at medium or higher expression level.

Study of Proteins by Atomic Force Microscopy

In contrast to other methods, specimens prepared for AFM remain in a plastic state, which enables direct observation of the dynamic molecular response, creating unique opportunities for studying the structure–function relationships of proteins and their functionally relevant assemblies. Electron crystallography and AFM enable the study of 2D membrane protein crystals. While electron crystallography provides atomic scale 3D density maps, AFM gives insight into the surface structure and dynamics at sub-nanometer resolution. Importantly, the membrane protein studied is in its native environment and its function can be assessed directly. The approach allows both the atomic structure of the membrane protein and the dynamics of its surface to be analyzed.

Comparisons of AFM topographs with protein structures determined by electron microscopy and X-ray crystallography have shown excellent agreement within a lateral resolution of <1 nm and a vertical resolution of ~0.1 nm. AFM application in imaging and nanomanipulation include the extraction of chromosomal DNA for genetic analysis, the disruption of antibody-antigen bonds, the dissection of biological membranes, the nanodissection of protein complexes, and the controlled modulation of protein conformations.

Observing proteins in their native environment is a prerequisite for the proper assessment of function. Conformational changes of molecular assemblies can be observed by time-lapse AFM; however, such experiments lack the time resolution required to observe the turnover of most biological 'machineries' owing to the relatively long time needed to record a topograph. One solution to this problem is to image the static conformations associated with different functional states of a biological macromolecule. Alternatively, the imaging speed of the AFM can be enhanced.

Study of Proteomics at Single Molecule Level

Study of Protein Synthesis and Single-Molecule Processes

All life relies on the actions and reactions of single molecules within cells but these molecules are so tiny that they have long eluded direct, real-time investigation using conventional light microscopes. Breakthrough technologies are enabling researchers to have an unprecedented view into the workings of individual molecules.

Single-molecule methods enable observation of the stepwise movement of aminoacyl-tRNA (aa-tRNA) into the ribosome during selection and kinetic proof-reading using single-molecule fluorescence resonance energy transfer (smFRET). Intermediate states in the pathway of tRNA delivery were observed using antibiotics and nonhydrolyzable GTP analogs. Three unambiguous FRET states have been identified corresponding to initial codon recognition, GTPase-activated and fully

accommodated states. The antibiotic tetracycline blocks progression of aa-tRNA from the initial codon recognition state, whereas cleavage of the sarcin-ricin loop impedes progression from the GTPase-activated state. These data support a model in which ribosomal recognition of correct codon-anticodon pairs drives rotational movement of the incoming complex of EF-Tu-GTP-aa-tRNA toward peptidyl-tRNA during selection on the ribosome. This is the basis of a mechanistic model of initial selection and proofreading.

Subsequently, tRNA molecules fluctuate between two configurations assigned as classical and hybrid states. The lifetime of classical and hybrid states, measured for complexes carrying aa-tRNA and peptidyl-tRNA at the A site, shows that peptide bond formation decreases the lifetime of the classical-state tRNA configuration by approximately six-fold. These data suggest that the growing peptide chain plays a role in modulating fluctuations between hybrid and classical states. smFRET has also been used to observe aa-tRNA accommodation coupled with elongation factor G-mediated translocation. Dynamic rearrangements in tRNA configuration are also observed after the translocation reaction. This work underscores the importance of dynamics in ribosome function and demonstrates single-particle enzymology in a system of more than two components.

Use of these technologies enable collection of photons of light coming from a single molecule. This information reports on a biomolecule's location, its interaction with other molecules, and tiny motions within the molecule itself. These tools allow view of an enzymatic reaction from the very intuitive perspective of movements. Enzymes are molecular machines with moving parts but these motions are on the order of a billionth of a centimeter. Nanoscale technologies will help to understand the mechanism of the ribosome, which is an assembly of about 60 different molecules working together, to read the instructions for making new proteins coded in DNA. These instructions are presented to the ribosome in the form of messenger RNA (mRNA). The process of translating mRNA instructions into protein involves the selection by the ribosome of adaptor RNA molecules, called transfer RNA (tRNA). It's the selection of specific tRNA molecules that determines the relationship between the gene sequence and the sequence of the resulting protein. The reaction between tRNA and the ribosome is the basis of what is called the universal genetic code. Ribosome is important for cell function and human health. Because protein synthesis is crucial to the life cycle of all bacteria, roughly 50% of antibiotics used today target ribosomal function. Ribosomal function is also a key to the success or failure of deadly viral infections such as HCV and HIV. Cancer cells, too, rely on protein synthesis to survive and multiply, so drugs that block ribosomal function in a cancer-specific manner might prove safe and effective chemotherapy. Genetic aberrations in the DNA-ribosome relationship can cause the enzyme to produce faulty proteins that trigger cystic fibrosis and other inherited illnesses. Understanding the mechanism of the ribosome may be a fundamental first step for developing antibiotics, cancer therapies, and antiviral drugs. The ribosome may 1 day even be a target for gene therapy.

Protein Expression in Individual Cells at the Single Molecule Level

Measurements single cells usually lack the sensitivity to resolve individual events of protein production. A microfluidic-based assay enables real-time observation of the expression of beta-galactosidase in living *E. coli* cells with single molecule sensitivity. It revealed that protein production occurs in bursts, with the number of molecules per burst following an exponential distribution. The two key parameters of protein expression – the burst size and frequency – can be either determined directly from real-time monitoring of protein production or extracted from a measurement of the steady-state copy number distribution in a population of cells. Application of this assay to probe gene expression in individual budding yeast and mouse embryonic stem cells demonstrates its generality. Many important proteins are expressed at low levels, and are thus inaccessible by current genomic and proteomic techniques. This microfluidic single cell assay opens possibilities for system-wide characterization of the expression of these low copy number proteins.

Single-Molecule Mass Spectrometry Using Nanotechnology

A 2D method for mass spectrometry (MS) in solution is based on the interaction between a nanometer-scale pore and analytes (Robertson et al. 2007). The technique involves creating a lipid bilayer membrane like those in living cells, and "drilling" a pore in it with a protein (α -hemolysin) produced by the *Staphyloccoccus aureus* bacteria specifically to penetrate cell membranes. Charged molecules (such as singlestranded DNA) are forced one-at-a-time into the nanopore, which is only 1.5 nm at its smallest point, by an applied electric current. As the molecules pass through the channel, the current flow is reduced in proportion to the size of each individual chain, allowing its mass to be easily derived. In this experiment, various-sized chains in solution of the uncharged polymer polyethylene glycol (PEG) were substituted for biomolecules. Each type of PEG molecule reduced the nanopore's electrical conductance differently as it moved through, allowing the researchers to distinguish one size of PEG chain from another. Because the dimensions of the lipid bilayer and the α -hemolysin pore, as well as the required amount of electrical current, are at the nanoscale level, the single-molecule mass spectrometry technology may 1 day be incorporated into "lab-on-a-chip" molecular analyzers and single-strand DNA sequencers. This single-molecule analysis technique could prove useful for the realtime characterization of biomarkers (i.e. nucleic acids, proteins, or other biopolymers). With automated, unsupervised analytical and statistical methods, this technique should prove viable as a generalized analytical technique with nanopore arrays containing nanopores both with specific affinities for single biomarkers and with nonspecific transducers. In situ monitoring of cellular metabolism with such arrays should provide the sensitivity to monitor subtle changes observed through the release of biomarkers.

Nanoelectromechanical systems provide unparalleled mass sensitivity, which is now sufficient for the detection of individual molecular species in real time. In a nanoelectromechanical-mass spectrometry system, nanoparticles and protein species are introduced by electrospray injection from the fluid phase in ambient conditions into vacuum, and are subsequently delivered to the system's detector by hexapole ion optics (Naik et al. 2009). Precipitous frequency shifts, proportional to the mass, are recorded in real time as analytes adsorb, one by one, onto a phase-locked, ultrahighfrequency nanoelectromechanical resonator. These first nanoelectromechanical system-mass spectrometry spectra, obtained with modest mass sensitivity from only several hundred mass adsorption events, indicate the future capabilities of this approach. Substantial improvements are feasible in the near term, some of which are unique to nanoelectromechanical system based-mass spectrometry.

Role of Nanotechnology in Study of Membrane Proteins

Nanoparticles for Study of Membrane Proteins

As a large fraction of proteins are likely to be membrane-bound, technical improvements are needed in the analysis of membrane proteins. An optical method for visualization of membrane proteins labeled with 10-nm gold nanoparticles in cells is based on photothermal interference contrast. The high sensitivity of the method and the stability of the signals allow 3D imaging of individual nanoparticles without the drawbacks of photobleaching and blinking inherent to fluorescent markers. The photothermal interference contrast method provides an efficient, reproducible, and promising way to visualize low amounts of proteins in cells by optical means.

Nanotube-vesicle networks with reconstituted membrane protein from cells and with interior activity have been defined by an injection of microparticles or molecular probes. The functionality of a membrane protein after reconstitution is verified by single-channel ion conductance measurements in excised inside-out patches from the vesicle membranes. The distribution of protein, determined by fluorescence detection, in the network membrane is homogeneous and can diffuse via a nanotube connecting two vesicles. This system can model a variety of biological functions and complex biological multicompartment structures and might serve as a platform for constructing complex sensor and computational devices.

Study of Single Protein Interaction with Cell Membrane

Aerogel, a semi-transparent and lightweight silica substance, has potential applications in biosensors and lab-on-a-chip devices. Formation of fluid planar biomembranes has been reported on hydrophilic silica aerogels and xerogels. Scanning electron microscopy shows the presence of interconnected silica beads of $\sim 10-25$ nm in diameter and nanoscale open pores of comparable size for the aerogel and grain size

of \sim 36–104 nm with \sim 9–24 nm diameter pores for the xerogel. Aerogel behaves like a living cell membrane and has been used to study single protein interaction with cell membrane.

Aerogel has advantages over most artificial membranes that are used in current studies. Most artificial membranes lack functionality because they are one-sided. Proteins can penetrate these membranes only on one side instead of both as in case of natural membranes in cells. The aerogel is unique in that it is accessible on both sides, just like the lipid bilayers that form actual membranes. This technique can be used for the detection of diseases in cases in which there is a need to study the specific protein involved. The researchers will not only test the traffic of molecules through their synthetic silica membranes but also develop aerogels out of new materials. Future aerogel materials will be nontoxic so that they may eventually be used in clinical trials. Possible materials used include aluminum oxide, carbon and even sugar-based compounds.

Quantum Dots to Label Cell Surface Proteins

Antibody-based labeling has been used for targeting quantum dots (QDs) to cells but there are two problems: the size of the QD conjugate after antibody attachment and the instability of many antibody-antigen interactions. One way to overcome these limitations is to tag the mammalian cell surface proteins with acceptor peptide (AP), which can be biotinylated by biotin ligase added to the medium, while endogenous proteins remain unmodified. The biotin group then serves as a handle for targeting streptavidin-conjugated-QDs. QDs have been targeted to cell surface cyan fluorescent protein and epidermal growth factor receptor in HeLa cells and to alpha-amino-3-hydroxy-5-methyl-4-isoxazolepropionate (AMPA) receptors in neurons. Labeling is specific for the AP-tagged protein, and is highly sensitive. Thus, biotin ligase labeling provides a specific, rapid, and generally applicable method for detecting and tracking cell surface proteins.

Study of Single Membrane Proteins at Subnanometer Resolution

High-resolution AFM enables observation of substructures of single membrane proteins at subnanometer resolution as well as their conformational changes, oligomeric state, molecular dynamics and assembly. Complementary to AFM imaging, single-molecule force spectroscopy experiments enable detection of molecular interactions established within and between membrane proteins. The sensitivity of this method makes it possible to detect the interactions that stabilize secondary structures such as transmembrane α -helices, polypeptide loops and segments within. It has elucidated unfolding and refolding pathways of membrane proteins as well as their energy landscapes. These approaches will provide insights into membrane protein structure, function, and unfolding. They could help to answer key questions on the molecular basis of certain neuropathological disorders.

Self-Assembling Peptide Scaffold Technology for 3D Cell Culture

Biomaterial scaffolds are components of cell-laden artificial tissues and transplantable biosensors. Some of the most promising new synthetic biomaterial scaffolds are composed of self-assembling peptides that can be modified to contain biologically active motifs. Peptide-based biomaterials can be fabricated to form 2D and 3D structures.

Until recently, 3D cell culture has required either animal-derived materials, with their inherent reproducibility and cell signaling issues, or much larger synthetic scaffolds, which fail to approximate the physical nanometer-scale and chemical attributes of native ECM. PuraMatrixTM (3DM Inc) nanometer-sized fibers provide a scaffold encapsulating cells in 3D and allow defined cell culture conditions, cell migration, nutrient diffusion, and cell harvesting. The hydrogels are composed of short strand of standard amino acids and 99.5% water, which then self-assemble into very fine fibers resembling a bare extracellular matrix (ECM). Researchers in the fields of cancer biology, stem cell biology, and tissue engineering have been the first to realize that ECM and a tuned 3D microenvironment are critical for the proper understanding required for drug discovery, cell biology, and cell therapy development. Mesenchymal stem cells (MSCs) can differentiate into mature osteoblasts to form mineralized matrices within the synthetic self-assembling hydrogel scaffold.

For the first time, the cell biology and drug discovery communities now have a biocompatible bare ECM which can be combined with relevant proteins and growth factors to more closely resemble in vivo milieu, and which is compatible with cGMP requirements for cell therapy, medical device and bioproduction applications. The PuraMatrix gels have undergone extensive in vivo toxicology safety testing.

There is a growing trend in 3D cell culture, moving cell biology research away from flat 2D cell cultures in traditional petri dishes. Some of the pioneers in 3D cell culture lend their observations that 3D microenvironments can radically alter cell behavior, enabling cells to mimic in vivo responses to drug targets and medical therapies much more accurately. Given the growing body of literature, drug discovery efforts at major pharmaceutical and biotechnology companies are beginning to adopt 3D culture techniques in their cell-based assays, especially in the context of high content screening. For creating synthetic ECM scaffolds and tuned 3D microenvironments, products like PuraMatrix have proven to yield better data while also reducing the number of animals used for expensive in vivo testing.

Nanobiotechnology and Ion Channels

Ion channels provide the basis for the regulation of electrical excitability in the central and peripheral nervous systems. They are proteins that are equipped with a membrane-spanning ion conducting pore. Disturbances in ion channels are cause of

many neurological disorders. Ion channels were traditionally studied by the patch clamp technique, which was derived from the conventional voltage clamp method. This method is now supplemented by nanotechniques, which are being used to study cell membranes and their proteins. Nanoscopy is the characterization of the membrane channels by techniques that resolve their morphological and physical properties and dynamics in space and time in the nano range. These techniques make the study of structure and function of single channel molecules in living cells possible and are currently being developed for automated and high throughput measurements and fluorescence. Nanopores and their applications were described in Chap. 2 and earlier in this chapter.

AFM for Characterization of Ion Channels

AFM has been combined directly with the patch clamp technique for the characterization of biological electromechanical transduction channels in living inner and outer hair cells of the cochlea. Using an AFM stylus with a tip diameter of only a few nanometers, it is possible to displace individual stereocilia of cochlear hair cells, resulting in opening of single transduction channels. In contrast to the outside-out and the inside-out patch clamp configuration, this technique enables investigation of single mechanosensitive ion channels in entire cells.

Aquaporin Water Channels

Aquaporin (AQP) water channels are proteins that enable water to move rapidly into and out of cells. The atomic structure of mammalian AQPs illustrates how this family of proteins is freely permeated by water but not protons (hydronium ions, H3O+). AQP4 water channels can assemble in cell plasma membranes in orthogonal arrays of particles, which can be visualized by QD single particle tracking.

Definition of the subcellular sites of expression predicted their physiological functions and potential clinical disorders. Analysis of several human disease states has confirmed that aquaporins are involved in these including abnormalities of kidney function, loss of vision, brain edema, starvation, and arsenic toxicity. Research in this area requires nanoscale both in size and time scales. In molecular dynamics simulations of water in short (0.8 nm) hydrophobic pores the water density in the pore fluctuates on a nanosecond time scale. In long simulations (460 ns in total) at pore radii ranging from 0.35 to 1.0 nm, researchers have quantified the kinetics of oscillations between a liquid-filled and a vapor-filled pore. One cannot assume that the behavior of water within complex biological pores may be determined by extrapolation from the knowledge of the bulk state or short simulations alone. Simulations aimed at collective phenomena such as hydrophobic effects may require simulation times >50 ns.

NanopatchTM for Study of Ion Channels at Single Molecule Level

Nanopatch[™] (Electronic Biosciences) measures the activity of ion channels at the single molecule level to provide a better understanding of their structure and function. Currently, single molecule recordings are typically obtained through either patch clamp or planar lipid bilayer (PLB) methods. Although patch clamp has delivered much higher sensitivity than PLB platforms, it requires extensive user training, complicated operations, and a wide array of expensive instruments. In contrast, PLB methods are easier to implement, allow for finer control over experimental conditions such as lipid and electrolyte composition, and enable investigation of ion channels present in intracellular membranes. However, standard PLB platforms produce high noise, thus precluding the measurement of low conductance ion channels except at very low bandwidth.

NanopatchTM combines the best of both worlds by providing the high sensitivity of patch clamp with PLB versatility. The quartz nanopore membranes (QNM) at the heart of the NanopatchTM system provide very low capacitance and dielectric loss, enabling high bandwidth measurements with exceptionally low noise. The QNM, containing a single conical shaped nanopore, provides an excellent solid support structure for lipid bilayers in ion channel recordings due to the large electrical resistivity of fused quartz. Electrical measurements demonstrate that the leakage current through 1,2-diphytanoyl-sn-glycero-3-phosphocholine (DPhPC) bilayers suspended across a 500-1000 nm radius QNM orifice is immeasurably small, corresponding to a bilayer resistance greater than 10(12) ohms. Translocation of single-stranded DNA oligomers through a protein ion channel (alpha-hemolysin) reconstituted in a DPhPC bilayer suspended across the QNM orifice has been demonstrated (Schibel et al. 2010). Electronic Biosciences and its collaborators at the University of Utah have also successfully demonstrated the insertion of bacterial porins aHL and gramicidin, multimeric proteins such as cardiac ryanodine receptors (RyR2), and the cold activated transient receptor potential melastatin channel, Trpm8. Proteins have been incorporated either through liposome formation, or in some cases, by direct insertion from detergent solubilized solutions. Nanopore detection of individual DNA abasic sites in single molecules was also achieved by this method (An et al. 2012).

Remote Control of Ion Channels Through Magnetic-Field Heating of Nanoparticles

An approach to remotely activate temperature-sensitive cation channels in cells is based on radio-frequency magnetic-field heating of nanoparticles (Huang et al. 2010). Superparamagnetic ferrite nanoparticles were targeted to specific proteins on the plasma membrane of cells expressing TRPV1, and heated by a radio-frequency

magnetic field. Using fluorophores as molecular thermometers, it was shown that the induced temperature increase is highly localized. Thermal activation of the channels triggers action potentials in cultured neurons without observable toxic effects. This approach can be adapted to stimulate other cell types and, moreover, may be used to remotely manipulate other cellular machinery for novel therapeutics.

Role of Nanobiotechnology in Engineering Ion Channels

Biological ionic channels contain precisely arranged arrays of amino acids that can efficiently recognize and guide the passage of K^+ or Na⁺ across the cell membrane. However, the design of inorganic channels with novel recognition mechanisms that control the ionic selectivity remains a challenge. A design for a controllable ion-selective nanopore (molecular sieve) is based on a single-walled carbon nanotube with specially arranged carbonyl oxygen atoms modified inside the nanopore, which was inspired by the structure of potassium channels in membrane spanning proteins (Gong et al. 2010). Molecular dynamics simulations show that the remarkable selectivity of this nanopore is attributed to the hydration structure of K⁺ or Na⁺ confined in the nanochannels, which can be precisely tuned by different patterns of the carbonyl oxygen atoms.

Supported membrane nanodevices can be based on natural or artificial ion channels embedded in a lipid membrane deposited on a chip wafer. Membrane conductance is modulated by biorecognitive events, with the use of intrinsic binding sites of the ion channel or via artificial sites fused to the channel protein. Artificial ion gates are constructed by coupling a specific ligand for the analyte near the channel entrance or a site important to triggering channel conformation. The binding event leads to the closure of the ion channel or induces a conformational change of the channel, reducing the ion flux. The signal transduced from the device is the decrease in the ion flux-induced electron current at a silver-silver chloride electrode at ultimate single-molecule sensitivity.

Among the natural ion channels, gramicidin A, a transport antibiotic, was found to be most suitable, and thus was used to set up prototypes of membrane biochips, using self-association of the dimer. Covalent dimerization-based devices make use of the down-regulation of the permanently open membrane-spanning bisgramicidine ion channel. The reactive group at the C-terminus, a hydroxy group, allows precise coupling of the analyte-binding moiety in gramicidin as well as bisgramicidin. The device is set up with bilayer membranes deposited on apertures of a hydrophobic frame structure produced via microlithography, facing an aqueous or hydro-gel micro-environment on both sides, constructing black lipid membranes or patchclamp devices "on chip." The setup of the device needs gel membrane supports that allow membrane formation and contribute to the stability of the bilayer by exposure of functional groups that promote electrostatic interaction and formation of hydrogen bridges and enable the introduction of covalent spacers and anchors. Photo-cross-linked polyvinylpyrrolidone and polyacrylamide, electropolymerized polydiaminobenzene and coated agarose, as well as various chemical modifications of these polymers, were employed as membrane supports. With optimized assemblies, the membrane support enables the formation of stable bilayer membranes. Supports, with and without hydrophilic and hydrophobic anchors, have been studied for promoting the formation of a self-assembled membrane, for their electric resistance, and for the capability to insert functional ionophores. All components, including novel chemically engineered ion channels, novel amphiphilic lipids, a microlithographically designed chip, isolating polymer frames, and a hydrogel membrane support, are combined in the new bionanodevice. Sensitivity and specificity were demonstrated, e.g. by use of an antibody-antigen coupling that downregulates ion flux through the membrane channel. Single ion channels incorporated in the supported lipid bilayer gave stable signals at an operational stability for several hours, which is sufficient to test and screen for membrane receptors, but still insufficient to use this device as a sensor for off-site application. Further optimization to increase operational and storage stability has been achieved by several groups to enable broad application of these devices.

Synthetic nanopore membranes can mimic the function of ligand-gated ion channels. It has been shown that transmembrane ion current in a hydrophobic alumina nanopore membrane can be switched from an "off" state to an "on" state by exposure of the membrane to hydrophobic ionic surfactants. However, in biological channels there are no electrodes, and the ion current is driven by an electrochemical potential difference across the cell membrane. This function of the ligand-gated ion channel can be mimicked by applying a porous battery cathode film to one face of the hydrophobic alumina membrane and a porous battery anode film to the other face. Like the naturally occurring channel, such a membrane has a built in electrochemical potential difference across the membrane. In the absence of the ligand, the membrane is in its "off" state, and the electrochemical potential difference cannot be utilized to drive a transmembrane ion current. In contrast, when the ligand is detected, the membrane switches to its "on" state and the transmembrane battery discharges, producing a corresponding transmembrane ion current.

Nanobiotechnology for Single Cell Analysis

The development of more intricate devices for the analysis of small molecules and protein activity in single cells, which are difficult to measure using current methods, would advance our knowledge of cellular heterogeneity and signaling cascades. A nanokit was generated by filling a nanometer-sized capillary with a ring electrode at the tip with components from traditional kits, and it was applied to characterize the reactivity and concentrations of cellular compounds in single cells (Pan et al. 2016). At the tip, femtoliter amounts of the kit components were reacted with the analyte to generate hydrogen peroxide for the electrochemical measurement by the ring electrode. Taking advantage of the nanotip and small volume injection, the nanokit was easily inserted into a single cell to determine the intracellular glucose levels and sphingomyelinase activity, which had rarely been achieved. High cellular

heterogeneities of these two molecules were observed, showing the significance of the nanokit. Compared with the current methods that use a complicated structural design or surface functionalization for the recognition of the analytes, the nanokit has adapted features of the well-established kits and integrated the kit components and detector in 1 nm-sized capillary could be applied to the analysis of cellular compounds that are challenging. The simple and low-cost device provides a specific strategy that should facilitate single-cell analyses.

Nanotechnology and Bioinformatics

Bioinformatics, also referred to as computational biology, is the use of highly sophisticated computer databases to store, analyze and share biological information. This is a discipline at the interface of computer science, mathematics and biology. The tremendous amount of data generated by new biotechnologies requires bioinformatic tools for analysis. Analyzing how multiple genes function together can produce terabytes of data. But as nanotech enables greater sensing and collecting of data, the information flow could become measured in petabytes, or quadrillion bytes of information. Bioinformatics is essential for microarray data analysis and even more so for nanoarray data. In nanotechnology, the investigation of behavior and properties across a wide range of length scales is vital. Over the past two decades, computational techniques have evolved to the point that they now cover all length and time scales from the electronic to the macroscale, the realm of nanotechnology.

In the future, it may be possible to fully model an individual cell's structure and function by computers connected to nanobiotechnology systems. Such a detailed virtual representation of how a cell functions might enable scientists to develop novel drugs with unprecedented speed and precision without any experiments in living animals. An example of application of this approach is construction of 3D nano-map of synapse.

SyNAPSE (Systems of Neuromorphic Adaptive Plastic Scalable Electronics) is a DARPA (Defense Advanced Research Projects Agency)-funded program to develop electronic neuromorphic machine technology that scales to biological levels (http://www.artificialbrains.com/darpa-synapse-program). It is an attempt to build a new kind of computer with similar form and function to the mammalian brain; such artificial brains would be used in robots. The program started in 2008 and is scheduled to run until 2016.

3D Nano-map of Synapse

Detailed nano-map of the 3D terrain of a neuronal synapse shows the tiny spines and valleys resolved at nanometer scale. It is already changing the conventional views of the synaptic landscape. A biologically accurate computer simulation of synaptic function combines 3D electron microscope maps with physiological measurements from real neurons. The textbook view of the synapse describes it as a place where rifle-like volleys of neurotransmitter are launched from one defined region of the sending neuron to another defined target on the receiving neuron. In contrast, the new data suggest that synapse can act like a shotgun, firing buckshotlike bursts of neurotransmitter to reach receptors arrayed beyond the known receiving sites. This method was applied to study the chick ciliary ganglion, which is a cluster of neurons that connect the brain to the iris of the eve. It launches the neurotransmitter acetylcholine from sac-like vesicles across the synapse to two types of receptors, called α 7 and α 3 nicotinic receptors. The image of this ganglion is not one of a simple synapse with a single release site, but multiple release sites. And it shows $\alpha 3$ receptors within the postsynaptic region, but α 7 receptors outside this region. This model showed that if the neurotransmitter were released only from vesicles in active zones, as previously believed, it would be a poor match to actual properties of the neuron. But according to the new model of neurotransmitter release, called ectopic release, the location of α 7 receptors can match the actual properties of the synapse very accurately. The new 3D modeling technique could offer a powerful tool for understanding neurological disease, such as myasthenia gravis. The model can also be used as a tool for drug discovery. Drug discovery efforts can be focused on the site of the anomaly.

References

- An N, Fleming AM, White HS, Burrows CJ. Crown ether-electrolyte interactions permit nanopore detection of individual DNA abasic sites in single molecules. Proc Natl Acad Sci U S A. 2012;109:11504–9.
- Bishnoi SW, Rozell CJ, Levin CS, et al. All-optical nanoscale pH meter. Nano Lett. 2006;6: 1687–92.
- Boukany PE, Morss A, Liao WC, et al. Nanochannel electroporation delivers precise amounts of biomolecules into living cells. Nat Nanotechnol. 2011;6:747–54.
- Chakraborty B, Sha R, Seeman NC. Colloquium paper: a DNA-based nanomechanical device with three robust states. Proc Natl Acad Sci U S A. 2008;105:17245–9.
- Charalambous A, Andreou M, Skourides PA. Intein-mediated site-specific conjugation of quantum dots to proteins in vivo. J Nanobiotechnology. 2009;7:9.
- Chiu DT. Interfacing droplet microfluidics with chemical separation for cellular analysis. Anal Bioanal Chem. 2010;397:3179–83.
- Choi YS, Wood TD. Polyaniline-coated nanoelectrospray emitters treated with hydrophobic polymers at the tip. Rapid Commun Mass Spectrom. 2007;21:2101–8.
- Collins MC, Gunst PR, Cascio WE, et al. Labeling and imaging mesenchymal stem cells with quantum dots. Methods Mol Biol. 2012;906:199–210.
- Dashti A, Schwander P, Langlois R, et al. Trajectories of the ribosome as a Brownian nanomachines. Proc Natl Acad Sci U S A. 2014;111:17492–7.
- Feng Y, Zhang Y, Ying C, et al. Nanopore-based fourth-generation DNA sequencing technology. Genomics Proteomics Bioinformatics. 2015;13:4–16.
- Gong X, Li J, Xu K, et al. A controllable molecular sieve for Na+ and K+ ions. J Am Chem Soc. 2010;132:1873–7.
- Gourley PL, McDonald AE. Ultrafast nanoLaser device for detecting cancer in a single live cell. Sandia National Laboratories, Albuquerque, New Mexico, Report # SAND2007-7456, 2007.

- Han HS, Niemeyer E, Huang Y, et al. Quantum dot/antibody conjugates for in vivo cytometric imaging in mice. Proc Natl Acad Sci U S A. 2015;112:E3087.
- Heerema SJ, Dekker C. Graphene nanodevices for DNA sequencing. Nat Nanotechnol. 2016;11:127–36.
- Hohng S, Zhou R, Nahas MK, et al. Fluorescence-force spectroscopy maps two-dimensional reaction landscape of the Holliday junction. Science. 2007;318:279–83.
- Huang H, Delikanli S, Zeng H, et al. Remote control of ion channels and neurons through magnetic-field heating of nanoparticles. Nat Nanotechnol. 2010;5:602–6.
- Iwata F, Mizuguchi Y, Ko H, Ushiki T. Nanomanipulation of biological samples using a compact atomic force microscope under scanning electron microscope observation. J Electron Microsc. 2011;60:359–66.
- Jungmann R, Scheible M, Simmel FC. Nanoscale imaging in DNA nanotechnology. Wiley Interdiscip Rev Nanomed Nanobiotechnol. 2012;4:66–81.
- Koster DA, Palle K, Bot ES, et al. Antitumour drugs impede DNA uncoiling by topoisomerase I. Nature. 2007;448:213–7.
- Lin C, Rinker S, Wang X, et al. In vivo cloning of artificial DNA nanostructures. Proc Natl Acad Sci U S A. 2008;105:17626–31.
- Liu Y, Thomas A, Sohrabi S, et al. Antibody-coated nanoparticles are promising molecular probes for microscopic analysis of cell behavior. Nanomedicine (Lond). 2016;11:2383–6.
- Mamin HJ, Kim M, Sherwood MH, et al. Nanoscale nuclear magnetic resonance with a nitrogenvacancy spin sensor. Science. 2013;339:557–60.
- Mansfield E, Oreskovic TL, Rentz NS, Jeerage KM. Three-dimensional hydrogel constructs for exposing cells to nanoparticles. Nanotoxicology. 2014;8:394–403.
- Mehta SB, McQuilken M, Riviere JL, et al. Dissection of molecular assembly dynamics by tracking orientation and position of single molecules in live cells. Proc Natl Acad Sci U S A. 2016;113:E6352–61.
- Naik AK, Hanay MS, Hiebert WK, et al. Towards single-molecule nanomechanical mass spectrometry. Nat Nanotechnol. 2009;4:445–50.
- Nivala J, et al. Nanopore-based protein sequencing. Nat Biotechnol. 2013;31:247-50.
- Pan R, Xu M, Jiang D, et al. Nanokit for single-cell electrochemical analyses. Proc Natl Acad Sci U S A. 2016;113:11436–40.
- Park K, Jang J, Irimia D, et al. 'Living cantilever arrays' for characterization of mass of single live cells in fluids. Lab Chip. 2008;8:1034–41.
- Peng C, Palazzo RE, Wilke I. Laser intensity dependence of femtosecond near-infrared optoinjection. Phys Rev E. 2007;75:041903.
- Qian L, Winfree E, Bruck J. Neural network computation with DNA strand displacement cascades. Nature. 2011;475:368–72.
- Robertson JW, Rodrigues CG, Stanford VM, et al. Single-molecule mass spectrometry in solution using a solitary nanopore. Proc Natl Acad Sci U S A. 2007;104:8207–11.
- Rosen CB, Rodriguez-Larrea D, Bayley H. Single-molecule site-specific detection of protein phosphorylation with a nanopore. Nat Biotechnol. 2014;32:179–81.
- Seeman NC. An overview of structural DNA nanotechnology. Mol Biotechnol. 2007;37:246-57.
- Schibel AE, Edwards T, Kawano R, et al. Quartz nanopore membranes for suspended bilayer ion channel recordings. Anal Chem. 2010;82:7259–66.
- Shen Y, Nakajima M, Yang Z, et al. Design and characterization of nanoknife with buffering beam for in situ single-cell cutting. Nanotechnology. 2011;22:305701.
- Shukla GC, Haque F, Tor Y, et al. A boost for the emerging field of RNA nanotechnology. ACS Nano. 2011;5:3405–18.
- Singer A, Wanunu M, Morrison W, et al. Nanopore based sequence specific detection of duplex DNA for genomic profiling. Nano Lett. 2010;10:738–42.
- Uehara H, Kunitomi Y, Ikai A, Osada T. mRNA detection of individual cells with the single cell nanoprobe method compared with in situ hybridization. J Nanobiotechnol. 2007;5:7.
- Wei R, Martin TG, Rant U, Dietz H. DNA Origami Gatekeepers for solid-state nanopores. Angew Chem Int Ed Engl 2012;51:4864–4867.

- Yang AH, Moore SD, Schmidt BS, et al. Optical manipulation of nanoparticles and biomolecules in sub-wavelength slot waveguides. Nature. 2009;457:71–5.
- Zhang X, Tung CS, Sowa GZ, et al. Global structure of a three-way junction in a phi29 packaging RNA dimer determined using site-directed spin labeling. J Am Chem Soc. 2012;134:2644–52.

Chapter 4 Nanomolecular Diagnostics

Introduction

Clinical application of molecular technologies to elucidate, diagnose and monitor human diseases is referred to as molecular diagnosis. It is a broader term than DNA (deoxyribonucleic acid) diagnostics and refers to the use of technologies that use DNA, RNA (ribonucleic acid), genes or proteins as bases for diagnostic tests. The scope of the subject is much wider and includes in vivo imaging and diagnosis at single molecule level. A more detailed description of molecular diagnostics is presented elsewhere (Jain 2017a).

Because of the small dimension, most of the applications of nanobiotechnology in molecular diagnostics fall under the broad category of biochips/microarrays but are more correctly termed nanochips and nanoarrays. Nanotechnology-on-a-chip is a general description that can be applied to several methods. Some of these do not use nanotechnologies but merely have the capability to analyze nanoliter amounts of fluids.

Biochips, constructed with microelectromechanical systems on a micron scale, are related to micromanipulation, whereas nanotechnology-based chips on a nanoscale are related to nanomanipulation. Even though microarray/biochip methods employing the detection of specific biomolecular interactions are now an indispensable tool for molecular diagnostics, there are some limitations. DNA microarrays and ELISA rely on the labeling of samples with a fluorescent or radioactive tag – a highly sensitive procedure that is time-consuming and expensive.

The chemical modification and global amplification of the nucleic acid samples are achieved by polymerase chain reaction (PCR), which can introduce artifacts caused by the preferential amplification of certain sequences. Alternative label-free methods include surface plasmon resonance (SPR) and quartz crystal microbalance, which rely on mass detection. Nanotechnologies also provide label-free detection. Nanotechnology is thus being applied to overcome some of the limitations of biochip technology. This chapter focuses on the application of nanotechnologies to nucleic acid as well as protein diagnostics.

Nanodiagnostics

Nanomolecular diagnostics is the use of nanobiotechnology in molecular diagnostics and can be termed "nanodiagnostics" (Jain 2003). Numerous nanodevices and nanosystems for sequencing single molecules of DNA are feasible. It seems quite likely that there will be numerous applications of inorganic nanostructures in biology and medicine as biomarkers. Given the inherent nanoscale of receptors, pores, and other functional components of living cells, the detailed monitoring and analysis of these components will be made possible by the development of a new class of nanoscale probes. Biological tests measuring the presence or activity of selected substances become quicker, more sensitive and more flexible when certain nanoscale particles are put to work as tags or labels. Nanotechnology will improve the sensitivity and integration of analytical methods to yield a more coherent evaluation of life processes.

It is difficult to classify such a variety of technologies but various nanotechnologies with potential applications in molecular diagnostics are listed in Table 4.1. Nanotechnology on a chip was described in Chap. 2. Some of the other technologies will be described briefly in the following text using examples of commercial products. Applications in clinical laboratory have been reviewed elsewhere (Jain 2007).

 Table 4.1
 Classification of applications of nanotechnologies in molecular diagnostics

Nanotechnology to improve polymerase chain reaction (PCR)
Nanobiotechnology-based biochips and microarrays
Nanotechnology on a chip: nanobiochips
Nanotechnology in microfluidics: nanoarrays
Protein nanobiochips/nanoarrays
Nanoparticle technologies
Carbon nanotubes
Dendrimers
Gold particles
Magnetic nanoparticles
Nanobarcodes
Quantum dot technology
Nanoparticle probes
Nanowires
DNA nanomachines for molecular diagnostics
Nanoparticle-based immunoassays
DNA-protein and nanoparticle conjugates
Nanosensors
Cantilever arrays
Living spores as nanodetectors
Quartz nanobalance DNA sensor
Nanosensor glucose monitor
Photostimulated luminescence in nanoparticles
Optical biosensors: surface plasmon resonance technology
(continnued

Nanotechnology-based biomarkers
Nanoparticles for discovering biomarkers
Nanoproteomics and biomarkers
Nanosensors for measuring biomarkers in blood
Nanotechnology-based cytogenetics
Study of chromosomes by atomic force microscopy (AFM)
Quantum dot fluorescent in situ hybridization (FISH)
Nanoscale single molecule identification
Nanotechnology-based DNA sequencing
Nanopore-based DNA sequencing
Nanoparticle-based DNA sequencing
Imaging applications of nanoparticles
Computer tomography image enhancement by nanoparticles
Functionalized carbon nanotubes as ultrasound contrast agents
Nanoparticles as contrast-enhancing agents for magnetic resonance imaging
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Table 4.1 (continued)

Rationale of Nanotechnology for Molecular Diagnostics

Numerous nanodevices and nanosystems for sequencing single molecules of DNA are feasible. It is likely that there will be numerous applications of inorganic nano-structures in biology and medicine as markers:

- Nanoscale probes would be suitable for detailed analysis of receptors, pores, and other components of living cells that are on a nanoscale.
- Nanoscale particles, used as tags or labels, increase the sensitivity, speed and flexibility of biological tests measuring the presence or activity of selected substances
- Nanotechnology will improve the sensitivity and integration of analytical methods to yield a more coherent evaluation of life processes.

Nanoarrays for Molecular Diagnostics

Several nanoarrays and nanobiochips are in development (Jain 2017b). Some of these will be reviewed here.

Fullerene Photodetectors for Chemiluminescence Detection on Microfluidic Chip

Solution-processed thin-film organic photodiodes have been used for microscale chemiluminescence (Wang et al. 2007). The active layer of the photodiodes comprised a blend of the conjugated polymer poly(3-hexylthiophene) and a soluble

derivative of fullerene C60. The devices had an active area of $1 \text{ mm} \times 1 \text{ mm}$, and a broad-band response from 350 to 700 nm, with an external quantum efficiency of more than 50% between 450 and 550 nm. The photodiodes have a simple layered structure that allows integration with planar chip-based systems. To evaluate the suitability of the organic devices as integrated detectors for microscale chemiluminescence, a peroxyoxalate based chemiluminescence reaction (PO-CL) was monitored within a poly(dimethyl-siloxane) (PDMS) microfluidic device. Quantitation of hydrogen peroxide indicated excellent linearity and yielded a detection limit of 10 microM, comparable with previously reported results using micromachined silicon microfluidic chips with integrated silicon photodiodes. The combination of organic photodiodes with PDMS microfluidic chips offers a means of creating compact, sensitive and potentially low-cost microscale CL devices with wide-ranging applications in chemical and biological analysis and clinical diagnostics.

Microfluidics and Nanotech Tools for Single Cell Analysis

Single cell biology is crucial for understanding the heterogeneity that often confounds the interpretation of biological or biomedical measurements. Single cell analysis is being increasingly applied for unraveling the functional behavior of heterogeneous healthy tissue or pathomechanism of diseased tissues and response to therapy. In addition to flow- and mass-cytometry methods, most single cell analyses involve microfluidics and/or nanotechology. Because a single cell has only a certain number of copies of any given analyte. By isolating a single cell within a nanoliter or subnanoliter volume, copy numbers correspond to to detectable concentrations, with minimal contamination. Nanochips enable analyses of very small tissue samples. Microfluidics and nanotech tools for single-cell analysis are shown in Fig. 4.1.

Nanofluidic/Nanoarray Devices to Detect a Single Molecule of DNA

One of the more promising uses of nanofluidic devices is isolation and analysis of individual biomolecules, such as DNA, which could lead to new detection schemes for cancer. One approach to this entails construction of silicon nanowires on a substrate, or chip, using standard photolithographic and etching techniques, followed by a chemical oxidation step that converts the nanowires into hollow nanotubes. Using this process, one can reliably create nanotubes with diameters as small as 10 nm, although devices used for biomolecule isolation contain nanotubes with a diameter of 50 nm. To trap DNA molecules requires a device consisting of a silicon nanotube connecting two parallel microfluidic channels. Electrodes provide a source of current used to drive DNA into the nanotubes. Each time a single DNA molecule moves into the nanotube, the electrical current changes suddenly. The current returns to its baseline value when the DNA molecule exits the nanotube. On average, a DNA molecule remains within the

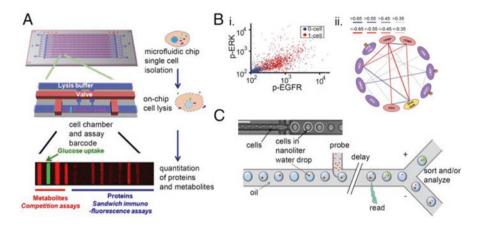


Fig. 4.1 Microfluidics and nanotech tools for single cell analysis. (a) Single-cell barcode chip (SCBC) in which individual cells are isolated within nanoliter or smaller volume microchambers within a microfluidics chip mounted on a microscope glass slide, which is patterned with a highdensity barcode for protein and/or metabolite assays from isolated single cells. Cells are lysed using the valved microchamber structure shown in the middle drawing, and the contents are captured on specific locations within the barcode array. The fluorescence intensities of the developed barcode stripes are related to calibration curves to yield the level of the specific analytes. (b) Sample of single-cell data taken on an SCBC. (i) The scatter plot shows the correlated levels of two phosphoproteins as measured from single cells (red dots) or zero-cell chambers (blue dots). (ii) A protein-protein correlation matrix from a multiplex SCBC protein and metabolite assay. (c) An illustration of a microfluidics platform for building a regular array of single cells within nanoliter droplets of water, entrained in oil. It shows some of the flexible design parameters that are used in this type of high-throughput assay. Cells can be probed with antibodies, viruses, mRNAencoded beads, NPs, etc. for a controllable amount of time, using a delay line or related method. Cells may be interrogated optically and sorted or otherwise analyzed at the protein, transcript, or functional level (Source: Heath 2015. By permission)

nanotube for about 7.5 msec, which should be sufficient to make a variety of analytical measurements that could reveal cancer-associated mutations. Optical and electrical circuitry is now being added to probe the trapped DNA molecules.

A nanostructured array platform, in which an electrophoretic particle entrapment system is used to immobilize nanoparticles coated with biological reagents, has been used to develop a highly sensitive immunoassay for detection of single biological molecules at multiple sites with nanometer scale precision (Han et al. 2013). Potential applications include those requiring portable, POC and real-time monitoring with high sensitivity.

The IrysChip (BioNano Genomics) for whole genome analysis has nanoscale channels on its surface that are specifically designed to enable a single long-strand DNA molecule to travel through, but prevent the molecule from folding back on itself. The platform is also anticipated to significantly reduce the cost and time needed for the extensive data and integrative analyses that have hindered widespread use of whole genome studies to date. It is expected to have broad application in systems biology, personalized medicine, pathogen detection, drug development and clinical research.

Protein Nanoarrays

Protein microarrays provide a powerful tool for the study of protein function. However, they are not widely used, in part because of the challenges in producing proteins to spot on the arrays. Protein microarrays can be generated by printing complementary DNAs onto glass slides and then translating target proteins with mammalian reticulocyte lysate. Epitope tags fused to the proteins allowed them to be immobilized in situ. This obviates the need to purify proteins, avoided protein stability problems during storage, and captured sufficient protein for functional studies. This technology has been used to map pairwise interactions among 29 human DNA replication initiation proteins, recapitulate the regulation of Cdt1 binding to select replication proteins, and map its geminin-binding domain.

NanoArray Assay System enables detection, identification, and quantitation of clinically relevant, low abundance proteins from a wide variety of sample types for applications such as biomarker analysis, translational medicine, and toxicology. These assays consume much smaller sample and reagent volumes than do traditional ELISA and bead-based assays, generating more proteomic data with less starting material and lowering assay costs for tests that are typically expensive to run.

Protein Nanobiochip

Biomarker proteins as early warning signs for diseases such as cancer can be identified for diagnostic purposes by finding their isoelectric points and their molecular weights. Isoelectric points are chemical features that refer to the electrical state of a molecule when it has no net charge. Conventional protein chips use a gel across which an electric current is applied to find the targeted protein's isoelectric points. In the protein nanobiochip, instead of being filtered through a block of gel, the protein molecules are separated by their isoelectric points by a capillary action as the proteins flow in a solution along channels in the chip. A chip measuring 21 mm² contains four sets of tiny channels in which the capillary action takes place. The protein molecules are then dried and irradiated by a laser. Their molecular weights are then measured by a mass spectrometer. The laser helps the proteins leave the chip, and the mass spectrometer is used to judge the molecular weights of the protein molecules in the samples by measuring how early they reach a detector. In the mass spectrometer, light molecules fly faster than heavy ones in an electric field. The mass spectrometer judges the weight of the molecules by monitoring the timing of when each molecule reaches a detector. In addition to being faster than techniques that use gel blocks, nanobiochip also needs blood samples of about 1 µL compared to about 20 µL or more that are needed using gel-based techniques.

Silver Nanorod Array for On-chip Detection of Microbes and Chemicals

Silver nanorod (AgNR) array substrates can be used for on-chip separation and detection of chemical mixtures by combining ultra-thin layer chromatography (UTLC) and SERS (Chen et al. 2012). The UTLC-SERS plate consists of an AgNR array fabricated by oblique angle deposition. The capability of the AgNR substrates to separate the different compounds in a mixture was explored using a mixture of four dyes and a mixture of melamine and Rhodamine 6G at varied concentrations with different mobile phase solvents. After UTLC separation, spatially-resolved SERS spectra were collected along the mobile phase development direction and the intensities of specific SERS peaks from each component were used to generate chromatograms. The limits of detection are between 10-5 and 10-6 M. Furthermore, we show that the coupling of UTLC with SERS improves the SERS detection specificity, as small amounts of target analytes can be separated from the interfering background components. The nanorods act as the detection medium as well as the separation medium, so it is a two-in-one system. This single-step method can rapidly and accurately detect viruses, bacteria and chemical contaminants. In a series of studies, the scientists could detect compounds such as lactic acid and the protein albumin in highly diluted samples and in mixtures that included dyes and other chemicals. Their results suggest that the same system could be used to detect pathogens and contaminants in biological mixtures such as food, blood, saliva and urine. Whereas the detection of viruses using techniques such as PCR can take days or even weeks and requires fluorescent labels, the on-chip method yields results in <1 h without the use of molecular labels.

AFM for Molecular Diagnostics

Nanofountain AFM Probe

Nanofountain AFM probe (NFP) has been used for nanofabrication of protein dot and line patterns (Loh et al. 2008). Biomolecules are continuously fed in solution through an integrated microfluidic system, and deposited directly onto a substrate. Deposition is controlled by application of an electric potential of appropriate sign and magnitude between the probe reservoir and substrate. Submicron dot and line molecular patterns were generated with resolution that depended on the magnitude of the applied voltage, dwell time, and writing speed. By using an energetic argument and a Kelvin condensation model, the quasi-equilibrium liquid-air interface at the probe tip was determined. The analysis revealed the origin of the need for electric fields in achieving protein transport to the substrate and confirmed experimental observations suggesting that pattern resolution is controlled by tip sharpness and not overall probe aperture. As such, the NFP combines the high-resolution of dip-pen nanolithography with the efficient continuous liquid feeding of micropipettes while enabling scalability to 1D and 2D probe arrays for high throughput.

AFM for Immobilization of Biomolecules in High-Density Microarrays

Nanoscale resolution is an important step in the preparation of nanoarrays and placement of probe biomolecules. A flexible procedure has been described for simultaneous spatially controlled immobilization of functional biomolecules with submicrometer resolution by molecular ink lithography using AFM (Breitenstein et al. 2010). Bottom-up fabrication of surface bound nanostructures enables the immobilization of different types of biomolecules. The method works on transparent as well as on opaque substrates. The spatial resolution is better than 400 nm and is limited only by the AFM's positional accuracy after repeated z-cycles since all steps are performed in situ without moving the supporting surface. The principle is demonstrated by hybridization to different immobilized DNA oligomers and was validated by fluorescence microscopy. This method not only enables deposition of DNA at submicrometer resolution but also proteins and other molecules of biological relevance that can be coupled to biotin.

AFM for Nanodissection of Chromosomes

Chromosomal dissection provides a direct advance for isolating DNA from cytogenetically recognizable region to generate genetic probes for fluorescence in situ hybridization (FISH), a technique that became very common in cytogenetics and molecular genetics research and diagnostics. Several methods for microdissection (glass needle or a laser beam) are available to obtain specific probes from metaphase chromosomes. There are limitations of the conventional methods of dissection because several of chromosomes are needed for the production of a probe. Moreover, these methods are not suitable for single chromosome analysis, because of the relatively large size of the microneedles. New dissection techniques are required for advanced research on chromosomes at the nanoscale level. Both AFM and scanning near-field optical microscopy (SNOM) have been used to obtain local information from G-bands and chromosomal probes.

AFM has been used as a tool for nanomanipulation of single chromosomes to generate individual cell specific genetic probes. Molecular and nanomanipulation techniques have been combined to enable both nanodissection and amplification of chromosomal and chromatidial DNA (Di Bucchianico et al. 2011). Cross-sectional analysis of the dissected chromosomes reveals 20 nm and 40 nm deep cuts. Isolated single chromosomal regions can be directly amplified and labeled by the Degenerate Oligonucleotide-Primed Polymerase Chain Reaction (DOP-PCR) and subsequently hybridized to chromosomes and interphasic nuclei. FISH, performed with the DOP-PCR products as test probes, has been tested successfully in avian microchromosomes and interphasic nuclei. Chromosome nanolithography, with a resolution beyond the limit of light microscopy, could be useful for the construction of chromosome band libraries and for molecular cytogenetic mapping in investigation of genetic diseases.

Nanoparticles for Molecular Diagnostics

Several types of nanomaterials are used in molecular diagnostics: gold nanoparticles, quantum dots, CNTs, nanocrystals, etc. Magnetic nanoparticles are used in molecular imaging. Some examples are described here briefly and in relevant chapters dealing with various disorders.

3DNA® Dendrimers for Diagnostics

3DNA® Dendrimers (Genisphere LLC) are powerful and adaptable molecular devices capable of improving the sensitivity of a wide variety of assays including lateral flow, immunoassays and nucleic acid hybridization. High profile and high value tests offered as point-of-care (POC) assays are adaptable to include 3DNA® reagents to improve the limit of detection. Genisphere has reported a 64-fold improvement of sensitivity in a model lateral flow (LF) POC test. Similar improvements in sensitivity have been observed in other LF assays, and it is expected that use of this technology will reduce the false negative rate and significantly improve the accuracy of the otherwise subjective reading of the outcome. The stability of dendrimer reagents in solution is known to exceed 12 months, and preliminary experiments studying the stability of dried dendrimer reagents suggest a similar stability profile. Improved fluorescent detection will further enable POC tests to become more quantitative and better predictive of disease, condition and outcome. Because it is a passive amplification technology (unlike PCR, for example), the 3DNA® target-specific probe may be used to improve the sensitivity of existing bioassays without significant modification. Utilization of 3DNA® Dendrimers can be achieved with minimal additional manufacturing cost and without altering end user protocols.

Carbon Nanotubes

Interaction of DNA and SWCNT has potential applications including molecular diagnostics. Efficiency of PCR in amplifying DNA presence of SWCNT and the ability to directly amplify the DNA sequence associated with the SWCNT scaffold have been investigated (Williams et al. 2014). These studies showed that the DNA directly associated with the SWCNT can be amplified using PCR and provides an inhibitory concentration of DNA-dispersed SWCNT in PCR reactions for different preparations as well as a basis for future DNA:SWCNT studies that require PCR amplification. This will be useful for future studies focused on the use of SWCNT in molecular diagnostics.

Both SWCNTs and MWCNTs are found to significantly enhance the specificity of the repeated PCR and are capable of inhibition of long DNA thermal degradation. SWCNTs have a better specificity in repeated PCR than MWCNTs. MWCNT-DNA binding is more favorable for protecting long DNA from thermal degradation than SWCNT-DNA binding. These results suggest that CNTs are very useful in repeated PCR when working on limited amount of DNA resources (Du et al. 2014).

Gold Nanoparticles

Bits of DNA and Raman-active dyes can be attached onto gold nanoparticles, which assemble onto a sensor surface only in the presence of a complementary target. If a patterned sensor surface of multiple DNA strands is used, the technique can detect millions of different DNA sequences simultaneously. The current non-optimized detection limit of this method is 20 femtomolars. Gold nanoparticles are particularly good labels for sensors because a variety of analytical techniques can be used to detect them, including optical absorption, fluorescence, Raman scattering, atomic or magnetic force, and electrical conductivity. Gold nanoparticles and Raman spectroscopy have been used to detect bacteria and viruses. This approach could replace PCR and fluorescent tags commonly used today. The detection system can also be used on biochips dotted with DNA. If the targeted disease exists in the sample, its DNA will bind onto the complementary strands of DNA on the chip and gold nanoparticle. The chip is treated with silver-based solution, which coats the nanoparticles. When exposed to a light scanner, the coating enhances the signal enough to detect minute amounts of DNA. Since the Raman band is narrower than the fluorescent band, it allows more dyes to detect more targets quickly. If the sequence of interest is present in the sample, it will bind to the DNA and cause the solution to change color. Labeling oligonucleotide targets with gold nanoparticle rather than fluorophore probes substantially alters the melting profiles of the targets from an array substrate. Nanoparticle-based DNA detection systems are more sensitive and specific than current genomic detection systems.

Quantum Dots for Molecular Diagnostics

There is considerable interest in the use of QDs as inorganic fluorophores because they offer significant advantages over conventionally used fluorescent markers. For example, QDs have broad excitation spectra – from ultraviolet to red – that can be tuned depending on their size and composition. At the same time, QDs have narrow emission spectra, making it possible to resolve the emissions of different nanoparticles simultaneously and with minimal overlap. Finally, QDs are highly resistant to degradation, and their fluorescence is remarkably stable. Advantages of QD technology are:

- Simple excitation. Lasers are not required.
- Simple instrumentation

- · Availability of red/infrared colors enables whole blood assays
- High sensitivity

QDs have been used as possible alternatives to the dyes for tagging viruses and cancer cells. A major challenge is that QDs have an oily surface, whereas the cellular environment is water-based. Attempts are being made to modify the surface chemistry of QDs so that they interact with water-friendly molecules like proteins and DNA. The current goal is to develop QDs that can target a disease site and light it up. This can someday lead to an integrated system that will also use the QDs to diagnose as well to deliver drug therapies to the disease site. QDs can be designed to emit light at any wavelength from the infrared to visible to ultraviolet. This enables the use of severalcolors and thus multiplexed assays can be performed. Potential applications of QDs in molecular diagnostics can be summarized as follows:

- Cancer
- Genotyping
- Whole blood assays
- Multiplexed diagnostics
- DNA mapping
- Immunoassays and antibody tagging
- Detection of pathogenic microorganisms

QDs for Detection of Pathogenic Microorganisms

QDs have been used as fluorescent labels in immunoassays for quantitative detection of foodborne pathogenic bacteria such as *Salmonella typhimurium*. QDs coated with streptavidin are added to react with biotin on the secondary antibody. Measurement of the intensity of fluorescence produced by QDs provides a quantitative method for microbial detection. QDs can be used for ultrasensitive viral detection of a small number of microorganisms.

Bioconjugated QDs for Multiplexed Profiling of Biomarkers

Bioconjugated QDs provide a new class of biological labels for evaluating biomarkers on intact cells and tissue specimens. Use of multicolor QD probes in immunohistochemistry is considered one of the most important and clinically relevant applications. At present, however, clinical applications of QD-based immunohistochemistry have achieved only limited success. A major bottleneck is the lack of robust protocols to define the key parameters and steps. Preliminary results and detailed protocols for QD-antibody conjugation, tissue specimen preparation, multicolor QD staining, image processing and biomarker quantification have been published (Xing et al. 2007). The results demonstrate that bioconjugated QDs can be used for multiplexed profiling of biomarkers, and ultimately for correlation with disease progression and response to therapy. In general, QD bioconjugation is completed within 1 day, and multiplexed molecular profiling takes 1–3 days depending on the number of biomarkers and QD probes used.

Imaging of Living Tissue with QDs

Tiny blood vessels, viewed beneath a mouse's skin with multi-photon microscopy appear so bright and vivid in high-resolution images that researchers can see the vessel walls ripple with each heartbeat. Capillaries, hundreds of microns below the skin of living mice, can be illuminated in an unprecedented detail using QDs circulating through the blood as fluorescent imaging labels. Although there are easier ways to take a mouse's pulse, this level of resolution with high signal-to-noise ratio illustrates how useful multi-photon microscopy with QDs can become in biological research for tracking cells and visualizing tissue structures deep inside living animals. Monitoring of vascular changes in malignant tumors is a potential application. This approach will pave the way for many new noninvasive in vivo imaging methods using QDs.

Carbohydrate-encapsulated QD can be used for medical imaging. Certain carbohydrates, especially those included on tumor glycoproteins are known to have affinity for certain cell types and this can be exploited for medical imaging. Conjugating luminescent QDs with target specific glycans permits efficient imaging of the tissue to which the glycans bind with high affinity. Accurate imaging of primary and metastatic tumors is of primary importance in disease management. Second generation QDs contain the glycan ligands and PEG of varying chain lengths. PEG modification produces QDs that maintain high luminescence while reducing non-specific cell binding.

Procedures have been developed for using QDs to label live cells and to demonstrate their use for long-term multicolor imaging. Two approaches are endocytic uptake of QDs and selective labeling of cell surface proteins with QDs conjugated to antibodies, which should permit the simultaneous study of multiple cells over long periods of time as they proceed through growth and development. Use of avidin permits stable conjugation of the QDs to ligands, antibodies or other molecules that can be biotinylated, whereas the use of proteins fused to a positively charged peptide or oligohistidine peptide obviates the need for biotinylating the target molecule. Specific labeling of both intracellular and cell-surface proteins can be achieved by bioconjugation of QDs. For generalized cellular labeling, QDs not conjugated to a specific biomolecule may be used.

Fluorescent semiconductor QDs hold great potential for molecular imaging in vivo. However, the utility of existing QDs for in vivo imaging is limited because they require excitation from external illumination sources to fluoresce, which results in a strong autofluorescence background and a paucity of excitation light at nonsuperficial locations. QD conjugates that luminesce by bioluminescence resonance energy transfer in the absence of external excitation, have been prepared by coupling carboxylate-presenting QDs to a mutant of the bioluminescent protein *Renilla reniformis* luciferase. The conjugates emit long-wavelength (from red to near-infrared) bioluminescent light in cells and in animals, even in deep tissues, and are suitable for multiplexed in vivo imaging. Compared with existing QDs, self-illuminating QD conjugates have greatly enhanced sensitivity in small animal imaging, with an in vivo signal-to-background ratio of $>10^3$ for 5 pmol of conjugate.

Several advances have recently been made using QDs for live cell and in vivo imaging, in which QD-labeled molecules can be tracked and visualized in 3D. QDs have been investigated for their use for multiplex immunohistochemistry and in situ hybridization which, when combined with multispectral imaging, has enabled quantitation and co-localization of gene expression in clinical tissue specimens (Byers and Hitchman 2011).

Use of Nanocrystals in Immunohistochemistry

Bright, negatively or positively charged, water-soluble CdSe/ZnS core/shell nanocrystals (NCs) are easy to prepare and stabilize in aqueous solution. Single NCs can be detected using a standard epifluorescent microscope, ensuring a detection limit of one molecule coupled with an NC. NC-antibody (Ab) conjugates were tested in dot-blots and exhibited retention of binding capacity within several nanogram of antigen detected. NC-Ab conjugates have advantages in the immunofluorescent detection and 3D confocal analysis of p-glycoprotein (p-gp), one of the main mediators of the multi-drug resistance phenotype. The labeling of p-gp with NC-Ab conjugates is highly specific. NC-Abs conjugates can be used for specific detection of antigens in paraffin-embedded formaldehyde-fixed cancer tissue specimens, using immunostaining of cytokeratin, e.g., in basal carcinoma of the skin. NC-Ab conjugates may serve as highly sensitive, photostable labels for immunofluorescent analysis, immunohistochemical detection, and 3D confocal studies of membrane proteins and cells.

Magnetic Nanoparticles

Magnetic Nanoparticles for Bioscreening

Iron nanoparticles, 15–20 nm in size with saturation magnetization have been synthesized, and embedded in copolymer beads of styrene and glycidyl methacrylate (GMA), which were coated with poly-GMA by seed polymerization. The resultant Fe/St-GMA/GMA beads have diameters of 100–200 nm. By coating with poly-GMA, the zeta potential of the beads changes from -93.7 to -54.8 mV, as measured by an electrophoresis method. This facilitates nonspecific protein adsorption suppression, as revealed by gel electrophoresis method, which is a requisite for nanoparticles to be applied to carriers for bioscreening. Magnetic nanoparticles can be used for detection of biomolecules and cells based on magnetic resonance effects using a general detection platform termed diagnostic magnetic resonance (DMR) technology, which covers numerous sensing principles, and magnetic nanoparticle biosensors have been designed to detect a wide range of targets including DNA/mRNA, proteins, enzymes, drugs, pathogens, and circulating tumor cells (Haun et al. 2010). The basic principle of DMR is the use of magnetic nanoparticles as proximity sensors that modulate the spin relaxation time of neighboring water molecules, which can be quantified using clinical MRI scanners or benchtop nuclear magnetic resonance (NMR) relaxometers. The capabilities of DMR technology have been advanced considerably with the development of miniaturized, chip-based NMR (μ NMR) detector systems that can do highly sensitive measurements on microliter sample volumes and in multiplexed format. Thus, DMR biosensor technology holds considerable promise to provide a high-throughput, low-cost, and portable platform for large scale molecular and cellular screening in clinical and point-of-care settings.

Monitoring of Implanted NSCs Labeled with Nanoparticles

Noninvasive monitoring of stem cells, using high-resolution molecular imaging, will be important for improving clinical neural transplantation strategies. Labeling of human neural stem cells (NSCs) grown as neurospheres with magnetic nanoparticles have been shown not to adversely affect survival, migration, and differentiation or alter neuronal electrophysiological characteristics (Guzman et al. 2007). Using MRI, the authors demonstrated that human NSCs transplanted either to the neonatal, the adult, or the injured rodent brain respond to cues characteristic for the ambient microenvironment resulting in distinct migration patterns. Nanoparticle-labeled human NSCs survive long-term and differentiate in a site-specific manner identical to that seen for transplants of unlabeled cells. The impact of graft location on cell migration and MRI characteristics of graft cell death and subsequent clearance were also described. Knowledge of migration patterns and implementation of noninvasive stem cell tracking might help to improve the design of future clinical NSC transplantation.

Perfluorocarbon Nanoparticles to Track Therapeutic Cells In Vivo

Using perfluorocarbon nanoparticles 200 nm in size to label endothelial progenitor cells taken from human UCB enables their detection by MRI in vivo following administration (Partlow et al. 2007). The MRI scanner can be tuned to the specific frequency of the fluorine compound in the nanoparticles, and only the nanoparticle-containing cells are visible in the scan. This eliminates any background signal, which often interferes with medical imaging. Moreover, the lack of interference means one can measure very low amounts of the labeled cells and closely estimate their number by the brightness of the image. Since several perfluorocarbon compounds are available, different types of cells potentially could be labeled with

different compounds, injected and then detected separately by tuning the MRI scanner to each one's individual frequency. This technology offers significant advantages over other cell-labeling technologies in development. Laboratory tests showed that the cells retained their usual surface markers and that they were still functional after the labeling process. The labeled cells were shown to migrate to and incorporate into blood vessels forming around tumors in mice. These could soon enable researchers and physicians to directly track cells used in medical treatments using unique signatures from the ingested nanoparticle beacons. They could prove useful for monitoring tumors and diagnosing as well as treating cardiovascular problems.

Superparamagnetic Nanoparticles for Cell Tracking

Magnetic nanoparticles are a powerful and versatile diagnostic tool in biology and medicine. It is possible to incorporate sufficient amounts of superparamagnetic iron oxide nanoparticles (SPIONs) into cells, enabling their detection in vivo using MRI. Because of their small size, they are easily incorporated into various cell types (stem cells, phagocytes, etc) allowing the cells to be tracked in vivo, for example to determine whether stem cells move to the correct target area of the body.

Superparamagnetic iron oxide nanoparticles (SPIONs), used clinically for specific magnetic sorting, can be used as a magnetic cell label for in vivo cell visualization. The fact that SPIONs coated with different commercially available antibodies can bind to specific cell types opens extensive possibilities for cell tracking in vivo. A study has investigated the biological properties, including proliferation, viability and differentiation capacity of MSCs labeled with clinically approved SPIONs (Jasmin et al. 2011). Rat MSCs were isolated, cultured, and incubated with dextran-covered SPIONs (ferumoxide) alone or with poly-L-lysine (PLL) or protamine chlorhydrate. Whereas labeling of MSCs incubated with ferumoxide alone was poor, 95% MSCs were labeled when incubated with ferumoxide in the presence of PLL or protamine. MSCs incubated with ferumoxide and protamine were efficiently visualized by MRI; they maintained proliferation and viability for up to 7 days and remained competent to differentiate. After 21 days MSCs pretreated with mitomycin C still showed many ferumoxide-labeled cells. The efficient and long lasting uptake and retention of SPIONs by MSCs using a protocol employing ferumoxide and protamine may be applicable to patients, since both ferumoxide and protamine are approved for human use.

Unfortunately, SPIONs are no longer being manufactured. Second generation, ultrasmall SPIONs (USPIONs), however, offer a viable alternative. Ferumoxytol (FerahemeTM) is one USPION composed of a non-stoichiometric magnetite core surrounded by a polyglucose sorbitol carboxymethylether coat. The colloidal, particle size of ferumoxytol is 17–30 nm. Ferumoxytol has been approved by the FDA as an iron supplement for treatment of iron deficiency in patients with renal failure. This agent has been used "off label" for stem cell labeling (Castaneda et al. 2011). This technique may be applied for non-invasive monitoring of stem cell therapies in preclinical and clinical settings. USPIONs are in clinical trials as contrast agents for MRI (see later in this chapter).

SPIONS for Real-Time Tracking of Viral Delivery

In vivo tracking of gene therapy vectors improves the biodistribution of these agents in the brain, an important requirement for targeting of infiltrative malignant gliomas. The glioma-targeting Ad5/3-cRGD gene therapy vector has beencovalently bound to SPION to monitor its distribution by MRI (Yun et al. 2012). Transduction of labeled and unlabeled vectors was assessed on the U87 glioma cell line and normal human astrocytes (NHA), and was higher in U87 compared to NHA, but was similar between labeled and unlabeled virus. An in vivo study was performed by intracranial subcortical injection of labeled-Ad5/3-cRGD particles into a pig brain. The labeled vector appeared in vivo as a T2-weighted hyperintensity and a T2-gradient echo signal at the injection site, persisting up to 72 h post-injection. Thus, a glioma-targeting vector that is labeled with SPION enables detection by MRI with no change in transduction capability.

SPIONs for Calcium Sensing

A family of calcium indicators for MRI is formed by combining a powerful SPIONbased contrast mechanism with the versatile calcium-sensing protein calmodulin and its targets. Calcium-dependent protein-protein interactions drive particle clustering and produce up to fivefold changes in T2 relaxivity, an indication of the sensors' potency. Robust MRI signal changes are achieved even at nanomolar particle concentrations that are unlikely to buffer calcium levels. When combined with technologies for cellular delivery of nanoparticulate agents, these sensors and their derivatives may be useful for functional molecular imaging of biological signaling networks in live, opaque specimens.

Magnetic Nanoparticles for Labeling Molecules

Bound to a suitable antibody, magnetic nanoparticles are used to label specific molecules, structures, or microorganisms. Magnetic immunoassay techniques have been developed in which the magnetic field generated by the magnetically labeled targets is detected directly with a sensitive magnetometer. Binding of antibody to target molecules or disease-causing organism is the basis of several tests. Antibodies labeled with magnetic nanoparticles give magnetic signals on exposure to a magnetic field. Antibodies bound to targets can thus be identified as unbound antibodies disperse in all directions and produce no net magnetic signal.

SPIONs have been functionalized to identify *Mycobacterium avium spp* paratuberculosis (MAP) through magnetic relaxation (Kaittanis et al. 2007). The results indicate that the MAP nanoprobes bind specifically to MAP and can quantify the bacterial target quickly in milk and blood with high sensitivity. The advantage of this approach is that detection is not susceptible to interferences caused by other bacteria. The use of these magnetic nanosensors is anticipated in the identification and quantification of bacteria in clinical and environmental samples.

Study of Living Cells by SPIONs

Technologies to assess the molecular targets of biomolecules in living cells are lacking. A technology called magnetism-based interaction capture (MAGIC) can identify molecular targets because of induced movement of SPIONs inside living cells. Intracellular proteins can be painted with fluorescent materials and drugs embedded with SPIONs inserted into the cell. These nanoprobes captured the small molecule's labeled target protein and were translocated in a direction specified by the magnetic field. Use of MAGIC in genome-wide expression screening can identify multiple protein targets of a drug. MAGIC can also be used to monitor signal-dependent modification and multiple interactions of proteins. Internalized SPIONs can be moved inside cells by an external magnetic field. MAGIC can be useful in the development of diagnostics and biosensors. Its ultimate use would be for the analysis of interactions inside living cells of patients.

Imaging Applications of Nanoparticles

Molecular imaging now encompasses all imaging modalities including those used in clinical care: optical imaging, nuclear medical imaging, ultrasound imaging, MRI, and photoacoustic imaging. Molecular imaging always requires accumulation of contrast agent in the target site, often achieved most efficiently by steering nanoparticles containing contrast agent into the target. This entails accessing target molecules hidden behind tissue barriers, necessitating the use of targeting groups. For imaging modalities with low sensitivity, nanoparticles bearing multiple contrast groups provide signal amplification. The same nanoparticles can in principle deliver both contrast medium and drug, allowing monitoring of biodistribution and therapeutic activity simultaneously. Nanoparticles with multiple bioadhesive sites for target recognition and binding share functionalities with many subcellular organelles (ribosomes, proteasomes, ion channels, and transport vesicles), which are of similar sizes. The materials used to synthesize nanoparticles include natural proteins and polymers, artificial polymers, dendrimers, fullerenes and other carbon-based structures, lipid-water micelles, viral capsids, metals, metal oxides, and ceramics. Signal generators incorporated into nanoparticles include iron oxide, gadolinium, fluorine, iodine, bismuth, radionuclides, QDs, and metal nanoclusters (Debbage and Jaschke 2008). Diagnostic imaging applications, now appearing, include sentinel node localization and stem cell tracking.

CT Image Enhancement by Nanoparticles

Computer tomography (CT) is among the most convenient imaging/diagnostic tools used currently in terms of availability, efficiency, and cost. In contrast to other imaging modalities, such as PET, single-photon emission computed tomography (SPECT) and MRI, CT is not usually considered as a molecular imaging modality. However, development of nanoparticles as contrast agents is enabling specific applications of CT for molecular imaging. Current clinical CT contrast agents are predominantly based on the high atomic number iodine molecules (Z = 53), which are effective in absorbing x-rays; but the small size of iodine molecules allows very short imaging times due to rapid clearance by the kidneys. Use of high-Z nanoparticles, e.g. polymers, liposomes, and micelles as contrast agents may enable CT imaging at lower radiation doses and with improved sensitivity as well as specificity (Shilo et al. 2012). There is some concern about the toxicity of these nanoparticle contrast agents. Once the toxicity issues are resolved, clinical trials could be could be initiated in humans. Concomitant encapsulation of metal nanoparticles (diagnosis) and drug molecules (therapy) into carriers, such as liposomes offers simultaneous in vivo imaging and tracking of drug efficacy, which will facilitate development of personalized medicine.

Dendritic Nanoprobes for Imaging of Angiogenesis

Angiogenesis is an important process in ischemia and cancer. A biodegradable positron-emitting dendritic nanoprobe targeted at $\alpha\nu\beta3$ integrin, a biomarker known to modulate angiogenesis, was developed for the noninvasive imaging of angiogenesis (Almutairi et al. 2009). The nanoprobe has a modular multivalent core-shell architecture consisting of a biodegradable heterobifunctional dendritic core chemoselectively functionalized with heterobifunctional polyethylene oxide (PEO) chains that form a protective shell, which imparts biological stealth and dictates the pharmacokinetics. Each of the eight branches of the dendritic core was functionalized for labeling with radiohalogens. Placement of radioactive moieties at the core was designed to prevent in vivo dehalogenation, a potential problem for radiohalogens in imaging and therapy. Targeting peptides of cyclic arginine-glycine-aspartic acid (RGD) motifs were installed at the terminal ends of the PEO chains to enhance their accessibility to $\alpha\gamma\beta\beta$ integrin receptors. This nanoscale design enabled a 50-fold enhancement of the binding affinity to avß3 integrin receptors with respect to the monovalent RGD peptide alone Cell-based assays of the ¹²⁵I-labeled dendritic nanoprobes using $\alpha\nu\beta$ 3-positive cells showed a sixfold increase in avß3 receptor-mediated endocytosis of the targeted nanoprobe compared with the nontargeted nanoprobe, whereas $\alpha\nu\beta$ 3-negative cells showed no enhancement of cell uptake over time. In vivo biodistribution studies of ⁷⁶Br-labeled dendritic nanoprobes showed excellent bioavailability for the targeted and nontargeted nanoprobes. In vivo studies in a murine hindlimb ischemia model for angiogenesis revealed high specific accumulation of ⁷⁶Br-labeled dendritic nanoprobes targeted at $\alpha\nu\beta3$ integrins in angiogenic muscles, allowing highly selective imaging of this critically important process.

Functionalized MWCNTs as Ultrasound Contrast Agents

Ultrasonography is a fundamental diagnostic imaging tool in everyday clinical practice. Functionalized multiwalled carbon nanotubes (MWCNTs) have been used as ultrasound contrast agents (Delogu et al. 2012). Initially, the authors carried out

a thorough investigation to assess the echogenic property of the nanotubes in vitro. It was shown that ultrasound signal of functionalized MWCNTs is higher than graphene oxide, pristine MWCNTs, and functionalized SWCNTs. Qualitatively, the ultrasound signal of CNTs was equal to that of sulfur hexafluoride (SonoVue), a commercially available contrast agent. They found that MWCNTs were highly echogenic in liver and heart through ex vivo experiments using pig as an animal model. In contrast to most of ultrasound contrast agents, CNTs can be visualized within a wide variety of frequencies in a phantom bladder using tissue harmonic imaging modality. In vivo in the pig bladder MWCNTs can be observed at low frequencies, which are appropriate for abdominal organs. No toxicity of CNTs was observed by animal autopsy, organ histology and immunostaining, blood count, and chemical profile. These results reveal the enormous potential of CNTs as ultrasound contrast agents, giving support for their future applications as nanoparticles that can combine diagnostic and therapeutic modalities.

Nanoparticles as Contrast-Enhancing Agents for MRI

There is rapid growth in the use of MRI for molecular and cellular imaging. Much of this work relies on the high relaxivity of nanometer-sized, ultrasmall dextrancoated iron oxide particles. Chemical modifications to nano-sized virus particles may improve MRI. Attachment of several gadolinium chelates, the chemical compound used in MRI contrast agents, onto the surface of the viral particles results in the generation of a very intense signal in a clinical MRI scanner. Dendrimers, magnetic nanoparticles, QDs and ferrofluids are examples of some of the nanoparticles that have been used along with imaging technologies for enhancement of contrast. Some of these are described in the preceding section.

Gadolinium-Loaded Dendrimer Nanoparticles for Tumor-Specific MRI

A target-specific MRI contrast agent for tumor cells expressing high affinity folate receptor was synthesized using a fifth generation polyamidoamine dendrimer (Swanson et al. 2008). Surface modified dendrimer was functionalized for targeting with folic acid and the remaining terminal primary amines of the dendrimer were conjugated with the bifunctional NCS-DOTA (Dow Chemical) chelator that forms stable complexes with gadolinium. In xenograft tumors in immunodeficient mice induced with human epithelial cancer cells expressing folate receptor, 3D MRI results showed specific and statistically significant signal enhancement in tumors generated with targeted nanoparticle compared with signal generated by non-targeted contrast nanoparticle. The targeted dendrimer contrast nanoparticles infiltrated tumor and were retained in tumor cells up to 48 h following injection. The presence of folic acid on the dendrimer resulted in specific delivery of the nanoparticle to tissues and xenograft tumor cells expressing folate receptor in vivo. The specificity of the dendrimer nanoparticles for targeted cancer imaging with the

prolonged clearance time compared favorably with the current clinically approved gadodiamide contrast agent. Potential applications of this approach include determination of the folate receptor status of tumors and monitoring of drug therapy.

Gadonanotubes for MRI

More than 25 million patients in the US undergo MRI each year and contrast agents are used in about 30% of these procedures. Gadolinium agents are the most effective and the most commonly used MRI contrast agents. Gadonanotubes are made of the same highly toxic metal, gadolinium (Gd³⁺) that is used in MRI currently but the metal atoms are encased inside a carbon nanotube. The ultrashort nanotubes are only about 20–100 times longer than they are wide, and once inside the nanotubes, the gadolinium atoms naturally aggregate into tiny clusters of about ten atoms each. Clustering causes the unexplained increases in magnetic and MRI effects. Gadonanotubes are at least 40–90 times more effective than Gd³⁺-based MRI agents now in use. Shrouding the toxic metals inside the benign carbon is expected to significantly reduce or eliminate the metal's toxicity. Currently available methods of attaching disease-specific antibodies and peptides can be applied to gadonanotubes so they can be targeted to malignant and other diseased cells.

Gold Nanorods and Nanoparticles as Imaging Agents

Gold nanorods excited at 830 nm on a far-field laser-scanning microscope produce strong two-photon luminescence (TPL) intensities, and the TPL excitation spectrum can be superimposed on to the longitudinal plasmon band. The TPL signal from a single nanorod is 58 times that of the two-photon fluorescence signal from a single rhodamine molecule. Gold nanorods can be used as imaging agents as demonstrated by in vivo imaging of single nanorods flowing in mouse ear blood vessels.

Nanoprobes Inc reported that 1.9 nm gold nanoparticles may overcome many limitations to traditional x-ray contrast agents. Gold has higher X-ray absorption than iodine with less bone and tissue interference, thus achieving better contrast with lower X-ray dose. Because nanoparticles clear the blood more slowly than iodine agents, they permit longer imaging times. In studies in mice, a 5-mm tumor growing in one thigh was evident from its increased vascularity and resultant higher gold content. The gold particles thus enable direct imaging, detection, and measurement of angiogenic and hypervascularized regions. The 1.9 nm gold nanoparticles were found to clear through the kidneys: a closer examination of the kidneys revealed a remarkably detailed anatomical and functional display, with blood vessels less than 100 μ m in diameter delineated, thus enabling in vivo vascular casting. Toxicity was also low: mice intravenously injected with the gold nanoparticles survived over 1 year without signs of illness.

In Vivo Imaging Using Nanoparticles

Fluorescence provides remarkable results for in vivo imaging but it has several limitations, particularly because of the need for tissue autofluorescence by external illumination and weak tissue penetration of low wavelength excitation light. An alternative optical imaging technique has been developed by using nanoparticles with persisting luminescence suitable for small animal imaging (le Masne de Chermont et al. 2007). These nanoparticles can be excited before injection, and their in vivo distribution can be followed in real-time for more than 1 h without the need for an external illumination source. Chemical modification of the nanoparticle surface can be done to target organs such as the lung or the liver or for prolonging luminescence during circulation of the nanoparticles in blood. Tumors have been identified by this technique.

A significant impediment to the widespread use of noninvasive in vivo vascular imaging techniques is the current lack of suitable intravital imaging probes. One strategy is the use of viral nanoparticles as a platform for the multivalent display of fluorescent dyes to image tissues deep inside living organisms. The bioavailable cowpea mosaic virus (CPMV) can be fluorescently labeled to high densities with no measurable quenching, resulting in exceptionally bright particles with in vivo dispersion properties that allow high-resolution intravital imaging of vascular endothe-lium for periods of at least 72 h. CPMV nanoparticles can be used to visualize the vasculature and blood flow in living mouse and chick embryos to a depth of up to 500 μ m. Intravital visualization of human fibrosarcoma-mediated tumor angiogenesis using fluorescent CPMV provides a means to identify arterial and venous vessels for monitoring tumor neovascularization.

Manganese Oxide Nanoparticles as Contrast Agent for Brain MRI

A MRI contrast agent using manganese oxide nanoparticles produces images of the anatomic structures of mouse brain which are as clear as those obtained by histological examination (Na et al. 2007). The new contrast agent will enable better research and diagnosis neurological disorders such as Alzheimer's disease, Parkinson's disease, and stroke. Furthermore, antibodies can be attached to the manganese oxide nanoparticles, which recognize and specifically bind to receptors on the surface of breast cancer cells in mouse brains with breast cancer metastases. The tumors were clearly highlighted by the antibody-coupled contrast agent. The same principle should allow other disease-related changes or physiological systems to be visualized by using the appropriate antibodies.

Magnetic Nanoparticles as Contrast Agents for MRI of Pancreas

Type 1A diabetes (T1D) is an autoimmune disease characterized by leukocyte infiltration of the pancreatic islets of Langerhans. A major impediment to advances in understanding, preventing, and curing T1D has been the inability to see the

disease initiate, progress, or regress, especially during the occult phase. A noninvasive method has been developed to visualize T1D at the target organ level in patients with active insulitis (Gaglia et al. 2011). Specifically, it visualizes islet inflammation, which manifests by microvascular changes as well as monocyte/macrophage recruitment and activation, using MRI with magnetic nanoparticles (MNPs) contrast material. As a proof of principle for this approach, imaging of infused ferumoxtran-10 nanoparticles permitted effective visualization of the pancreas and distinction of recent-onset diabetes patients from nondiabetic controls. The observation that MNPs accumulate in the pancreas of T1D patients opens the door to exploiting this noninvasive imaging method to follow T1D progression and monitoring the clearance of insulitis by immunomodulatory agents.

Nanoparticles as Contrast Agent for MRI

The determination of brain tumor margins both during the presurgical planning phase and during surgical resection has long been a challenging task in the therapy of brain tumor patients. Multimodal (near-infrared fluorescent and magnetic) nanoparticles were used as a preoperative MRI contrast agent and intraoperative optical probes. Key features of nanoparticle metabolism, namely intracellular sequestration by microglia and the combined optical and magnetic properties of the probe, allowed delineation of brain tumors both by preoperative MRI and by intraoperative optical imaging. This prototypical multimodal nanoparticle has unique properties that may allow radiologists and neurosurgeons to see the same probe in the same cells and may offer a new approach for obtaining tumor margins.

Alphanubeta3-targeted paramagnetic nanoparticles have been employed to noninvasively detect very small regions of angiogenesis associated with nascent melanoma tumors. Each particle is filled with thousands of molecules of the metal that is used to enhance contrast in conventional MRI scans. The surface of each particle is decorated with a substance that attaches to newly forming blood vessels, which are present at tumor sites. The goal is to create a high density of the glowing particles at the site of tumor growth so they are easily visible. Molecular MRI results have been corroborated by histology. This lowers the limit for detecting sparse biomarkers with molecular MRI in vivo when the growths are still invisible to conventional MRI. Earlier detection can potentially increase the effectiveness of treatment. This is especially true with melanoma, which begins as a highly curable disorder, then progresses into an aggressive and deadly disease. A second benefit of the approach is that the same nanoparticles used to find the tumors could potentially deliver stronger doses of anticancer drugs directly to the tumor site with fewer side effects. Targeting the drugs to the tumor site in this way would also allow stronger doses without systemic toxicity than would be possible if the drug were injected or delivered in some other systemic way. The nanoparticles might also allow physicians to more readily assess the effectiveness of the treatment by comparing MRI scans before and after treatment. Other cancer types might be accessible to this approach as well, because all tumors recruit new blood vessels as they grow.

Inflammation following acute myocardial infarction (MI) has detrimental effects on reperfusion, myocardial remodeling, and ventricular function. MRI using USPIONs as contrast agents can detect cellular inflammation in tissues, and therefore their role in acute MI in humans has been explored. Following acute MI, uptake of USPIONs was shown to occur within the infarcted and to less extent in the remote myocardium (Alam et al. 2012). This technique is promising as a potential method for assessing cellular myocardial inflammation and left ventricular remodeling, which may have a range of applications in patients with MI and other inflammatory cardiac conditions. It is in clinical trials.

Optical Molecular Imaging Using Targeted Magnetic Nanoprobes

Dynamic magnetomotion of magnetic nanoparticles (MNPs) detected with magnetomotive optical coherence tomography (MM-OCT) represents a new method for contrast enhancement and therapeutic interventions in molecular imaging. In vivo imaging of dynamic functionalized iron oxide MNPs using MM-OCT was demonstrated in a preclinical mammary tumor model (John et al. 2010). Using targeted MNPs, in vivo MM-OCT images exhibit strong magnetomotive signals in mammary tumor, and no significant signals were measured from tumors of rats injected with nontargeted MNPs or saline. The results of in vivo MM-OCT are validated by MRI, ex vivo MM-OCT, Prussian blue staining of histological sections, and immunohistochemical analysis of excised tumors and internal organs. The MNPs are antibody functionalized to target the human epidermal growth factor receptor 2 (HER2 neu) protein. Fc-directed conjugation of the antibody to the MNPs aids in reducing uptake by macrophages in the reticulo-endothelial system, thereby increasing the circulation time in the blood. These engineered magnetic nanoprobes have multifunctional capabilities enabling them to be used as dynamic contrast agents in MM-OCT and MRI.

QDs for Biological Imaging

Targeted QDs, coated with paramagnetic and pegylated lipids, have been developed for detection by MRI. The QDs are functionalized by covalently linking v3-specific peptides, and the specificity was assessed and confirmed on cultured endothelial cells. The bimodal character, the high relaxivity, and the specificity of this nanoparticulate probe make it an excellent contrast agent for molecular imaging purposes. Among other applications, those in cancer are most important.

Accurate imaging of diseased cells (e.g. primary and metastatic tumors) is of primary importance in disease management. The NIH has developed carbohydrateencapsulated QDs with detectable luminescent properties useful for imaging of cancer or other disease tissues. Certain carbohydrates, especially those included on tumor glycoproteins are known to have affinity for certain cell types. One notable glycan used in this technology is the Thomsen-Freidenreich disaccharide (Galbeta1-3GalNAc) that is readily detectable in 90% of all primary human carcinomas and their metastases. These glycans can be exploited for medical imaging. Encapsulating luminescent QDs with target- specific glycans permits efficient imaging of the tissue to which the glycans bind with high affinity.

Multifunctional nanoparticle probes based on semiconductor QDs have been used for cancer targeting and imaging in living animals. The structural design involves encapsulating luminescent QDs with an ABC triblock copolymer and linking this amphiphilic polymer to tumor-targeting ligands and drug-delivery functionalities. In vivo targeting studies of human cancer growing in nude mice indicate that the QD probes accumulate at tumors both by the enhanced permeability and retention of tumor sites and by antibody binding to cancer-specific cell surface biomarkers. Using both subcutaneous injection of QD-tagged cancer cells and systemic injection of multifunctional QD, sensitive and multicolor fluorescence imaging of cancer cells have been achieved under in vivo conditions. These results raise new possibilities for ultrasensitive and multiplexed imaging of molecular targets in vivo.

SPIONs Combined with MRI

Highly lymphotropic SPIONs measuring 2–3 nm on average, which gain access to lymph nodes by means of interstitial-lymphatic fluid transport, have been used in conjunction with high-resolution MRI to reveal small and otherwise undetectable lymph-node metastases. In patients with prostate cancer who undergo surgical lymph-node resection or biopsy, MRI with lymphotropic SPIONs can identify all patients with nodal metastases, which is not possible with conventional MRI alone, and has implications for the management. In men with metastatic prostate cancer, adjuvant androgen-deprivation therapy with radiation is the mainstay of management.

Sentinel lymph node (SLN) imaging and biopsy is an important part of the workup of some cancers in humans. The presence of lymph node metastases is an important factor in breast cancer patient prognosis. Therefore, the precise identification of SLNs in these patients is critical. Conventional methods have drawbacks including lack of depth, skin staining (blue dye), poor spatial resolution, and exposure to ionizing radiation. Among the newer methods, magnetic resonance lymphography, in which a gadolinium labeled nanoparticle is injected and imaged provide superior anatomic resolution and assessment of lymphatic dynamics, overcoming some of the drawbacks of other methods. Optical imaging employing various nanoparticles, including QDs, also provides the capability of mapping each lymphatic drainage in a different color'. However, autofluorescence arising from normal tissues can compromise the sensitivity and specificity of in vivo fluorescence imaging using QDs by lowering the target-to-background signal ratio. Since bioluminescence resonance energy transfer QD (BRET-QD) nanoparticles can selfilluminate in NIR in the presence of the substrate, imaging using BRET-QDs does not produce any autofluorescence. These advantages of BRET-QD enable real-time, quantitative lymphatic imaging without image processing (Kosaka et al. 2011).

Use of lymphatic imaging agents will improve our understanding of the lymphatic system. It is conceivable that an anticancer drug and a tumor vaccine can be incorporated into the imaging agent for the delivery of regional therapy (Ravizzini et al. 2009).

Concluding Remarks and Prospects of Nanoparticles for Imaging

Surface functionalization has expanded further the potential of nanoparticles as probes for molecular imaging. Ongoing research of nanoparticles for biomedical imaging focuses on increased selectivity and reduced nonspecific uptake with increased spatial resolution containing stabilizers conjugated with targeting ligands. Structural design of nanomaterials for biomedical imaging continues to expand and diversify. Synthetic methods aim to control the size and surface characteristics of nanoparticles to optimize distribution, half-life and elimination. Although molecular imaging applications using nanoparticles are advancing into clinical applications, challenges such as storage stability and long-term toxicology should continue to be addressed (Nune et al. 2009).

Applications of Nanopore Technology for Molecular Diagnostics

Nanopore Technology for Detection of Single DNA Molecules

Nanopore sequencing was described in Chap. 3. Nanopores hold great promise as single-molecule analytical devices and biophysical model systems because the ionic current blockades they produce contain information about the identity, concentration, structure, and dynamics of target molecules. Nanopore technology can distinguish between and count a variety of different molecules in a complex mixture. For example, it can distinguish between hybridized or unhybridized unknown RNA and DNA molecules that differ only by a single nucleotide. Nanopore biosensors can enable direct, microsecond-time scale nucleic acid characterization without the need for amplification, chemical modification, surface adsorption, or the binding of probes.

A mutant was constructed of porin MspA of *Mycobacterium smegmatis* that is capable of electronically detecting and characterizing single molecules of ssDNA as they are electrophoretically driven through the pore (Butler et al. 2008). A second mutant with additional exchanges of negatively-charged residues for positively-charged residues in the vestibule region exhibited a factor of \approx 20 higher interaction rates, required only half as much voltage to observe interaction, and allowed ssDNA to reside in the vestibule \approx 100 times longer than the first mutant. These results introduce MspA as a nanopore for nucleic acid analysis and highlight its potential as an engineerable platform for single-molecule detection and characterization applications.

Protein binding site on DNA can be mapped or genetic information can be read at a single molecule level using solid-state nanopores (Yu et al. 2015). A nanopore based method can detect SNPs at the single molecule level (Kong et al. 2017). Designed DNA carriers are used to distinguish DNA strands containing only one single base difference and follow strand displacement kinetics.

Nanocytometry

Nanocytometry is a nanotechnology-based approach to flow cytometry. It incorporates previous work on a nanoelectronic technique for detecting the binding of unlabeled antibody-antigen pairs. Nanocytometry uses resistive-pulse sensing and artificial nanopores to detect and measure cell size, which is determined by the change in resistance when an individual cell passes through the pore (Carbonaro et al. 2008). As a proof-of-principle, it was shown that it was possible to measure the change in size when cells undergo apoptosis. The novel method has an integrated microfluidic chip, which can adapt to sort cancer and other types of cells based on their cell-surface protein expression.

A low-cost, flow-through nanocytometer has been presented that utilizes a colloidal suspension of non-functionalized magnetic nanoparticles for label-free manipulation and separation of microparticles (Kose and Koser 2012). The sizebased separation is mediated by magnetically excited biocompatible ferrofluid particles with up to 99% separation efficiency and a throughput of 3×10^4 particles/s per mm² of channel cross-section. The device is readily scalable and applicable to live cell sorting offering competitive cytometer performance in a simple and inexpensive package.

Nanocytometry is a significant improvement over conventional flow cytometry, because the system permits label-free signal detection, extreme reproducibility and sensitivity, and cell separations using only a few cells. Conventional flow cytometry requires a large sample of cells and usually requires labeling. Nanocytometry could provide an important new technology applicable to cancer. For example, nanocytometry could be used to improve upon physicians' ability to detect minimal residual disease states as well as circulating tumor cells (CTCs) and upon a scientist's ability to study cell populations that occur in very small numbers such as stem cells.

DNA-Protein and -Nanoparticle Conjugates

Semi-synthetic conjugates composed of nucleic acids, proteins and inorganic nanoparticles have been synthesized and characterized. For example, self-assembled oligomeric networks consisting of streptavidin and double-stranded DNA are applicable as reagents in immunoassays. Covalent conjugates of ssDNA and streptavidin

are utilized as biomolecular adapters for the immobilization of biotinylated macromolecules at solid substrates via nucleic acid hybridization. This 'DNA-directed immobilization' enables reversible and site-selective functionalization of solid substrates with metal and semiconductor nanoparticles or, vice versa, for the DNA-directed functionalization of gold nanoparticles with proteins, such as immunoglobulins and enzymes. This approach is applicable for the detection of chip-immobilized antigens. Moreover, covalent DNA-protein conjugates allow for their selective positioning along single-stranded nucleic acids, and thus for the construction of nanometer-scale assemblies composed of proteins and/or nanoclusters. Examples include the fabrication of functional biometallic nanostructures from gold nanoparticles and antibodies, applicable as diagnostic tools in bioanalytics. Gold nanoparticles decorated with fluorescein-modified DNA enables improvement of the detection limit of ascorbic acid quantification by two orders of magnitude due to enhanced cleavage of DNA catalyzed by gold clusters (Malashikhina and Pavlov 2012).

Resonance Light Scattering Technology

Resonance Light Scattering (RLS) technology, developed at Genicon Sciences Corporation (acquired by Life Technologies), offers uniquely powerful signal generation and detection capabilities applicable to a wide variety of analytical bioassay formats. RLS exploits submicroscopic metallic particles (e.g. gold and silver) of uniform diameter (in the nanometer range) which scatter incident white light to generate monochromatic colored light that appears as highly intense fluorescence Each RLS particle produces intense light scattering that can be viewed with the naked eye. Under low power microscope magnification, individual 80 nm gold particles can be readily observed. The scattering produced by these particles creates a 'halo' with an apparent one-micron diameter. Therefore, one can conduct ultra-sensitive assays to define location and relative frequency of target molecules. RLS signal generation technology is up to 1,000,000 times more sensitive than current fluorescence signaling technology. Other advantages of RLS technology are that RLS signals do not require computer-enhanced imaging of data as they are so intense. Research applications of RLS technology are:

- Gene Expression. Relative gene expression studies on slide-based cDNA microarrays.
- DNA Sequencing. RLS-based DNA sequencing on sequence-by-hybridization biochips.
- Microfluidics. RLS Particles for solution-based assays in nanofluidic flow-through microarrays.
- Immunohistology. Rapid in situ localization/quantitation of proteins in tissue sections using RLS-coupled antibodies.
- · Homogeneous. RLS particles for bimolecular, microvolume studies in solution.

Clinical Applications of RLS technology are:

- RLS technology is being used to score SNPs for discrimination of therapeutically relevant alleles.
- RLS technology provides ultrahigh-sensitivity probes for in situ hybridizations to quantitate therapeutically important DNA and RNA molecules.
- Antibody-coupled RLS particles can deliver increased sensitivity for detection of rare analytes in diagnostic assays.
- Nanoparticle-labeled bacterial RNA generates reproducible RLS signals that are at least 50 times more intense than state-of-the-art confocal-based fluorescence signals for detection of bacterial pathogens.

Nanobarcodes Technology

Metallic nanobarcodes have been produced with striping patterns prepared by sequential electrochemical deposition of metal ions. The differential reflectivity of adjacent stripes enables identification of the striping patterns by conventional light microscopy. This readout mechanism does not interfere with the use of fluorescence for detection of analytes bound to particles by affinity capture, as demonstrated by DNA and protein bioassays. Among other applications such as SNP mapping and multiplexed assays for proteomics, nanobarcodes can be used for population diagnostics and in POC hand-held devices. Multiplexed biodetection based on barcoded nanowires has potential use in cancer detection. Key performance advantages relative to existing encoded bead technologies include:

- The ability to use the widely-installed base of optical microscopes for readout.
- The ability to use multiple colors of fluorophores for quantitation.
- The ability to generate hundreds to thousands of unique codes that can be distinguished at high speed.

Nanobarcode Particle Technology for SNP Genotyping

Nanobarcode particle technology has been used in universal array for highthroughput SNP genotyping. The particles are encoded submicron metallic nanorods manufactured by electroplating inert metals such as gold and silver into templates and releasing the resulting striped nanoparticles. The power of this technology is that the particles are intrinsically encoded by different reflectivity of adjacent metal stripes, enabling the generation of many thousands of unique encoded substrates. Using SNP found within the cytochrome P450 gene family, and a universal short oligonucleotide ligation strategy, simultaneous genotyping of 15 SNPs was demonstrated; a format requiring discrimination of 30 encoded nanowires (one per allele). To demonstrate applicability in practice, 160 genotypes were determined from multiplex PCR products from 20 genomic DNA samples. Whereas conventional SNP detection techniques are mainly PCR-based. Nanosphere's Verigene technology enables multiplex SNP genotyping in total human genomic DNA without the need for target amplification by PCR. This direct SNP genotyping method requires no enzymes and relies on the high sensitivity of the gold nanoparticle probes.

A simple and rapid MS-based disulfide barcode method relies on magnifying the signal from a dual-modified gold nanoparticle and enables direct SNP genotyping of total human genomic DNA without the need for primer-mediated enzymatic amplification (Yang et al. 2010). Disulfides that are attached to the gold nanoparticle serve as a "barcode" that allows different sequences to be detected. Specificity is based on two sequential oligonucleotide hybridizations, which include two steps: the first is the capture of the target by gene-specific probes immobilized onto magnetic beads; the second is the recognition of gold nanoparticles functionalized with allele-specific oligonucleotides. The sensitivity of this method reaches down to the 0.1 fM range, thus approaching that of PCR. The feasibility of this method was demonstrated by applying it to genomic DNA samples representing all possible genotypes of the SNPs G2677T and C3435T in the human MDR1 gene.

QD Nanobarcode for Multiplexed Gene Expression Profiling

OD nanobarcode-based microbead random array platform (Life Technologies) has been used for accurate and reproducible gene expression profiling in a highthroughput and multiplexed format. Four different sizes of QDs, with emissions at 525, 545, 565, and 585 nm are mixed with a polymer and coated onto the magnetic microbeads (8 µm-diameter) to generate a nanobarcoded QBeads. Twelve intensity levels for each of the four colors are used. Gene-specific oligonucleotide probes are conjugated to the surface of each spectrally nanobarcoded bead to create a multiplexed panel, and biotinylated cRNAs are generated from sample total RNA and hybridized to the gene probes on the microbeads. A fifth streptavidin QD (655 nm or infrared QD) binds to biotin on the cRNA, acting as a quantification reporter. The intensity of the 655 nm Qdot reflects the level of biotinylated cRNA captured on the beads and provides the quantification for the corresponding target gene. The system shows a level of sensitivity, which is better than that with a high-density microarray system, and approaches the level usually observed for quantitative PCR. The QBead nanobarcode system has a dynamic range of 3.5 logs, better than the 2-3 logs observed on various microarray platforms. The hybridization reaction is performed in liquid phase and completed in 1-2 h, at least 1 order of magnitude faster than microarray-based hybridizations. Detectable fold change is lower than 1.4-fold, showing high precision even at close to single copy per cell level. Reproducibility for this proof-of-concept study approaches that of Affymetrix GeneChip microarray. In addition, it provides increased flexibility, convenience, and cost-effectiveness in comparison to conventional gene expression profiling methods.

Biobarcode Assay for Proteins

An ultrasensitive method for detecting protein analytes relies on nanoparticle probes that are encoded with DNA that is unique to the protein target of interest and antibodies. Magnetic separation of the complexed probes and target followed by dehybridization of the oligonucleotides on the nanoparticle probe surface allows the determination of the presence of the target protein by identifying the oligonucleotide sequence released from the nanoparticle probe. Because the nanoparticle probe carries with it several oligonucleotides per protein binding event, there is substantial amplification and PSA can be detected at 30 attomolar concentration. Alternatively, a PCR on the oligonucleotide bar codes can boost the sensitivity to three attomolar. Comparable clinically accepted conventional assays for detecting the same target have sensitivity limits of three picomolar, six orders of magnitude less sensitive than what is observed with this method. Further development of this technology has resulted in a biobarcode assay with a 500 zeptomolar target DNA sensitivity limit (Nam et al. 2004). Magnetic separation and subsequent release of bar code DNA from the gold nanoparticles leads to many barcode DNA strands for every target DNA (see Fig. 4.2).

One reagent is a gold nanoparticle only 30 nm in diameter; the other is a 1-µm magnetic microparticle (MMP). During the assay, the two spheres capture and sandwich the analytes. The MMPs and whatever is bound to them are then captured using a magnet, and unreacted gold NPs are washed away. Thus, only those gold spheres that have captured the analyte remain. Each gold bead also bears an abundance of bio-barcodes, custom oligonucleotides that uniquely identify the reaction.

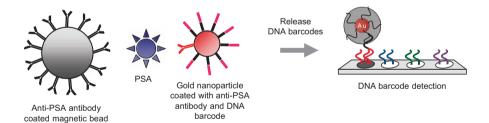


Fig. 4.2 Scheme of bio-barcode assay. Schematic illustrating PSA (prostate-specific antigen) detection using the Biobarcode assay. Antibody-coated magnetic beads capture and concentrate the protein targets. The captured protein targets are labeled with gold nanoparticle probes that are co-loaded with target specific secondary antibodies and DNA barcodes. The resulting complexes are separated magnetically and washed to remove excess probe. The DNA barcodes are then released from the complex and detected via hybridization to a surface immobilized DNA probe and an oligonucleotide functionalized gold nanoparticle. The gold particles are enlarged through silver deposition, and the light scattered from the particles is detected using the Verigene Reader optical detection system. Increased detection sensitivity is derived from: (1) capturing and concentrating protein targets with an antibody coated magnetic bead, (2) releasing multiple DNA barcodes per captured protein target (hundreds of barcode are attached to a 30 nm diameter gold particle, and (3) ultrasensitive DNA detection via silver amplified gold nanoparticles. Courtesy of Nanosphere Inc

The system ultimately detects barcodes released from the beads by heating to 55 $^{\circ}$ C and not the analytes themselves. Chip-based bar code DNA detection can be done with PCR-like sensitivity but without the use of PCR.

A nanoparticle-based biobarcode assay (BCA) has been used to measure the concentration of A β -derived diffusible ligands (ADDLs) in the cerebrospinal fluid (CSF) as a biomarker for Alzheimer's disease. Commercial enzyme-linked immunoassays (ELISA) can only detect ADDLs in brain tissue where the biomarker is most highly concentrated. Studies of ADDLs in the CSF have not been possible because of their low concentration. The bio-barcode amplification technology, which is a million times more sensitive than ELISA, can detect ADDLs in the CSF where the biomarker is present in very low concentrations. This study is a step toward a diagnostic tool, based on soluble pathogenic markers for Alzheimer's disease. The goal is to ultimately detect and validate the biomarker in blood.

Using the Verigene ID system (Nanosphere Inc), one can quantify the barcodes using the kind of technology found in a flatbed scanner, providing results as clear as an at-home pregnancy strip test. Biobarcode system is extremely sensitive for protein detection. At 30 attomolar, it is five orders of magnitude more sensitive than is ELISA (peak sensitivity of around 3 picomolars). The system has enormous potential for multiplexing. It could hypothetically test for 415 different analytes simultaneously by tagging the different gold beads with different barcode sequences. The assay, however, the fundamental issues with antibodies, such as cross-reactivity, nonspecific binding, and lot-to-lot variability remain. Antibodies can distort, fall apart, or cling to the wrong analyte. These issues are being addressed. In 2007, the FDA cleared Verigene® Warfarin Metabolism nucleic acid test followed by clearance of Verigene® F5/F2/MTHFR nucleic acid test, which detects diseaseassociated gene mutations that can contribute to blood coagulation disorders and difficulties metabolizing folate (vitamin B12). Mutations in three specific genes can increase an individual's risk for dangerous blood clots and their leading complication, stroke. Patients that test positively for an increased risk of blood clots can be managed with anticoagulant therapy such as warfarin. Hypercoagulation tests for mutations associated with a predisposition to blood clots are currently among the most frequently conducted human genetic tests. The test is available in single and multitarget (multiplex) formats, allowing users to select the test cartridge that best fits the clinical indications for testing.

A modified form of the BCA called the surface immobilized biobarcode assay (SI-BCA) is available in a microfluidic chip format (Goluch et al. 2009). The SI-BCA employs microchannel walls functionalized with antibodies that bind with the intended targets. Compared with the conventional BCA, it reduces the system complexity and results in shortened process time, which is attributed to significantly reduced diffusion times in the microscale channels. Raw serum samples, without any pretreatment, were evaluated with this technique. PSA in the samples was detected at concentrations ranging from 40 pM to 40 fM. The detection limit of the assay using buffer samples is 10 fM. The entire assay, from sample injection to final data analysis was completed in 1 h 20 min. This ability to easily and quickly detect very low levels of PSA, not detectable by conventional assays, may enable diagnosis of prostate cancer recurrence years

earlier than is currently possible. Furthermore, the effectiveness of post-operative treatment could be assessed by monitoring a patient's PSA levels. This level of sensitivity in detecting low concentrations of PSA will require revision of the normal laboratory values as currently written in reference manuals.

Single-Molecule Barcoding System for DNA Analysis

Molecular confinement offers new routes for arraying large DNA molecules, enabling single-molecule schemes aimed at the acquisition of sequence information. Such schemes can rapidly advance to become platforms capable of genome analysis if elements of a nascent system can be integrated at an early stage of development. Integrated strategies are needed for surmounting the stringent experimental requirements of nanoscale devices regarding fabrication, sample loading, biochemical labeling, and detection. Disposable devices featuring both micro- and nanoscale features have been shown to greatly elongate DNA molecules when buffer conditions are controlled for alteration of DNA stiffness (Jo et al. 2007). Analytical calculations that describe this elongation were presented. A complementary enzymatic labeling scheme was developed that tags specific sequences (bar codes) on elongated molecules within described nanoslit devices that are imaged via fluorescence resonance energy transfer. Collectively, these developments enable scaleable molecular confinement approaches for genome analysis.

Nanoparticle-Based Colorimetric DNA Detection Method

Nucleic acid diagnostics is dominated by fluorescence-based assays that use complex and expensive enzyme-based target or signal-amplification procedures. Many clinical diagnostic applications will require simpler, inexpensive assays that can be done in a screening mode. Nanosphere Inc's VerigeneTM platform uses a 'spot-andread' colorimetric detection method for identifying nucleic acid sequences based on optical properties of gold nanoparticles without the need for conventional signal or target amplification. Nucleic acid targets are recognized by DNA-modified gold probes, which undergo a color change that is visually detectable when the solutions are spotted onto an illuminated glass waveguide. Sensitivity of the spot test is improved by monitoring scattered light rather than reflected light from 40- to 50-nm diameter gold particles. This scatter-based method enables detection of zeptomole quantities of nucleic acid targets without target or signal amplification when coupled to an improved hybridization method that facilitates probe-target binding in a homogeneous format. In comparison to a previously reported absorbance-based method, this method increases detection sensitivity by over four orders of magnitude and has been applied to the rapid detection of mecA in methicillin-resistant *Staphylococcus aureus* genomic DNA samples.

Nanoparticle assemblies interconnected with DNA triple helixes can be used to colorimetrically screen for triplex DNA binding molecules and simultaneously determine their relative binding affinities based on melting temperatures. Nanoparticles assemble only when DNA triple helixes form between DNA from two different particles and a third strand of free DNA. In addition, the triple helix structure is unstable at room temperature and only forms in the presence of triplex DNA binding molecules which stabilize the triple helix. The resulting melting transition of the nanoparticle assembly is much sharper than the analogous triplex structure without nanoparticles. Upon nanoparticle assembly, a concomitant red-to-blue color change occurs. The assembly process and color change do not occur in the presence of duplex DNA binding molecules compared to standard methods.

Rapid colorimetric analysis of a specific DNA sequence has been achieved by combining gold nanoparticles (AuNPs) with an asymmetric PCR (Deng et al. 2012). In the presence of the correct DNA template, the bound oligonucleotides on the surface of AuNPs selectively hybridize to form complementary sequences of ssDNA target generated from asymmetric PCR with a concomitant color change from ruby red to blue-purple. It is a simple colorimetric method for specific nucleic acid sequence analysis with high specificity and sensitivity and has been used for the detection of *Bacillus anthracis* in clinical samples.

Nanoparticle-Based Up-Converting Phosphor Technology

Up-converting phosphor technology (UPT) is a label detection technology that can be applied to the detection of minute quantities of various substances such as antigens, proteins, and DNA. UPT particles are small ceramic nanospheres composed of rare earth metals and have been shown to be 1000 times more sensitive than current fluorescent technologies. This particle-based detection provides a stronger signal for each event detected and thereby enhances sensitivity in diagnostic assay systems. UPT has potential in a broad array of DNA testing applications including drug discovery, SNP analysis, and infectious disease testing. Employment of UPT, by by-passing target amplification, brings genetic-based testing a step closer to the point-of-care environment.

A rapid and quantitative UPT-based lateral-flow assay was developed for on-site quantitative detection of different Brucella species with high specificity, reproducibility and stability (Qu et al. 2009). UPT-lateral flow IL-10 assay is a user-friendly, rapid alternative for IL-10 ELISAs, which is suitable for multiplex detection of different cytokines, and can be merged with antibody-detection assays for simultaneous detection of cellular- and humoral immunity (Corstjens et al. 2011).

Surface-Enhanced Resonant Raman Spectroscopy

SERRS (Surface-Enhanced Resonant Raman Spectroscopy)-Beads brings various components of the technology into a single robust nano-sized polymer-bead support with broad applications in molecular and immunodiagnostics. Focusing on organic fluorescent dyes, because of their strong excitation cross-section, compounds are selected experimentally for strong affinity for the silver enhancing surfaces and good spectral resolution. Initially using four dyes, the possibilities for tens to hundreds of unique labels is currently under development. The chosen dyes also have excitation peaks that overlap with the metal plasmon frequency, thereby adding the all-important resonant amplification to the signal intensity.

At the core of the bead is the Raman-active substrate, where silver colloid, with defined physical characteristics, provides the surface-enhancement substrate and is combined with the dye or dyes for specific bead encoding. Control of the various parameters surrounding dye:colloid aggregate permits SERRS response to be modulated as desired.

To protect the SERRS-active complex from degradation, the aggregate is encapsulated in a polymer coating, a process that incorporates a multitude of dye:colloid particles into the same bead. This leads to highly sensitive beads with responses greater than those achieved by using the conformation of single dye molecules on an enhancing surface.

The polymer coating is treated further with a polymer shell to allow a variety of biologically relevant probe molecules (e.g. antibodies, antigens, nucleic acids) to be attached through standard bioconjugation techniques. While most of the development is focused on heterogeneous assays in a 96-well assay sample presentation, other designs include higher plate capacities (384-well) for higher throughput screening and microarray slide reading for DNA and proteomic analysis. Photonic crystal surfaces are used for enhancing the detection of SERR, and the development of high resolution photonic crystal-based laser biosensors, which can be used for gene expression analysis, and protein biomarker detection (Cunningham 2010).

Near-Infrared (NIR)-Emissive Polymersomes

In vivo fluorescence imaging with near-infrared (NIR) light has enormous potential for a wide variety of molecular diagnostic applications. Because of its quantitative sensitivity, inherent biological safety, and relative ease of use, fluorescence-based imaging techniques are being increasingly used in small-animal research. Moreover, there is substantial interest in the translation of novel optical techniques into the clinic, where they will prospectively aid in noninvasive and quantitative screening, disease diagnosis, and post-treatment monitoring of patients. Effective deep-tissue fluorescence imaging requires the application of exogenous NIR-emissive contrast agents. Currently, available probes fall into two major categories: organic and

inorganic NIR fluorophores (NIRFs). Various studies have used polymersomes (50 nm–50 μ m diameter polymer vesicles) for the incorporation and delivery of large numbers of highly emissive oligo (porphyrin)-based, organic NIRFs (Ghoroghchian et al. 2009). The total fluorescence emanating from the assemblies gives rise to a localized optical signal of sufficient intensity to penetrate through the dense tumor tissue of a live animal. Robust NIR-emissive polymersomes thus define a soft matter platform with exceptional potential to facilitate deep-tissue fluorescence-based imaging for in vivo diagnosis.

Nanobiotechnology for Detection of Proteins

Detection of proteins is an important part of molecular diagnostics. Uses of protein nanobiochips and nano-barcode technology for detection of proteins have been described in preceding sections. Other methods will be included in this section.

Captamers with Proximity Extension Assay for Proteins

Multivalent circular aptamers or 'captamers' are formed through the merger of aptameric recognition functions with the DNA as a nanoscale scaffold. Whereas the sequence immobilized to the microtiter plate is termed captamer, the sequence used for detection is called detectamer. Aptamers are useful as protein-binding motifs for diagnostic applications, where their ease of discovery, thermal stability and low cost make them ideal components for incorporation into targeted protein assays. Captamers are compatible with a highly sensitive protein detection method termed the 'proximity extension' assay. The circular DNA architecture facilitates the integration of multiple functional elements into a single molecule: aptameric target recognition, nucleic acid hybridization specificity and rolling circle amplification. Successful exploitation of these properties is demonstrated for the molecular analysis of thrombin, with the assay delivering a detection limit nearly three orders of magnitude below the dissociation constants of the contributing aptamer-thrombin interactions.

Use of liposomes as labels for aptamer-based assays and successful incorporation of cholesteryl–TEG DNA aptamers into liposomal lipid bilayers with subsequent successful function in target recognition further demonstrates the versatility of liposomes as signaling reagents and their potential as a standard platform technology for various analyses. Such an assay yields a limit of detection of 64 pM or 2.35 ng/mL, corresponding to 6.4 fmol or 235 pg, respectively, in a 100 μ L volume (Edwards et al. 2010).

Real-time signal amplification, detection under isothermal conditions, specificity and sensitivity would suggest potential application of captamer-based protein assay for further development of personalized medicine.

Immunoliposome-PCR

The accurate quantification of antigens at low concentrations over a wide dynamic range is needed for identifying biomarkers associated with disease and detecting protein interactions in high-throughput microarrays used in proteomics. An ultrasensitive quantitative assay format called immunoliposome polymerase chain reaction (ILPCR) has been developed that fulfills these requirements (He et al. 2012). This method uses a liposome, with reporter DNA encapsulated inside and biotinlabeled PEG phospholipid conjugates incorporated into the outer surface of the 117 nm liposomes as a detection reagent. The liposomes were ruptured to release the reporter DNA to serve as a surrogate to quantify the protein target using real-time PCR.

This liposome detection reagent was used in an assay to quantify the concentration of CEA in human serum. The assay detection limit was 13 fg/mL, which is 1500-times more sensitive than current clinical assays for CEA. The ILPCR assay has several advantages over other immuno-PCR methods. The reporter DNA and biotin-labeled PEG phospholipids spontaneously incorporate into the liposomes as they form, simplifying preparation of the detection reagent. Encapsulation of the reporter inside the liposomes allows nonspecific DNA in the assay medium to be degraded with DNase I prior to quantification of the encapsulated reporter by PCR, which reduces false-positive results and improves quantitative accuracy. The ability to encapsulate multiple reporters per liposome also helps overcome the effect of polymerase inhibitors present in biological specimens. Finally, the biotin-labeled liposome detection reagent can be coupled through a NeutrAvidin bridge to a multitude of biotin-labeled probes, making ILPCR a highly generic assay system.

Nanobiosensors

Nanosensors are devices that employ nanomaterials, exploiting novel size-dependent properties, to detect gases, chemicals, biological agents, electric fields, light, heat, or other targets. The term "nanobiosensors" implies use of nanosensors for detection of chemical or biological materials. Nanomaterials are exquisitely sensitive chemical and biological sensors.

The sensors can be electronically gated to respond to the binding of a single molecule. Prototype sensors have demonstrated detection of nucleic acids, proteins and ions. These sensors can operate in the liquid or gas phase, opening an enormous variety of downstream applications. The detection schemes use inexpensive low voltage measurement schemes and detect binding events directly so there is no need for costly, complicated and time-consuming labeling chemistries such as fluorescent dyes or the use of bulky and expensive optical detection systems. Therefore, these sensors are inexpensive to manufacture and portable. It may even be possible to develop implantable detection and monitoring devices based on these detectors. Some of the technologies that can be incorporated in biosensing are already covered in earlier sections. An example is nanopore technology, which can form the basis of nanosensors. Some of the biosensor devices are described in the following sections.

Cantilevers as Biosensors for Molecular Diagnostics

Cantilevers (Concentris) are small beams like those used in AFM to screen biological samples for the presence of genetic sequences. The surface of each cantilever is coated with DNA that can bind to one specific target sequence. On exposure of the sample to beams, the surface stress bends the beams by approximately 10 nm to indicate that the beams have found the target in the sample. This is considered biosensing.

Cantilever technology complements and extends current DNA and protein microarray methods because nanomechanical detection requires no labels, optical excitation, or external probes and is rapid, highly specific, sensitive, and portable. The nanomechanical response is sensitive to the concentration of oligonucleotides in solution, and thus one can determine how much of a given biomolecule is present and active. In principle cantilever arrays also could quantify gene-expression levels of mRNA, protein-protein, drug-binding interactions, and other molecular recognition events in which physical steric factors are important. It can detect a single gene within a genome. Furthermore, fabricating thinner cantilevers will enhance the molecular sensitivity further, and integrating arrays into microfluidic channels will reduce the amount of sample required significantly. In contrast to SPR, cantilevers are not limited to metallic films, and other materials will be explored, e.g., cantilevers made from polymers. In addition to surface-stress measurements, operating cantilevers in the dynamic mode will provide information on mass changes, and current investigations will determine the sensitivity of this approach. Currently it is possible to monitor more than 1000 cantilevers simultaneously with integrated piezoresistive readout, which in principle will allow high-throughput nanomechanical genomic analysis, proteomics, biodiagnostics, and combinatorial drug discovery.

Cantilevers in an array can be functionalized with a selection of biomolecules. Researchers at IBM, Zurich, Switzerland reported the specific transduction, via surface stress changes, of DNA hybridization and receptor-ligand binding into a direct nanomechanical response of microfabricated cantilevers. The differential deflection of the cantilevers was found to provide a true molecular recognition signal despite large nonspecific responses of individual cantilevers. Hybridization of complementary oligonucleotides shows that a single base mismatch between two 12-mer oligonucleotides is clearly detectable. Similar experiments on protein A-immunoglobulin interactions demonstrate the wide-ranging applicability of nanomechanical transduction to detect biomolecular recognition. Microarray of cantilevers has been used to detect multiple unlabeled biomolecules simultaneously at nanomolar concentrations within minutes. A specific test that uses micrometer-scale beams or 'microcantilever' can detect prostate-specific antigen (PSA). PSA antibodies are attached to the surface of the microcantilever, which is applied to a sample containing PSA. When PSA binds to the antibodies, a change in the surface stress on the microcantilever makes it bend enough to be detected by a laser beam. This system can detect clinically relevant concentrations of PSA in a background of other proteins. The technique is simpler and potentially more cost-effective than other diagnostic tests because it does not require labeling and can be performed in a single reaction. It is less prone to false positives, which are commonly caused by the nonspecific binding of other proteins to the microcantilever.

Potential applications in proteomics include devices comprising many cantilevers, each coated with a different antibody, which might be used to test a sample rapidly and simultaneously for the presence of several disease-related proteins. One application is for detection of biomarkers of myocardial infarction such as creatine kinase at point-of-care. Other future applications include detection of disease by breath analysis, e.g. presence of acetone and dimethylamine (uremia). Detection of a small number of Salmonella enterica bacteria is achieved due to a change in the surface stress on the silicon nitride cantilever surface in situ upon binding of bacteria. Scanning electron micrographs indicate that less than 25 adsorbed are required for detection.

Advantages of Cantilever Technology for Molecular Recognition

Cantilever technology has the following advantages over conventional molecular diagnostics:

- It circumvents the use of PCR.
- For DNA, it has physiological sensitivity and no labeling is required.
- In proteomics, it enables detection of multiple proteins and direct observation of proteins in diseases such as those involving the cardiovascular system.
- It enables the combination of genomics and proteomics assays.
- It is compatible with silicon technology.
- It can be integrated into microfluidic devices.

Antibody-Coated Nanocantilevers for Detection of Microorganisms

Nanocantilevers could be crucial in designing a new class of ultra-small sensors for detecting viruses, bacteria and other pathogens. The cantilevers, coated with antibodies to detect certain viruses, attract different densities or quantity of antibodies per area depending on the size of the cantilever. The devices are immersed into a liquid containing the antibodies to allow the proteins to stick to the cantilever surface. Instead of simply attracting more antibodies, the longer cantilevers also contained a greater density of antibodies. The density is greater toward the free end of the cantilevers. The cantilevers vibrate faster after the antibody attachment if the devices have about the same nanometer-range thickness (~20 nm) as the protein layer. Moreover, the

longer the protein-coated nanocantilever, the faster the vibration, which could only be explained if the density of antibodies were to increase with increasing lengths.

The cantilever's vibration frequency can be measured using an instrument called a laser Doppler vibrometer, which detects changes in the cantilever's velocity as it vibrates. This work may have broad impact on microscale and nanoscale biosensor design, especially when predicting the characteristics of nanobioelectromechanical sensors functionalized with biological capture molecules. The nanocantilevers could be used in future detectors because they vibrate at different frequencies when contaminants stick to them, revealing the presence of dangerous substances. Because of the nanocantilever's minute size, it is more sensitive than larger devices, promising the development of advanced sensors that detect minute quantities of a contaminant to provide an early warning that a dangerous pathogen is present. At the nanoscale, just adding the mass of one bacterium, virus or large molecule is enough to change the resonant frequency of vibration of the cantilever by a measurable amount, thereby signaling the presence of the pathogen. If one is trying to detect E. coli, other organisms in the fluid can weakly absorb on the detector by electrostatic forces. This is a problem in any biodetection and can be resolved by making the resonator vibrate from side to side. This will shake off loosely adhered materials, while whatever is tightly bound to an antibody will remain.

One method for the rapid and sensitive detection of disease- and treatmentrelevant genes is based on direct measurement of their transcripts (mRNA), which represent the intermediate step and link to protein synthesis. Short complementary nucleic acid segments (sensors) are attached to silicon cantilevers which are 450 nm thick and therefore react with extraordinary sensitivity. Binding of the targeted gene transcript to its matching counterpart on one of the cantilevers results in optically measurable mechanical bending.

Differential gene expression of the gene 1-8U, a potential marker for cancer progression or viral infections, could be observed in a complex background. The measurements provide results within minutes at the picomolar level without target amplification, and are sensitive to base mismatches. An array of different gene transcripts can even be measured in parallel by aligning appropriately coated cantilevers alongside each other like the teeth of a comb. The new method complements current molecular diagnostic techniques such as the gene chip and real-time PCR. It could be used as a real-time sensor for continuously monitoring various clinical parameters or for detecting rapidly replicating pathogens that require prompt diagnosis. These findings qualify the technology as a rapid method to validate biomarkers that reveal disease risk, disease progression or therapy response. Cantilever arrays have potential as a tool to evaluate treatment response efficacy for personalized medical diagnostics.

Carbon Nanotube Biosensors

Over the years, researchers have sought to tailor carbon nanotubes to detect chemicals ranging from small gas molecules to large biomolecules. The tubes' small size and unique electronic properties make them especially adept at detecting minute changes

in the environment. Optical nanosensors can use single-walled carbon nanotubes that modulate their emission in response to the adsorption of specific biomolecules with two distinct mechanisms of signal transduction - fluorescence quenching and charge transfer. The nanotube-based chemical sensors developed so far generate an electric signal in the presence of a particular molecule. The basic design is widely applicable for such analytical tasks as detecting genes and proteins associated with diseases.

To test the feasibility of implanting the sensors in the body, oxidase- and ferricyanide-coated nanotubes were placed inside a sealed glass tube a centimeter long and 200 microns thick. The tube is riddled with pores large enough to let glucose enter but small enough to keep the nanotubes inside. The tube was then implanted in a sample of human skin and the sensor could be excited with infrared light and detect its fluorescence.

Carbon Nanotube Sensors Coated with ssDNA and Electronic Readout

Nanoscale chemical sensors can be based on ssDNA as the chemical recognition site and single-walled carbon nanotube field effect transistors (SWCN-FETs) as the electronic read-out component. SWCN-FETs with a nanoscale coating of ssDNA respond to gas odors that do not cause a detectable conductivity change in bare devices. Responses of ssDNA/SWCN-FETs differ in sign and magnitude for different gases and can be tuned by choosing the base sequence of the ssDNA. ssDNA/SWCN-FET sensors detect a variety of odors, with rapid response and recovery times on the scale of seconds. The arrays of nanosensors could detect molecules on the order of one part per million. The sensor surface is self-regenerating: samples maintain a constant response with no need for sensor refreshing through at least 50 gas exposure cycles. The nanosensors could sniff molecules in the air or taste them in a liquid. This remarkable set of attributes makes sensors based on ssDNA decorated nanotubes promising for "electronic nose" and "electronic tongue" applications ranging from homeland security to disease diagnosis.

Carbon Nanotubes Sensors Wrapped with DNA and Optical Detection

SWCNs wrapped with DNA can be placed inside living cells and detect trace amounts of harmful contaminants using near infrared light. The sensor is constructed by wrapping the double-stranded DNA around the surface of a single-walled carbon nanotube, in much the same fashion as a telephone cord wraps around a pencil. The DNA starts out wrapping around the nanotube with a certain shape that is defined by the negative charges along its backbone. Subtle rearrangement of an adsorbed biomolecule can be directly detected by such a carbon nanotube. At the heart of the new detection system is the transition of DNA secondary structure from the native, right-handed "B" form to the alternate, left-handed "Z" form. The thermodynamics that drive the switching back and forth between these two forms of DNA structure would modulate the electronic structure and optical emission of the carbon nanotube.

When the DNA is exposed to ions of certain atoms such as calcium or mercury, the negative charges become neutralized and the DNA changes shape in a similar manner to its natural shape-shift from the B form to Z form. This reduces the surface area covered by the DNA, perturbing the electronic structure and shifting the nanotube's natural, near infrared fluorescence to a lower energy. The change in emission energy indicates how many ions bind to the DNA. Removing the ions will return the emission energy to its initial value and flip the DNA back to the starting form, making the process reversible and reusable. The viability of this measurement technique was demonstrated by detecting low concentrations of mercury ions in whole blood, opaque solutions, and living mammalian cells and tissues where optical sensing is usually poor or ineffective. Because the signal is in the near infrared, a property unique to only a handful of materials, it is not obscured by the natural fluorescence of polymers and living tissues. The nanotube surface acts as the sensor by detecting the shape change of the DNA as it responds to the presence of target ions. This discovery opens the door to new types of optical sensors and biomarkers that exploit the unique properties of nanoparticles in living systems.

A pair of SWCNs provides at least four modes that can be modulated to uniquely fingerprint agents by the degree to which they alter either the emission band intensity or wavelength. This identification method was validated in vitro by demonstrating the detection of six genotoxic analytes, including chemotherapeutic drugs and reactive oxygen species, which are spectroscopically differentiated into four distinct classes, and demonstrate single-molecule sensitivity in detecting hydrogen peroxide (Heller et al. 2009). A SWCN sensor can be placed in living cells, healthy or malignant, to detect several different classes of molecules that damage DNA.

FRET-Based DNA Nanosensor

Rapid and highly sensitive detection of DNA is critical in diagnosing genetic diseases. Conventional approaches often rely on cumbersome, semi-quantitative amplification of target DNA to improve detection sensitivity. In addition, most DNA detection systems (microarrays, for example), regardless of their need for target amplification, require separation of unhybridized DNA strands from hybridized stands immobilized on a solid substrate, and are thereby complicated by solutionsurface binding kinetics. An ultrasensitive nanosensor is based on fluorescence resonance energy transfer (FRET) capable of detecting low concentrations of DNA in a separation-free format. This system uses quantum dots (QDs) linked to DNA probes to capture DNA targets. The target strand binds to a dye-labeled reporter strand thus forming a FRET donor-acceptor ensemble. The QD also functions as a concentrator that amplifies the target signal by confining several targets in a nanoscale domain. Unbound nanosensors produce near-zero background fluorescence, but on binding to even a small amount of target DNA (~50 copies or less), they generate a very distinct FRET signal. A nanosensor-based oligonucleotide ligation assay has been demonstrated to successfully detect a point mutation typical of some ovarian tumors in clinical samples.

Graphene Biosensor Based on Raman Spectroscopy

In Raman spectroscopy, when a laser light irradiates crystals or molecules, it scatters and shifts colors. That scattered light can be detected in the form of a Raman spectrum, which serves almost as a fingerprint for every Raman-active irradiated system. Different colors in the visible spectrum are associated to different energies and each molecule has a distintive light color emission. However, the Raman signal is quite weak and several methods have been used to enhance the signal. Pristine graphene can enhance the Raman signal by several orders of magnitude. A highly sensitive chemical biosensor is based on Raman spectroscopy and uses nitrogen-doped graphene as a substrate, i.e., introducing nitrogen atoms into the carbon structure of graphene (Feng et al. 2016). This technique can detect trace amounts of molecules in a solution at very low concentrations, ~10,000 times more diluted than can be seen by the naked eye. This technique will be effective for detecting trace amounts of organic molecules

Ion Channel Switch Biosensor Technology

The ion channel switch is a biosensor technology based upon a synthetic selfassembling membrane, which acts like a biological switch and can detect the presence of specific molecules, and signaling their presence by triggering an electrical current. It candetect a change in ion flow upon binding with the target molecule resulting in a rapid result currently unachievable using existing technologies. An ion-channel biosensor comprised of gramicidin A channels embedded in a synthetic tethered lipid bilayer provides a highly sensitive and rapid detection method, e.g. for influenza A in untreated clinical samples (Krishnamurthy et al. 2010).

Electrochemical Nanobiosensor

An electrochemical biosensor combining microfluidics and nanotechnology has been developed by GeneFluidics with 16 sensors in the array, each consisting of three single-layer gold electrodes - working, reference, and auxiliary. Each of the working electrodes contains one representative from a library of capture probes, which are specific for a clinically relevant bacterial urinary pathogen. The library included probes for *Escherichia coli, Proteus mirabilis, Pseudomonas aeruginosa, Enterocococcus spp*, and the *Klebsiella-Enterobacter* group. A bacterial 16S rRNA target derived from single-step bacterial lysis was hybridized both to the biotinmodified capture probe on the sensor surface and to a second, fluorescein-modified detector probe. Detection of the target-probe hybrids is achieved through binding of a horseradish peroxidase (HRP)-conjugated anti-fluorescein antibody to the detector probe. Amperometric measurement of the catalyzed HRP reaction is obtained at a fixed potential of -200 mV between the working and reference electrodes. Speciesspecific detection of as few as 2600 pathogenic bacteria in culture, inoculated urine, and clinical urine samples can be achieved within 45 min from the beginning of sample processing. In a feasibility study of this amperometric detection system using blinded clinical urine specimens, the sensor array had 100% sensitivity for direct detection of gram-negative bacteria without nucleic acid purification or amplification. Identification was demonstrated for 98% of gram-negative bacteria for which species-specific probes were available. When combined with a microfluidics-based sample preparation module, the integrated system could serve as a point-of-care device for rapid diagnosis of urinary tract infections.

Electronic Nanobiosensors

An earlier form of electronic DNA biosensor achieved a label-free subpicomolar detection. The sensor, which is based on a target-induced strand displacement mechanism, is composed of a "capture probe" attached by its 5' terminus to a gold electrode and a 5' methylene blue-modified "signaling probe" that is complementary at both its 3' and 5' termini to the capture probe. In the absence of target, hybridization between the capture and signaling probes minimizes contact between the methylene blue and electrode surface, limiting the observed redox current. Target hybridization displaces the 5' end of the signaling probe, generating a short, flexible single-stranded DNA element and producing up to a sevenfold increase in redox current. The observed signal gain is sufficient to achieve a demonstrated (not extrapolated) detection limit of 400 fM, which is among the best reported for single-step electronic DNA detection.

A 3D real-time and label-free nanotip array with a nano-sized thin film as the sensing area (~20 nm) sandwiched between two sensing electrodes, has been used for sequence-specific DNA screening (Esfandyarpour et al. 2016). The tip is conjugated to a DNA oligonucleotide complementary to the sequence of interest, which is electrochemically detected in real-time via impedance changes following formation of a dsDNA helix at the sensor interface. This highly sensitive, inexpensive nanotip array has potential for development for POC diagnostics, and high-throughput DNA analysis applications.

Electronic field effect transistor (FET) nanosensors based on synthetic nanomaterials have been used for real-time label-free detection of a wide range of biological species with high sensitivity, although direct analysis of biological samples is limited due to Debye charge screening in physiological solutions. A strategy to overcome this challenge involves comodification of the surface of silicon nanowire FET sensors with a polymer and receptor, where the polymer forms a permeable layer to increase the effective screening length, and receptor enables selective detection of analytes (Gao et al. 2016). The capability of this strategy was demonstrated by selective detection of cancer biomarkers in physiological solution, indicating clinical applications for real-time sensing.

Metallic Nanobiosensors

Fano resonances have been observed in the optical response of plasmonic nanocavities due to the coherent coupling between their superradiant and subradiant plasmon modes and multiple Fano resonances occur as structure size is increased (Verellen et al. 2009). By putting together two specific nanostructures made of gold or silver, a prototype device can be constructed, which exhibits a highly sensitive ability to detect specific chemicals in the immediate surroundings once it is optimized. The nanostructures measure about 200 nm. One is shaped like a flat circular disk while the other looks like a doughnut with a hole in the middle. When brought together they interact with light very differently to the way they behave on their own. When they are paired up they scatter some specific colors within white light much less, leading to an increased amount of light passing through the structure undisturbed. This is distinctly different to how both structures scatter light separately. Metal nanostructures have been used as sensors but they interact very strongly with light due to so-called localized plasmon resonances. But this is the first time a pair with such a carefully tailored interaction with light has been created. This decrease in the interaction with light is in turn affected by the composition of molecules close to the structures. These nanosensors could be tailor-made to instantly detect the presence of certain molecules, for example poisons or explosives in transport screening situations, or proteins in patients' blood samples, with high sensitivity.

Nanomaterial-Based Sensors for Diagnosis from Exhaled Breath

To develop breath testing for identifying Alzheimer's disease (AD) and Parkinson's disease (PD), alveolar breath was collected from volunteers (AD patients, PD patients and healthy controls) and analyzed using combinations of nanomaterial-based sensors (Tisch et al. 2013). Discriminant factor analysis was applied to detect statistically significant differences between study groups and classification success was estimated using cross-validation. The pattern identification was supported by chemical analysis of the breath samples using gas chromatography combined with MS. The combinations of sensors could clearly distinguish AD from healthy states, PD from healthy states, and AD from PD states, with a classification accuracy of 85, 78 and 84%, respectively. Gas chromatography combined with MS analysis showed statistically significant differences in the average abundance of several volatile organic compounds in the breath of AD, PD and healthy subjects, thus supporting the breath prints observed with the sensors. Conclusion is that breath prints identified with combinations of nanomaterial-based sensors have future potential as cost-effective, fast and reliable biomarkers for AD and PD.

Quartz Nanobalance Biosensor

Single-strand DNA-containing thin films are deposited onto quartz oscillators to construct a device capable of sensing the presence of the complementary DNA sequences, which hybridize with the immobilized ones. DNA, once complexed with aliphatic amines, appears as a monolayer in a single-stranded form by X-ray small angle scattering. A quartz nanobalance is then utilized to monitor mass increment related to specific hybridization with a complementary DNA probe. The crystal quartz nanobalance, capable of high sensitivity, indeed appears capable of obtaining a prototype of a device capable of sensing the occurrence of specific genes or sequences in the sample under investigation.

Viral Nanosensor

Virus particles are essentially biological nanoparticles. Scientists at the Massachusetts General Hospital (Boston, MA) have used herpes simplex virus (HSV) and adenovirus to trigger the assembly of magnetic nanobeads as a nanosensor for clinically relevant viruses. The nanobeads had a supramagnetic iron oxide core coated with dextran. Protein G was attached as a binding partner for antivirus antibodies. By conjugating anti-HSV antibodies directly to nanobeads using a bifunctional linker to avoid non-specific interactions between medium components and protein G and using a magnetic field, the scientists could detect as few as five viral particles in a 10 mL serum sample. This system is more sensitive than ELISA-based methods and is an improvement over PCR-based detection because it is cheaper, faster and has fewer artifacts. Upon target binding, these nanosensors cause changes in the spin-spin relaxation times of neighboring water molecules, which can detect specific mRNA, proteins and enzymatic activity by (NMR/MRI) techniques.

A QD-DNA nanosensor, based on fluorescence resonance energy transfer (FRET), has been used for the detection of the target DNA and single mismatch in hepatitis B virus (HBV) gene (Wang et al. 2010a). This DNA detection method is simple, rapid and efficient due to the elimination of the washing and separation steps. In this study, oligonucleotides were attached to the QD surface to form functional QD-DNA conjugates. With the addition of DNA targets and Cy5-modified signal DNAs into the QD-DNA conjugates, sandwiched hybrids were formed leading to fluorescence from the acceptor by means of FRET on illumination of the donor. Oligonucleotide ligation assay was employed to efficiently detect single-base mutants in HBV gene. This simple method enables efficient detection that could be used for high throughput and multiplex detections of viral gene mutations.

PEBBLE Nanosensors

PEBBLE (Probes Encapsulated by Biologically Localized Embedding) nanosensors consist of sensor molecules entrapped in a chemically inert matrix by a microemulsion polymerization process that produces spherical sensors in the size range of 20–200 nm. PEBBLE sensors, have been developed for many important intracellular analytes and functions, including ions, small molecules, reactive oxygen species, physical properties, and enzyme activities, which are involved in many chemical, biochemical, and physical processes taking place inside the cell (Lee and Kopelman 2012). PEBBLE nanosensors can be used with a standard microscope for simultaneous optical imaging of cellular structures and sensing of composition and function, just like investigations performed with molecular probes. PEBBLE nanosensors also show very good reversibility and stability to leaching and photobleaching, as well as very short response times and no perturbation by proteins. In human plasma, they demonstrate a robust oxygen sensing capability, little affected by light scattering and autofluorescence. PEBBLE can also be used for early detection of cancer and has been developed further as a tool for diagnosis as well as treatment of cancer.

Detection of Cocaine Molecules by Nanoparticle-Labeled Aptasensors

Metallic or semiconductor nanoparticles (NPs) are used as labels for the electrochemical, photoelectrochemical, or surface plasmon resonance (SPR) detection of cocaine using a common aptasensor configuration (Golub et al. 2009). The aptasensors are based on the use of two anticocaine aptamer subunits, where one subunit is assembled on an Au support, acting as an electrode or a SPR-active surface, and the second aptamer subunit is labeled with Pt-NPs, CdS-NPs, or Au-NPs. In the different aptasensor configurations, the addition of cocaine results in the formation of supramolecular complexes between the NPs-labeled aptamer subunits and cocaine on the metallic surface, enabling quantitative analysis of cocaine. The supramolecular Au-NPs-aptamer subunits-cocaine complex generated on the Au support allows the SPR detection of cocaine through the reflectance changes stimulated by the electronic coupling between the localized plasmon of the Au-NPs and the surface plasmon wave. All aptasensor configurations enable the analysis of cocaine with a detection limit in the range of $10^{-6}-10^{-5}$ M. The major advantage of the sensing platform is the lack of background interfering signals.

Nanosensors for Glucose Monitoring

One of the main reasons for developing in vivo glucose sensors is the detection of hypoglycemia in people with insulin dependent (type 1) diabetes. It is possible to engineer fluorescent micro/nanoscale devices for glucose sensing. Deployment of

nanoparticles in the dermis may allow transdermal monitoring of glucose changes in interstitial fluid. Using electrostatic self-assembly, an example of nanotechnology for fabrication, two types of sensors are being studied: (1) solid nanoparticles coated with fluorescent enzyme-containing thin films and (2) hollow nanocapsules containing fluorescent indicators and enzymes or glucose-binding proteins. Nanoengineering of the coated colloids and nanocapsules allows precision control over optical, mechanical, and catalytic properties to achieve sensitive response using a combination of polymers, fluorescent indicators, and glucose-specific proteins. Challenges to in vivo use include understanding of material toxicity and failure modes, and determining methods to overcome fouling, protein inactivation, and material degradation. Noninvasive glucose sensing will maximize acceptance by patients and overcome biocompatibility problems of implants. Near infrared spectroscopy has been most investigated but the precision needs to be improved for eventual clinical application.

The nanotube-based optical biosensor could free people with diabetes from the daily pinprick tests now required for monitoring blood sugar concentrations. Carbon nanotubes are coated with glucose oxidase, an enzyme that breaks down glucose molecules. Then ferricyanide, an electron-hungry molecule, is sprinkled, onto the nanotubes' surfaces. Ferricyanide draws electrons from the nanotubes, quenching their capacity to glow when excited by infrared light. When glucose is present, it reacts with the oxidase, producing hydrogen peroxide. In turn, the hydrogen peroxide reacts with ferricyanide in a way that reduces that molecule's hunger for electrons. The higher the glucose level, the greater is the nanotube's infrared fluorescence.

Micromechanical detection of biologically relevant glucose concentrations can be achieved by immobilization of glucose oxidase (GOx) onto a microcantilever surface. The enzyme-functionalized microcantilever undergoes bending due to a change in surface stress induced by the reaction between glucose in solution and the GOx immobilized on the cantilever surface.

Nanobiosensors for Protein Detection

High sensitivity biosensors for the detection of proteins have been developed using several kinds of nanomaterials. The performance of the sensors depends on the type of nanostructures with which the biomaterials interact. 1D structures such as nanowires, nanotubes and nanorods are proven to have high potential for bio-applications. Different types of nanostructures that have attracted much attention by their performance as biosensors utilize materials such as polymers, carbon and zinc oxide because of their sensitivity, biocompatibility, and ease of preparation (M et al. 2011). This publication describes the three stages in the development of biosensors: (1) fabrication of biomaterials into nanostructures; (2) alignment of the nanostructures; and (3) immobilization of proteins.

Optical Biosensors

Many biosensors that are currently marketed rely on the optical properties of lasers to monitor and quantify interactions of biomolecules that occur on specially derived surfaces or biochips. An integrated biosensor, based on phototransistor integrated circuits, has been developed for use in medical detection, DNA diagnostics, and gene mapping. The biochip device has sensors, amplifiers, discriminators, and logic circuitry on board. Integration of light-emitting diodes into the device is also possible. Measurements of fluorescent-labeled DNA probe microarrays and hybridization experiments with a sequence-specific DNA probe for HIV-1 on nitrocellulose substrates illustrate the usefulness and potential of this DNA biochip. Several variations of optical biosensors offer distinct methods of sample application and detection in addition to different types of sensor surface. Surface plasmon resonance technology is an example of this technology.

Laser Nanosensors

In a laser nanosensor, laser light is launched into the fiber, and the resulting evanescent field at the tip of the fiber is used to excite target molecules bound to the antibody molecules. A photometric detection system is used to detect the optical signal (e.g. fluorescence) originating from the analyte molecules or from the analyte-bioreceptor reaction. Laser nanosensors can be used for in vivo analysis of proteins and biomarkers in individual living cells (Vo-Dinh and Zhang 2011). The nanosensors are made of tapered optical fibers with distal ends having nanometer-sized diameters. Bioreceptors, such as antibody, peptides, and nucleic acids, are immobilized on the fiber tips and designed to be selective to target analyte molecules of interest. A laser beam is transmitted through the fiber and excites target molecules bound to the bioreceptor molecules. The resulting fluorescence from the analyte molecules is detected by a photo-detection system. Nanosensors can provide minimally invasive tools to probe subcellular compartments inside individual living cells.

Physicists at University of Rochester have assembled a simple laser system to detect nanoparticles. They split a laser beam in two, sending one half to a sample. When the light hits a small particle, it is scattered back and recombines with the reserve half of the laser beam, producing a detectable interference pattern detectable only when a moving particle is present. This laser method works where others do not because it relies on the amplitude rather than intensity of light. The amplitude is the square root of intensity, so it decays much less than intensity as the particles get smaller. Single particles, as small as 7 nm in diameter, have been detected.

Interferometric Reflectance Imaging Sensors

An interferometric reflectance imaging (an optical sensing technology) sensor that could potentially be used in a handheld device to detect various viruses and measure their concentration within minutes has been developed (Ymeti et al. 2007). It requires only a tiny sample of saliva, blood, or other body fluid. The device uses a silicon

substrate containing channels that guide laser light. Light enters the substrate at one end and is split into four parallel beams. When these beams emerge at the other end, they spread out and overlap with one another, creating a pattern of bright and dark bands, known as an interference pattern, which are recorded. Although the sensor has been shown to detect only the herpes-simplex virus, it could be used to quickly screen people at hospitals and emergency clinics for control of outbreaks of diseases such as SARS and avian flu. Interferometric reflectance imaging-based sensors enable digital detection of individual nanoparticles. Their applications include label-free detection of multiplexed protein chips, measurement of single nucleotide polymorphisms, quantification of transcription factor DNA binding, and characterization of nanoparticles (Avci et al. 2015).

Nanoshell Biosensors

Nanoshells can enhance chemical sensing by as much as ten billion times. That makes them about 10,000 times more effective at Raman scattering than traditional methods. When molecules and materials scatter light, a small fraction of the light interacts in such a way that it allows scientists to determine their detailed chemical makeup. This property, known as Raman scattering, is used by medical researchers, drug designers, chemists and other scientists to determine what materials are made of. An enormous limitation in the use of Raman scattering has been its extremely weak sensitivity. Nanoshells can provide large, clean, reproducible enhancements of this effect, opening the door for new, all-optical sensing applications. Each individual nanoshell can act as an independent Raman enhancer. That creates an opportunity to design all-optical nanoscale sensors - essentially molecular diagnostic instruments - that could detect as little as a few molecules of a target substance, which could be anything from a drug molecule or a key disease protein to a deadly chemical agent.

The metal cover of the nanoshell captures passing light and focuses it, a property that directly leads to the enormous Raman enhancements observed. Furthermore, nanoshells can be tuned to interact with specific wavelengths of light by varying the thickness of their shells. This tunability allows for the Raman enhancements to be optimized for specific wavelengths of light. The finding that individual nanoshells can vastly enhance the Raman effect opens the door for biosensor designs that use a single nanoshell, something that could prove useful for engineers who are trying to probe the chemical processes within small structures such as individual cells, or for the detection of very small amounts of a material, like a few molecules of a deadly biological or chemical agent. Nanoshells are already being developed for applications including cancer diagnosis, cancer therapy, testing for proteins associated with Alzheimer's disease, drug delivery and rapid whole-blood immunoassays.

Plasmonics and SERS Nanoprobes

Surface plasmons are collective oscillations of free electrons at metallic surfaces. These oscillations can give rise to the intense colors of solutions of plasmon resonance nanoparticles and very intense scattering. While the use of plasmonic particle absorption based bioaffinity sensing is now widespread throughout biological research, the use of their scattering properties is relatively less studied. Plasmon scatter can be used for long-range immunosensing and macromolecular conformation studies.

A variety of sensors, metallic nanostructured probes, metallic nanoshells and halfshells, nanoarrays for SERS sensing have been developed at the Oak Ridge National Laboratory. The SERS technology can detect the chemical agents and biological species (e.g. spores, biomarkers of pathogenic agents) directly. A DNA-based technique based on surface-enhanced Raman gene (SERGen) probes can be also used to detect gene targets via hybridization to DNA sequences complementary to these probes. Advanced instrumental systems designed for spectral measurements and for multiarray imaging as well as for field monitoring (RAMiTS technology) have been constructed. Plasmonics and SERS nanoprobes are useful for biological sensing.

Optical mRNA Biosensors

mRNA quantification is important in molecular diagnostics. Traditional spectrophotometric method cannot distinguish DNA, rRNA and tRNA species from mRNA. Scheme of an optical mRNA biosensor for examination of pathological samples is shown in Fig. 4.3.

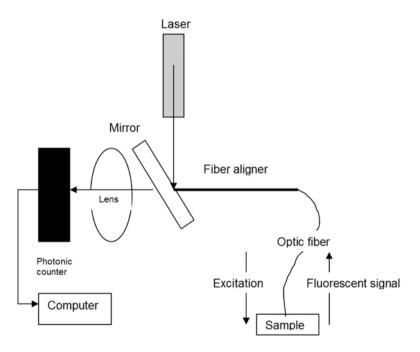


Fig. 4.3 Scheme of an optical mRNA biosensor. Sequence specific molecular beacons are used as molecular switches. This biosensor detects single molecules in fluids and can be used to search for molecular biomarkers to predict the prognosis of disease

Surface Enhanced Microoptical Fluidic Systems

The aim of the Surface Enhanced Microoptical Fluidic Systems (SEMOFS) European project is to develop a new concept for biosensors: a polymer-based card type integrated "Plasmon enhanced SPR"-sensor. The card will combine biologically active surfaces with integrated optics (light source, detection) and biocompatible multi-channel micro-fluidics. The project aims to achieve a significant breakthrough, since all functions will be totally integrated on a single polymer-based chip. The final product shall be manufactured with large scale, mass production techniques. The card will therefore be extremely low cost and disposable while providing increased sensitivity and diagnosis possibilities. The project will focus on:

- Increasing detection sensitivity and access to new information of the biological sample.
- Microfluidics on polymer substrate enabling multi-channeling (further enhancing sensitivity by parallel analysis) and integrated fluid actuators.
- Integrated optical detection concept based on Organic Light Emmitting Display (OLED)/waveguide/miniaturized spectrometer enabling card type integrated solution and multi-channeling.
- Hybrid micro-machining to ensure compatibility of the mastering and replication protocols with constraints of industrial scale manufacturing.
- Validation of expected applications and evaluation in clinical cancer diagnosis.

Nanoparticle-Enhanced Sensitivity of Fluorescence-Based Biosensors

Sensitivity required for high-performance bioassays can be achieved using fluorescence-based techniques for biosensors. There is still a need for enhancement strategies, which can reduce limit of detection and increase sensitivity for the detection of low analyte concentrations in small sample volumes. Possible solutions include the use of SPR effect associated with metal nanostructures, each of which contains a high concentration of dye molecules (McDonagh et al. 2009). The degree of enhancement achieved is dependent on the nanoparticle, dye label and nanoparticle deposition technique. For optimum assay enhancement, the antibody label must be located outside the quenching range and within the optimum distance from the metal nanoparticle. Nanoparticles with high brightness, low toxicity, biocompatibility and ease of biomolecule conjugation are selected. For enhancement of bioassays, the nanoparticle is conjugated to the antibody, replacing the single dye label.

Nanowire Biosensors

Since their surface properties are easily modified, nanowires can be decorated with virtually any potential chemical or biological molecular recognition unit, making the wires themselves independent of the analyte. The nanomaterials transduce the chemical binding event on their surface into a change in conductance of the nanowire in an extremely sensitive, real time and quantitative fashion. Boron-doped silicon nanowires (SiNWs) have been used to create highly sensitive, real-time electrically based sensors for biological and chemical species. Biotin-modified SiNWs were used to detect streptavidin down to at least a picomolar concentration range. The small size and capability of these semiconductor nanowires for sensitive, label-free, real-time detection of a wide range of chemical and biological species could be exploited in array-based screening and in vivo diagnostics.

A novel approach to synthesizing nanowires (NWs) allows their direct integration with microelectronic systems for the first time, as well as their ability to act as highly sensitive biomolecule detectors that could revolutionize biological diagnostic applications. An interdisciplinary team of engineers in Yale University's Institute for Nanoscience and Quantum Engineering has overcome hurdles in NW synthesis by using a tried-and-true process of wet-etch lithography on commercially available silicon-on-insulator wafers. These NWs are structurally stable and demonstrate an unprecedented sensitivity as sensors for detection of antibodies and other biologically important molecules. According to researchers, not only can the NWs detect extremely minute concentrations (as few as 1000 individual molecules in a cubic millimeter), they can do it without the hazard or inconvenience of any added fluorescent or radioactive detection probes. The study demonstrated ability of the NWs to monitor antibody binding, and to sense real-time live cellular immune response using T lymphocyte activation as a model. Within ~ 10 s, the NW could register T cell activation as the release acid to the device. The basis for the sensors is the detection of hydrogen ions or acidity, within the physiological range of reactions in the body. Traditional assays for detection of immune system cells such as T cells or for antibodies usually take hours to complete.

SiNW field effect transistors (SiNW-FETs) are promising biosensors for highly sensitive, selective, real-time and label-free measurements. Strategies for improving sensitivity include (Shen et al. 2014):

- · Reducing non-specific binding
- Alignment of the probes
- · Enhancing signals by charge reporter
- Sensing in the sub-threshold range

When biological molecules bind to their receptors on the nanowire, they usually alter the current moving through the sensor and signal the presence of substance of interest. This direct detection dispenses with the time-consuming labeling chemistry and speeds up the detection process considerably. Nanowire biosensors are used for the detection of proteins, viruses or DNA in a highly sensitive manner. They can be devised to test for a complex of proteins associated with cancer and used for diagnosis as well as monitoring the progress of treatment.

Nanowire Biosensors for Detection of Cancer Biomarkers

Nanowires can electronically detect a few proteins molecules along with other biomarkers that are early signs of cancer. Nanowire sensors are in development at California Institute of Technology (Pasadena, CA) for very early diagnosis of cancer, when there are just a few thousand cells. Nanowires in a set are coated with different compounds, each of which binds to a specific biomarker, and changes the conductivity of the nanowire that can be measured. Thousands of such nanowires are combined on a single chip that enables identification of the type of cancer. Currently such a chip can detect between 20 and 30 biomarkers and is being used for the early diagnosis of brain cancer.

MicroRNAs (miRNAs) are promising biomarkers for the diagnosis and prognosis of early-stage cancer A complementary metal oxide semiconductor (CMOS)-compatible SiNW-FET biosensor nanosensor shows a rapid (<1 min) detection of miR-21 and miR-205, with ultrahigh sensitivity as well as an excellent discrimination for single-nucleotide mismatched sequences of tumor-associated miRNAs (Lu et al. 2014).

Nanowire Biosensors for Detection of Single Viruses

Rapid, selective, and sensitive detection of viruses is crucial for implementing an effective response to viral infection, such as through medication or quarantine. Established methods for viral analysis include plaque assays, immunological assays, transmission electron microscopy, and PCR-based testing of viral nucleic acids. These methods have not achieved rapid detection at a single virus level and often require a relatively high level of sample manipulation that is inconvenient for infectious materials.

Direct, real-time electrical detection of single virus particles with high selectivity has been achieved by using nanowire field effect transistors. Measurements made with nanowire arrays modified with antibodies for influenza A showed discrete conductance changes characteristic of binding and unbinding in the presence of influenza A but not paramyxovirus or adenovirus. Simultaneous electrical and optical measurements using fluorescently labeled influenza A were used to demonstrate conclusively that the conductance changes correspond to binding/unbinding of single viruses at the surface of nanowire devices. pH-dependent studies further show that the detection mechanism is caused by a field effect, and that the nanowire devices can be used to determine rapidly isoelectric points and variations in receptor-virus binding kinetics for different conditions. Larger arrays of reproducible nanowire devices might simultaneously screen for the presence of 100 or more different viruses. Finally, studies of nanowire devices modified with antibodies specific for either influenza or adenovirus show that multiple viruses can be selectively detected in parallel. The possibility of large-scale integration of these nanowire devices suggests potential for simultaneous detection of several distinct viral threats at the single virus level.

Nanowires for Detection of Genetic Disorders

The surfaces of the silicon nanowire devices have been modified with peptide nucleic acid (PNA) receptors designed to recognize wild type versus the F508 mutation site in the cystic fibrosis transmembrane receptor gene. Conductance measurements made while sequentially introducing wild type or mutant DNA samples exhibit a time-dependent conductance increase consistent with the PNA-DNA hybridization and enable identification of fully complementary versus mismatched DNA samples. Concentration-dependent measurements show that detection can be carried out to at least the tens of femtomolar range. It provides more rapid results than current methods of DNA detection. This nanowire-based approach represents a step forward for direct, label-free DNA detection with extreme sensitivity and good selectivity, and could provide a pathway to integrated, high-throughput, multiplexed DNA detection for genetic screening.

Nanowires Biosensor for Detecting Biowarfare Agents

A multi-striped biosensing nanowires system can be used for detecting biowarfare agents in the field. Such biosensors are constructed from submicrometer layers of different metals including gold, silver and nickel that act as "barcodes" for detecting a variety of pathogens ranging from anthrax, smallpox and ricin to botulinum. Antibodies of specific pathogens can be attached to the nanowires producing a small, reliable, sensitive detection system. The system could also be used during an outbreak of an infectious disease.

Concluding Remarks and Prospects of Nanowire Biosensors

Nanowire biosensors modified with specific surface receptors represent a powerful nanotechnology-enabled diagnostic/detection platform for medicine and the life sciences. Key features of these devices include direct, label-free and real-time electrical signal transduction, ultra-high sensitivity, exquisite selectivity and potential for integration of addressable arrays on a massive scale, which sets them apart from other sensor technologies that are currently available. Nanowire biosensors have unique capabilities for multiplexed real-time detection of proteins, single viruses, DNA, enzymatic processes and small organic molecule-binding to proteins. Apart from their value as research tools, they have a significant impact on disease diagnosis, genetic screening and drug discovery. They will facilitate the development of personalized medicine. Because these nanowire sensors transduce chemical/ biological-binding events into electronic/digital signals, they have the potential for a sophisticated interface between nanoelectronic and biological information processing systems in the future.

Future Issues in the Development of Nanobiosensors

New biosensors and biosensor arrays are being developed using new materials, nanomaterials and microfabricated materials including new methods of patterning. Biosensor components will use nanofabrication technologies. Use of nanotubes, Buckminster fullerenes (buckyballs), silica and its derivatives can produce nanosized devices. Some of the challenges will be:

- Development of real-time non-invasive technologies that can be applied to detection and quantitation of biological fluids without the need for multiple calibrations using clinical samples.
- Development of biosensors utilizing new technologies which offer improved sensitivity for detection with high specificity at single molecular level.
- Development of biosensor arrays that can successfully detect, quantify and quickly identify individual components of mixed gases and liquid in an industrial environment.

It would be desirable to develop multiple integrated biosensor systems that utilize doped oxides, polymers, enzymes or other components to give the system the required specificity. A system with all the biosensor components, software, plumbing, reagents and sample processing is an example of an integrated biosensor. There is also a need for reliable fluid handling systems for "dirty" fluids and for relatively small quantities of fluids (nanoliter to attoliter quantities). These should be low cost, disposable, reliable and easy to use as part of an integrated sensor system. Sensing in picoliter to attoliter volumes might create new problems in development of microreactors for sensing and novel phenomenon in very small channels.

Applications of Nanodiagnostics

Applications of nanotechnologies in clinical diagnostics have been expanding. Although some of these were mentioned along with individual technologies in the preceding section, other important applications will be identified here. Applications for diagnosis in special areas such as cancer are described in chapters dealing with these therapeutic areas.

Nanotechnology for Detection of Biomarkers

A biomarker is a characteristic that can be objectively measured and evaluated as an indicator of a physiological as well as a pathological process or pharmacological response to a therapeutic intervention. Classical biomarkers are measurable alterations

in blood pressure, blood lactate levels following exercise and blood glucose in diabetes mellitus. Any specific molecular alteration of a cell on DNA, RNA, metabolite or protein level can be referred to as a molecular biomarker. From a practical point of view, the biomarker would specifically and sensitively reflect a disease state and could be used for diagnosis as well as for disease monitoring during and following therapy (Jain 2010). Currently available molecular diagnostic technologies have been used to detect biomarkers of various diseases such as cancer, metabolic disorders, infections and diseases of the central nervous system. Nanotechnology has further refined the detection of biomarkers. Some biomarkers also form the basis of innovative molecular diagnostic tests.

The physicochemical characteristics and high surface areas of nanoparticles make them ideal candidates for developing biomarker harvesting platforms. Given the variety of nanoparticle technologies that are available, it is feasible to tailor nanoparticle surfaces to selectively bind a subset of biomarkers and sequestering them for later study using high sensitivity proteomic tests. Biomarker harvesting is an underutilized application of nanoparticle technology and is likely undergo substantial growth. Functional polymer-coated nanoparticles can be used for quick detection of biomarkers and DNA separation.

A magnetic nanosensor technology that is up to 1000 times more sensitive than any technology now in clinical use, is accurate regardless of which bodily fluid is being analyzed and can detect biomarker proteins over a range of concentrations three times broader than any existing method (Gaster et al. 2009). The nanosensor chip also can search for up to 64 different proteins simultaneously and has been shown to be effective in early detection of tumors in mice, suggesting that it may open the door to significantly earlier detection of even the most elusive cancers in humans. The magnetic nanosensor can successfully detect malignant tumors in mice when levels of cancer-associated proteins are still well below concentrations detectable using the current standard method, ELISA. The sensor also can be used to detect biomarkers of diseases other than cancer.

Nanotechnology for Genotyping of Single-Nucleotide Polymorphisms

Nanoparticles for Detecting SNPs

There are two types of DNA-nanoparticles aggregation assays: one of the methods relies on cross-linking of the gold nanoparticle by hybridization and the other is a non-crosslinking system. The crosslinking system has been used not only to detect target DNA sequences, but also to detect metal ions or small molecules, which are recognized by DNAzymes. The non-crosslinking approach shows high performance in the detection of SNPs. These methods do not need special equipment and open a new possibility of POC diagnoses.

The primer extension (PEXT) reaction is the most widely used approach to genotyping of SNPs. Current methods for analysis of PEXT reaction products are based on electrophoresis, fluorescence resonance energy transfer, fluorescence polarization, pyrosequencing, mass spectrometry, microarrays, and spectrally encoded microspheres. A dry-reagent dipstick method can be used for rapid visual detection of PEXT products without instrumentation. The genomic region that spans each SNP of interest is amplified by PCR. Two primer extension reactions are performed with allele-specific primers (for one or the other variant nucleotide), which contain an oligo(dA) segment at the 5'-end. Biotin-dUTP is incorporated in the extended strand. The product is applied to the strip followed by immersion in the appropriate buffer. As the DNA moves along the strip by capillary action, it hybridizes with oligo(dT)-functionalized gold nanoparticles, such that only extended products are captured by immobilized streptavidin at the test zone, generating a red line. A second red line is formed at the control zone of the strip by hybridization of the nanoparticles with immobilized oligo(dA). The dipstick test is complete within 10 min. The described PEXT-dipstick assay is rapid and highly accurate; it shows 100% concordance with direct DNA sequencing data. It does not require specialized instrumentation or highly trained technical personnel. It is appropriate for a diagnostic laboratory where a few selected SNP markers are examined per patient with a low cost per assay.

Nanopores for Detecting SNPs

Use of nanopore technology for sequencing was described earlier in this chapter. The focus in this section is the application for detection of SNPs. There is a voltage threshold for permeation through a synthetic nanopore of dsDNA bound to a restriction enzyme that depends on the sequence. Molecular dynamic simulations reveal that the threshold is associated with a nano-newton force required to rupture the DNA-protein complex. A single mutation in the recognition site for the restriction enzyme, i.e., a SNP, can easily be detected as a change in the threshold voltage. Consequently, by measuring the threshold voltage in a synthetic nanopore, it may be possible to discriminate between 2 variants of the same gene (alleles) that differ in 1 base.

Nanobiotechnologies for Single Molecule Detection

Various nanobiotechnologies for single molecule detection are shown in Table 4.2. Some of these have been described in preceding sections.

The smallest RNA virus MS2 with a mass of 6 ag has been detection d from the resonance frequency shift of a whispering gallery mode-nanoshell hybrid resonator (WGM-h) upon adsorption on the nanoshell. Detection of single thyroid cancer

Table 4.2	Nanobiotechnologies	s for single molecule detection	n
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Visualization of biomolecules by near nanoscale microscopy		
Atomic force microscope		
Scanning probe microscope		
3D single-molecular imaging by nanotechnology		
Near-field scanning optical microscope		
Spectrally resolved fluorescence lifetime imaging microscopy		
Nanolaser spectroscopy for detection of cancer in single cells		
Nanoproteomics		
Study of protein expression at single molecule level		
Detection of a single molecule of protein		
Erenna TM Bioassay System: digital single molecule detection platform		
Nanofluidic/nanoarray devices: detection of a single molecule of DNA		
Carbon nanotube transistors for genetic screening		
Nanopore technology		
Portable nanocantilever system for diagnosis		
Nanobiosensors		
QD-FRET nanosensors for single molecule detection		

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marker (Thyroglobulin, Tg) and bovine serum albumin (BSA) proteins with masses of only 1 ag and 0.11 ag (66 kDa), respectively has now been reported (Dantham et al. 2013). However, the wavelength shifts are enhanced beyond those anticipated in the earlier work by 240% for Tg and 1500% for BSA. This surprising sensitivity is traced to a short-range reactive field near the surface of Au nanoshell receptor due to intrinsic random bumps of protein size, leading to an unanticipated increase in sensitivity to single protein, which grows larger as the protein diminishes in size. As a result of the largest signal-to-noise ratio in BSA experiments, a new protein limit of detection has been conservatively estimated for WGM-h of 5 kDa.

Protease-Activated QD Probes

QDs have been programmed to glow in presence of enzyme activity and give off NIR light only when activated by specific proteases. Altered expression of certain proteases is a common hallmark of cancer, atherosclerosis, and many other diseases. NIR light also passes harmlessly through skin, muscle and cartilage, so the new probes could detect tumors and other diseases at sites deep in the body without the need for a biopsy or invasive surgery. The probe's design makes use of a technique called "quenching" that involves tethering a gold nanoparticle to the QD to inhibit luminescence. The tether, a peptide sequence measuring only a few nanometers, holds the gold close enough to prevent the QD from giving off its light. The peptide tether used is one that is cleaved by the enzyme collagenase. The luminescence of the QDs is cut by more than 70% when they are attached to the gold particles. They remain dark until the nanostructures were exposed to collagenase after which the luminescence steadily returns. The aim of the research is to pair a series of QDs, each with a unique NIR optical signature, to an index of linker proteases. This probe would be important for understanding and monitoring the efficacy of therapeutic interventions, including the growing class of drugs that act as protease inhibitors. An important feature of the protease imaging probes described in this study is the combination of the contrast enhancement achievable through a probe that can be activated and is combined with the brightness, photostability, and tunability of QDs.

Labeling of MSCs with QDs

QDs are useful for concurrently monitoring several intercellular and intracellular interactions in live normal cells and cancer cells over periods ranging from less than a second to over several days (several divisions of cells). QDs offer an alternative to organic dyes and fluorescent proteins to label and track cells in vitro and in vivo. These nanoparticles are resistant to chemical and metabolic degradation, demonstrating long term photostability. Fluorescent QDs have been used to label MSC effectively, are easy to use, and show a high yield as well as survival rate with minimal cytotoxic effects. Dose-dependent effects, however, suggest limiting MSC QD exposure.

The peptide CGGGRGD has been immobilized on CdSe-ZnS QDs coated with carboxyl groups by cross linking with amine groups. These conjugates are directed by the peptide to bind with selected integrins on the membrane of hMSCs. Upon overnight incubation with optimal concentration, QDs effectively labeled all the cells. Long-term labeling of bone marrow-derived hMSCs with RGD-conjugated QDs was demonstrated during self-replication and differentiation into osteogenic cell lineages. Labeling of hMSCs with QDs has been carried out during self-replication, and multilineage differentiations into osteogenic, chondrogenic, and adipogenic cells. QD-labeled hMSCs remained viable as unlabeled hMSCs from the same subpopulation suggesting the use of bioconjugated QDs as an effective probe for long-term labeling of stem cells.

Nanotechnology for Point-of-Care Diagnostics

Point-of-care (POC) or near patient testing means that diagnosis is performed in the doctor's office or at the bed side in case of hospitalized patients or in the field for several other indications including screening of populations for genetic disorders and cancer. POC involves analytical patient testing activities provided within the healthcare system, but performed outside the physical facilities of the clinical laboratories. POC does not require permanent dedicated space but includes kits and instruments, which are either hand carried or transported to the vicinity of the patient for immediate testing at that site. The patients may even conduct the tests.

An example of POC test is CD4 T-cell count as guide to treatment of HIV/ AIDS. The number of circulating CD4 T-cells drops significantly when patients are infected with HIV/AIDS. CD4 counts assist in the decisions on when to initiate and when to stop the treatment, which makes this test so important at POC. While such testing is routine in Western countries and used repeatedly over the course of treatment to see if interventions are effective it is unavailable to many people in the developing world, especially in rural areas. A cheap test for CD4+ T lymphocytes in the blood is in development using biosensor nanovesicles to enhance the signal.

After the laboratory and the emergency room, the most important application of molecular diagnostics is estimated to be at the POC. Nanotechnology would be another means of integrating diagnostics with therapeutics. Nanotechnology-based diagnostics provides the means to monitor drugs administered by nanoparticle carriers. Some devices based on nanotechnology are among those with potential applications in POC testing.

Nanotechnology-Based Biochips for POC Diagnosis

The use of metal nanoparticles as labels represents a promising approach. They exhibit a high stability in signal and new detection schemes that would allow for robustness and low-cost readout in biochips. First examples of this kind have been established and are in the market, and more are in the development pipeline. Nanosphere Inc's VerigeneTM platform will be suitable for development of POC testing.

Carbon Nanotube Transistors for Genetic Screening

Carbon nanotube network field-effect transistors (NTNFETs) function as selective detectors of DNA immobilization and hybridization. NTNFETs with immobilized synthetic oligonucleotides can specifically recognize target DNA sequences, including a SNP in the HFE gene that is responsible for hereditary hemochromatosis, a disease in which too much iron accumulates in body tissues. The electronic responses of NTNFETs upon single-stranded DNA immobilization and subsequent DNA hybridization events have been confirmed by using fluorescence-labeled oligonucleotides and then further explored for label-free DNA detection at picomolar to micromolar concentrations. A strong effect of DNA counterions on the electronic response has been observed, suggesting a charge-based mechanism of DNA detection using NTNFET devices. Implementation of label-free electronic detection assays using NTNFETs constitutes an important step toward low-cost, low-complexity, highly sensitive and accurate molecular diagnostics. Label-free electronic detection of DNA has several advantages over state-of-the-art optical techniques, including cost, time, and simplicity. The sensitivity of the new device is good enough to detect a single-base mutation in an amount of DNA present in one milliliter of blood. This technology can bring to market hand-held, POC devices for genetic screening, as opposed to laboratory methods using labor-intense labeling and sophisticated optical equipment. This device will be commercially developed by Nanomix Inc.

POC Monitoring of Vital Signs with Nanobiosensors

Researchers at the University of Arkansas (Fayetteville, AR) have worked with pentacene, a hydrocarbon molecule, and carbon nanotubes (CNTs) to develop the two types of nanobiosensors for vital signs: a temperature sensor and a strain sensor for respiration. The two similar but slightly different biosensors are integrated into "smart" fabrics - garments with wireless technology and will be able to monitor a patient's respiration rate and body temperature in real time. The addition of CNTs with pentacene increases biosensor sensitivity. As an organic semiconductor, pentacene is efficient and easy to control. Both biosensors were fabricated directly on flexible polymeric substrates. The strain sensor, which would monitor respiration rate, consisted of a Wheatstone bridge, an instrument that measures unknown electrical resistance, and a thin pentacene film that acted as a sensing layer. The system would work when a physiological strain, such as breathing, creates a mechanical deformation of the sensor, which then affects the electrical current's resistance. For the temperature sensor, the researchers used a thin-film transistor that helped them to observe electrical current in linear response to temperature change. Most importantly, in low voltage areas, the current displayed the highest sensitivity to temperature changes. This device is useful for patients whose vital signs must be continuously monitored on bedside either at home or in hospital. The sensors and wireless networks can fit on garments such as undershirts. With this technology, the smart fabric can monitor vital signs and collect and send data to an information center in real time. The information can enable immediate detection of physiological abnormalities, which will allow physicians to begin treatment or prevent illness before full-blown disease manifestation.

Shri Lakshmi Nano Technologies Ltd. is collaborating with the University of Arkansas to optimize utilization of upcoming nanotechnologies to invent, design and manufacture advanced conductive fabric incorporating a biosensor that will allow the monitoring of body temperature, blood pressure, ECG, heartbeat rate and other vital health signs.

Nanodiagnostics for the Battle Field and Biodefense

One of the areas of interest at the MIT's Institute for Soldier Nanotechnologies (http://isnweb.mit.edu/) concerns ultrasensitive nanoengineered chemical detectors. Researcher have taken a major step towards making an existing miniature lab-on-a-chip fully portable, so the tiny device can perform hundreds of chemical experiments in any setting including the battlefield. This will make testing soldiers to see if they have been exposed to biological or chemical weapons much faster and easier. Neither of the previous approaches, such as mechanically forcing fluid through microchannels or capillary electro-osmosis, offer portability. Within the lab-on-a-chip, biological fluids such as blood are pumped through channels about 10 microns wide. Each channel has its own pumps, which direct the fluids to certain areas of the chip so they can be tested for the presence of specific molecules. In the new system, known as a 3D AC electro-osmotic pump, tiny electrodes with raised steps generate

opposing slip velocities at different heights, which combine to push the fluid in one direction, like a conveyor belt. Simulations predict a dramatic improvement in flow rate, by almost a factor of twenty, so that fast (mm/s) flows, comparable to pressuredriven systems, can be attained with battery voltages. If exposure to chemical or biological weapons is suspected, the device can automatically and rapidly test a miniscule blood sample, rather than sending a large sample to a laboratory and waiting for the results. The chips are so small and cheap to make that they could be designed to be disposable, or they could be made implantable. Another project focuses on research to develop different approaches to sensing and characterization of materials, including toxins, with identifiable chemical signatures. Each project exploits manipulation of nanoscale features of materials to achieve one or more of specificity, spatial resolution, convenience of use, reduced power demand, or multi-functionality.

NANOANTENNA Project of European Commission

NANOANTENNA (Development of a high sensitive and specific nanobiosensor based on surface enhanced vibrational spectroscopy dedicated to the in vitro proteins detection and disease diagnosis) project under FP7 program of European Commission stated in 2009 (http://cordis.europa.eu/project/rcn/92196 en.html). The main goal of project is to develop a novel optical nanobiosensor based on extraordinary vibrational signal enhancement of the proteins to be detected. To reach vibrational signal enhancement, the optical properties of specially designed metallic nanoparticles will be exploited, which should act as nanoantenna and the associated field enhancement to obtain a direct detection of proteins bound to the nanoparticle. Thus, this sensor will reach high sensitivity provided by the recently established large enhancement of vibration signals due to the resonant excitation of the nanoantenna device used as substrates. The aim is to detect only a few proteins with concentration much lower than 1pM and finally to reach detection threshold such as femtomole or lower. High molecular selectivity will be reached with the functionalization of the nanoantenna. Such functionalization will selectively favor the immobilization of the protein to be detected at the vicinity of the nanoparticle surface, providing the best enhancement and then the detection of the targeted protein. The nanobiosensor will include two main components: the nanoantenna device which corresponds to the sensor transducer and the functionalization which corresponds to its bioreceptor. Each functionalized nanoantenna device used as vibrational signal enhanced system is an individual and specific nanosensor of proteins. Therefore, this nanobiosensor integrated in a vibrational spectroscope will enable the detection and the analysis of the enhanced vibrational signal from the targeted proteins corresponding to the diagnosis instrument. Our nanobiosensor will be validated on the detection of proteins on body fluids. These proteins have been chosen because they were identified as specific biomarkers of common pathologies. This validation will improve their detection (better sensitivity, decrease of the detection threshold) and open the way to the early diagnosis.

Nanodiagnostics for Integrating Diagnostics with Therapeutics

Molecular diagnostics is an important component of personalized medicine. Improvement of diagnostics by nanotechnology has a positive impact on personalized medicine. Nanotechnology has potential advantages in applications in POC diagnosis: on patient's bedside, self-diagnostics for use in the home and integration of diagnostics with therapeutics. These will facilitate the development of personalized medicines.

Concluding Remarks about Nanodiagnostics

It is now obvious that direct analysis of DNA and protein could dramatically improve speed, accuracy, and sensitivity over conventional molecular diagnostic methods. Since DNA, RNA, protein and their functional subcellular scaffolds and compartments, are in the nanometer scale, the potential of single molecule analysis approach would not be fully realized without the help of nanobiotechnology. Advances in nanotechnology are providing nanofabricated devices that are small, sensitive and inexpensive enough to facilitate direct observation, manipulation and analysis of single biological molecule from single cell. This opens new opportunities and provides powerful tools in the fields such as genomics, proteomics, molecular diagnostics and high throughput screening. A review of articles published over the past 10 years investigating the use of QDs, gold nanoparticles, cantilevers, and other nanotechnologies concluded that nanodiagnostics promise increased sensitivity, multiplexing capabilities, and reduced cost for many diagnostic applications as well as intracellular imaging. Further work is needed to fully optimize these diagnostic nanotechnologies for clinical laboratory setting and to address the issues of potential health and environmental risks related to ODs.

Various nanodiagnostics that have been reviewed will improve the sensitivity and extend the present limits of molecular diagnostics. Numerous nanodevices and nanosystems for sequencing single molecules of DNA are feasible. It seems quite likely that there will be numerous applications of inorganic nanostructures in biology and medicine as biomarkers. Given the inherent nanoscale of receptors, pores, and other functional components of living cells, the detailed monitoring and analysis of these components will be made possible by the development of a new class of nanoscale probes. Biological tests measuring the presence or activity of selected substances become quicker, more sensitive and more flexible when certain nanoscale particles are put to work as tags or labels. Nanoparticles are the most versatile material for developing diagnostics.

Nanomaterials can be assembled into massively parallel arrays at much higher densities than is achievable with current sensor array platforms and in a format compatible with current microfluidic systems. Currently, quantum dot technology is the most widely employed nanotechnology for diagnostic developments. Among the recently emerging technologies, cantilevers are the most promising. This technology complements and extends current DNA and protein microarray methods, because nanomechanical detection requires no labels, optical excitation, or external probes and is rapid, highly specific, sensitive, and portable. This will have applications in genomic analysis, proteomics and molecular diagnostics. Nanosensors are promising for detection of bioterrorism agents that are not detectable with current molecular diagnostic technologies and some have already been developed.

Clinical Trials of Nanodiagnostics

Several nanodiagnostics are approved for clinical use. Other diagnostics, particularly nanobiotechnology-based imaging, are in clinical trials as listed in Table 4.3.

	le 4.5 Chinear trais of hand		
Product/procedure	Indication/aim	Sponsor	Status
Ferumoxytol (iron oxide NP) administered IV + MRI heart	Visualization of area of heart muscle damage after myocardial infarction (Alam et al. 2012)	University of Edinburgh, Scotland	Open, placebo- controlled
USPION MRI using Feraheme (an approved agent)	Pre-operative detection of small lymph node metastases in pancreatic cancer	Massachusetts General Hospital, Boston	Phase IV research study
Ferumoxytol: a NP agent to enhance contrast in MRI	For imaging lymph node metastases in esophageal cancer	OHSU Knight Cancer Institute, Portland, OR	Phase I
Rapid blood assay: cyanine dyes linked to Fe/Fe ₃ O ₄ NPs via protease- selective cleavage sequence and fluorescence sensor	For detection of pancreatic cancer biomarkers in blood	University of Kansas	Phase I completed
NA-NOSE (Nanoscale artificial nose) breath test	Testing recurrence of cancer after surgery for NSCLC	Fox Chase Cancer Center/NCI	Open, single center
NA-NOSE study: nanoparticle breath testing for biomarkers of cancer such as volatile organic compounds	Detection of breast and colon cancer. To be confirmed by biopsy	Rambam Health Care Campus, Israel	Open study recruiting patients
NA-NOSE: breath samples analyzed by chemical nanosensors based on gold NPs and carbon nanotubes	Discrimination between malignant and benign gastric lesions	Anhui Medical University, China	Study completed

Table 4.3	Clinical	trials of	nanodiagnostics
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Abbreviations: NP nanoparticle, USPION ultrasmall superparamagnetic iron oxide nanoparticle

Future of Nanodiagnostics

Within the next decade, measurement devices based on nanotechnology, which can make thousands of measurements very rapidly and very inexpensively, will become available. The most common clinical diagnostic application will be blood protein analysis. Blood in systemic circulation reflects the state of health or disease of most organs. Therefore, detection of blood molecular fingerprints will provide a sensitive assessment of health and disease. Another important area of application will be cancer diagnostics. Molecular diagnosis of cancer including genetic profiling would be widely used by the year 2025. Nanobiotechnology would play an important part, not only in cancer diagnosis but also in linking diagnosis with treatment.

In the future, nanodiagnostics would reduce the waiting time for the test results. For example, the patients with sexually transmitted diseases could give the urine sample when they first arrive at the outpatient clinic or physician's practice; the results could then be ready by the time they go in to see the doctor. They could then be given the prescription immediately, reducing the length of time worrying for the patient and making the whole process cheaper.

Future trends in diagnostics will continue in miniaturization of biochip technology to nano range. The trend will be to build the diagnostic devices from bottom up starting with the smallest building blocks. Whether interest and application of nanomechanical detection will hold in the long range remains to be seen. Another trend is to move away from fluorescent labeling as miniaturization reduces the signal intensity but there have been some improvements making fluorescent viable with nanoparticles.

Molecular electronics and nanoscale chemical sensors will enable the construction microscopic sensors capable of detecting patterns of chemicals in a fluid. Information from several such devices flowing passively in the bloodstream allows estimates of the properties of tiny chemical sources in a macroscopic tissue volume. Such devices should be cable to discriminate a single cell-sized chemical source from the background chemical concentration in vivo, providing high-resolution sensing in both time and space. With currently used methods for blood analysis, such a chemical source would be difficult to distinguish from background when diluted throughout the blood volume and withdrawn as a blood sample.

References

- M AK, Jung S, Ji T. Protein biosensors based on polymer nanowires, carbon nanotubes and zinc oxide nanorods. Sensors (Basel). 2011;11:5087–111.
- Alam SR, Shah AS, Richards J, et al. Ultrasmall superparamagnetic particles of iron oxide in patients with acute myocardial infarction: early clinical experience. Circ Cardiovasc Imaging. 2012;5:559–65.
- Almutairi A, Rossin R, Shokeen M, et al. Biodegradable dendritic positron-emitting nanoprobes for the noninvasive imaging of angiogenesis. Proc Natl Acad Sci U S A. 2009;106:685–90.
- Avci O, Ünlü NL, Özkumur AY, Ünlü MS. Interferometric reflectance imaging sensor (IRIS) a platform technology for multiplexed diagnostics and digital detection. Sensors (Basel). 2015;15:17649–65.

- Breitenstein M, Holzel R, Bier FF. Immobilization of different biomolecules by atomic force microscopy. J Nanobiotechnol. 2010;8:10.
- Butler TZ, Pavlenok M, Derrington IM, et al. Single-molecule DNA detection with an engineered MspA protein nanopore. Proc Natl Acad Sci U S A. 2008;105:20647–52.
- Byers RJ, Hitchman ER. Quantum dots brighten biological imaging. Prog Histochem Cytochem. 2011;45:201–37.
- Carbonaro A, Mohanty SK, Huang H, et al. Cell characterization using a protein-functionalized pore. Lab Chip. 2008;8:1478–85.
- Castaneda RT, Khurana A, Khan R, Daldrup-Link HE. Labeling stem cells with ferumoxytol, an FDA-approved iron oxide nanoparticle. J Vis Exp. 2011;57:e3482.
- Chen J, Abell J, Huang YW, Zhao Y. On-chip ultra-thin layer chromatography and surface enhanced raman spectroscopy. Lab Chip. 2012;12:3096–102.
- Corstjens PL, de Dood CJ, van der Ploeg-van Schip JJ, et al. Lateral flow assay for simultaneous detection of cellular- and humoral immune responses. Clin Biochem. 2011;44:1241–6.
- Cunningham BT. Photonic crystal surfaces as a general purpose platform for label-free and fluorescent assays. JALA Charlottesv Va. 2010;15:120–35.
- Dantham VR, Holler S, Barbre C, et al. Label-free detection of single protein using a nanoplasmonicphotonic hybrid microcavity. Nano Lett. 2013;13:3347–51.
- Debbage P, Jaschke W. Molecular imaging with nanoparticles: giant roles for dwarf actors. J Histochem Cell Biol. 2008;130:845–75.
- Delogu LG, Gemma L, Vidili G, et al. Functionalized multiwalled carbon nanotubes as ultrasound contrast agents. Proc Natl Acad Sci U S A. 2012;109:16612–7.
- Deng H, Xu Y, Liu Y, et al. Gold nanoparticles with asymmetric polymerase chain reaction for colorimetric detection of DNA sequence. Anal Chem. 2012;84:1253–8.
- Di Bucchianico S, Poma AM, Giardi MF, et al. Atomic force microscope nanolithography on chromosomes to generate single-cell genetic probes. J Nanobiotechnol. 2011;9:27.
- Du X, An H, Jin B, et al. Carbon nanotubes altering specificity of repeated PCR and DNA integrity properties. J Nanosci Nanotechnol. 2014;14:5547–51.
- Edwards KA, Wang Y, Baeumner AJ. Aptamer sandwich assays: human α-thrombin detection using liposome enhancement. Anal Bioanal Chem. 2010;398:2645–54.
- Esfandyarpour R, Yang L, Koochak Z, et al. Nanoelectronic three-dimensional (3D) nanotip sensing array for real-time, sensitive, label-free sequence specific detection of nucleic acids. Biomed Microdevices. 2016;18(1):7.
- Feng S, dos Santos MC, Carvalho BR, et al. Ultrasensitive molecular sensor using N-doped graphene through enhanced Raman scattering. Sci Adv. 2016;2(7):e1600322.
- Gaglia JL, Guimaraes AR, Harisinghani M, et al. Noninvasive imaging of pancreatic islet inflammation in type 1A diabetes patients. J Clin Invest. 2011;121:442–5.
- Gao N, Gao T, Yang X, et al. Specific detection of biomolecules in physiological solutions using graphene transistor biosensors. Proc Natl Acad Sci U S A. 2016;113:14633–8.
- Gaster RS, Hall DA, Nielsen CH, et al. Matrix-insensitive protein assays push the limits of biosensors in medicine. Nat Med. 2009;15:1327–32.
- Ghoroghchian PP, Therien MJ, Hammer DA. In vivo fluorescence imaging: a personal perspective. Wiley Interdiscip Rev Nanomed Nanobiotechnol. 2009;1:156–67.
- Golub E, Pelossof G, Freeman R, et al. Electrochemical, photoelectrochemical, and surface plasmon resonance detection of cocaine using supramolecular aptamer complexes and metallic or semiconductor nanoparticles. Anal Chem. 2009;81:9291–8.
- Goluch ED, Stoeva SI, Lee JS, et al. A microfluidic detection system based upon a surface immobilized biobarcode assay. Biosens Bioelectron. 2009;24:2397–403.
- Guzman R, Uchida N, Bliss TM, et al. Long-term monitoring of transplanted human neural stem cells in developmental and pathological contexts with MRI. Proc Natl Acad Sci U S A. 2007;104:10211–6.
- Han JH, Kim HJ, Sudheendra L, et al. Electrophoretic build-up of multi nanoparticle array for a highly sensitive immunoassay. Biosens Bioelectron. 2013;41:302–8.

- Haun JB, Yoon TJ, Lee H, Weissleder R. Magnetic nanoparticle biosensors. WIREs Nanomed Nanobiotechnol. 2010;2:291–304.
- He J, Evers DL, O'Leary TJ, Mason JT. Immunoliposome-PCR: a generic ultrasensitive quantitative antigen detection system. J Nanobiotechnol. 2012;10:26.
- Heath JR. Nanotechnologies for biomedical science and translational medicine. Proc Natl Acad Sci U S A. 2015;112:14436–43.
- Heller DA, Jin H, Martinez BM, et al. Multimodal optical sensing and analyte specificity using single-walled carbon nanotubes. Nat Nanotechnol. 2009;4:114–20.
- Jain KK. Nanodiagnostics: application of nanotechnology in molecular diagnostics. Expert Rev Mol Diagn. 2003;4:153–61.
- Jain KK. Applications of nanobiotechnology in clinical diagnostics. Clin Chem. 2007;53:2002-9.
- Jain KK. Handbook of biomarkers. New York: Springer; 2010.
- Jain KK. Molecular diagnostics: technologies, markets and companies. Basel: Jain PharmaBiotech Publications; 2017a.
- Jain KK. Biochips & Microarrays. Technologies, markets and companies. Basel: Jain PharmaBiotech Publications; 2017b.
- Jasmin, Torres AL, Nunes HM, et al. Optimized labeling of bone marrow mesenchymal cells with superparamagnetic iron oxide nanoparticles and in vivo visualization by magnetic resonance imaging. J Nanobiotechnology. 2011;9:4.
- Jo K, Dhingra DM, Odijk T, et al. A single-molecule barcoding system using nanoslits for DNA analysis. Proc Natl Acad Sci U S A. 2007;104:2673–8.
- John R, Rezaeipoor R, Adie SG, et al. In vivo magnetomotive optical molecular imaging using targeted magnetic nanoprobes. Proc Natl Acad Sci U S A. 2010;107:8085–90.
- Kaittanis C, Naser SA, Perez JM. One-step, nanoparticle-mediated bacterial detection with magnetic relaxation. Nano Lett. 2007;7:380–3.
- Kong J, Zhu J, Keyser UF. Single molecule based SNP detection using designed DNA carriers and solid-state nanopores. Chem Commun. 2017;53:436–9.
- Kosaka N, Mitsunaga M, Bhattacharyya S, et al. Self-illuminating in vivo lymphatic imaging using a bioluminescence resonance energy transfer quantum dot nano-particle. Contrast Media Mol Imaging. 2011;6:55–9.
- Kose AR, Koser H. Ferrofluid mediated nanocytometry. Lab Chip. 2012;12:190-6.
- Krishnamurthy V, Monfared SM, Cornell B. Ion-channel biosensors—part I: construction, operation, and clinical studies. IEEE Transactions Nanotechnol. 2010;9:303–12.
- le Masne de Chermont Q, Chaneac C, Seguin J, et al. Nanoprobes with near-infrared persistent luminescence for in vivo imaging. Proc Natl Acad Sci U S A. 2007;104:9266–71.
- Lee YE, Kopelman R. Nanoparticle PEBBLE sensors in live cells. Methods Enzymol. 2012;504:419–70.
- Loh OY, Ho AM, Rim JE, et al. Electric field-induced direct delivery of proteins by a nanofountain probe. Proc Natl Acad Sci U S A. 2008;105:16438–43.
- Lu N, Gao A, Dai P, et al. CMOS-compatible silicon nanowire field-effect transistors for ultrasensitive and label-free microRNAs sensing. Small. 2014;10:2022–8.
- Malashikhina N, Pavlov V. DNA-decorated nanoparticles as nanosensors for rapid detection of ascorbic acid. Biosens Bioelectron. 2012;33:241–6.
- McDonagh C, Stranik O, Nooney R, Maccraith BD. Nanoparticle strategies for enhancing the sensitivity of fluorescence-based biochips. Nanomedicine. 2009;4:645–56.
- Na HB, Lee JH, An K, et al. Development of a T1 contrast agent for magnetic resonance imaging using MnO nanoparticles. Angew Chem Int Ed Engl. 2007;46:5397–401.
- Nam JM, Stoeva SI, Mirkin CA. Bio-bar-code-based DNA detection with PCR-like sensitivity. J Am Chem Soc. 2004;126:5932–3.
- Nune SK, Gunda P, Thallapally PK, et al. Nanoparticles for biomedical imaging. Expert Opin Drug Deliv. 2009;6:1175–94.
- Partlow KC, Chen J, Brant JA, et al. 19F magnetic resonance imaging for stem/progenitor cell tracking with multiple unique perfluorocarbon nanobeacons. FASEB J. 2007;21:1647–54.

- Qu Q, Zhu Z, Wang Y, et al. Rapid and quantitative detection of Brucella by up-converting phosphor technology-based lateral-flow assay. J Microbiol Methods. 2009;79:121–3.
- Ravizzini G, Turkbey B, Barrett T, et al. Nanoparticles in sentinel lymph node mapping. WIREs Nanomed Nanobiotechnol. 2009;1:610–23.
- Shen MY, Li BR, Li YK. Silicon nanowire field-effect-transistor based biosensors: from sensitive to ultra-sensitive. Biosens Bioelectron. 2014;60:101–11.
- Shilo M, Reuveni T, Motiei M, Popovtzer R. Nanoparticles as computed tomography contrast agents: current status and future perspectives. Nanomedicine. 2012;7:257–69.
- Swanson SD, Kukowska-Latallo JF, Patri AK, et al. Targeted gadolinium-loaded dendrimer nanoparticles for tumor-specific magnetic resonance contrast enhancement. Int J Nanomedicine. 2008;3:201–10.
- Tisch U, Schlesinger I, Ionescu R, et al. Detection of Alzheimer's and Parkinson's disease from exhaled breath using nanomaterial-based sensors. Nanomedicine. 2013;8:43–56.
- Verellen N, Sonnefraud Y, Sobhani H, et al. Fano resonances in individual coherent plasmonic nanocavities. Nano Lett. 2009;9:1663–7.
- Vo-Dinh T, Zhang Y. Single-cell monitoring using fiberoptic nanosensors. Wiley Interdiscip Rev Nanomed Nanobiotechnol. 2011;3:79–85.
- Wang X, Hofmann O, Das R, et al. Integrated thin-film polymer/fullerene photodetectors for on-chip microfluidic chemiluminescence detection. Lab Chip. 2007;7:58–63.
- Wang X, Lou X, Wang Y, et al. QDs-DNA nanosensor for the detection of hepatitis B virus DNA and the single-base mutants. Biosens Bioelectron. 2010a;25:1934–40.
- Williams RM, Nayeem S, Dolash BD, Sooter LJ. The effect of DNA-dispersed single-walled carbon nanotubes on the polymerase chain reaction. PLoS One. 2014;9(4):e94117.
- Xing Y, Chaudry Q, Shen C, et al. Bioconjugated quantum dots for multiplexed and quantitative immunohistochemistry. Nat Protoc. 2007;2:1152–65.
- Yang B, Zhou G, Huang LL. PCR-free MDR1 polymorphism identification by gold nanoparticle probes. Anal Bioanal Chem. 2010;397:1937–45.
- Ymeti A, Greve J, Lambeck PV, et al. Fast, ultrasensitive virus detection using a young interferometer sensor. Nano Lett. 2007;7:394–7.
- Yu JS, Lim MC, Huynh DT, et al. Identifying the location of a single protein along the DNA strand using solid-state nanopores. ACS Nano. 2015;9:5289–98.
- Yun J, Sonabend AM, Ulasov IV, et al. A novel adenoviral vector labeled with superparamagnetic iron oxide nanoparticles for real-time tracking of viral delivery. J Clin Neurosci. 2012;19:875–80.

Chapter 5 Nanopharmaceuticals

Introduction

The term "nanopharmaceuticals", an important part of nanomedicine, covers discovery/ development and delivery of drugs using nanobiotechnology as well as the use of nanoparticles as therapeutic agents. The post-genomic era is revolutionizing the drug discovery process. The new challenges in the identification of therapeutic targets require efficient and cost-effective tools. Label-free detection systems use proteins or ligands coupled to materials the physical properties of which are measurably modified following specific interactions. Among the label-free systems currently available, the use of metal nanoparticles offers enhanced throughput and flexibility for real-time monitoring of biomolecular recognition at a reasonable cost. This chapter will deal with use of nanobiotechnologies for drug discovery and development, an important part of nanobiopharmaceuticals. Some technologies will accelerate target identification whereas others will evolve into therapeutics. Application of nanobiotechnology is essential for optimal delivery of some drug. Use of nanoparticles as anticancer agents, antimicrobials and neuroprotectives will be dealt with in chapters dealing with these therapeutic areas.

Nanobiotechnology for Drug Discovery

Current drug discovery process needs improvement in several areas. Although many targets are being discovered through genomics and proteomics, the efficiency of screening and validation processes need to be increased. Through further miniaturization, nanotechnology will improve the ability to fabricate massive arrays in small spaces using microfluidics and the time efficiency. This would enable direct reading of the signals from microfluidic circuits in a manner like a microelectronics circuit where one does not require massive instrumentation. This would increase the ability to do high-throughput drug screening. QDs and other nanoparticles (gold colloids,

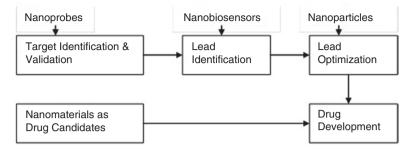


Fig. 5.1 Application of nanobiotechnology at various stages of drug discovery ($\mbox{${\odot}$}$ Jain PharmaBiotech)

magnetic nanoparticles, nanobarcodes, nanobodies, dendrimers, fullerenes and nanoshells) have received a considerable attention because of their unique properties that are useful for drug discovery (Jain 2005). Application of nanobiotechnologies to various stages of drug discovery is shown schematically in Fig. 5.1 and basic nanotechnologies applicable to drug discovery are listed in Table 5.1.

Nanofluidic Devices for Drug Discovery

Development of nanofluidic devices with dimensions in the range of 1–100 nm provide opportunities for probing single molecules as fluids can no longer be considered as continua but rather as ensembles of individual molecules. Diffusion becomes an efficient mass transport mechanism on nanoscale and these characteristics can be exploited to develop new analytical platforms for drug discovery and development.

As described in the preceding chapters, a nanopore can act as a single-molecule sensor to explore discrete molecular phenomena, while operating at extremely high analytical throughput. Most of nanopore-based studies involve the use of a protein channel that spontaneously inserts itself into a lipid membrane. A limitation of it is that it is not possible to control the pore diameter or to use it over a wide range of pH, salt concentration, temperature and mechanical stress. An alternative to protein nanopores is the use of solid-state nanopores, which can be tuned in size with nanometer precision and display improved mechanical, chemical and electrical stability. A novel approach for the optical detection of DNA translocation events through solid-state nanopores shows the potential for ultra-high-throughput and parallel analysis at the single-molecule level (Chansin et al. 2007). Individual subwavelength pore acts as a waveguide for fluorescence excitation with a metallic layer on the free-standing membrane acting as an optical barrier between the illumination region and the analyte reservoir. This configuration enables high-contrast imaging of single-molecule translocation events through multiple pores and with minimal background or noise (Hong et al. 2009).

Table 5.1 Basic nanobiotechnologies relevant to drug discovery		
Nanoparticles		
Gold nanoparticles		
Lipoparticles		
Magnetic nanoparticles		
Micelles		
Polymer nanoparticles		
Quantum dots		
Nanofibers		
Nanowires		
Carbon nanofibers		
Nanoconduits		
Nanotubes		
Nanopipettes		
Nanoneedles		
Nanochannels		
Nanopores		
Nanofluidics		
Nanobiotechnology applications in proteomics relevant to drug discovery		
Nanoflow liquid chromatography		
High-field asymmetric waveform ion mobility mass spectrometry		
Use of nanotube electronic biosensor in proteomics		
Fluorescence planar wave guide technology		
Miscellaneous nanobiotechnologies		
Visualization and manipulation at biological structures at nanoscale		
Surface plasmon resonance (SPR)		
Drug discovery through study of endocytosis on nanoscale		
Nanosubstances as drug candidates		
Dendrimers		
Fullerenes		
Nanobodies		
Nanodevices		
Nanobiosensors		
Nanowire devices		
Nanoarrays and nanobiochips		
Cantilevers		
Atomic force microscopy		
© Jain PharmaBiotech		

Table 5.1 Basic nanobiotechnologies relevant to	drug discovery
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Gold Nanoparticles for Drug Discovery

Tracking Drug Molecules in Cells

Gold nanoparticles have been used to demonstrate multiphoton absorption induced luminescence (MAIL), in which specific tissues or cells are fluorescently-labeled using special stains that enable them to be studied. Gold nanoparticles can emit light

so strongly that it is readily possible to observe a single nanoparticle at laser intensities lower than those commonly used for MAIL – sub-100 fs pulses of 790 nm light. Moreover, gold nanoparticles do not blink or burn out, even after hours of observation. These findings suggest that metal nanoparticles are a viable alternative to fluorophores or semiconductor nanoparticles for biological labeling and imaging. Other advantages of the technique are that the gold nanoparticles can be prepared easily, have very low toxicity, and can readily be attached to molecules of biological interest. In addition, the laser light used to visualize the particles is a wavelength that causes only minimal damage to most biological tissues. This technology could enable tracking of a single molecule of a drug in a cell or other biological samples.

SPR with Colloidal Gold Particles

Conventional SPR is applied in specialized biosensing instruments. These instruments use expensive sensor chips of limited reuse capacity and require complex chemistry for ligand or protein immobilization. SPR has also been successfully applied with colloidal gold particles in buffered solution, which offers many advantages over conventional SPR. The support is cheap, easily synthesized, and can be coated with various proteins or protein-ligand complexes by charge adsorption. With colloidal gold, the SPR phenomenon can be monitored in any UV-vis spectrophotometer. For high-throughput applications, the technology has been adapted in an automated clinical chemistry analyzer. Among the label-free systems currently available, the use of metal nanocolloids offers enhanced throughput and flexibility for real-time biomolecular recognition monitoring at a reasonable cost.

Use of QDs for Drug Discovery

The use of QDs for drug discovery has been explored extensively. Both advantages and drawbacks have been investigated.

Advantages of the Use of QDs for Drug Discovery

- Enhanced optical properties as compared with organic dyes. QDs offer great imaging results that could not be achieved by organic dyes as they have narrow band emission together with large UV absorption spectra, which enables multiplexed imaging under a single light source.
- Multiple leads can be tested on cell culture simultaneously. Similarly, the absorption of several drug molecules can be studied simultaneously for a longer period.
- Using the surface functionalization properties of QDs, targeting capabilities can be added as well.
- Due to the inorganic nature of QDs, their interaction with their immediate environment at in vivo states can be minimal compared with their organic counterparts.

QDs carrying a surface-immobilized antagonist remain with nanomolar affinity on the cell surface, and particles carrying an agonist are internalized upon receptor binding. The receptor functions like a logic "and-gate" that grants cell access only to those particles that carry a receptor ligand "and" where the ligand is an agonist (Hild et al. 2010). Agonist- and antagonist-modified nanoparticles bind to several receptor molecules at a time. This multiligand binding leads to five orders of magnitude increased-receptor affinities, compared with free ligand, in displacement studies. More than 800 G protein-coupled receptors in humans provide an opportunity that targeting of a plethora of cells is possible for drug discovery, and that switching from cell recognition to cell uptake is simply a matter of nanoparticle surface modification with the appropriate choice of ligand type.

Drawbacks of the Use of QDs for Drug Discovery

QDs have not been totally perfected and some of the drawbacks are:

- Size variation during the synthesis of single color QDs is 2–4%, which could create false results for applications such as capillary electrophoresis or gel electrophoresis. Therefore, QD synthesis techniques need to have improved quality control with respect to size distribution before they can be seriously utilized in drug discovery research.
- For ADME purposes, blue QDs (diameter of 3.7 nm) are the smallest class of the QD family but they are considerably larger than organic dyes. Hence, the use of QDs for this purpose might not be desirable in special cases.
- Similarly, the number of functional groups attached to an organic dye is usually one, or it can be controlled very precisely. However, in the case of QDs, the functional groups usually decorate the entire surface and thus cause multiple attachments of target molecules.
- The transport of a large volume (due to multiple attachments of drug molecules to a single QD) across the membrane will be more difficult than a single molecule itself.
- To satisfy all the available surface groups, larger numbers of target molecules are needed; this could affect the cost of the experiment. Although, several methods have been reported to reduce the number of surface groups around a single dot, each of these methods adds to the final size of the QDs, which might not be desired in many cases, especially in studies related to kinetics and transport of drug molecules.
- The 'blinking' characteristics of QDs when they are excited with high-intensity light could be a limiting factor for fast scan systems such as flow cytometry.
- Under combined aqueous-UV excitation conditions, QDs demonstrate oxidation and release of Cd ions into the environment. This is a definite concern for in vivo applications. As an alternative, capping the surface of a core dot with a large band-gap-semiconductor or proteins can eliminate or reduce the toxicity. But each additional step on the QDs will add to their final size and could even affect their final size distribution during these additional process steps.

QDs for Imaging Drug Receptors in the Brain

Cellular receptors are a critical target studied by scientists who develop new drug candidates for diseases including neurological disorders such as epilepsy and depression. More detailed understanding of the behavior of these receptors can open new treatment options. Older imaging tools such as fluorescent dyes or polymer spheres are either too unstable or too big to effectively perform single-molecule tracking. Single-molecule properties in living cells can be tracked by using OD conjugates, and produce photo resolutions up to eight times more detailed than the older imaging tools. OD conjugates are also an order of magnitude brighter than fluorescent dyes, and can be observed for as long as 40 min compared to about 5 s for the dyes. Individual receptors of glycine (GlyRs), the main inhibitory neurotransmitter in the human CNS, and their dynamics in the neuronal membrane of living cells can be studied for periods ranging from milliseconds to minutes using QDs. Entry of GlyRs into the synapse by diffusion has been observed and confirmed by electron microscopy imaging of QD-tagged receptors. Length of observation time is critical for studying cellular processes, which change rapidly over a span of several minutes.

G-protein–coupled receptors (GPCRs) are the largest protein superfamily in the human genome; they comprise 30% of current drug targets and regulate diverse cellular signaling responses. Role of endosomal trafficking in GPCR signaling regulation is significant but this process remains difficult to study due to the inability to distinguish among many individual receptors because of simultaneously trafficking within multiple endosomal pathways. Accurate measurement of the internalization and endosomal trafficking of single groups of serotonin (5-hydroxytryptamine, 5-HT) receptors was shown by using single QD probes and quantitative colocalization (Fichter et al. 2010). Presence of a QD tag does not interfere with 5-HT receptor internalization or endosomal recycling. Direct measurements show simultaneous trafficking of the 5-HT1A receptor in two distinct endosomal recycling pathways. Single-molecule imaging of endosomal trafficking will significantly impact the understanding of cellular signaling and provide powerful tools to elucidate the actions of GPCR-targeted therapeutics.

Lipoparticles for Drug Discovery

Lipoparticle technology (Integral Molecular Inc) enables integral membrane proteins to be solubilized while retaining their intact structural conformation. Retaining the native structural conformation of membrane-bound receptors is essential during assay development for optimal lead selection and optimization. Lipoparticles can be paired with a multitude of detection systems, permitting the optimal detection system to be used depending on the target protein, the goal of the assay, and the preference of customers. Biosensors are one class of detection system currently being used with Lipoparticles.

Biosensor for Drug Discovery with Lipoparticles

Interactions with integral membrane proteins have been particularly difficult to study because the receptors cannot be removed from the lipid membrane of a cell without disrupting the structure and function of the protein. Cell-based assays are the current standard for drug discovery against integral membrane proteins, but are limited in important ways. Biosensors can address many of these limitations. Biosensors are currently being used in target identification, validation, assay development, lead optimization, and ADMET () studies, but are best suited for soluble molecules. Integral is using Lipoparticles to effectively solubilize integral membrane proteins for use in biosensors and other microfluidic devices.

A primary application of current biosensor technologies is the optimization of limited-scope drug libraries against specific targets. Paired with Lipoparticle technology, biosensors can be used to address some of the most complex biological problems facing the drug discovery industry, including cell-cell recognition, cell-adhesion, cell-signaling, lipid interactions, and protein-protein interactions:

- · Where high throughput screening of random libraries does not work
- · Only weak ligands known, ultra-sensitivity required
- When high-content information is needed (affinity, kinetics)
- Structure-based rational drug design
- ADMET: drug binding to cytochromes, serum proteins, lipid solubility
- · Peptide-based ligand design where no ligand available

Lipoparticles provide a means for solubilizing integral membrane proteins that would lose their structure if extracted away from the lipid membrane. The methods for using lipoparticles range from traditional fluorescent detection technologies to emerging biosensor technologies. The optimal detection system can be used depending on the target protein, the goal of the assay, and the preference of customers.

Lipoparticles will be used for identification and optimization of chemical compounds and for antibody development. Lipoparticles will also be used to purify and concentrate structurally intact receptors from naturally occurring cell lines. This technology offers a "better-and-different" discovery platform for complex and difficult targets, but can also be adapted to "faster-and-cheaper" detection systems.

Magnetic Nanoparticles Assays

Several assays are used for screening drug targets. Magnetic nanoparticles are used in many biochemical assays as labels for concentration, manipulation and, more recently, detection. Typically, one attaches the magnetic particles to the biochemical species of interest (target) using a chemically specific binding interaction. Once bound, the labels enable the manipulation of the target species through the application of magnetic forces. Spintronic sensors, specifically Giant Magnetoresistive and Spin Dependent Tunneling, sensors have been developed to detect and quantify labels in two main formats: flowing in a microfluidic channel, and immobilized labels on a chip surface.

Analysis of Small Molecule-Protein Interactions by Nanowire Biosensors

Development of miniaturized devices that enable rapid and direct analysis of the specific binding of small molecules to proteins could be of substantial importance to the discovery of and screening for new drug molecules. A highly sensitive and label-free direct electrical detection of Small-molecule inhibitors of ATP binding to Abl can be detected by using silicon nanowire field-effect transistor devices. Abl, a protein tyrosine kinase, whose constitutive activity is responsible for chronic myelogenous leukemia, has been covalently linked to the surfaces of silicon nanowires within microfluidic channels to create active electrical devices. Concentration-dependent binding of ATP and concentration-dependent inhibition of ATP binding by the competitive smallmolecule antagonist Gleevec were assessed by monitoring the nanowire conductance. In addition, concentration-dependent inhibition of ATP binding was examined for four additional small molecules, including reported and previously unreported inhibitors. These studies demonstrate that the silicon nanowire devices can readily and rapidly distinguish the affinities of distinct small-molecule inhibitors and, thus, could serve as a technology platform for drug discovery.

Cells Targeting by Nanoparticles with Attached Small Molecules

Multivalent attachment of small molecules to nanoparticles can increase specific binding affinity and reveal new biological properties of such nanomaterial. Multivalent drug design has yielded antiviral and antiinflammatory agents several orders of magnitude more potent than monovalent agents. Parallel synthesis of a library, which is comprised of nanoparticles decorated with different synthetic small molecules has been achieved. Screening of this library against different cell lines led to discovery of a series of nanoparticles with high specificity for endothelial cells, activated human macrophages, and pancreatic cancer cells. This multivalent approach could facilitate development of functional nanomaterials for applications such as differentiating cell lines, detecting distinct cellular states and targeting specific cell types. It has potential applications in high throughput drug discovery, diagnostics and human therapeutics.

Role of AFM for Study of Biomolecular Interactions for Drug Discovery

An approach called TREC (topography and recognition imaging) uses any of several different ligands such as antibodies, small organic molecules, and nucleotides bound to a carefully designed AFM tip-sensor, which can estimate affinity and structural data. If a ligand is attached to the end of an AFM probe, one can simulate various physiological conditions and look at the strength of the interaction between

the ligand and receptor under a wide range of circumstances. By functionalizing the tip, one can use it to probe biological systems and identify certain chemical entities on the surface of a biological sample. This opens the door to more effective use of AFM in drug discovery.

AFM has been used to study the molecular-scale processes underlying the formation of the insoluble plaques associated with Alzheimer's disease (AD). As one of a class of neurological diseases caused by changes in a protein's physical state, called "conformational" diseases, it's particularly well suited for study with AFM. Extensive data suggest that the conversion of the A β peptide from soluble to insoluble forms is a key factor in the pathogenesis of Alzheimer's disease (AD). In recent years, AFM has provided useful insights into the physicochemical processes involving Aβ morphology. AFM was the key in identifying the nanostructures which are now recognized as different stages of A β aggregation in AD and has revealed other forms of aggregation, which are observable at earlier stages and evolve to associate into mature fibrils. AFM can now be used to explore factors that either inhibit or promote fibrillogenesis, e.g. AFM can be used to compare monoclonal antibodies being studied as potential treatments for AD to select the one that does a better job of inhibiting the formation of these protofibrils. AFM can be not only be reliably used to study the effect of different molecules on Aß aggregation, but it can also provide additional information such as the role of epitope specificity of antibodies as potential inhibitors of fibril formation.

Nanoscale Devices for Drug Discovery

Miniature devices are being used to study synthetic cell membranes to speed the discovery of new drugs for a variety of diseases, including cancer. Examples of these are "laboratories-on-a-chip" and Lab-on-Bead.

Laboratories-on-a-Chip

Microfluidic systems and nanoporous materials enable construction of miniature "laboratories-on-a-chip" that might contain up to a million test chambers, each capable of screening an individual drug. Such chips can be used to screen candidate compounds to find drugs to overcome anticancer drug resistance by deactivating the pumps in cell membranes that remove chemotherapy drugs from tumor cells, making the treatment less effective. The chips could dramatically increase the number of experiments that are possible with a small amount of protein.

Lab-on-Bead

A nanotechnology-based method for selecting peptide nucleic acid (PNA) encoded molecules with specific functional properties from combinatorially generated libraries consists of 3 essential stages: (1) creation of a Lab-on-Bead library, a one-bead,

one-sequence library that, in turn, displays a library of candidate molecules; (2) fluorescence microscopy-aided identification of single target-bound beads and the extraction – wet or dry – of these beads and their attached candidate molecules by a micropipette manipulator; and (3) identification of the target-binding candidate molecules via amplification and sequencing (Gassman et al. 2010). This novel integration of techniques harnesses the sensitivity of DNA detection methods and the multiplexed and miniaturized nature of molecule screening to efficiently select and identify target-binding molecules from large nucleic acid encoded chemical libraries and has the potential to accelerate assays currently used for the discovery of new drug candidates by screening millions of chemicals simultaneously using nanosized plastic beads. One batch of nanoscopic beads can replace the work of thousands of conventional, repetitive laboratory tests. This process that could be up to 10,000 times faster than current methods. By working at nanoscale, it will be possible to screen more than a billion possible drug candidates per day as compared to the current limit of hundreds of thousands per day.

Nanotechnology for Drug Design at Cellular Level

To create drugs capable of targeting some of the most devastating human diseases, one must first decode exactly how a cell or a group of cells communicates with other cells and reacts to a broad spectrum of complex biomolecules surrounding it. But even the most sophisticated tools currently used for studying cell communications suffer from significant deficiencies and typically can only detect a narrowly selected group of small molecules or, for a more sophisticated analysis, the cells must be destroyed for sample preparation. A nanoscale probe, the scanning mass spectrometry (SMS) probe, can capture both the biochemical make-up and topography of complex biological objects. SMS exploits an approach to electrospray ionization that enables continuous sampling from a highly localized picoliter volume in a liquid environment, softly ionizes molecules in the sample to render them amenable for mass spectrometric analysis, and sends the ions to the mass spectrometer (Kottke et al. 2010). The SMS probe can help map all those complex and intricate cellular communication pathways by probing cell activities in the natural cellular environment, which might lead to better disease diagnosis and drug design on the cellular level.

Role of Nanobiotechnology in the Future of Drug Discovery

None of the nanoparticles available is ideal for all requirements of drug discovery. The choice may depend on the needs. QDs can be used for high-throughput cell-based studies with the advantage of multiplexing (i.e. multiple leads can be tested at the same time). However, as discussed earlier there are some limitations yet to be resolved for their use in the drug discovery studies, namely, toxicity, size variation, agglomeration, potential multiple drug attachment to a single QD and blinking.

An increasing use of nanobiotechnology by the pharmaceutical and biotechnology industries is anticipated. Nanotechnology will be applied at all stages of drug development – from formulations for optimal delivery to diagnostic applications in clinical trials. In future, it may be possible to fully model an individual cell's structure and function by computers connected to nanobiotechnology systems. Such a detailed virtual representation of how a cell functions might enable scientists to develop novel drugs with unprecedented speed and precision without any experiments in living animals. In another promising area of application non-biodegradable 3D scaffolds are being developed to hold stem cells for pharmaceutical and biological research. These tissue constructs can be used to test new drugs. Since tissues grow in three dimensions and not two, 3D would be more suitable for early drug screening.

Nanobiotechnology-Based Drug Development

Dendrimers as Drugs

Dendrimers are a novel class of 3D nanoscale, core-shell structures that can be precisely synthesized for a wide range of applications. Specialized chemistry techniques allow for precise control over the physical and chemical properties of the dendrimers. They are most useful in drug delivery but can also be used for the development of new pharmaceuticals with novel activities. Polyvalent dendrimers interact simultaneously with multiple drug targets. They can be developed into novel targeted cancer therapeutics. Polymer-protein and polymer-drug conjugates can be developed as anticancer drugs. These have the following advantages:

- · Tailor-made surface chemistry
- Non-immunogenic
- Inherent body distribution enabling appropriate tissue targeting.
- Possibly biodegradable

Dendrimer conjugation with low molecular weight drugs has been of increasing interest recently for improving pharmacokinetics, targeting drugs to specific sites, and facilitating cellular uptake. Opportunities for increasing the performance of relatively large therapeutic proteins such as streptokinase (SK) using dendrimers have been explored. Using the active ester method, a series of streptokinase-poly(amido amine) (PAMAM) G3.5 conjugates can be synthesized with varying amounts of dendrimer-to-protein molar ratios. All SK conjugates display significantly improved stability in phosphate buffer solution, compared to free SK. The high coupling reaction efficiencies and the resulting high enzymatic activity retention achieved can enable a desirable way for modifying many bioactive macromolecules with dendrimers.

Glycodendrimers are carbohydrate functionalized dendrimers for use in therapeutics, antigen presentation and as biologically active compounds. GlycoSyn, a joint venture between Starpharma Holdings and Industrial Research Ltd., will provide manufacturing and specialized expertise in carbohydrate design, synthesis and analysis. One of the first projects in the pipeline involves research undertaking cGMP manufacture of intermediates used in the production of Starpharma's vaginal microbicide – VivaGeIT, a polyvalent dendrimer-based pharmaceutical being developed to prevent the spread of HIV/AIDS, and potentially other sexually transmitted infections including genital herpes.

Fullerenes as Drug Candidates

A key attribute of the fullerene molecules is their numerous points of attachment, allowing for precise grafting of active chemical groups in three-dimensional orientations. This attribute, the hallmark of rational drug design, allows for positional control in matching fullerene compounds to biological targets. In concert with other attributes, namely the size of the fullerene molecules, their redox potential and its relative inertness in biological systems, it is possible to tailor requisite pharmacokinetic characteristics to fullerene-based compounds and optimize their therapeutic effect.

Fullerene antioxidants bind and inactivate multiple circulating intracellular free radicals, giving them unusual power to stop free radical injury and to halt the progression of diseases caused by excess free radical production. Fullerenes provide effective defense against all principal damaging forms of reactive oxygen species. C-60 fullerene has 30 conjugated carbon-carbon double bonds, all of which can react with a radical species. In addition, the capture of radicals by fullerenes is too fast to measure and is referred to as "diffusion controlled", meaning the fullerene forms a bond with a radical every time it encounters one. Numerous studies demonstrate that fullerene antioxidants work significantly better as therapeutic antioxidants than other natural and synthetic antioxidants, at least for CNS degenerative diseases. In oxidative injury or disease, Fullerene antioxidants can enter cells and modulate free radical levels, thereby substantially reducing or preventing permanent cell injury and cell death. Mechanisms of action of fullerene are:

- Fullerenes can capture multiple electrons derived from oxygen free radicals in unoccupied orbitals.
- When an attacking radical forms a bond with fullerene creating a stable and relatively nonreactive fullerene radical.
- A tris-malonic acid derivative of the fullerene C60 molecule (C3) is capable of removing the biologically important superoxide radical.
- C3 localizes to mitochondria, suggest that C3 functionally replaces manganese superoxide dismutase (SOD), acting as a biologically effective SOD mimetic.

Fullerenes have potential applications in the treatment of diseases where oxidative stress plays a role in the pathogenesis. These include the following:

- Degenerative diseases of the central nervous system including Parkinson's disease, Alzheimer's disease, and amyotrophic lateral sclerosis
- · Multiple sclerosis

- · Ischemic cardiovascular diseases
- Atherosclerosis
- · Major long-term complications of diabetes
- · Sun-induced skin damage and physical manifestations of aging

The first-generation antioxidant fullerenes are based on the C3 compound, produced by the precise grafting of three malonic acid groups to the C-60 fullerene surface. C3 has shown significant activity against a spectrum of neurodegenerative disorders in animal models. These animal models replicate many of the features of important human neurodegenerative diseases, including amyotrophic lateral sclerosis and Parkinson's disease.

The second-generation antioxidant fullerenes are based on DF-1, the dendrofullerene, produced by attaching a highly water-soluble conjugate to the C-60 fullerene core. In preclinical testing, C-60 has shown DF-1 to be highly soluble, nontoxic, and able to retain a high level of antioxidant activity in both cultured cells and animals.

Several water-soluble C60 derivatives have been suggested for various medical applications. These applications include neuroprotective agents, HIV-1 protease inhibitors, bone-disorder drugs, transfection vectors, X-ray contrast agents, photo-dynamic therapy agents, and a C60–paclitaxel chemotherapeutic.

Another possible application of fullerenes is to be found in nuclear medicine, in which they could be used as an alternative to chelating compounds that prevent the direct binding of toxic metal ions to serum components. This could increase the therapeutic potency of radiation treatments and decrease their adverse effect profile, because fullerenes are resistant to biochemical degradation within the body.

Nanobodies

Nanobodies (Nbs), derived from naturally occurring single-chain antibodies, are the smallest fragments of naturally occurring heavy-chain antibodies that have evolved to be fully functional in the absence of a light chain. The Nanobody technology (Ablynx) was originally developed following the discovery that camelidae (camels and llamas) possess a unique repertoire of fully functional antibodies that lack light chains. Like conventional antibodies, Nbs show high target specificity and low inherent toxicity; however, like small molecule drugs they can inhibit enzymes and can access receptor clefts. Their unique structure consists of a single variable domain (VHH), a hinge region, and two constant domains (CH2 and CH3). The cloned and isolated VHH domain is a perfectly stable polypeptide harboring the full antigen-binding capacity of the original heavy chain. This newly discovered VHH domain is the basic component of Ablynx's Nanobodies. Ablynx's Nanobodies are naturally highly homologous to human antibodies. They can also be humanized to within 99% sequence homology of human VH domains. Ablynx's Nanobody platform can quickly deliver therapeutic leads for a wide range of targets. Advantages of Nbs are:

- They combine the advantages of conventional antibodies with important features of small molecule drugs.
- Nbs can address therapeutic targets not easily recognized by conventional antibodies such as active sites of enzymes.
- Nbs are very stable.
- They can be administered by means other than injection.
- They can be produced cost-effectively on a large scale.
- Nbs have an extremely low immunogenic potential. In animal studies, the administration of Nbs does not yield any detectable humoral or cellular immune response.

The cloning and selection of antigen-specific Nbs obviate the need for construction and screening of large libraries, and for lengthy and unpredictable in vitro affinity maturation steps. The unique and well-characterized properties enable nanobodies to excel conventional therapeutic antibodies in terms of recognizing uncommon or hidden epitopes, binding into cavities or active sites of protein targets, tailoring of halflife, drug format flexibility, low immunogenic potential and ease of manufacture. Moreover, the favorable biophysical and pharmacological properties of Nbs, together with the ease of formatting them into multifunctional protein therapeutics, leaves them ideally placed as a new generation of antibody-based therapeutics. Nbs are being explored as therapeutics in many fields of medicine, including oncology, inflammatory, infectious and neurological diseases (Steeland et al. 2016). As imaging agents, they have potential for use in the diagnosis and monitoring of diseases. Several Nbs are in clinical trials.

An example of use of Nbs as novel drugs is Nb-conjugated human trypanolytic factor for treatment of human African trypanosomiasis (HAT). Normal human serum (NHS) contains apolipoprotein L-I (apoL-I), which lyses African trypanosomes except resistant forms such as *Trypanosoma brucei rhodesiense*, which expresses the apoL-I–neutralizing serum resistance–associated (SRA) protein, endowing this parasite with the ability to infect humans and cause HAT. A truncated apoL-I (Tr-apoL-I) has been engineered by deleting its SRA-interacting domain, which makes it lytic for *T. b. rhodesiense*. Tr-apoL-I has been conjugated with a Nb that efficiently targets conserved cryptic epitopes of the variant surface glycoprotein of trypanosomes to generate a new type of immunotoxin with potential for trypanosomiasis therapy. Treatment with this engineered conjugate resulted in clear curative and alleviating effects on acute and chronic infections of mice with both NHS-resistant and NHS-sensitive trypanosomes. First-in-class' anti-thrombotic agent ALX-0081 (Ablynx NV) is in phase I trials (Van Bockstaele et al. 2009).

Companies Involved in Nanobodies

Several companies including major pharmaceutical companies are involved in the development of Nbs with several in collaboration with Ablynx. These companies along with their technologies or services or applications are listed in Table 5.2.

	Table 5.2 Companies involved in nanobodies		
Company	Technology/services/applications		
121 Bio	Develops approaches for enzymatic conjugation and Nb development with an aim to advance immunotherapy, patient selection, and management		
AbbVie	Has a global license agreement with Ablynx for development of ALX-0061 for RA and SLE		
Ablynx	First and leading company developing Nbs as therapeutics for cancer, inflammation, and immune diseases		
Boehringer Ingelheim	Has a global strategic alliance with Ablynx for the discovery, development and commercialization of up to 10 different Nb therapeutics		
Camel-IDS	Involved in the development, preclinical validation, and clinical translation of Nbs as molecular-imaging probes for cancer in the form of targeted radionuclides		
EddingPharm	License from Ablynx for the development and commercialization of ALX-0141 and ATN-103 for all indications including RA in China		
GenScript	Offers a comprehensive Nb service for research and therapeutic applications via selection and optimization of Nbs from immunized llamas of synthetic libraries		
Genzyme (Sanofi)	Has an exclusive research collaboration with Ablynx for the investigation and development of Nbs to treat multiple sclerosis		
Hydribody by Hybrigenics Services	Selects and validates antibodies derived from a fully synthetic humanized VHH antibody library; provides Nbs fused to the tag of choice		
Merck & Co (Merck Sharp & Dohme)	License agreements with Ablynx for the preclinical and clinical development and commercialization of 4 Nbs for immunooncology		
Merck KGaA	Collaborations with Ablynx to co-discover and codevelop Nbs against four targets in immunology (rheumatology) and oncology		
Novartis	Has a license agreement with Ablynx to discover and develop Nb-based therapeutics for disease targets that are difficult to address with conventional antibodies		
Novo Nordisk	Global exclusive collaboration and licensing agreement with Ablynx for the discovery and development of novel multi-specific Nb drug candidates		
QVQuality	Develops custom-made Nb-based imaging agents for imaging and research		
Taisho Pharmaceutical Co	License agreement with Ablynx for the development and commercialization of ozoralizumab in Japan		

 Table 5.2
 Companies involved in nanobodies

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Preclinical Studies of Nanoparticles in Animals and Humans

Nanoparticles are currently being investigated in in preclinical studies as well as human clinical trials (see Chap. 9). As information on how nanoparticles function in humans is difficult to obtain, animal studies that can be correlative to human behavior are needed to provide guidance for human clinical trials. Correlative studies have been reported on animals and humans for CRLX101, a 20- to 30-nm-diameter,

multifunctional, polymeric nanoparticle containing camptothecin (CPT), which is currently in phase II clinical trials (Eliasof et al. 2013). Pharmacokinetics of polymerconjugated CPT (indicative of the CRLX101 nanoparticles) in mice, rats, dogs, and humans reveal that the area under the curve (AUC) scales linearly with milligrams of CPT per square meter for all species. Plasma concentrations of unconjugated CPT released from CRLX101 in animals and humans are consistent with each other after accounting for differences in serum albumin binding of CPT. Urinary excretion of polymer-conjugated CPT occurs primarily within the initial 24 h after dosing in animals and humans. The urinary excretion dynamics of polymer-conjugated and unconjugated CPT appear similar between animals and humans. CRLX101 accumulates into solid tumors and releases CPT over a period of several days to give inhibition of its target in animal xenograft models of cancer and in the tumors of humans. The evidence provided from animal models on the CRLX101 mechanism of action suggests that the behavior of CRLX101 in animals is translatable to humans.

Manufacture of Nanomedicines

Although many scale up and manufacturing problems of a new nanomedicines are the same as those of any other new therapeutics, manufacturing of nanomedicines poses special issues. Perhaps the most common is the need for nanoscale characterization at all stages of discovery, development, and commercialization. In addition, nanomaterials that meet medical-grade requirements for purity and reproducibility can be difficult to obtain. It is not uncommon that expensive nanomedicines, produced under FDA's current cGMPs, fail to meet specifications or have poor reproducibility of efficacy. Safety applies not only to dosage and clinical results, but also to manufacturing and the need to avoid contamination. It covers toxicological aspects as well.

Role of Nanobiotechnology in Microbial Biofabrication

Combination of systems biotechnology and industrial microbiology has enabled adaptation of microbial cell factories from plain bioproduction of molecules of biotechnological and biomedical interest to the biofabrication of nanoparticles and sophisticated self-organizing constructs useful for nanomedicine whose structural and functional complexity demand a precise upstream design (Vázquez and Villaverde 2013). In addition, the screening of unconventional microbes in natural environments has expanded the catalog of nanostructured products that can be obtained by microbial synthesis. Both classical genetic engineering and more complex systems-level reprograming of microbial metabolic routes open an avenue for exploitation of microbial diversity and biosynthetic potential in biofabrication for nanomedicine, which could, in turn, result in cost-effective, fully scalable and versatile alternatives to chemical synthesis of pharmaceuticals.

Nanobiotechnology in Drug Delivery

Drug delivery is one of the important considerations in drug development and therapeutics. New technologies are applied for constructing innovative formulations and delivering them. The focus is on targeted drug delivery. This is important for delivery of biopharmaceuticals and treatment of diseases such as cancer and neurological disorders. In the pharmaceutical industry, there is potential to provide new formulations and routes of drug delivery. Among new technologies, nanobiotechnology has evoked considerable interest for application in the pharmaceutical industry. Applications of nanotechnology for drug delivery will be considered in this chapter.

Ideal Properties of Material for Drug Delivery

Properties of an ideal macromolecular drug delivery or biomedical vector are:

- Structural control over size and shape of drug or imaging-agent cargo-space.
- Biocompatible, nontoxic polymer/pendant functionality.
- Well-defined scaffolding and/or surface modifiable functionality for cell-specific targeting moieties.
- Lack of immunogenicity or ability to evade the immune system.
- Appropriate cellular adhesion, endocytosis and intracellular trafficking to allow therapeutic delivery or imaging in the cytoplasm or nucleus.
- Acceptable bioelimination or biodegradation.
- Targeted delivery with binding to the target sites and accumulation in the target tissue with sparing of normal or non-target tissues.
- Controlled or triggerable drug release.
- Molecular level isolation and protection of the drug against inactivation during transit to target cells.
- Minimal nonspecific cellular and blood-protein binding properties.
- Ease of consistent, reproducible, clinical grade synthesis.

Nanobiotechnology fulfills many of these requirements for improved drug delivery. Nanoparticles as well as nanodevices are used for this purpose.

Improved Absorption of Drugs in Nanoparticulate Form

Micronization was in use prior to introduction of techniques for producing nanoparticles. Although several claims were made for increased absorption, no significant improvement was documented because the microparticle size was still above 3 μ m (3000 nm) and nanoparticle size could be as much as 30 times less. Reduction of particle size from 5 μ m to 200 nm increases the surface area of the particle by a factor of 25 with increase in solubility. As an example, reduction of iron phosphate to the nanoscale increases its absorption in the body.

Interaction of Nanoparticles with Human Blood

Nanoparticle size and plasma binding profile contribute to a particle's longevity in the bloodstream, which can have important consequences for therapeutic efficacy. Approximate doubling in nanoparticle hydrodynamic size was observed upon in vitro incubation of 30–50 nm colloidal gold nanoparticles in human plasma due to binding of plasma proteins to their surface (Dobrovolskaia et al. 2009).

Nanoscale Devices Delivery of Therapeutics

There are several requirements for developing a device small enough to efficiently leave the vasculature and enter cells to perform multiple, smart tasks. However, the major requirement involves size. Vascular pores limit egress of therapeutics to materials less than ~50 nm in diameter, and cells will not internalize materials much greater than 100 nm. Therefore, the only currently available technology that fulfills these criteria consists of synthetic nanodevices. These are designed synthetic materials with structures less than 100 nm in size. Unlike fictional mechanical nanomachines, based on machines that have been "shrunken" to nanometer dimensions, several true nanomolecular structures have now been synthesized and applied to drug delivery, gene transfer, antimicrobial therapeutics, and immunodiagnostics.

Nanobiotechnology Solutions to the Problems of Drug Delivery

One of the major problems with drugs is solubility, which is an essential factor for drug effectiveness, independent of administration route. It is also a major challenge for pharmaceutical companies developing new pharmaceutical products since nearly half of new chemically-based drugs are insoluble, or poorly soluble, in water. Many, otherwise promising, compounds never reach the market. Others reach the market but in a sub-optimal formulation, possibly providing low or unpredictable bioavailability, or posing an increased side effect risk. Enhanced solubility technology can be used to reformulate such drugs and increase their commercial potential. Nanobiotechnology provides the following solutions to the problems of drug delivery:

- The particle size is reduced to nanometer size range to increase the surface area, thereby increasing the rate of dissolution, e.g. Nanoedge technology (Baxter).
- Improving solubilization of the drug.
- Using non-invasive routes of administration eliminates the need for administration of drugs by injection.
- Development of novel nanoparticle formulations with improved stabilities and shelf-lives.
- Development of nanoparticle formulations for improved absorption of insoluble compounds and macromolecules enable improved bioavailability and release

rates, potentially reducing the amount of dose required and increasing safety through reduced side effects.

- Manufacture of nanoparticle formulations with controlled particle sizes, morphology, and surface properties would be more effective and less expensive than other technologies.
- Nanoparticle formulations that can provide sustained-release profiles up to 24 h can improve patient compliance with drug regimens.
- Direct coupling of drugs to targeting ligand, restricts the coupling capacity to a
 few drug molecules but coupling of drug carrier nanosystems to ligands allows
 import of thousands of drug molecules by means of one receptor targeted ligand.
 Nanosystems offer opportunities to couple drugs with newly discovered diseasespecific targets.

Nanocomposites for Protein Delivery

Delivery of therapeutic proteins is often hampered by their inadequate physicochemical and biopharmaceutical properties, i.e. low stability and poor bioavailability. Considerable research effort has been focused on development of biocompatible polymers to produce appropriate formulations of proteins that enhance their therapeutic performance. Polymers have been exploited to obtain a variety of formulations including biodegradable microparticles, 3D hydrogels, bioconjugates and soluble nanocomposites (Salmaso and Caliceti 2013). Several soluble polymers, bearing charges or hydrophobic moieties along the macromolecular backbone, physically associate with proteins to form soluble nanocomplexes. Physical complexation is a better alternative to chemical bioconjugation. Soluble protein/polymer nanocomplexes formed by physical interactions increase protein stability, enhance bioavailability, promote absorption across the biological barriers, and prolong protein residence in the bloodstream. Furthermore, a few polymers have been found to favor the protein internalization into cells or boost their immunogenic potential by acting as immunoadjuvant in vaccination protocols.

Nanosuspension Formulations

Nanosuspension formulations can be used to improve delivery of poorly soluble drugs. Several new drug candidates emerging from drug discovery programs are water insoluble, and therefore poorly bioavailable, leading to abandoned development efforts. These can now be rescued by formulating them into crystalline nanosuspensions. Techniques such as media milling and high-pressure homogenization have been used commercially for producing nanosuspensions. The unique features of nanosuspensions have enabled their use in various dosage forms, including specialized delivery systems such as mucoadhesive hydrogels. Nanosuspensions can be delivered by parenteral, oral, ocular and pulmonary routes. Applications of several

drugs available as nanosuspensions are being extended for site-specific drug delivery. Advantages of nanosuspension are (Patel and Agrawal 2011):

- · Higher drug loading can be achieved
- Dose reduction is possible
- · Enhancement of physical and chemical stability of drugs
- Suitable for hydrophilic drugs

Baxter scientists have used Nanoedge technology to formulate the antifungal agent itraconazole as an intravenous nanosuspension. In studies on rats, formulation as a nanosuspension was shown to enhance efficacy of itraconazole relative to a solution formulation, because of altered pharmacokinetics, leading to increased tolerability, permitting higher dosing and resultant tissue drug levels.

A study has compared the in vitro and in vivo antitumor efficacy as well as dose dependent toxicity of camptothecin nanosuspension (Nano-CPT) with that of topotecan (TPT). Nano-CPT showed approximately 6 times in vitro cytotoxicity than TPT against cell lines MCF-7, and the same in vivo antitumor activity as TPT but with lower toxicity (Yao et al. 2012). The results indicate that Nano-CPT formulation has higher antitumor efficacy and lower toxicity than the conventional formulation of the drug. Compared to microoparticles, nanoparticles penetrate deeper with higher diffusional pressure and have a higher concentration gradient.

- Advantages of drug delivery by nanoparticle nanosuspension by various routes of administration are (Suri et al. 2016):
- Nanoparticles in suspension, by increasing the area of absorption under the curve, can markedly improve bioavailability of drugs that are poorly absorbed following oral administration.
- Nanosuspension formulations are suitable for parenteral routes of drug administration such as intravenous, interperitoneal and intra-articular.
- Nebulized nanosuspensions facilitate use of drugs by pulmonary route.
- Nanosuspensions are suitable for ocular drug delivery.
- Topical drug delivery

Nanotechnology-Based Refilling of Drug Delivery Depots Through Circulation

Local drug delivery depots are useful and there is a need for noninvasive technique to refill these systems once their payload is exhausted. Blood-borne drug payloads introduced into the blood circulation can be modified to home to and refill hydrogel drug delivery systems. Hydrogels have been modified with oligodeoxynucleotides (ODNs) that provide a target for drug payloads in the form of free alginate strands carrying complementary ODNs. Coupling ODNs to alginate strands has led to specific binding to complementary-ODN-carrying alginate gels in vitro and to injected gels in vivo. When coupled to a drug payload, sequence-targeted refilling of a delivery depot consisting of intratumor hydrogels was shown to completely abolish tumor growth (Brudno et al. 2014). These results suggest a new paradigm for nanotherapeutic drug delivery, and this concept is expected to have applications in refilling drug depots in cancer therapy, wound healing, and drug-eluting vascular grafts as well as stents.

Self-Assembled Nanostructures with Hydrogels for Drug Delivery

Drug delivery systems based on physical hydrogels with self-assembled nanostructures are attracting increasing attention as complements to chemically crosslinked hydrogels, because of advantages of reduced toxicity, convenience of in situ gel formation, stimuli-responsiveness, reversible sol-gel transition, and improved drug loading and delivery profiles. The driving forces of the self-assembly include hydrophobic interaction, hydrogen bonding, electrostatic interaction, and weak van der Waals forces. Stimuli-responsive properties of physical hydrogels include thermoand pH-sensitivity. Fabrication of self-assembled nanostructures in drug delivery hydrogels, via physical interactions between polymer–polymer and polymer–drug, requires accurately controlled macro- or small molecular architecture and a comprehensive knowledge of the physicochemical properties of the therapeutics (Tang et al. 2009). Nanostructures within hydrogels, which interact with payloads, provide useful means to stabilize the drug form and control its release kinetics. Biocompatibles UK Ltd., a subsidiary of BTG plc, is developing these systems.

Nanomaterials and Nanobiotechnologies Used for Drug Delivery

Table 5.3 shows various nanomaterials and nanobiotechnologies used for drug delivery.

Viruses as Nanomaterials for Drug Delivery

Specific targeting of tumor cells is an important goal for the design of nanotherapeutics for the treatment of cancer. Recently, viruses have been explored as nanocontainers for specific targeting applications, but these systems typically require modification of the virus surface using chemical or genetic means to achieve tumorspecific delivery. However, there is a subset of viruses with natural affinity for receptors on tumor cells that could be exploited for nanotechnology applications, e.g. the canine parvovirus for targeted drug delivery in cancer.

Structure	Size	Role in drug delivery
Bacteriophage NK97 (a virus that attacks bacteria)	~28 nm	Emptied of its own genetic material, NK97, which is covered by 72 interlocking protein rings, can act as a nanocontainer to carry drugs and chemicals to targeted locations.
Canine parvovirus (CPV)-like particles	~26 nm	Targeted drug delivery: CPV binds to transferrin receptors, which are over-expressed in some tumors
Carbon magnetic nanoparticles	40–50 nm	For drug delivery and targeted cell destruction
Ceramics nanoparticles	~35 nm	Accumulate exclusively in the tumor tissue and allow the drug to act as sensitizer for PDT without being released
Cerasomes	60–200 nm	Cerasome is filled with C6-ceramide for use as an anticancer agent
Dendrimers	1–20 nm	Holding therapeutic substances such as DNA in their cavities
Gold nanoparticles	2–4 nm	Enable externally controlled drug release
HTCC nanoparticles	110–180 nm	Encapsulation efficiency is up to 90%. In vitro release studies show a burst effect followed by a slow and continuous release
Micelle/Nanopill	25–200 nm	Made from two polymer molecules – one water- repellant and the other hydrophobic – that self- assemble into a sphere called a micelle that can deliver drugs to specific structures within the cell.
Low density lipoproteins	20–25 nm	Drugs solubilized in the lipid core or attached to the surface
Nanocochleates	~275 nm	Nanocochleates facilitate delivery of biologicals such as DNA and genes
Nanocrystals	<1000 nm	NanoCrystal technology (Elan) can rescue a significant number of poorly soluble chemical compounds by increasing solubility
Nanodiamonds	550–800 nm	Biocompatibility and unique surface properties for drug delivery
Nanoemulsions	20–25 nm	Drugs in oil and/or liquid phases to improve absorption
Nanoliposomes	25–50 nm	Incorporate fullerenes to deliver drugs that are not water-soluble and tend to have large molecules
Nanoparticle composites	~40 nm	Attached to guiding molecules such as MAbs for targeted drug delivery
Nanopore membrane		An implanted titanium device using silicone nanopore membrane can release encapsulated protein and peptide drugs
Nanospheres	50–500 nm	Hollow ceramic nanospheres created by ultrasound
Nanosponges	10 nm	A long, linear molecule scrunched into a sphere ~10 nm in ø with several surface sites for drug molecules attachment
Nanostructured organogels	~50 nm	Mixture of olive oil, liquid solvents and adding a simple enzyme to chemically activate a sugar. Used to encapsulate drugs

 Table 5.3
 Nanomaterials used for drug delivery

(continued)

Structure	Size	Role in drug delivery
Nanotubes	Single wall 1–2 nm Multiwall 20–60 nm	Resemble tiny drinking straws and that might offer advantages over spherical nanoparticles for some applications.
Nanovalve	~500 nm	Externally controlled release of drug into a cell
Nanovesicles	25-100 nm	Bilayer spheres containing the drugs in lipids
Polymer nanocapsules	50–200 nm	Enclosing drugs
PEG-coated PLA nanoparticles	Variable size	PEG coating improves the stability of PLA nanoparticles in the gastrointestinal fluids and helps the transport of encapsulated protein across the intestinal and nasal mucus membranes.
Quantum dots	2–10 nm	Combine imaging with therapeutics
Superparamagnetic iron oxide nanoparticles	10–100 nm	As drug carriers for intravenous injection to evade RES as well as to penetrate the very small capillaries within the body tissues and thus offer the most effective distribution in certain tissues

 Table 5.3 (continued)

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Abbreviations: *PEG* poly(ethylene glycol), *PLA* poly(lactic acid), *HTCC* N-(2-hydroxyl) propyl-3-trimethyl ammonium chitosan chloride, *RES* reticuloendothelial system

Bacteria-Mediated Delivery of Nanoparticles and Drugs into Cells

Nanoparticles and bacteria have been independently used to deliver genes and proteins into mammalian cells for monitoring or altering gene expression and protein production. Harmless strains of bacteria could be used as vehicles, harnessing bacteria's natural ability to penetrate cells and their nuclei. Researchers at Purdue University's Birck Nanotechnology Center have demonstrated the simultaneous use of nanoparticles and bacteria to deliver nucleic acid-based model drug molecules into cells in mice (Akin et al. 2007). In this approach, the gene or cargo is loaded onto the nanoparticles, ranging in size from 40 to 200 nm which are attached to the bacteria with linker molecules. The bacteria successfully deliver the molecules, and the genes are released from the nanoparticles and expressed in cells. When the cargo-carrying bacteria attach to the recipient cell they are engulfed by its outer membrane, forming "vesicles," or tiny spheres that are drawn into the cell's interior. Once inside the cell, the bacteria dissolve the vesicle membrane and release the cargo as shown in Fig. 5.2.

This technique may be used to deliver different types of cargo into a variety of cells and live animals for gene therapy without the need for complicated genetic manipulations. This delivery system also is more efficient than techniques using viruses as they usually incorporate only one copy of a gene cargo to virus particle. In this approach, bacteria can carry hundreds of nanoparticles, each of which can in

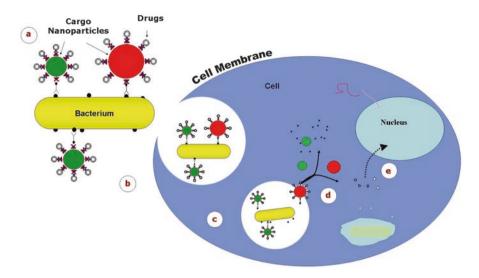


Fig. 5.2 Bacteria plus nanoparticles for drug delivery into cells. Delivery system begins with (a) cargo carrying bacteria that is (b) "swallowed" by the receiving cell. The bacterium then (c) dissolves the cell membrane and (d) releases its cargo which may also be (e) sent to the nucleus at will to make useful proteins or regulate genes (Source: Akin et al. 2007)

turn carry hundreds of drug molecules, depending on the size of the nanoparticles. Released cargo can be designed to be transported to different locations in the cells to carry out disease detection and treatment simultaneously. The method might be used to take images of diseased tissues by inserting a cargo of fluorescent molecules into tumors that are ordinarily too small to be detected. It could enable insertion of relatively large structures, such as biosensors into the interiors of cells for the early detection of cancer and other diseases and to monitor the progress of disease as well as response to drug therapy. The carbon nanotubes could be delivered into diseased cells and then exposed to light, causing them to heat up and selectively kill only the diseased cells.

Cell-Penetrating Peptides

Cell-penetrating peptides (CPPs) are short basic peptide sequences that might display amphipathic properties. CPPs generally contain a small number (<20–30) of amino acids, amongst which are a great number of positively charged amino acids that confer cell internalization properties on those peptides. Originally derived from natural proteins, the number of designed CPPs with similar cell penetration properties has now expanded widely. These positively charged peptides internalize into all cell types, but with different efficiency. CPPs use all routes of pinocytosis to internalize, in addition to direct membrane translocation that requires interaction with lipid

membrane domains. These differences in internalization efficiency according to the peptide sequence and cell type suggest that the CPPs interact with different molecular partners at the cell surface. The most popular CPPs are penetratin, Tat and oligoarginine, which interact with carbohydrates and lipids. Cell surface composition influences cell internalization, and the interaction with molecules found in membranes reflect the internalization efficiency of the peptides (Walrant et al. 2012). For specific drug-delivery, the exact molecular and chemical nature of membranes and their interactions with CPPs need to be identified.

Nanoparticle-Based Drug Delivery

Trend towards miniaturization of carrier particles had already started prior to the introduction of nanotechnology in drug delivery. As a part of introduction microparticles and nanoparticles will be compared for their role as carriers of therapeutic substances

The suitability of nanoparticles for use in drug delivery depends on a variety of characteristics, including size and porosity. Nanoparticles can be used to deliver drugs to patients through various routes of delivery. Nanoparticles are important for delivering drugs intravenously so that they can pass safely through the body's smallest blood vessels, for increasing the surface area of a drug so that it will dissolve more rapidly, and for delivering drugs via inhalation. Porosity is important for entrapping gases in nanoparticles, for controlling the release rate of the drug and for targeting drugs to specific regions.

It is difficult to create sustained release formulations for many hydrophobic drugs because they release too slowly from the nanoparticles used to deliver the drug, diminishing the efficacy of the delivery system. Modifying water uptake into the nanoparticles can speed the release, while retaining the desired sustained release profile of these drugs. Water uptake into nanoparticles can be modified by adjusting the porosity of the nanoparticles during manufacturing and by choosing from a wide variety of materials to include in the shell. Different types of nanoparticles and nanotechnologies used for drug delivery will be mentioned briefly here and specialized drug delivery for various disorders will be described in chapters dealing with those disorders.

Cationic Nanoparticles

Cationic nanoparticles built from drug, cationic lipid and polyelectrolytes are excellent and active carriers of amphotericin B against *Candida albicans*. Assemblies of amphotericin B and cationic lipid, at extreme drug to lipid molar ratios, were wrapped by polyelectrolytes forming cationic nanoparticles of high colloid stability and fungicidal activity against *C. albicans*. Experimental strategy involved dynamic light scattering for particle sizing, zeta-potential analysis, determination of colloid stability, determination of AmB aggregation state by optical spectra and determination of activity against *C. albicans* in vitro from cfu countings. The multiple assembly of antibiotic, cationic lipid and cationic polyelctrolyte, consecutively nanostructured in each particle produced a strategical and effective attack against fungal infections.

Ceramic Nanoparticles

Ceramic (inorganic) particles with entrapped biomolecules have potential pharmaceutical applications in including drug delivery. Ceramic nanoparticles have several advantages such as:

- Manufacture processes are similar to well-known sol-gel process, require ambient temperature condition, and can be easily prepared with the desired size, shape and porosity
- Their small size (less than 50 nm) can help them to evade being trapped by the reticulo-endothelial system of the body.
- There is no swelling or change in porosity with change in pH.
- These particles effectively protect doped molecules (enzymes, drugs, etc) against denaturation induced by external pH and temperature
- Such particles, including silica, aluminum, titanium, etc., are known for their compatibility with biological systems
- Their surfaces can be easily modified for conjugation to monoclonal antibodies or ligands to target them to desired sites in vivo.

Cyclodextrin Nanoparticles for Drug Delivery

Cyclodextrins are a family of cyclic oligosaccharides with a hydrophilic outer surface and a lipophilic center. Cyclodextrin molecules are relatively large with several hydrogen donors and acceptors and, thus, in general they do not permeate lipophilic membranes. Cyclodextrins have mainly been used as complexing agents to increase aqueous solubility of poorly soluble drugs, and to increase their bioavailability and stability.

Amphiphilic cyclodextrin nanoparticles, resulting from the esterification of primary hydroxyl groups by hydrocarbon chains varying from C6 to C14, can spontaneously form nanoparticles, which can be loaded with drugs. The drug can be released in a controlled manner following targeting delivery by the oral or the parenteral route. For injectable preparations, sterile filtration is not feasible since nanoparticle sizes are larger than the filter pore size and the yield after sterilization is very low. However, blank as well as drug loaded cyclodextrin nanospheres and nanocapsules are capable of being sterilized by gamma irradiation with no effect on particle size, drug loading and drug release properties.

Incorporation of cyclodextrins in poly(anhydride) nanoparticles improves their bioadhesive capability, the loading of lipophilic drugs and influences efflux membrane proteins as well as cytochrome P450. The combination between bioadhesive nanoparticles and P-gp inhibitors without pharmacological activity may be useful for promoting the oral bioavailability of drugs (Agüeros et al. 2011). CALAA01 (Arrowhead Research), a targeted, self-assembling nanoparticle system based on cyclodextrin complexed with siRNA, overcomes delivery problems of siRNAs, and has been shown to be effective in phase I clinical trials.

Dendrimers for Drug Delivery

Well-characterized, commercially available dendritic polymers have been subjected to functionalization for preparing drug delivery systems of low toxicity, high loading capacity, ability to target specific cells and transport through their membranes. This has been achieved by surface targeting ligands, which render the carriers specific to certain cells and PEG, securing water solubility, stability and prolonged circulation. Moreover, transport agents facilitate transport through cell membranes while fluorescent probes detect their intracellular localization. A common feature of surface groups is multivalency, which considerably enhances their binding strength with complementary cell receptors. To these properties, one should also add the property of attaining high loading of active ingredients coupled with controlled and/or triggered release (Paleos et al. 2010).

The unique properties of dendrimers such as high degree of branching and welldefined molecular weight make them ideal scaffolds for drug delivery. Advantages of dendrimers over linear polymers are:

- The large number of active functional groups on the surface of dendrimers allows them to be meticulously tailored and to act as nanoscaffolds or nanocontainers for various categories of drugs.
- Because of their well-defined molecular weight, they provide reproducible pharmacokinetic behavior compared to linear polymers containing fractions within a sample that vary greatly in molecular weight.
- The globular structure of dendrimers, as contrasted with the coil structure of most linear polymers can modify their biological properties, enabling discovery of new effects related to macromolecular architecture.

Dendrimers are particularly useful for the delivery of anticancer drugs such as cisplatin and doxorubicin. Dendrimers are also agents for boron neutron capture therapy and photodynamic therapy for cancer. By adding stimuli-responsive properties to the dendrimers, dendritic polymers capable of controlled release can be produced (Kojima 2010). These stimuli-responsive dendrimers are potential next generation drug carriers.

DNA-Assembled Dendrimers for Drug Delivery

A wide variety of nanoparticle drug delivery systems have been developed using DNA molecules to bind the dendrimers together. Nanometer-scaled dendrimers can be assembled in many configurations by using attached lengths of ssDNA molecules, which naturally bind to other DNA strands in a highly specific fashion. This approach enables targeting of a wide variety of molecules – drugs, contrast agents – to almost any cell. Nanoparticle complexes can be specifically targeted to cancer cells and are small enough to enter a diseased cell, either killing it from within or sending out a signal to identify it. However, construction of the particles is difficult and time-consuming.

Fullerenes for Drug Delivery

Amphiphilic Fullerene Derivatives

The amphiphilic fullerene monomer (AF-1) consists of a buckyball cage to which a Newkome-like dendrimer unit and five lipophilic C12 chains positioned octahedrally to the dendrimer unit are attached. An AF-1-based liposome termed buckysome is water soluble and forms stable spherical nanometer sized vesicles. Cryogenic electron microscopy Cryo-EM indicates the formation of large (400 nm diameter) multilamellar, liposome-like vesicles and unilamellar vesicles in the size range of 50–150 nm diameter. In addition, complex networks of cylindrical, tube-like aggregates with varying lengths and packing densities were observed. Under controlled experimental conditions, high concentrations of spherical vesicles could be formed. In vitro results suggest that these supra-molecular structures impose little to no toxicity. Ongoing studies are aimed at understanding cellular internalization of these nanoparticle aggregates. This delivery vector might provide promising features such as ease of preparation, long-term stability and controlled release.

Fullerene Conjugates for Intracellular Delivery of Peptides

Cell walls, or membranes, form a protective covering around the cell's inner machinery and its DNA blueprints. Drugs are far more effective if they are delivered through the membrane directly into the cell but this is difficult. A fullerene-peptide conjugate formed via the incorporation of a fullerene substituted phenylalanine derivative, "Bucky amino acid" (Baa), to a cationic peptide, acts as a passport for intracellular delivery, enabling transport of peptides that, in the absence of the fullerene amino acid, cannot enter the cell. Delivery of the fullerene species to either the cytoplasm or nucleus of the cell has been demonstrated. The hydrophobic nature of the fullerene assisting peptide transport is suggested by the effect of gammacyclodextrin in lowering the efficacy of transport. These data suggest that the incorporation of a fullerene-based amino acid provides a route for the intracellular delivery of peptides and creation of a new class of cell penetrating peptides. The peptides were found effective at penetrating the defenses of both liver cancer cells and neuroblastoma cells.

Gold Nanoparticles as Drug Carriers

Gold nanoparticles (AuNPs), in addition to their applications in molecular diagnostics, can be conjugated with peptides, drugs, and other molecules for drug delivery as well as for thermal treatment of cancer. AuNPs have received considerable attention as model drug delivery platforms because of their surface characteristics that enable easy functionalization with chemicals and biological molecules as well as due to their apparently low toxicity (Papasani et al. 2012). Efforts are being made to develop intelligent delivery systems by lining the walls of polymer 'delivery-vehicle' particles with gold nanoparticles. By simply shining a laser on loaded delivery vehicles (i.e. particles filled with various contents, such as an enzyme or drug), the walls could be opened and the contents released. This technique has been used successfully for the release of an encapsulated enzyme on demand with a single nanosecond laser pulse. In contrast to the common approach for drug release by changes in the local environment at the site where drug delivery is needed, gold nanoparticle technology enables externally controlled drug release. In addition to drugs, these gold-coated vehicles could be used for the controlled delivery of a wide range of other substances including genes. There is no risk that the laser energy will be significantly absorbed by biological structures such as bodily organs because the absorption of the gold-coated delivery vehicles in the NIR region is intentionally engineered in the wavelength regime for which light has a maximum penetration depth in tissue.

Layered Double Hydroxide Nanoparticles

Layered double hydroxides (LDHs) were well known as catalyst and ceramic precursors, traps for anionic pollutants, catalysts and additives for polymers. Their successful synthesis on the nanometer scale opened up a whole new application for delivery of drugs and other therapeutic/bioactive molecules (e.g. peptides, proteins, nucleic acids) to mammalian cells. LDH nanoparticles have advantages as well as disadvantages as carriers for nucleic acids and drugs and some challenges need to be overcome before LDH nanoparticles can be used in a clinical setting (Ladewig et al. 2009). Size-dependent toxicity of LDH was examined in cultured human lung cells; 50 nm particles were determined to be more toxic than larger particles, while LDHs within the size range of 100 to 200 nm exhibited very low cytotoxicity in terms of cell proliferation, membrane damage, and inflammation response (Choi et al. 2008).

Micelles for Drug Delivery

Polymeric micelles are formed through the multimolecular assembly of block copolymers as novel core-shell typed colloidal carriers for drug and gene targeting. The process of micellization in aqueous milieu is based on differences in the driving force of core segregation, including hydrophobic interaction, electrostatic interaction, metal complexation, and hydrogen bonding of constituent block copolymers. The segregated core embedded in the hydrophilic palisade is shown to function as a reservoir for genes, enzymes, and a variety of drugs with diverse characteristics. Functionalization of the outer surface of the polymeric micelle to modify its physicochemical and biological properties is used for designing micellar carrier systems for receptor-mediated drug delivery. Polymeric micelles persist in circulation for long duration of time and have significant tumor accumulation, indicating their potential for tumor-targeting therapy.

Polymerizable and hydrolytically cleavable dexamethasone (DEX) derivatives have been covalently entrapped in core-cross-linked polymeric micelles that were prepared from a thermosensitive block copolymer (Crielaard et al. 2012). By varying the oxidation degree of the thioether in the drug linker, the release rate of DEX could be controlled. The DEX-loaded micelles were used for efficient treatment of inflammatory arthritis in two animal models. Potential relevant applications in human medicine include drug delivery for rheumatoid arthritis.

A novel approach for the intravenous delivery of peptides uses core-cross-linked polymeric micelles. Peptides have poor pharmacokinetics due to rapid renal elimination. Covalent linking to core-cross-linked polymeric micelles (CCL-PMs) via two different hydrolysable ester linkages yields a nanoparticulate system with tuneable drug release kinetics (Hu et al. 2015). Compared to the soluble peptide, the leuprolide-entrapped CCL-PMs showed a prolonged circulation half-life (14.4 h) following a single intravenous injection in healthy rats and the released leuprolide was detected in blood for 3 days. In addition, the area under the plasma concentration-time curve (AUC) value was >100-fold higher for leuprolide-entrapped CCL-PMs than for soluble leuprolide. Importantly, the released peptide remained biologically active as demonstrated by increased and long-lasting plasma testosterone levels. This study shows that covalent linkage of peptides to CCL-PMs via hydrolytically sensitive ester bonds is a promising approach to achieving sustained systemic levels of peptides after intravenous administration.

Nanocomposite Membranes for Magnetically Triggered Drug Delivery

Nanocomposite membranes based on thermosensitive, poly(N-isopropylacrylamide)based nanogels and magnetite nanoparticles have been designed to achieve "on-demand" drug delivery upon the application of an oscillating magnetic field (Hoare et al. 2009). On-off release of sodium fluorescein over multiple magnetic cycles has been successfully demonstrated using prototype membrane-based devices. The total drug dose delivered was directly proportional to the duration of the "on" pulse. The membranes were noncytotoxic, were biocompatible, and retained their switchable flux properties after 45 days of subcutaneous implantation.

Nanocrystals

Nanocrystalline Silver

Silver has been valued for centuries for its medicinal properties. From ancient Greece to the American settlers, silver was used as a preservative for drinking water and other liquid storage. Decades ago, doctors would apply a thin layer of silver to large wounds to prevent infection and promote healing. Nucryst's silver nanocrystalline technology decreases the particle size, thus changing the physical and chemical properties. As the proportion of atoms on the surface increases, the result is a more powerful compound than conventional silver treatments. In vitro tests have demonstrated that active silver clusters of ions begin providing antimicrobial activity immediately and kill many organisms in 30 min, faster than other forms of silver.

SilcrystTM nanocrystals release sustained, uniform doses of silver. Silver nanocrystalline technology can deliver a sustained release of active silver to the dressings over a longer period of time than any other silver treatment. Other treatments, such as Silver Sulfadiazine and Silver Nitrate, are characterized by the rapid depletion of active silver, forcing the regular scraping of creams from or applications of solutions to open wounds multiple times per day. This process is labor intensive and extremely traumatic for patients. Silver nanocrystalline technology dressings cover the wound providing sustained release of silver to the dressing, acting as a barrier to infection for up to 7 days. ActicoatTM (Smith & Nephew) dressings for burns and chronic wounds use Nucryst's proprietary SilcrystTM silver nanocrystalline technology. In vitro studies of Acticoat have demonstrated:

- Extensive antimicrobial spectrum of 150 different pathogens
- Rapid kill rates
- Effective against drug-resistant forms of bacteria, such as MRSA (Methicillinresistant *Staphylococcus aureus*) and VRE (Vancomycin-resistant *Enterococci*), sometimes referred to as "superbugs"
- Fast-acting release of ionic silver to the dressing over a sustained period of time (effective for up to 7 days)

The company also is conducting preclinical studies on the use of nanocrystalline silver inhaled into the lungs for the treatment of serious lung inflection or lung inflammation. In the future, the company plans to conduct research on the nanocrystalline structures of other metals, including gold, which is well-known as a treatment for arthritis, and platinum, which is a well- known treatment for cancer, to determine if the behavior and performance of these metals also can be enhanced.

Elan's NanoCrystal Technology

NanoCrystal® (Elan) particles are small particles of drug substance, typically less than 1000 nm in diameter, which are produced by milling the drug substance using a proprietary milling technique. The NanoCrystal® particles of the drug are stabilized against agglomeration by surface adsorption of selected GRAS (Generally Regarded As Safe) stabilizers. The result is a suspension of the drug substance that behaves like a solution-a NanoCrystal® colloidal dispersion, which can be processed into dosage forms for all routes of administration. NanoCrystal® technology is being used by Johnson & Johnson Pharmaceutical Research & Development in a phase III clinical trial of a long acting injectable formulation of its paliperidone palmitate in patients with schizophrenia.

NanoCrystal® technology represents a valuable, enabling technology to evaluate new chemical entities which exhibit poor water solubility and is also a valuable tool for optimizing the performance of established drugs. NanoCrystal technology has the potential to rescue a significant number of poorly soluble chemical compounds. The drug in nanoform can be incorporated into common dosage forms, including tablets, capsules, inhalation devices, sterile forms for injection, with the potential for substantial improvements to clinical performance. There are currently two pharmaceutical products that have been commercialized incorporating NanoCrystal technology, with several additional product launches anticipated over the near future. Advantages of this technology are:

- More rapid absorption of active drug substance
- · Higher dose loading with smaller dose volume
- · Aqueous based with no organic solvents needed
- Capability for sterile filtering
- · Longer dose retention in blood and tumors for some compounds

Biorise System

Biorise[™] sytem (Adair Pharmaceuticals) creates new physical entities by physically breaking down a drug's crystal lattice. This results in drug nanocrystals and/or amorphous drug, which are then stabilized with biologically inert carriers. The carriers used in the Biorise system are biocompatible and readily disperse in the body's GI fluids. The final product is a free-flowing powder that can be incorporated into a variety of dosage forms to achieve the most effective delivery.

Adair uses three types of carriers; swellable microparticles, composite swellable microparticles or cyclodextrins. When used in the Biorise system, all three carrier types improve both solubility and dissolution rate as well as the rate and overall percentage of drug absorption. The selection of the appropriate type of Biorise carrier is a critical step in the process and is dependent upon the drug delivery objective, drug carrier compatibility and its drug loading capacity.

Adair has developed several activation systems that can convert a drug into its thermodynamically activated state. These systems provide flexibility and allow the technology to be applied to a range of compounds with differing characteristics. These systems include:

High Energy Mechanochemical Activation (HEMA) This system involves the application of friction and impact energy to the drug thereby increasing its entropy and transforming the drug into its activated state. This system is a dry system and maintains the drug/carrier matrix in a powder form at all times.

Solvent Induced Activation (SIA) This system is particularly suitable for thermolabile compounds and compounds with a low melting point. With this system, a drug can be solubilized in an appropriate solvent and layered onto swellable, crosslinked carriers. Controlled evaporation of the solvent and drying the material creates nanoparticles and/or amorphous drug that is stabilized in a carrier.

Super Critical Fluid Activation (SCFA) A drug and carrier are placed in a solvent system within a soluble environment. The solvent is removed by controlled displacement using super critical fluids resulting in the precipitation of nanocrystal-line and/or amorphous drug that is stabilized in a carrier.

Before Aptalis begins working on a compound, its experienced teams of scientists evaluate the compound and apply a mathematical model to predict the impact that Biorise will have on a drug. This model simulates an in-vitro release profile and also determines the most appropriate carrier system as well as drug to carrier ratios. Modeling is a key component in the Biorise process as it helps to:

- Expedite development programs and accelerate the time to market
- Reduce the need for experimentation
- Speed up the rational screening process
- Rapidly predict the outcome of the project

Aptalis' Biorise system can be used to improve a product already on the market, a drug currently in development as well as to rescue a drug that has been shelved due to solubility difficulties. The system also offers faster and more efficient processing times compared to other marketed technologies and is currently one of the few bioavailability enhancement technologies that is commercialized and being used in a marketed product. The Biorise system offers additional advantages including:

- No use of surfactants
- Produces a drug powder which can be incorporated into a variety of dosage forms including tablets and capsules
- Stable
- Cost effective process
- · Scaled-up, validated, approved by a regulatory agency and commercialized
- · Ability to control and vary the ratio of nanocrystal and amorphous drug
- Uses GRAS materials

Nanodiamonds

Nanodiamonds are nanoparticles varying in size from 2 to 8 nm and can be used for diagnostic as well as therapeutic purposes. They are also formed as byproducts of diamond refining and mining. Water-dispersion of previously insoluble drugs when complexed with nanodiamonds demonstrates great promise in expanding current drug delivery options (Lam and Ho 2009). Bovine insulin was non-covalently bound to detonated nanodiamonds via physical adsorption in an aqueous solution and demonstrated pH-dependent desorption in alkaline environments of sodium hydroxide (Shimkunas et al. 2009).

Carbon nanodiamonds are much more biocompatible than most other carbon nanomaterials, including carbon blacks, fullerenes and carbon nanotubes. The noncytotoxic nature of nanodiamonds, together with their unique strong and stable photoluminescence, tiny size, large specific surface area and ease with which they can be functionalized with biomolecules, makes nanodiamonds attractive for various biomedical applications both in vitro and in vivo (Xing and Dai 2009). Applications include drug delivery, surgery and dentistry. Another unique attribute of nanodiamonds is bright stable fluorescence based on crystallographic defects that has a potential for developing multimodal imaging/therapy platforms (Vaijayanthimala et al. 2015).

Nanodiamonds (with attached molecules) are able to penetrate the BBB. The anticancer drug ND-DOX was created by bonding doxorubicin molecules nanodiamond surfaces, and tumors were unable to eject the drug. Nanodiamonds are suitable for transdermal drug delivery as they are well-absorbed by human skin and enable drugs to penetrate the deeper layers of skin.

Polymer Nanoparticles

Biodegradable polymer nanoparticles include chitosan (CS) nanoparticles, polyethylene glycol (PEG) nanoparticles, and polylactide-co-glycolic acid (PLGA) nanoparticles.

Biodegradable PEG Nanoparticles for Penetrating the Mucus Barrier

Protective mucus coatings typically trap and rapidly remove foreign particles from the eyes, gastrointestinal tract, airways, nasopharynx, and female reproductive tract, thereby strongly limiting opportunities for controlled drug delivery at mucosal surfaces. A preparation of nanoparticles composed of a biodegradable diblock copolymer of polysebacic acid and polyethylene glycol (PSA-PEG), both of which are routinely used in humans, can diffuse through mucous membranes (Tang et al. 2010). In fresh undiluted human cervicovaginal mucus (CVM), which has a bulk viscosity approximately 1800-fold higher than water at low shear, PSA-PEG nanoparticles diffused at an average speed only 12-fold lower than the same particles in pure water. In contrast, similarly sized biodegradable nanoparticles composed of PSA or PLGA diffused at least 3300-fold slower in CVM than in water. PSA-PEG particles also rapidly penetrated sputum expectorated from the lungs of patients with cystic fibrosis, a disease characterized by hyperviscoelastic mucus secretions. Rapid nanoparticle transport in mucus is made possible by the efficient partitioning of PEG to the particle surface during formulation. Biodegradable polymeric nanoparticles capable of overcoming human mucus barriers and providing sustained drug release open significant opportunities for improved drug and gene delivery at mucosal surfaces. Beyond their potential applications for cystic fibrosis patients, the nanoparticles also could be used to help treat disorders such as lung and cervical cancer, and inflammation of the sinuses, eyes, lungs and gastrointestinal tract. Chemotherapy is typically given to the whole body and has many undesired side effects. If drugs are encapsulated in these nanoparticles and inhaled directly into the lungs of lung cancer patients, drugs may reach lung tumors more effectively, and improved outcomes may be achieved, especially for patients diagnosed with early stage NSCLC. PEG acts as a shield to protect the particles from interacting with proteins in mucus that would cause them to be cleared before releasing their contents. Nanoparticles can efficiently encapsulate several chemotherapeutics, and a single dose of drug-loaded particles is able to limit tumor growth in a mouse model of lung cancer for up to 20 days.

Additionally, PEG coating improves the stability of PLGA nanoparticles in the gastrointestinal fluids and helps the transport of the encapsulated protein, tetanus toxoid, across the intestinal and nasal mucous membranes. Furthermore, intranasal administration of these nanoparticles provided high and long-lasting immune responses.

PLGA-Based Nanodelivery Technologies

Polylactide-co-glycolic acid (PLGA) is a FDA approved copolymer which is used in a host of therapeutic devices, owing to its biodegradability and biocompatibility. PLGA is synthesized by means of random ring-opening co-polymerization of two different monomers. PLGA nanoparticles deliver molecules considered too large and complex to transport with known vectors. PLGA is nontoxic, does not illicit an immune response, causes comprehensive transfection, crosses the blood-brain barrier, and supports sustained drug release. PLGA has been successful as a biodegradable polymer because it undergoes hydrolysis in the body to produce the original monomers, lactic acid and glycolic acid. These two monomers under normal physiological conditions are by-products of various metabolic pathways in the body. Since the body effectively deals with the two monomers, there is very minimal systemic toxicity associated with using PLGA for drug delivery or biomaterial applications. Also, the possibility to tailor the polymer degradation time by altering the ratio of the monomers used during synthesis has made PLGA a common choice in the production of a variety of biomedical devices such as: grafts, sutures, implants and prosthetic devices. As an example, a commercially available drug delivery device using PLGA is Abbott's Lupron Depot® (leuprolide acetate) for the treatment of advanced prostate cancer.

Polymeric Micelles

Micelles are biocompatible nanoparticles varying in size from 50 to 200 nm in which poorly soluble drugs can be encapsulated represent a possible solution to the delivery problems associated with such compounds and could be exploited to target the drugs to certain sites in the body, potentially alleviating toxicity problems. pH-sensitive drug delivery systems can be engineered to release their contents or change their physicochemical properties in response to variations in the acidity of the surroundings. One example of this is the preparation and characterization of novel polymeric micelles (PM) composed of amphiphilic pH-responsive poly(N-isopropylacrylamide) (PNIPAM) or poly(alkyl(meth)acrylate) derivatives. On one hand, acidification of the PNIPAM copolymers induces a coil-to-globule transition that can be exploited to destabilize the intracellular vesicle membranes. PNIPAM-based PMs, loaded with either doxorubicin or aluminum chloride phthalocyanine, are cytotoxic in murine tumor models. On the other hand, poly(alkyl(meth)acrylate) copolymers can be designed to interact with either hydrophobic drugs or polyions and release their cargo upon an increase in pH. The self-assembly of well-defined polypeptide-based diblock copolymers into micelles and stimuli-responsive behavior of polypeptides to pH and ionic strength is used to produce nanoparticles with controlled size and shape, which are particularly useful for encapsulation and delivery purpose at a controlled pH.

Chitosan Nanoparticles

Chitin, a polymer, is commercially extracted from shrimp shells and has several medical applications. Chitin is a very large sugar molecule with severalacetic acid molecules attached to it. Treatments with soda remove some of this acetic acid from the sugar backbone, converting chitin into biopolymer chitosan. Chitosan is prone to chemical and physical modifications, and is very responsive to environmental stimuli such as temperature and pH. These features make chitosan a smart material with great potential for developing multifunctional nanocarrier systems to deliver large varieties of therapeutic agents administrated in multiple ways with reduced side effects. Chitosan modification with a variety of ligands specific for cell surface receptors can increase recognition and uptake of nanocarriers into cells through receptor-mediated endocytosis (Duceppe and Tabrizian 2010).

Chitosan nanoparticles are known for their ability to overcome biological barriers and facilitate the delivery of complex drugs such as insulin, vaccines, plasmid DNA and genes. In the NanoBioSaccharides project which is financed by the European Union, scientists from universities and commercial companies in Germany, France, Spain, Denmark, and Italy will collaborate to optimize these technologies to further improve the delivery of macromolecules, e.g. insulin, via the nasal, pulmonary, and oral routes instead of via an injection into the blood vessels.

N-(2-hydroxyl) propyl-3-trimethyl ammonium chitosan chloride (HTCC) is water-soluble derivative of chitosan (CS), synthesized by the reaction between glycidyl-trimethyl-ammonium chloride and CS. HTCC nanoparticles have been formed based on ionic gelation process of HTCC and sodium tripolyphosphate (TPP). Bovine serum albumin (BSA), as a model protein drug, is incorporated into the HTCC nanoparticles measuring 110–180 nm in size with encapsulation efficiency up to 90%. In vitro release studies showed a burst effect and a slow and continuous release followed. Encapsulation efficiency was obviously increased with increase of initial BSA concentration.

Coating of PLGA nanoparticles with the mucoadhesive CS improves the stability of the particles in the presence of lysozyme and enhanced the nasal transport of the encapsulated tetanus toxoid. Nanoparticles made solely of CS are stable upon incubation with lysozyme. Moreover, these particles are very efficient in improving the nasal absorption of insulin as well as the local and systemic immune responses to tetanus toxoid, following intranasal administration.

By encapsulating drugs in CS cubes, the cells of the body are tricked into absorbing drugs that could not normally be transported across the cell membrane. After delivering its load directly into the cells affected, CS is broken down in the body and disappears without a trace. CS capsules can transport siRNA into the cell to switch off faulty genes selectively. A siRNA against the respiratory syncytial virus (RSV), RSV-NS1gene (siNS1), has been tested for its potential in decreasing RSV infection and infection-associated inflammation in rats. Plasmids encoding siNS1 were complexed with a chitosan nanoparticle delivery agent and administered intranasally. They were shown to be effective in reducing virus titers in the lung and in preventing the inflammation and airway hyperresponsiveness associated with the infection.

QDs for Drug Delivery

Engineered QDs with integrated targeting, imaging and therapeutic functions are excellent materials for study of drug delivery in cells and experimental animals. They can provide important information for the rational design of biocompatible drug carriers and can serve as a superior alternative to magnetic and radioactive imaging contrast agents in preclinical drug screening, validation and delivery research. In a multifunctional QD coated with amphiphilic polymer, hydrophobic drugs can be trapped between the nanoparticle core and amphiphilic polymer coating layer, and hydrophilic targeting molecules can be immobilized on the outer surface.

To meet some challenges of drug delivery, the engineered QDs would be able to stabilize therapeutic compounds, increase their plasma circulation time while reducing the concentration of free drug to minimize unwanted side effects, and to release the drug with a well-controlled profile. In addition, it should be possible to covalently link the therapeutic compounds to the target on QD surface via cleavable chemical bonds, so that the bioconjugates are initially large enough to avoid renal filtration, but following cleavage of the ligands, are small enough to be cleared out of the body. With advances being made in the identification of new targeting ligands, the development of specialized nanoparticles and the discovery of better conjugation techniques, the QD-based drug delivery has excellent prospects. Role of QDs in drug delivery for cancer is described later in this chapter.

Special Procedures in Nanoparticle-Based Drug Delivery

Coated Nanoparticles for Penetrating Cell Membranes Without Damage

Most nanoscale objects are typically internalized by cells into membrane-bounded endosomes and fail to access the cytosolic cell machinery. Gold nanoparticles coated with alternating bands of two different types of molecules can penetrate a cell without damaging it, while those randomly coated with the same materials cannot. This is the first fully synthetic material that can pass through a cell membrane without rupturing it, and is significant for drug delivery across biological membranes. In addition to the practical applications of such nanoparticles for drug delivery, they have been used to deliver fluorescent imaging agents to cells that could help explain how some biological materials such as peptides can enter cells.

Combinatorial Synthesis of Nanoparticles for Intracellular Delivery

Evaluation of a large library of structurally distinct nanoparticles with cationic cores and variable shells was carried out by using robotic automation. Nanoparticles were combinatorially cross-linked with a diverse library of amines, followed by measurement of molecular weight, diameter, RNA complexation, cellular internalization, and in vitro siRNA and pDNA delivery (Siegwart et al. 2011). Analysis revealed structure-function relationships and beneficial design guidelines. Cross-linkers optimally possessed tertiary dimethylamine or piperazine groups and potential buffering capacity. Covalent cholesterol attachment enabled intracellular delivery in vivo to liver hepatocytes in mice.

Drug Delivery Using "Particle Replication in Nonwetting Templates"

Most current techniques for particle formation are incompatible with organic materials because they involved baking, etching or processing robust metals using with solvents that destroy fragile organic matter such as genes or drugs. The relatively simple process, called Particle Replication in Nonwetting Templates (PRINT) avoids creating films or "scum layers" that would clump particles together rather than allowing them to be harvested independent of one another. PRINT affords the simple, straightforward encapsulation of a variety of important bioactive agents, including proteins, DNA, and small-molecule therapeutics, which indicates that PRINT can be used to fabricate next-generation particulate drug-delivery agents. The particles are so small they can be designed and constructed to measure <200 nm in diameter. The method avoids harsh treatment but also allows formation of uniform particles in any shape that designers choose: spheres, rods, cones, trapezoidal solids, etc. Besides drug delivery, this technology will have a profound impact on human health care in areas such as chemotherapy, gene therapy, and disease detection. Particles injected into the body can be designed to be biodegradable and incorporate as "cargo" any biological material that designers want to introduce into patients' bloodstreams for more efficient uptake by cells for diagnostic testing or therapy. Preliminary in vitro and in vivo studies have demonstrated future utility of PRINT particles as delivery vectors in nanomedicine.

Encapsulating Water-Insoluble Drugs in Nanoparticles

Many of the most potent anticancer agents are poorly soluble in water, presenting a challenge for medicinal chemists who must develop methods of delivering these drugs in the watery environment of the human body. Nanoparticles appear to be perfectly suited to this task, and indeed, numerous research groups are developing nanoparticles specifically for delivering water-insoluble drugs to tumors. A fundamental understanding of particle size control in antisolvent precipitation is beneficial for designing mixing systems and surfactant stabilizers for forming nanoparticles of poorly water soluble drugs with the potential for high dissolution rates.

Inverse emulsion photopolymerization – a method that uses light to create a well-defined polymeric nanoparticle with internal spaces that can provide a friendly environment to water-insoluble drugs and channels through which the entrapped drugs can escape into malignant cells. These nanoparticles are made up of two different polymers that crosslink to each other when exposed to light from an argon laser for 1 h. The nanoparticles are then added to a solution of doxorubicin and the solvent used to dissolve the anticancer drug is evaporated. Nearly half of the drug in solution became encapsulated within the nanoparticles. The researchers note that the resulting nanoparticles contain a protein-repelling surface coating that should result in favorable pharmacokinetic behavior. Experiments to test the drug-release characteristics of these nanoparticles showed that maximum release occurred at approximately 8 h and then remained close to that level for a week. The data imply that release occurs through a diffusion mechanism, that is, drug travels through channels in the nanoparticle to the nanoparticle surface, as opposed to a disintegration mechanism in which the nanoparticle falls apart and releases drug. This novel colloidal system can be as a controlled delivery system for small hydrophobic drugs for cancer.

Filomicelles Vs Spherical Nanoparticles for Drug Delivery

Shape may be important in designing better nanotechnology-based drug delivery vehicles. A study in rodents has compared highly stable, polymer micelle assemblies known as filomicelles with spheres of similar chemistry and shown that filomicelles persisted in the circulation up to 1 week after intravenous injection (Geng et al. 2007). This is about ten times longer than their spherical counterparts and is more persistent than any known synthetic nanoparticle. Under fluid flow conditions, spheres and short filomicelles are taken up by cells more readily than longer filaments because the latter are extended by the flow. Preliminary results further demonstrate that filomicelles can effectively deliver the anticancer drug paclitaxel and shrink human-derived tumors in mice. Although these findings show that long-circulating vehicles need not be nanospheres, they also lend insight into possible shape effects of natural filamentous viruses.

Flash NanoPrecipitation

Flash NanoPrecipitation produces stable nanoparticles at high concentrations using amphiphilic diblock copolymers to direct self-assembly. In NanoPrecipitation, two streams of liquid are directed toward one another in a confined area. The first stream consists of an organic solvent that contains the medicines and imaging agents, as well as long-chain molecules called polymers. The second stream of liquid contains pure water. When the streams collide, the hydrophobic medicines, metal imaging agents and polymers precipitate out of solution to avoid the water molecules. The technique has been applied to the anticancer agent paclitaxel. The polymers immediately selfassemble onto the drug and imaging agent cluster to form a coating with the hydrophobic portion attached to the nanoparticle core and the hydrophilic portion stretching out into the water. By carefully adjusting the concentrations of the substances, as well as the mixing speed, the researchers can control the sizes of the nanoparticles. Uniform particles with tunable sizes from 50 to 500 nm can be prepared. The key to the process is the control of time scales for micromixing, polymer self-assembly, and particle nucleation and growth. The diffusion-limited assembly enables particles of complex composition to be formed. The stretched hydrophilic polymer layer keeps the particles from clumping together and prevents recognition by the immune system so that the particles can circulate through the bloodstream. The hydrophobic interior of the particles ensures that they are not immediately degraded by watery environments, though water molecules will, over time, break the particles apart, dispersing the medicine. Ideally, the particles would persist for 6–16 h after they are administered intravenously, which would allow enough time for the potent packages to slip into the solid tumor cells whenever they encounter them throughout the body.

Applications include controlled delivery of multiple drugs from nanoparticles as well as aerosol drug delivery. It enables the simultaneous encapsulation and controlled release of both hydrophobic and hydrophilic actives. The incorporation of gold nanoparticles and organic compounds into single nanoparticles enables simultaneous delivery and medical imaging. Finally, the ability to dry the nanoparticles by lyophilization or spray drying and to reconstitute them without aggregation greatly enhances the applicability of the technology.

These nanoparticles can deliver medicine deep into the lungs or infiltrate cancer cells while leaving normal ones alone. Only 100 to 300 nm wide, the particles can be loaded with medicines or imaging agents, like gold and magnetite, that will enhance the detection capabilities of CT scans and MRIs. The nanoparticles are too large to pass through the membrane of normal cells, but will pass through larger defects in the capillaries in rapidly growing solid tumors.

Particles in this size range also could improve the delivery of inhaled drugs because they are large enough to remain in the lungs, but too small to trigger the body's lung-clearing defense systems. This trait could maximize the effectiveness of inhaled, needle-free vaccination systems. It has potential applications in the development of nanoparticle-based aerosol vaccines for tuberculosis and diphtheria. Because of their potential for use on a large scale at relatively low cost, these systems that are particularly attractive for use in the developing world.

Magnetic Nanoparticles for Drug Delivery

These particles have a magnetic core with a polymer or metal coating, which can be functionalized. A therapeutic agent such as a cytotoxic drug or a therapeutic DNA can be attached to the particle. The particles are delivered by a catheter close to the site of action and further guided by external magnetis. Investigations of magnetic micro- and nanoparticles for targeted drug delivery began more than 30 years ago and major advances has been made in particle design and synthesis techniques. Although very few clinical trials have taken place, with this technique, it appears to be promising. NanoTherics is developing magnefect-nanoTM, which has the following advantages:

- Up to 1000-fold higher transfection efficiencies at short transfection times when compared to cationic lipid reagents
- No adverse effects on cell viability
- Potential to target/penetrate physical barriers in vivo (e.g. mucous layers for cystic fibrosis gene transfection)
- Successful with "hard to transfect" cells/cell lines
- · Cost-effective, saving time and materials
- · Can be used with adherent and suspension cells
- Scalable for high throughput screening

Nanoparticles Bound Together in Spherical Shapes

Altair Nanotechnologies Inc. has developed unique micron size structures (TiNano SpheresTM) made by its patented "growth-in-film" nanotechnology. They consist of hundreds of nanoparticles bound together in spherical and near spherical shapes that can carry active pharmaceutical ingredients (API), biocides, or fungicides on either the interior or exterior surfaces. The nanoparticles have a very high surface area and

when coated with an API delivers a very large amount of drug to biosystem interface. This larger interface could improve solubility and/or reaction rates.

Altair's nanotechnology is used to create competent porous microstuctures consisting of high surface area nano primary particles to enable new applications for hard to dissolve drugs. A sustained release of drugs is possible by applying the drug to the inside of the TiNano SpheresTM. Dual action properties are possible by applying one drug to the inside and another to the outside of the TiNano Sphere. Altair has successfully deposited at least one of these drugs on the surface of TiNano SpheresTM. Some of the many possible applications of TiNano SpheresTM are:

- Drug delivery by topical applications
- Sustained release of antibiotic and fungicides
- · Sustained release of drugs for cholesterol lowering
- · Pain and itch preparations with sustained release action
- Sunscreen and after-sun care

Perfluorocarbon Nanoparticles for Imaging and Targeted Drug-Delivery

Perfluorocarbon (PFC) nanoparticles are approximately 200 nm in diameter and are encapsulated in a phospholipid shell, which provides an ideal surface for the incorporation of targeting ligands, imaging agents and drugs. PFC nanoparticles can serve as a platform technology for molecular imaging and targeted drug-delivery applications. For molecular imaging, PFC nanoparticles can carry very large payloads of gadolinium to detect pathological biomarkers with MRI. A variety of different epitopes, including $\alpha\nu\beta3$, tissue factor and fibrin, have been imaged using nanoparticles formulated with appropriate antibodies or peptidomimentics as targeting ligands. Lipophilic drugs can also be incorporated into the outer lipid shell of nanoparticles for targeted delivery. Upon binding to the target cell, the drug is exchanged from the particle surfactant monolayer to the cell membrane through a novel process called 'contact facilitated drug delivery'. By combining targeted molecular imaging and localized drug delivery, PFC nanoparticles provide diagnosis and therapy with a single agent and would facilitate the development of personalized medicine.

The contrast agents in development by Kereos Inc. comprise tiny perfluorocarbon nanoparticles suspended in an emulsion. Agents such as Technetium-99 m, may be attached to the nanoparticles to provide the contrast that allows for imaging. In addition, nanoparticles are labeled with a specific ligand that causes the agent to target newly developing blood vessels. When injected into the body, the resulting agent will find and illuminate these vessels. Anticancer drugs and therapeutic radionuclides may also be incorporated into the nanoparticles to deliver therapy directly and selectively.

Prolonging Circulation of Nanoparticles by Attachment to RBCs

Polymeric nanoparticles are used as carriers for systemic and targeted drug delivery. They protect drugs from degradation until they reach their target and provide sustained release of drugs. However, applications of nanoparticles are limited by their short in vivo circulation lifetimes. They are quickly removed from the blood, sometimes in minutes, rendering them ineffective in delivering drugs. It is now possible to dramatically improve the in vivo circulation lifetime of polymeric nanoparticles by attaching them to the surface of red blood cells (RBCs) without affected their circulation. The particles remain in circulation so long as they remain attached to RBCs, theoretically up to the circulation lifetime of a RBC, which is 120 days. Particles eventually detach from RBCs due to shear forces and cell-cell interactions and are subsequently cleared in the liver and spleen.

The researchers have learned that particles adhered to RBCs can escape phagocytosis because red blood cells have a knack for evading macrophages. Nanoparticles are not the first to be piggybacking on red blood cells; the strategy has already been adopted by certain bacteria, such as hemobartonella, that adhere to RBCs and can remain in circulation for several weeks. Using RBCs to extend the circulation time of the particles avoids the need to modify the surface chemistry of the entire particle, which offers the potential to attach chemicals to the exposed surface for targeting applications. The exposed surface of the particles could be used to immobilize enzymes and improve their in vivo circulation lifetime. The enzyme would have direct access to plasma in the systemic circulations in which extended circulation may also be applied to gene delivery applications in which extended circultion times are difficult to achieve. Synthetic gene delivery vectors suffer from rapid clearance by the reticulo-endothelial system, restricting transfection to the liver and lung. RBC attachment of gene vectors may provide a long-circulating depot, thereby increasing their residence time in blood.

RBC membrane-coated nanoparticles present a breakthrough in drug delivery technology and show great promise for clinical applications (Fang et al. 2012). This technique could be applied for the delivery of drugs and circulating bioreactors in a wide variety of conditions such as cancer and heart disease.

Self-Assembling Nanoparticles for Intracellular Drug Delivery

EAK16-II, a self-assembling peptide, has been found to stabilize the hydrophobic anticancer agent ellipticine (EPT) in aqueous solution and form nanoparticles with an average size of ~100 nm (Bawa et al. 2012). This nanoformulation is cytotoxic to human lung carcinoma A549 cells that is comparable to EPT dissolved in dimethyl sulfoxide. It enhances EPT uptake significantly as compared to the micro-formulation. Promising therapeutic efficacy, specific delivery pathway, and intracellular distribution pattern discovered in this study may help further develop EPT as a nanoformulation for clinical applications.

Researchers at the University of Ulsan College of Medicine (Seoul, Korea), have developed self-assembling nanoparticles that can sense the low pH of endosomes and disintegrate, which not only releases their drug payload but enables it to exit the endosomes. Chitosan serves as the starting material for these self-assembling nanoparticles. The investigators modify the polymer by attaching a chemical derivative of the amino acid histidine to each of the sugar units in the chitosan backbone. At neutral pH, histidine is hydrophobic, or poorly soluble in water. The presence of multiple histidines on the water-soluble, or hydrophilic, chitosan backbone creates a molecule that naturally self-assembles into a structure that surrounds the hydrophobic histidines with a protective shell of hydrophilic chitosan. When added to cells grown in culture, the nanoparticles fuse with the cell membrane, forming endosomes inside the cell. At the low pH found inside an endosome, histidine takes on a positive charge and becomes hydrophilic. Therefore, the physical forces that held together the self-assembling nanoparticle no longer exist and the nanoparticle falls apart. Any drug molecules entrapped within the nanoparticle is then released into the endosomes.

Trojan Nanoparticles

Trojan particles combine the drug release and delivery potential of nanoparticle systems with the ease of flow, processing, and aerosolization potential of large porous particle systems by spray drying solutions of polymeric and nonpolymeric nanoparticles into extremely thin-walled macroscale structures. These hybrid particles exhibit much better flow and aerosolization properties than the nanoparticles; yet, unlike the large porous particles, which dissolve in physiological conditions to produce molecular constituents, hybrid particles dissolve to produce nanoparticles with drug release and delivery. Formation of the large porous nanoparticle aggregates occurs via a spray-drying process that ensures the drying time of the sprayed droplet is sufficiently shorter than the characteristic time for redistribution of nanoparticles by diffusion within the drying droplet. Additional control over the physical characteristics is achieved by adding other components to the spray-dried solutions, including sugars, lipids, polymers, and proteins. The ability to produce large porous nanoparticles appears to be largely independent of molecular component type as well as the size or chemical nature of the nanoparticles.

These particles range in size from 25 nm to several hundred nanometes and can be used to deliver drugs to specific sites within the body. They are robust drug delivery systems that can be used to encapsulate drugs of varying chemistry and molecular weights. Trojan nanoparticles will be discussed further under the topic of drug delivery across the BBB.

Therapeutic Protein Delivery from Nanoparticle-Protein Complexes

Gold nanoparticles attached to proteins form sheets of protein-gold arrays, which can be used to identify functional parts of proteins and to construct new nanoparticleprotein complexes as precision vehicles for targeted drug delivery. Therapeutic protein delivery from nanoparticle aggregates depends on several independent variables including nanoparticle size and chemical composition of the particle. The nanoparticle aggregate technology allows remarkable versatility in protein loading and subsequent release. Optimization of a formulation can be achieved in a relatively short time for a given protein drug. Importantly, this technology can substantially reduce the "burst release" of the protein, which occurs with other delivery systems. In preclinical animal studies the ability to control the release of the protein for periods of 3 months and greater has been established. Additional preclinical animal studies have shown that the materials used to produce the aggregates, which are included in several FDA-approved products, are biocompatible and therefore suitable for use in a drug delivery system. It represents one of the simplest delivery systems with great versatility for incorporating and delivering proteins. The ability to load the protein in a cost-effective manufacturing process without using solvents or polymerization and to tightly control the drug release profile are potentially very significant advantages over other protein delivery technologies. Protein delivery is important as therapeutic proteins are being increasingly used to treat a wide variety of disease including cancer, infections, rheumatoid arthritis and autoimmune diseases.

Triggered Release of Drugs from Nanoparticles

Controlling location and timing of the release enables use of potent drugs in a personalized manner so that the interaction with the right target is ensured. One method for this is externally triggered release of encapsulated compounds, which can be accomplished if drug delivery vehicles, such as liposomes or polyelectrolyte multilayer capsules, incorporate NP actuators. NPs can efficiently harvest energy from tissue penetrating, external stimuli, such as near infrared (NIR) light and alternating magnetic fields (AMFs), localize it by local field enhancement or convert it into heat, and thus trigger release of cargo from thermoresponsive vehicles. Cargo release can be externally triggered by magnetic or electromagnetic fields from vesicles loaded with superparamagnetic or metallic NPs. Control over the assembly of NPs into a responsive vesicle determines the vesicle stability, and the ability to control timing and dose of the cargo released from the vesicle. Thus, nondestructive, reversible changes in permeability of delivery vehicles enables pulsed cargo release, and therefore e close control over timing and dose of released cargo.

Liposomes

Basics of Liposomes

Liposome properties vary substantially with lipid composition, size, surface charge and the method of preparation. They are therefore divided into three classes based on their size and number of bilayers.

- 1. Small unilamellar vesicles are surrounded by a single lipid layer and measure 25–50 nm in diameter.
- 2. Large unilamellar vesicles are a heterogeneous group of vesicles similar to and are surrounded by a single lipid layer.
- 3. Multilamellar vesicles consist of several lipid layers separated from each other by a layer of aqueous solution.

Lipid bilayers of liposomes are similar in structure to those found in living cell membranes and can carry lipophilic substances such as drugs within these layers in the same way as cell membranes. AFM is useful in evaluating the physical characteristics and stability of liposomes as drug delivery systems (Spyratou et al. 2009). The pharmaceutical properties of the liposomes depend on the composition of the lipid bilayer and its permeability and fluidity. Cholesterol, an important constituent of many cell membranes is frequently included in liposome formulations because it reduces the permeability and increases the stability of the phospholipid bilayers. Until recently, the use of liposomes as therapeutic vectors was hampered by their toxicity and lack of knowledge about their biochemical behavior. The simplest use of liposomes is as vehicles for drugs and antibodies for the targeted delivery of anticancer agents. Furthermore, liposomes can be conjugated to antibodies or ligands to enhance target-specific drug therapy.

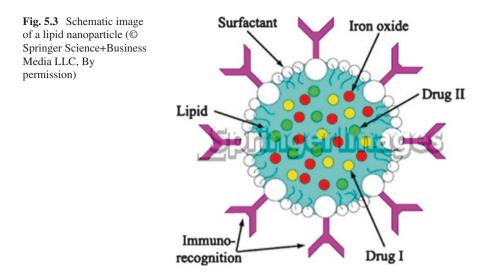
Stabilization of Phospholipid Liposomes Using Nanoparticles

A simple strategy of mixing phospholipid liposomes with charged nanoparticles and using sonication to mix them at low volume fraction produces particle-stabilized liposomes that repel one another and do not fuse. Subsequently, the volume fraction can be raised as high as 50%, reversibly, still without fusion. The nanoparticles adhere to the capsules and prevent further growth, freezing them at the desired size. The lipid concentration can then be increased without limits. As proof of concept, fluorescent dyes were encapsulated within lipid capsules. No leakage occurred, and the lipids proved stable against further fusion. Although these particle-stabilized liposomes were stable against fusion, 75% of the outer liposome surface remained unoccupied.

This opens the door to using particle-stabilized liposomes in various applications. The biocompatible containers could carry cargo such as enzymes, DNA, proteins and drug molecules throughout living organisms. They could also serve as surrogate factories where enzyme-catalyzed reactions are performed. By attaching biomolecules to the capsule's surface, novel colloidal-size sensors could be produced. An additional use for stabilized lipid capsules is the study of behavior of a drug contained in this nano environment.

Lipid Nanoparticles

Lipoparticles or lipid nanoparticles (LNPs) are nanometer-sized spheres surrounded by a lipid bilayer and embedded with conformationally intact integral membrane proteins. Nanoliposomes are made up of lipids that assemble on their own into spherical particles or liposomes. Interactions with integral membrane proteins have been particularly difficult to study because the proteins cannot be removed from the



lipid membrane of a cell without disrupting the structure and function of the protein. The ability to solubilize integral membrane proteins has applications for microfluidics, biosensors, high throughput screening, antibody development, and structural studies of complex receptors.

Various types of LNPs include solid lipid nanoparticles (SLNs), nanostrucured lipid carriers (NLCs), lipid-drug conjugates (LDCs), lipid nanospheres (LNSs) and lipid nanocapsules (LNCs). This technology differs from conventional liposome technology in that the lipids used contain polymerizable functional groups that are crosslinked when exposed to UV light. Therefore, the surface of the polymerized nanoparticle more closely resembles a nanosphere or a bead than a droplet of fat (liposome) and drugs/targeting agents can be attached. Schematic image of a lipid nanoparticle is shown in Fig. 5.3.

Advantages of the Lipid Nanoparticle Technology

Advantages of the LNP technology are:

- Unlike conventional bilayer liposomes, they do not randomly fuse with themselves or other membranes
- The surface character, in terms of charge and molecular makeup, is easily modified
- The spherical assemblies are easy to synthesize and very stable
- Multivalent presentation of small molecule ligands on nanoparticles offers vastly improved performance over the ligand alone.
- In addition to the multivalent attachment of ligands/antibodies to the surface, nanoparticles can carry a high payload of radiation, chemotherapeutic, or imaging agent to the target cell.

• Since the nanoparticle is larger than either antibodies or small molecule ligands, the complex does not quickly leak from the blood vessel. Therefore, the biodistribution and safety profile of the drug can be significantly improved.

Applications of Lipid Nanoparticles

The nanoparticle technology has broad therapeutic and diagnostic applications. The multivalent presentation of ligands or antibodies on nanoparticles makes this new class of drug ideally suited to treat diseases, which involve proliferation of blood vessels such as cancer, atherosclerosis, apoptosis, inflammation, rheumatoid arthritis, macular degeneration, unstable plaque, stroke, heart disease, and psoriasis. Acuitas Therapeutics is developing lipid nanoparticles for intracellular delivery of nucleic acids.

When LNPs are used in the treatment of cancer, their powerful targeting ability and potential for large cytotoxic payload dramatically enhance the efficacy of conventional pharmaceuticals as well as novel therapeutics such as gene therapy, radioimmunotherapy, and photodynamic therapy. Integrin-targeted nanoparticles can be used for site-specific delivery of a therapeutic payload by using an anticancer gene. These targeted nanoparticles can deliver radionuclides and chemotherapeutics to tumors. Further applications are discussed under drug delivery for cancer.

LNPs are useful for peptide and protein delivery due to the stabilizing effect of lipids and facilitation of absorption by the lipidic material. LNPs can protect nucleic acids from digestion in biological fluids and enter cells by endocytosis. LNPs can be used as adjuvants for vaccination by parenteral and mucosal routes with protein antigens or nucleic acids. Cationic SLNs are considered as alternative carriers for DNA delivery, due to many technological advantages such as large-scale production from substances generally recognized as safe and good storage stability. Success of cationic SLNs for administration of genetic material will depend on their ability to efficiently cross the physiological barriers, selectively targeting a specific cell type in vivo and expressing therapeutic genes (Bondi and Craparo 2010). LNPs could facilitate delivery of protein drugs to the brain across the BBB by overcoming P-gp efflux transporters.

Lipid Nanocapsules

Due to their small size, lipid nanocapsules (LNC) might be promising as an injectable as well as for an oral drug delivery system. LNC provides sufficient drug solubility to avoid embolization during intravenous injection and facilitates drug absorption after oral administration. Biocompatible ibuprofen LNC has been developed with a particle size of ~50 nm. Pain relief after intravenous administration of ibuprofen is prolonged by at least 2 h when administering LNC formulation. A drug delivery system for intravenous administration of ibuprofen is available, which exhibits sustained release properties by either oral or intravenous route and could be useful in the treatment of postoperative pain. LNCs can also be used as a transdermal drug delivery system as described later in this chapter.

Lipid Emulsions with Nanoparticles

An artificial lipoprotein-like particle, lipid nanosphere (LNS), is 25–50 nm in diameter and is composed of soybean oil and egg lecithin. Because of the lower uptake of LNS particles containing dexamethasone palmitate by the liver, LNS shows good recovery from the liver and prolonged the plasma half-life of after intravenous injection. In addition, higher antiinflammatory efficicacy of LNS is observed in targeting of dexamethasone palmitate into sites of inflammation. LNS easily and selectively pass through the leaky capillary wall by passive diffusion depending on the plasma concentration. LNS seems to be a promising carrier system for passive targeting of lipophilic drugs.

LNS has also been studied as a low-dose therapeutic system for amphotericin B (AmB), a potent antifungal drug. As a small-particle lipid emulsion, LNS is taken up by the liver to a lesser extent than a conventional lipid emulsion leading higher plasma concentrations of a radiochemical tracer than does the conventional lipid emulsion. LNS incorporating AmB (LNS-AmB) is a homogeneous emulsion with mean particle diameters ranging from 25 to 50 nm and yields higher plasma concentrations of AmB than Fungizone, a conventional intravenous dosage form of AmB, following intravenous administration in laboratory animals. This difference between LNS-AmB and Fungizone is also observed for constant intravenous infusion. In contrast to Fungizone, LNS-AmB shows a linear relationship between dose and are under the curve (AUC). These pharmacokinetic characteristics of LNS-AmB make it a suitable candidate for an effective low-dose therapeutic system for AmB.

Nanolipispheres are colloidal systems of drugs in a solid lipid matrix. These systems possess a sub-micron mean diameter and a uniform size distribution. A microemulsion-solidification process for manufacture produces a suspension of solid nanoparticles, which is then dried to obtain physically stable nanolipispheres in a powder form. Nanolipispheres provide for:

- · Carrier incorporation of lipophilic and hydrophilic drugs
- Oral delivery of macromolecules that can be absorbed as a whole or as fragments through the gastrointestinal tract
- Therapeutic efficacy of some drugs by preferential and consistent absorption and metabolism through the lymphatic system
- · Modified drug release

Nanotechnology has been applied to improve the absorption of CoQ10, a lipid-soluble compound found in the mitochondria of all living cells. It is a powerful antioxidant that is essential in the production of cellular energy and has been clinically shown to support healthy heart function, regulate blood pressure, increase energy and vitality, scavenge free radicals and enhance the immune system. Although endogenously produced in the liver, there are conditions in which adequate production of CoQ10 in the body is impaired. In such situations, supplementation of CoQ10 has been shown to be very beneficial. However, many currently available dosage forms of CoQ10 exhibit negligible dissolution properties indicating potentially poor bioavailability thereby limiting the therapeutic effect.

CoQ10 loaded PLGA nanoparticles, produced by a scalable emulsion-diffusionevaporation method and measuring <100 nm have been shown to significantly quench reactive oxygen species (ROS) with nearly 10-fold higher efficacy than free CoQ10 (Swarnakar et al. 2011). Further, positively charged CoQ10-NPs were localized in two major sources of ROS generation: mitochondria and lysosomes. CoQ10 nanoparticles showed improved oral bioavailability (4.28 times) as compared to free CoQ10. The higher antiinflammatory activity of CoQ10 nanoparticles is attributed to significant accumulation of these in the inflamed tissues.

Polymerized Liposomal Nanoparticle

Polymerized liposomal nanoparticle (PLN) is a nonviral nanoparticle incorporating a customizable drug delivery system for chemotherapeutic applications. PLNs are created using the self-assembling ability of a unique class of diacetylenic lipids that can be polymerized into stable, bimolecular membrane structures capable of delivering a drug payload. The PLN technology lends itself especially well to the display of multiple functions. These particles are comprised of individual lipid monomers part of which are functionalized for targeting, and may include additional moieties to control other physical properties such as surface charge, polarity, and fluidity. Different functionalized lipids can be rapidly mixed and matched in an infinite number of combinations and relative concentrations to create tailor-made particles with desirable targeting and circulation properties. The nanoparticles are non-immunogenic, display no acute toxicity and can be highly concentrated. Intracellular degradation and excretion rates of the particles can be modulated by controlling the degree of polymerization.

Solid Lipid Nanoparticles

Solid lipid nanoparticles (SLNs) have emerged as oral bioavailability enhancer vehicles for various drugs. Protective effect of SLNs, coupled with their sustained/ controlled release properties, prevents drugs/macromolecules from premature degradation and improves their stability in the gastrointestinal tract. Review of various publications reveals that direct oral administration of SLNs improves the bioavailability of drugs 2- to 25-fold (Harde et al. 2011).

Nanostructured Organogels

Organic gel nanomaterials can be used to encapsulate pharmaceutical, food and cosmetic products. Using olive oil and six other liquid solvents, a simple enzyme has been added to chemically activate a sugar that changes the liquids to organic gels, thus using building blocks provided by nature to create new nanomaterials that

are completely reversible and environmentally benign (John et al. 2006). In this study, researchers activated a sugar using a simple enzyme, which generated a compound that self-assembles into 3D fibers measuring approximately 50 nm in diameter. As the fibers entangle, a large amount of solvent gets packed together, trapping some 10,000 molecules.

Niosomes

A niosome is a non-ionic surfactant-based liposome. Niosomes, ranging in size from 300 to 500 nm, are formed mostly by incorporation of cholesterol as an excipiet but other excipients can also be used. They are structurally similar to liposomes in having a bilayer, however, the materials used to prepare niosomes make them more stable and thus they offer many more advantages over liposomes such as better penetrating capability. As drug delivery systems, niosomes have been used with anticancer drugs and for transdermal drug delivery.

Limitations of Liposomes for Drug Delivery

The use of liposomes may be limited because of problems related to stability, the inability to deliver to the right site, and the inability to release the drug when it gets to the right site. However, liposome surfaces can be readily modified by attaching polyethylene glycol (PEG)-units to the bilayer (producing what is known as stealth liposomes) to enhance their circulation time in the bloodstream.

Several attempts have been made to use liposomes, targeted by specific ligands, for the delivery of antithrombotic/thrombolytic agents to increase their efficacy and decrease side effects. Although liposomes loaded with various antithrombotic drugs have been the subject of a significant number of experimental studies, they are not considered as candidates for clinical application (Elbayoumi and Torchilin 2008).

Liposomes Incorporating Fullerenes

Buckysomes are a new generation of liposomes that incorporate fullerenes to deliver drugs that are not water-soluble, or tend to have large molecules, and are very hard to get into the body. Buckysomes appear to have much more flexibility in incorporating a wider range of drugs, as well as large molecule drugs, and delivering and releasing them more effectively. Buckysomes are being investigated for delivery of cancer therapeutics and anesthesia.

A study has examined the antioxidant activity of fullerene-C60 incorporated in liposome with a diameter of 75.6 nm, which was shown to have an antioxidant

action characterized by long-term persistence, and is attributed to fullerene-C60 but hardly to liposome in all the tests examined (Kato et al. 2011). The combination is expected to be effective as a skin-protecting agent against oxidative stress.

Arsonoliposomes

Arsonolipids, are analogs of phosphonolipids, in which P has been replaced by arsenic (As). Although arsonolipids possess interesting biophysical and biochemical properties their anticancer or antiparasitic activity is not considered adequate for therapeutic applications. But when arsonolipids are incorporated in liposomes, arsonoliposomes, show increased toxicity against cancer cells (compared to that of arsenic trioxide) but at the same time were less toxic than arsenic trioxide for normal cells. Furthermore, arsonoliposomes also demonstrate antiparasitic activity in vitro. Nevertheless, As arsonoliposomes are rapidly cleared from blood after in vivo administration, possible therapeutic applications will be limited. In addition, the fact that arsonoliposomes were observed to aggregate and subsequently fuse into larger particles in presence of cations, may also be considered as a problem. Thereby, methods to modulate the stability of arsonoliposomes and, perhaps, their in vivo distribution (as surface property modification) are currently being investigated. It has been shown that arsonoliposome PEGylation results in the formation of liposomes with very high membrane integrity. In addition, pegylation results in increased physical stability of arsonoliposomes and abolishment of cation-induced aggregation and fusion. Nevertheless, further in vivo studies are required to prove if PEGylation alters arsonoliposome in vivo kinetics in a positive way, without affecting their activity. Further development of arsonoliposomes to develop therapeutic systems for cancer or parasitic diseases is justified. Toxicity issues would need to be resolved

Liposome-Nanoparticle Hybrids

Small iron nanoparticles, quantum dots, liposomes, silica and polystyrene nanoparticles have been incorporated into liposomes for a variety of applications. Different techniques to achieve encapsulation of solid or semisolid nanoparticles within liposomes have been described. These offer improvements in nanoparticle aqueous solubilization and offer a viable platform (the liposome surface) for further bioconjugation. Moreover, these hybrids have increased survival time in blood circulation following systemic administration and accumulate at sites of leaky vasculature such as in tumors or inflammatory lesions providing opportunities for a combination of diagnostic imaging and therapeutics. Some examples of liposome-nanoparticle hybrids and their applications are shown in Table 5.4. Nanogels

Nanoparticle	Method of encapsulation	Rationale	Applications
Superparamagnetic iron oxide (SPIO) particles/ magnetite	Lipid film hydration and sonication	Cationic magnetoliposome provides selective intracellular hyperthermia and immune response induction	Cancer therapy
Quantum dots PEG-coated QD	QDs–liposome electrostatic complexation	High intracellular QD delivery	Intracellular trafficking
Phospholipid vesicles	Glass bead method	Preparation of double liposomes, which retard the drug release	Vaccines Drug delivery
Silicon-based nanoparticles	Adsorption and rupture of small unilamellar vesicle on nanoparticles surface forming a lipid monolayer or bilayer	Combining the intrinsic properties of silica and the bilayer	Design of biosensors
Polystyrene nanospheres	Adsorption and rupture of small unilamellar vesicle on nanoparticles surface forming a lipid monolayer or bilayer	Production of monodispersed and smooth bilayer nanosphere	Design of biosensors

Table 5.4 Liposome-nanoparticle hybrid systems

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Nanogels

Nanogels are colloidal microgel carriers, in which crosslinked protonated polymer network binds oppositely charged drug molecules, encapsulating them into nanoparticles with a core-shell structure. The nanogel network also provides a suitable template for chemical engineering, surface modification and vectorization.

Attempts are being made to develop novel drug formulations of nanogels with antiviral and antiproliferative nucleoside analogs in the active form of 5'-triphosphates. Notably, nanogels can improve the CNS penetration of nucleoside analogs that are otherwise restricted from passing through the blood-brain barrier. An efficient intracellular release of nucleoside analogs has been demonstrated, which encourages applications of nanogel carriers for targeted drug delivery.

Nanogel-Liposome Combination

An appropriate assemblage of spherical nanogel particles and liposomes, termed lipobead, combines the properties of both classes of materials and may find a variety of biomedical applications. Biocompatibility and stability, ability to deliver a broad

range of bioactive molecules, environmental responsiveness of both inner nanogel core and external lipid bilayer, and individual specificity of both compartments make the liposome-nanogel design a versatile drug delivery system relevant for all known drug administration routes and suitable for different diseases with possibility of efficient targeting to different organs. New developments in reversible and irreversible aggregation of lipobeads can lead to novel combined drug delivery systems regarding lipobeads as multipurpose containers.

Nanospheres

Hollow ceramic nanospheres (50–500 nm), created by using high-intensity ultrasound, were the first hollow nanocrystals that could be used in drug delivery. A hollow nanocrystal of molybdenum oxide is prepared using high intensity ultrasound to form a layer of amorphous material around a silica nanosphere. The nanosphere is then dissolved away with hydrofluoric acid and upon heating the shell crystallizes into a single hollow nanocrystal. TEM studies on the hollow ceramic materials indicate the formation of dispersed free spheres with a hollow core.

Nanotubes

Micro- and nanotubes or -structures that resemble tiny drinking straws are alternatives that might offer advantages over spherical nanoparticles for some applications. Tubular structure of nanoparticles is highly attractive due to their structural attributes, such as the distinctive inner and outer surfaces, over conventional spherical nanoparticles.

When a PEG-silane is attached to the silica nanotubes, adsorption of IgG immunoglobulins is strongly suppressed relative to nanotubes that do not contain the attached PEG. This has potential usefulness for the delivery of biopharmaceuticals. A payload can be incorporated into the nanotubes by either covalent bonding or other chemical interactions between the payload and the inside walls of the nanotubes. For some applications, it might be useful to fill the nanotubes with the payload and then to apply caps to the nanotubes to keep the payload encapsulated. Uncapping and release of payload can be triggered by a biochemical signal.

Inner voids of nanotubes can be used for capturing, concentrating, and releasing species ranging in size from large proteins to small molecules. Distinctive outer surfaces can be differentially functionalized with environment-friendly and/or probe molecules to a specific target. By combining the attractive tubular structure with magnetic property, the magnetic nanotube can be an ideal candidate for the multifunctional nanomaterial toward biomedical applications, such as targeting drug delivery with MRI capability. Magnetic silica-iron oxide composite nanotubes have been successfully synthesized and shown to be useful for magnetic-field-assisted chemical and biochemical separations, immunobinding, and drug delivery.

Carbon Nanotubes for Drug Delivery

Carbon nanotubes (CNTs) are ready-made, strong, electrically useful microscopic tubes that form naturally in soot from sheets of carbon atoms. Various proteins adsorb spontaneously on the sidewalls of CNTs enabling protein-nanotube conjugates. Proteins can be readily transported inside various mammalian cells via the endocytosis pathway with CNTs acting as the transporter. CNTs are useful for future in vitro and in vivo protein delivery applications. CNTs, used as liquid filled nanoparticles, act as absorption enhancers and improve the bioavailability of erythropoietin following administration into the small intestinal in experimental animals.

CNTs can pierce cell membranes like tiny needles without damaging the cell. If proteins or nucleic acids are attached to the nanotubes, they can also go right through the cell membrane. CNTs can also carry small pharmaceutical molecules such as antibiotics or cancer drugs directly into cells and have been successfully used to inject antifungal agents into cells. It is also possible to attach two agents to nanotubes enabling combination therapies or to trace the uptake of a drug by adding a marker.

CNTs can be formed into nanopipettes by tapering the diameter from 700 nm to only a few nanometers with central channels that could sense chemicals at very specific locations and eventually deliver tiny amounts of fluids under the skin. Dense arrays of nanopipettes could be used for drug delivery.

CNT-Liposome Conjugates for Drug Delivery into Cells

CNTs can be used as carriers for drug delivery due to their facile transport through cellular membranes. However, the amount of loaded drug on a CNT is rather small; therefore, liposomes are employed as a carrier of a large amount of drug. In a CNT-liposomes conjugate (CLC) drug delivery system, drug-loaded liposomes are covalently attached to CNT so that a high dose of the drug can be delivered into cells without potential adverse systemic effects when administered with CNTs without liposomes (Karchemski et al. 2012). This system is expected to provide versatile and controlled means for enhanced delivery of one or more agents that can be stably conjugated with liposomes.

Lipid-Protein Nanotubes for Drug Delivery

Nanotubes for drug or gene delivery applications can be developed with open or closed ends. The nanotubes could be designed to encapsulate and then open to deliver a drug or gene in a particular location in the body. This can be achieved by manipulating the electrical charges of lipid bilayer membranes and microtubules (MT) from cells. Synchrotron X-ray scattering and electron microscopy studies of self-assembly of cationic liposome-MT complexes shows that vesicles either adsorb

onto MTs, forming a "beads on a rod" structure, or undergo a wetting transition and coat the MT. Tubulin oligomers then coat the external lipid layer, forming a tunable lipid-protein nanotube. The beads on a rod structure are a kinetically trapped state. The energy barrier between the states depends on the membrane bending rigidity and charge density. The inner space of the nanotube in these experiments measures about 16 nm in diameter and the whole capsule is about 40 nm in diameter (Safinya et al. 2011). By controlling the cationic lipid/tubulin stoichiometry it is possible to switch between two states of nanotubes with either open ends or closed ends with lipid caps, a process that forms the basis for controlled chemical and drug encapsulation and release. Taxol is one type of drug that can be delivered with these nanotubes.

Halloysite Nanotubes for Drug Delivery

Halloysite is a natural clay material typically used in ceramics. Some clay reserves contain halloysite in the form of naturally occurring nanotubes that are approximately 10–100 nm in internal diameter and vary in length from a few hundred nanometers to several micrometers. Halloysite nanotubes can be loaded with drugs for sustained release, extending the effective life of drugs as they migrate out of the tubes over time. Once loaded, these tubes can also be encapsulated to further influence the rate of elution. This enables alteration of the drug release profile and extends the effectiveness of drugs without increasing potency. Compared to CNTs, halloysite nanotubes are far less expensive and have an extraordinarily large surface area. This feature promises significant advantages for drug delivery applications, since surface area contact allows for greater control of drug loading and elution profiles.

Loaded nanotubes can also be combined with other technologies for non-invasive activation. Nanotubes can be coated with nanomagnetic material that can subsequently be heated selectively and non-invasively using specific electromagnetic energy. Heating can thus provide elution on demand. The benefits of using naturally occurring halloysite material for specific drug delivery applications are: longer delivery times, more control of the drug release profile, and improved safety profiles. This technology can be applied to several product platforms, including transdermal drug delivery and drug-loaded wound care products. Transdermal delivery with halloysite nanotubes can enable a more controlled elution profile with several potential benefits:

- Eliminates the high initial delivery rate and improves the safety profile, particularly with drugs such as stimulants or hormones.
- More uniform delivery can result in better maintenance of the effective clinical dose.
- Less drug loading is required per patch. Since much of the drug is discarded when the patch is removed, this can lead to reduced costs.

Wound care products range from simple bandages to long-term treatments to promote healing and reduce the chances of infection and scarring. Drugs loaded into halloysite tubes and embedded into the base layer of a bandage can be released over an extended period of time. This increases the duration of drug effectiveness and reduces the frequency with which a bandage needs to be changed. This novel delivery form can provide new dosage formulations with several advantages:

- Linear release ensures maintenance of clinically effective doses.
- Compliance and ease of use; longer elution times mean fewer bandage changes.
- Uniformity of drug delivery: elution from halloysite

Nanocochleates

Cochleate, a lipid-based delivery system, is formed due to interaction between cations, e.g. Ca²⁺ and negatively charged phospholipids such as phosphatidylserine. Cochleates are stable precipitates with a unique structure consisting of a large, continuous, solid, lipid bilayer sheet rolled up in spiral, with no internal aqueous space. They are non-toxic and non-inflammatory and have been used as vehicles for oral and parenteral delivery of protein and peptide antigens.

Smart PharmaceuticalsTM (BioDelivery Sciences International, BDSI) are based on BioralTMTechnology, which uses nanocochleates and allows biopharmaceutical manufacturers to offer biologically-active compounds with unparalleled convenience, shelf-life, and reduced side effects. This drug delivery technology has been applied to generic, off-patent injectable drugs to make them patent-protected oral drugs. The company has developed food processing technology to encochleate sensitive and easily-degraded nutrients (beta carotene, anti-oxidants, and other) for addition to processed food and beverages. Nanoencochleation's all-natural process encochleates and preserves essential nutrients like anti-oxidants into a protected "shell" for in high-temperature/pressure canning and bottling applications.

Bioral® technology was used to encapsulate and deliver a siRNA therapeutic in a mouse model of influenza. The siRNA targets critical gene segments shared by avian influenza (H5N1). A single intranasal dose of encochleated siRNA administered 4 h after influenza exposure reduced virus titers in the lung by 200 times. It was 25 times more effective in reducing the virus than intravenous delivery as siRNA is destroyed rapidly when introduced into the blood directly.

Nanobiotechnology and Drug Delivery Devices

There is a need to improve devices introduced into the human body. Some drug delivery devices are implanted in the body for release of therapeutic substances. The lining of these devices can be improved by nanotechnology. For example, implants can be coated by nanolayers of polymers.

Nano-encapsulation

The NanocoatTM process (Nanotherapeutics Inc) is a patented, solvent-free encapsulation system for coating micron and sub-micron size powders. Adapted from commercial fluidization systems, a core nanoparticle/microparticle is excapsulated with a thin layer of a coating material, such as a surfactant or a biodegradable polymer. The coating may be applied to slow the rate of release of an active component, improve the dispersion/flow properties, or increase the absorption into the systemic circulation. The NanocoatTM process has been shown to provide a method of producing complete, or continuous, coated drug particles of high encapsulation efficiency while requiring minimal processing. The process also has several advantages over current techniques including:

- It is a fast process with run-times on the order of minutes.
- A variety of coating materials can be used, making it possible to produce films from materials with proven biocompatibility.
- It is a dry, solvent-free technique that can be conducted under a sterile cGMP conditions.
- Particle agglomeration/adhesion can be minimized by applying coatings that affect the bonding nature and electrostatic charge on the surface.

Formation of microcapsules by depositing coatings onto the nanoparticle surface will make it possible to control drug release kinetics by: (a) diffusion of the drug though a polymeric coating, (b) degradation of a biodegradable polymer coating on the drug particles, releasing the core drug material.

GeneSegues' nanocapsules are designed using a flexible formulation process and have the following characteristics:

- The drug is condensed to a small molecule <50 nm in diameter
- The drug is fully encapsulated in a stable, controlled-release capsule
- Ability to carry large or small molecules,
- Capsule coating can be made of ligands for receptor-mediated targeted delivery to different organs, tissues and cells
- Choices of route of administration include topical application, tablets, intravenous, or via devices.

Nanotechnology-Based Device for Insulin Delivery

One of the main aims of insulin therapy for diabetes is to appropriately mimic physiological insulin secretion levels and their correlation with glucose concentration in healthy individuals. A nanoscale device with channels and insulin monomers/dimers enclosed can sense the increase in glucose levels and release monomeric insulin through channels in the nanocapsule. Ideally, insulin dimers would be blocked from passage, which will provide physiologically relevant insulin monomers to bind to the insulin receptor. Upon return of glucose levels to basal levels, the channels will close and insulin passage is stopped. Developments in functionalized nanocontainers will enable glucose-sensitive receptacles to be engineered. Such devices could be used to provide new therapeutic approaches in insulin treatment.

Nanoporous Materials for Drug Delivery Devices

Nanoporous materials with ordered and controlled pore structures, high surface area and pore volume are particularly suited for implantable drug delivery systems. Considerable progress has been made in electrochemically engineered nanopores/ nanotube materials such as nanoporous alumina and nanotubular titanium (Losic and Simovic 2009). Nanoporous devices can be used for cell encapsulation in hormonal therapy. Biosensors mounted on these devices can be used for non-invasive signal detection.

Nanopore Membrane in Implantable Titanium Drug Delivery Device

Implanted titanium drug delivery devices using silicon nanopore membranes can control the release by diffusion of an encapsulated drug at a nearly constant rate. Nearly zero order drug kinetics can be achieved over long periods of time. Such nanodevices are suitable for the delivery of protein and peptide drugs and avoid the poor pharmacokinetics associated with injections, providing an optimized method of delivery for these compounds. The drug can be formulated as a dry powder or a concentrated suspension and maintains its stability. The drug is protected from the immunological reaction of the body by the nanopore membrane, which releases the drug but excludes entry of unwanted cells.

Measuring the Permeability of Nanomembranes

To design molecular transport systems effectively, one needs to know how big the pores in the vehicle's membranes are and how easily the contents can pass through them. This has proved quite difficult. A method for determining the permeability of thin films has been developed. A molecular beacon immobilized inside a porous silica particle that is subsequently encapsulated within a thin film can be used to determine the size of DNA that can permeate through the film. Using this technique, it has been determined that over 3 h, molecules larger than 4.7 nm do not permeate 15-nm thick polyelectrolyte multilayers and after 75 h molecules larger than 6 nm were excluded. This technique has applications for determining the permeability of films used for controlled drug and gene delivery. A molecular beacon made from single DNA strands has been used to measure how easily DNA or genes can pass through the wall of drug delivery particles.

The beacons used are single DNA strands which have a light-emitting molecule (a fluorophore) at one end and a quencher at the other. The DNA strand self assembles so that the two end segments pair up, forming a loop in the center – much like the shape of a round-bottomed flask. This is the closed molecular beacon. When the beacon is closed the fluorophore on one end of the DNA strand is close to the "quencher" on the other end, which stops the fluorophore from giving off light. To determine the permeability of the capsule, the molecular beacons are placed inside the delivery vehicle. If DNA passes through the capsule wall, the beacon opens and the fluorophore emits light. Therefore, when DNA passes through the capsule, the beacon remains switched 'on'. If no DNA passes through the capsule, the beacon remains switched off. This technique can be used in the design of intelligent drug delivery systems which can transport medicine to target locations and release the contents in a controlled way.

Nanovalves for Drug Delivery

A nano valve that can be opened and closed at will to trap and release molecules could be used as a drug delivery system. Such a nanovalve consists of moving parts – switchable rotaxane molecules that resemble linear motors – attached to a tiny piece of glass (porous silica), which measures about 500 nm. It is big enough to let molecules in and out, but small enough so that the switchable rotaxane molecules can block the hole. The valve is uniquely designed so one end attaches to the opening of the hole that will be blocked and unblocked, and the other end has the switchable rotaxanes whose movable component blocks the hole in the down position and leaves it open in the up position. The researchers used chemical energy involving a single electron as the power supply to open and shut the valve, and a luminescent molecule that allows them to tell from emitted light whether a molecule is trapped or has been released. The nano-valve is much smaller than living cells. A nano valve combined with biomolecules could be inserted into a cell and activated by light to release a drug inside a cell.

Switchable rotaxanes are molecules composed of a dumbbell component with two stations between which a ring component can be made to move back and forth in a linear fashion. Switchable rotaxanes have been used in molecular electronics and are now being adapted for use in the construction of artificial molecular machinery. Further research will test the size hole that can be blocked to see whether larger molecules such as enzymes can be transported inside the container.

Nanochips for Drug Delivery

MicroCHIPS Inc. (Bedford, MA) is working on a silver dollar-size device to implant under a patient's skin or in the abdomen that would provide tiny, precise doses of hormones, pain medication or other pharmaceuticals. The chips, made of silicon or polymer, feature hundreds of tiny micromachined wells that can be loaded with a mixture of medicines. A microcontroller could release small amounts of different chemicals on a customizable schedule. Or biosensors could trigger releases by detecting blood sugar levels or other biochemical conditions. If approved, such a device could provide diabetics with doses of insulin so that they could forgo daily injections for as much as a year. Or it could help liberate AIDS patients from following complicated daily regimens of multiple medications. To more closely imitate how the body releases hormones, the device could dispense compounds such as estrogen in periodic bursts.

Products currently in development include external and implantable microchips for the delivery of proteins, hormones, pain medications, and other pharmaceutical compounds. A clinical trial of an implantable microchip for delivery of human parathyroid hormone fragment (hPTH₁₋₃₄) has been conducted successfully in osteoporotic postmenopausal women. Potential advantages of these microchips include small size, low power consumption, absence of moving parts, and the ability to store and release multiple drugs or chemicals from a single device.

Nanobiotechnology-Based Transdermal Drug Delivery

Introduction

Transdermal drug delivery is an approach used to deliver drugs through the skin for therapeutic use as an alternative to oral, intravascular, subcutaneous and transmucosal routes. Technical details are described in a special report on transdermal drug delivery (Jain 2017). Nanoparticles and nano-emulsions have better skin penetration than larger particles.

There is experimental evidence for the potential of nanoparticles as delivery vectors for antigens and DNA for transdermal vaccination protocols. Fluorescent particles ranging in size and charge are applied to the surface of full thickness pig skin in a diffusion chamber and the receptor fluid is assayed to determine permeation. Fluorescence microscopy is used to visualize the skin after experiments. Only 50 and 500 nm particles that are negatively charged are able to permeate the skin, indicating that negative particles with sufficient charge may be ideal carriers for this purpose.

Delivering genes and drugs within cells with devices approaching the nanoscale allows for new levels of precision and minimal damage to cells. Nanopatches can be used to target immunologically sensitive cells for DNA vaccination of malaria and allergies. This technology will also enable pain-free and needle-free immunotherapy of asthma.

The focus in this section is on the use of transdermal route for systemic delivery of therapeutics. Use of nanobiotechnology to improve skin penetration of drugs used for treatment of skin disorders will be described separately later in this book.

Delivery of Nanostructured Drugs from Transdermal Patches

Nanobiotechnology has been applied for the painless transdermal delivery of vaccines, peptide hormones and other drugs. The patches are structured on the skin side with microprotrusions, which hold the drugs to be delivered. The protrusion face of the patch is applied to the skin where they cross the outer surface layer of the skin only reaching as far as the interstitial space avoiding nerves and blood vessels. In this interstitial space, the nanostructured drugs are released from the surface of the protrusions, and as the biocompatible polymer biodegrades the drugs are released continuously from the body of the protrusions. The nanostructured drugs are either taken up by the cells of the immune system (for vaccination applications) or flow through the interstitial fluid to other compartments in the body.

Effect of Mechanical Flexion on Penetration of Bucky Balls Through the Skin

Normally bucky amino clusters form spherical clusters that are up to 12 times larger than the width of the intercellular gaps in skin. In one study, confocal microscopy depicted dermal penetration of fullerene-substituted phenylalanine (Baa) derivative of a nuclear localization peptide at 8 h in skin flexed for 60 and 90 min, whereas Baa-Lys(FITC)-NLS, but did not penetrate the dermis of unflexed skin until 24 h (Rouse et al. 2007). Transmission electron microscopy analysis revealed fullerene-peptide localization within the intercellular spaces of the stratum granulosum. This study shows that repetitive movement can speed the passage of nanoparticles through the skin.

Ethosomes for Transdermal Drug Delivery

Ethosomes – soft, malleable vesicles with size ranging from 30 nm to a few microns – form the basis of ethosome delivery systems, which are significantly superior at delivering drugs through the skin in terms of both quantity and depth when compared to liposomes and to many commercial transdermal and dermal delivery systems. Visualization by dynamic light scattering showed that ethosomes could be unilamellar or multilamellar through to the core. These novel delivery systems contain soft phospholipid vesicles in the presence of high concentrations of ethanol. Ethosomal systems are sophisticated conceptually, but characterized by simplicity in their preparation, safety and efficiency – a rare combination that can expand their applications.

Because of their unique structure, ethosomes can encapsulate and deliver through the skin highly lipophilic molecules such as cannabinoids, testosterone, and minoxidil, as well as cationic drugs such as propranolol and trihexyphenidil. A study on abdominal skin of rats has shown that transdermal fluxes of aanticancer drug vinpocetine from ethosome gel are significantly higher than that of vinpocetine gel solution and vinpocetine aqueous solution (Mao et al. 2013). The study demonstrated that ethosome is a promising vesicular carrier for enhancing percutaneous absorption of vinpocetine. Results obtained in a double-blind two-armed randomized clinical study showed that treatment with the ethosomal acyclovir formulation significantly improved all the evaluated parameters.

Ethosomes penetrate cellular membrane releasing the entrapped molecule within cells. Studies focused on skin permeation behavior of fluorescently labeled bacitracin from ethosomal systems through human cadaver and rat skin demonstrated that the antibiotic peptide was delivered into deep skin layers through intercorneocyte lipid domain of stratum corneum. Ethosomal delivery systems could be considered for the treatment of several skin infections, requiring intracellular delivery of antibiotics, whereby the drug must bypass two barriers: the stratum corneum and the cell membrane. Ethosomal formulation of testosterone enhance testosterone systemic absorption and can be used for designing new products that could solve the drawbacks of current testosterone replacement therapies.

Advantages of Ethosomes over other transdermal delivery systems are:

- Enhanced permeation
- Platform for the delivery of large and diverse group of drugs including peptides and very lipophilic molecules.
- · Safe and approved components
- · Passive, non-invasive delivery system
- Available for immediate commercialization.
- High patient compliance
- High cost to benefit ratio

NanoCyte Transdermal Drug Delivery System

NanoCyte drug delivery system is based on a sophisticated injection system developed by the sea anemone during million years of evolution. Each microcapsule contains a coiled microscopic nanotube, which unfolds on activation – a process whereby high pressure of 200 atmospheres is developed within the microcapsule. The long thin nanotube evaginates out of the microcapsule and penetrates the skin at an acceleration of 40,000 g to deliver the drug efficiently in a fraction of a second into the epidermis skin layer. NanoCyte can be formulated as a suspension, lotion, cream or a stick. NanoCyte can also be activated after attaching to an adhesive patch. Advantages of this system include:

- · Immediate intradermal delivery
- Device-less active delivery
- Painless administration

- · Avoidance of large dosages and side effects
- Treatment of large skin areas
- · Multipoint penetration using nanoinjectors
- Ease of use

Safety Issues of Applications of Nanomaterial Carriers on the Skin

The European Commission has requested the Scientific Committee on Consumer Products (SCCP) in 2007 to prepare an opinion on "Safety of Nanomaterials in Cosmetic Products". The preliminary version of the opinion can be found online (http://ec.europa.eu/health/ph_risk/committees/04_sccp/docs/sccp_o_099.pdf). The results obtained with nanosized delivery systems were not consistent. The following list of potential properties was considered that are relevant to transdermal drug delivery:

- Nanomaterials constituents (such as lipids or surfactants) may act as penetration enhancers by penetrating individually into the stratum corneum (after particle disruption on skin surface) and subsequently altering the intercellular lipid lamellae within this skin layer.
- Nanomaterials may serve as a depot for sustained release of dermally active compounds.
- Nanomaterials may serve as a rate-limiting membrane barrier for the modulation of systemic absorption, hence providing a controlled transdermal delivery system.

Transdermal Administration of Lipid Nanocapsules

Due to their small size, lipid nanocapsules (LNC) are a promising as a drug delivery system – as injectable or an oral or by transdermal route. Biocompatible ibuprofen LNC has been developed with a particle size of ~50 nm. Pain relief after intravenous administration of ibuprofen is prolonged by at least 2 h when administering LNC formulation. LNCs can also be used as a transdermal drug delivery system using ibuprofen as a model drug. A comparison to other lipid nanocarriers such as solid lipid nanoparticles (SLN) and nanostructured lipid carriers (NLC) and polymeric nanocarriers has been made. Polymeric carriers had fourfold higher accumulation in the skin compared to that of the LNC and twice the accumulation of SLN and NLC (Abdel-Mottaleb et al. 2011). These results would suggest that the LNC can be considered as efficient as SLN and NLC for the transdermal drug delivery whereas polymeric nanoparticles are more suitable for localized drug delivery to the skin.

Transdermal Nanoparticle Preparations for Systemic Effect

Nanoparticles have been used to facilitate transdermal delivery of several systemic drugs. Some examples are as follows:

CaCO₃-nanoparticle system successfully delivered insulin transdermally, as evidenced by a significant sustained decrease in blood glucose in experiments on normal mice and those with diabetes. These results support the feasibility of developing transdermal nanoinsulin for human applications.

A multicenter, randomized, double-blind, placebo-controlled study showed that once-daily application of micellar nanoparticle estradiol emulsion was safe and effective in providing significant relief of vasomotor symptom frequency and severity in postmenopausal women. This is the basis of Estrasorb® (Novavax), a transdermal lotion containing estrogen for relief of menopausal symptoms, and Androsorb® (Novavax), a transdermal lotion containing androgen.

Indomethacin loaded poly n-butylcyanoacrylate nanocapsules can improve the transdermal delivery of indomethacin compared to a conventional gel formulation. This might be due to their ultra-fine particle size and their hydrophilic and hydrophobic surface characteristics.

Lipid nanoparticles have been used for transdermal delivery of flurbiprofen (Bhaskar et al. 2009). The bioavailability of flurbiprofen by oral administration was found to increase by 4.4 times when gel formulations were applied and sustained drug release was demonstrated over a period of 24 h in studies on experimental animals.

Celecoxib, a selective cyclo-oxygenase-2 inhibitor has been recommended orally for the treatment of arthritis and osteoarthritis. Long term oral administration of celecoxib produces serious gastrointestinal side effects. It is a highly lipophilic, poorly soluble drug with oral bioavailability of around 40% (capsule). The skin permeation mechanism and bioavailability of celecoxib by transdermally applied nanoemulsion formulation has been investigated (Shakeel et al. 2008). Optimized oil-in-water nanoemulsion of celecoxib was prepared by the aqueous phase titration method. Fourier transform infra-red spectra and differential scanning calorimeter thermogram of skin treated with nanoemulsion indicated that permeation occurred due to the disruption of epidermal lipid bilayers by nanoemulsion, which was demonstrated by photomicrograph of skin sample. The absorption of celecoxib through transdermally applied nanoemulsion gel resulted in approximately three-fold increase in bioavailability as compared to oral capsule formulation. Thus, nanoemulsions are potential vehicles for enhancement of skin permeation and bioavailability of poorly soluble drugs.

Nasal Drug Delivery Using Nanoparticles

The nasal cavity is an ideal site for delivery of both locally and systemically acting drugs. Topical administration includes agents for the treatment of nasal congestion, rhinitis, sinusitis and related allergic and other chronic conditions.

Various medications include corticosteroids, antihistaminics, anticholinergics and vasoconstrictors. The focus in recent years has been on the use of nasal route for systemic drug delivery. Intranasal route is considered for drugs which are ineffective orally, are used chronically, require small doses and where rapid entry into the circulation is desired. The rate of diffusion of the compounds through the nasal mucous membranes, like other biological membranes, is influenced by the physico-chemical properties of the compound. Impressive improvements in bioavailability have been achieved with a range of compounds.

Chitosan, a naturally occurring polysaccharide derived from chitin, is used as an absorption enhancer for transnasal drug delivery. Chitosan is bioadhesive and binds to the mucosal membrane, prolonging retention time of the formulation on the nasal mucosa. It may also facilitate absorption through promoting paracellular transport. The chitosan nasal technology can be exploited as solution, dry powders or nanoparticle formulations to further optimize the delivery system for individual compounds. For compounds requiring rapid onset of action, the nasal chitosan technology can provide a fast peak concentration compared with oral or subcutaneous administration. Density and size of PEG coating of poly(lactic acid)-poly(ethylene glycol) (PLA-PEG) nano- and microparticles has an important effect on their transport across the nasal mucosa. PLA-PEG particles with a high PEG coating density and a small size are more significantly transported than noncoated PLA nanoparticles or PLA-PEG nanoparticles with a lower coating density.

Nanoparticles made of low molecular weight chitosan are promising carriers for nasal vaccine delivery. Compacted DNA nanoparticles, encoding cystic fibrosis transmembrane regulator gene, can be safely administered by perfusion to the nose of cystic fibrosis subjects. A double-blind, dose escalation gene therapy trial with this technique showed evidence of vector gene transfer and partial correction of nasal potential difference that is typical for subjects with classic cystic fibrosis.

Mucosal Drug Delivery with Nanoparticles

The layers of mucus that protect sensitive tissue throughout can also prevent the entry of drugs into the body. The role of nanoparticles as drug delivery vehicles has been explored to overcome this hurdle. Cervicovaginal mucus was used for these investigations because its viscoelastic properties and mucin concentration are like those in many other human mucus secretions. Large nanoparticles, 500 and 200 nm in diameter, if coated with polyethylene glycol, diffused through mucus with an effective diffusion coefficient (Deff) only four and sixfold lower than that for the same particles in water (Lai et al. 2007). In contrast, for smaller but otherwise identical 100-nm coated particles, Deff was 200-fold lower in mucus than in water. For uncoated particles 100–500 nm in diameter, Deff was 2400- to 40,000-fold lower in mucus than in water. Much larger fractions of the 100-nm particles were immobilized or otherwise hindered by mucus than the large 200- to 500-nm particles. Thus, in contrast to the

prevailing belief, these results demonstrate that large nanoparticles, if properly coated, can rapidly penetrate physiological human mucus, and they offer the prospect that large nanoparticles can be used for mucosal drug delivery.

Future Prospects of Nanotechnology-Based Drug Delivery

A desirable situation in drug delivery is to have smart drug delivery systems that can integrate with the human body. This is an area where nanotechnology will play an extremely important role. Even time-release tablets, which have a relatively simple coating that dissolves in specific locations, involve the use of nanoparticles. Pharmaceutical companies are already involved in using nanotechnology to create intelligent drug release devices. For example, control of the interface between the drug/particle and the human body can be programmed so that when the drug release its target, it can then become active. The use of nanotechnology for drug release devices requires autonomous device operation. For example, in contrast to converting a biochemical signal into a mechanical signal and being able to control and communicate with the device, autonomous device operation would require biochemical recognition to generate forces to stimulate various valves and channels in the drug delivery systems, so that it does not require any external control.

Subcellular or organelle-specific targeting has emerged as a new frontier in drug delivery. Nanocarriers will create the next generation of 'magic bullets' that are capable of delivering a drug payload to a molecular target at a subcellular location (D'Souza and Weissig 2009). It is now seems that we are on the verge of bioengineering molecular motors for specialized applications on nanoscale. These systems might be the key to yet unsolved biomedical applications that include nonviral gene therapy and interneuron drug delivery. Examples of some potential nanotechnology-based drug delivery systems are given in the following paragraphs.

Nanomolecular Valves for Controlled Drug Release

A macroscopic valve is a device with a movable control element that regulates the flow of gases or liquids by blocking and opening passageways. Construction of such a device on the nanoscale level requires (i) suitably proportioned movable control elements, (ii) a method for operating them on demand, and (iii) appropriately sized passageways. These three conditions can be fulfilled by attaching organic, mechanically interlocked, linear motor molecules that can be operated under chemical, electrical, or optical stimuli to stable inorganic porous frameworks (i.e. by self-assembling organic machinery on top of an inorganic chassis). A reversibly operating nanovalve has been demonstrated that can be turned on and off by redox chemistry. It traps and releases molecules from a maze of nanoscopic passageways in silica by controlling

the operation of redox-activated bistable rotaxane molecules tethered to the openings of nanopores leading out of a nanoscale reservoir. Future applications could include nanofluidic systems and the controlled release of drugs from implants with nanoscopic properties.

Nanosponge for Drug Delivery

Nanosponges are hyper-cross-linked cyclodextrin polymers nanostructured to form 3D networks and are obtained by complexing cyclodextrin with a cross-linker such as carbonyldiimidazole. They have been used to increase the solubility and stability of poorly soluble drugs. β -cyclodextrin nanosponges loaded with anticancer agent tamoxifen have been used for oral drug delivery (Torne et al. 2013). In experimental studies, tamoxifen nanosponge complex with particle size of 400–600 nm was shown to be more cytotoxic than plain tamoxifen after 24 and 48 h of incubation.

Another method for making a nanosponge uses extensive internal cross-linking to scrunch a long, linear molecule into a sphere about 10 nm in diameter. Instead of trying to encapsulate drugs in nanoscale containers, this approach creates a nanoparticle with numerous surface sites where drug molecules can be attached. A molecular transporter attached to the nanosponge can carry it and its cargo across biological barriers into specific intracellular compartments. The transporter can deliver large molecules – specifically peptides and proteins – into specific subcellular locations. A targeting unit attached to this delivery system can deliver drugs to the surface of tumors in the lungs, brain and spinal cord. This delivery system can be adapted to carry the chemotherapy agents for targeted delivery to tumors.

Nanomotors for Drug Delivery

Basics of nanomotors – nanometer-scale machines, which are powered by chemical reactions – have been described in Chap. 3 as molecular motors. A technique to create catalytic nanomotors uses "dynamic shadowing growth", which involves a simple modification of existing methods to allow for greater flexibility in designing desired nanomotor structures (He et al. 2007). These could be used as tools to open constricted or clogged blood vessels too small for conventional stents, or they could deliver drugs by drilling through the cell wall of an organism. The researchers looked at the hundreds of moving parts in an automobile for designing each part of a nanomotor to achieve a controlled, flexible range of motion for the parts to work together. After successfully using the new technique to design nanorods to rotate, they broke the symmetry of the rods to form L-shaped rods which could then be aggregated to form larger particles. Then they transformed the rod into a spiral shape so that its rotation would mimic the turning of a drill. The team used the new technique to deposit a platinum or silver catalyst on different portions of the L-shaped rods, and then designed different experiments to test their ability to control

the motion. In a solution of hydrogen peroxide, they captured images of the nanorods turning precisely in the directions proscribed by the catalyst depositions.

Magnetically guided ultrasound-powered nanowire motors, functionalized with bioreceptors and a drug-loaded polymeric segment, have been described for "capture and transport" and drug-delivery processes (Garcia-Gradilla et al. 2013). These highperformance fuel-free motors display advanced capabilities and functionalities, including magnetic guidance, coordinated aligned movement, cargo towing, capture and isolation of biological targets, drug delivery, and operation in real-life biological and environmental media. The template-prepared 3-segment Au-Ni-Au nanowire motors are propelled acoustically by mechanical waves produced by a piezoelectric transducer. An embedded nickel segment facilitates a magnetically guided motion as well as transport of large "cargo" along predetermined trajectories. Substantial improvement in the speed and power is realized by the controlled concavity formation at the end of the motor nanowire using a sphere lithography protocol. Functionalization of the Au segments with lectin and antiprotein A antibody bioreceptors allows capture and transport of E. coli and S. aureus bacteria, respectively. Examples of potential therapeutic applications include those in connection to the addition of a pH-sensitive drug-loaded polymeric segment. The attractive capabilities of these fuel-free acoustically driven functionalized Au-Ni-Au nanowires, along with the simple preparation procedure and minimal adverse effects of ultrasonic waves, make them highly attractive for diverse in vivo biomedical applications.

References

- Abdel-Mottaleb MM, Neumann D, Lamprecht A. Lipid nanocapsules for dermal application: a comparative study of lipid-based versus polymer-based nanocarriers. Eur J Pharm Biopharm. 2011;79:36–42.
- Agüeros M, Espuelas S, Esparza I, et al. Cyclodextrin-poly(anhydride) nanoparticles as new vehicles for oral drug delivery. Expert Opin Drug Deliv. 2011;8:721–34.
- Akin D, Sturgis J, Ragheb K, et al. Bacteria-mediated delivery of nanoparticles and cargo into cells. Nat Nanotechnol. 2007;2:441–4.
- Bawa R, Fung SY, Shiozaki A, et al. Self-assembling peptide-based nanoparticles enhance cellular delivery of the hydrophobic anticancer drug ellipticine through caveolae-dependent endocytosis. Nanomedicine. 2012;8:647–54.
- Bhaskar K, Anbu J, Ravichandiran V, et al. Lipid nanoparticles for transdermal delivery of flurbiprofen: formulation, in vitro, ex vivo and in vivo studies. Lipids Health Dis. 2009;8:6.
- Bondi ML, Craparo EF. Solid lipid nanoparticles for applications in gene therapy: a review of the state of the art. Expert Opin Drug Deliv. 2010;7:7–18.
- Brudno Y, Silva EA, Kearney CJ, et al. Refilling drug delivery depots through the blood. Proc Natl Acad Sci U S A. 2014;111:12722–7.
- Chansin GA, Mulero R, Hong J, et al. Single molecule spectroscopy using nanoporous membranes. Nano Lett. 2007;7:2901–6.
- Choi SJ, Oh JM, Choy JH. Safety aspect of inorganic layered nanoparticles: size-dependency in vitro and in vivo. J Nanosci Nanotechnol. 2008;8:5297–301.
- Crielaard BJ, Rijcken CJ, Quan L, et al. Glucocorticoid-loaded core-cross-linked polymeric micelles with tailorable release kinetics for targeted therapy of rheumatoid arthritis. Angew Chem Int Ed Engl. 2012;51:7254–8.

- Dobrovolskaia MA, Patri AK, Zheng J, et al. Interaction of colloidal gold nanoparticles with human blood: effects on particle size and analysis of plasma protein binding profiles. Nanomedicine. 2009;5:106–17.
- D'Souza GG, Weissig V. Subcellular targeting: a new frontier for drug-loaded pharmaceutical nanocarriers and the concept of the magic bullet. Expert Opin Drug Deliv. 2009;6:1135–48.
- Duceppe N, Tabrizian M. Advances in using chitosan-based nanoparticles for in vitro and in vivo drug and gene delivery. Expert Opin Drug Deliv. 2010;7:1191–207.
- Elbayoumi TA, Torchilin V. Liposomes for targeted delivery of antithrombotic drugs. Expert Opin Drug Deliv. 2008;5:1185–98.
- Eliasof S, Lazarus D, Peters CG, et al. Correlating preclinical animal studies and human clinical trials of a multifunctional, polymeric nanoparticle. Proc Natl Acad Sci U S A. 2013;110:15127–32.
- Fang RH, Hu CM, Zhang L. Nanoparticles disguised as red blood cells to evade the immune system. Expert Opin Biol Ther. 2012;12:385–9.
- Fichter KM, Flajolet M, Greengard P, Vu TQ. Kinetics of G-protein–coupled receptor endosomal trafficking pathways revealed by single quantum dots. Proc Natl Acad Sci U S A. 2010;107:18658–63.
- Garcia-Gradilla V, Orozco J, Sattayasamitsathit S, et al. Functionalized ultrasound-propelled magnetically guided nanomotors: toward practical biomedical applications. ACS Nano. 2013;7:9232–40.
- Gassman NR, Nelli JP, Dutta S, et al. Selection of bead-displayed, PNA-encoded chemicals. J Mol Recognit. 2010;23:414–22.
- Geng Y, Dalhaimer P, Cai S, et al. Shape effects of filaments versus spherical particles in flow and drug delivery. Nat Nanotechnol. 2007;2:249–55.
- Harde H, Das M, Jain S. Solid lipid nanoparticles: an oral bioavailability enhancer vehicle. Expert Opin Drug Deliv. 2011;8:1407–24.
- He Y, Wu J, Zhao Y. Designing catalytic nanomotors by dynamic shadowing growth. Nano Lett. 2007;7:1369–75.
- Hild W, Pollinger K, Caporale A, et al. G protein-coupled receptors function as logic gates for nanoparticle binding and cell uptake. Proc Natl Acad Sci U S A. 2010;107:10667–72.
- Hoare T, Santamaria J, Goya GF, et al. A magnetically triggered composite membrane for ondemand drug delivery. Nano Lett. 2009;9:3651–7.
- Hong J, Edel JB, deMello AJ. Micro- and nanofluidic systems for high-throughput biological screening. Drug Discov Today. 2009;14:134–46.
- Hu Q, van Gaal EV, Brundel P, et al. A novel approach for the intravenous delivery of leuprolide using core-cross-linked polymeric micelles. J Control Release. 2015;205:98–108.
- Jain KK. The role of nanobiotechnology in drug discovery. Drug Discov Today. 2005;10:1435–42.
- Jain KK. Transdermal drug delivery: technologies, markets and companies. Basel: Jain PharmaBiotech Publications; 2017.
- John G, Zhu G, Li J, Dordick JS. Enzymatically derived sugar-containing self-assembled organogels with nanostructured morphologies. Angew Chem Int Ed Engl. 2006;45:4772–5.
- Karchemski F, Zucker D, Barenholz Y, Regev O. Carbon nanotubes-liposomes conjugate as a platform for drug delivery into cells. J Control Release. 2012;160:339–45.
- Kato S, Aoshima H, Saitoh Y, Miwa N. Fullerene-C60 incorporated in liposome exerts persistent hydroxyl radical-scavenging activity and cytoprotection in UVA/B-irradiated keratinocytes. J Nanosci Nanotechnol. 2011;11:3814–23.
- Kojima C. Design of stimuli-responsive dendrimers. Expert Opin Drug Deliv. 2010;7:307–19.
- Kottke PA, Degertekin FL, Fedorov AG. Scanning mass spectrometry probe: a scanning probe electrospray ion source for imaging mass spectrometry of submerged interfaces and transient events in solution. Anal Chem. 2010;82:19–22.
- Ladewig K, Xu ZP, Lu GQ. Layered double hydroxide nanoparticles in gene and drug delivery. Expert Opin Drug Deliv. 2009;6:907–22.
- Lai SK, O'hanlon DE, Harrold S, et al. Rapid transport of large polymeric nanoparticles in fresh undiluted human mucus. Proc Natl Acad Sci U S A. 2007;104:1482–7.

- Lam R, Ho D. Nanodiamonds as vehicles for systemic and localized drug delivery. Expert Opin Drug Deliv. 2009;6:883–95.
- Losic D, Simovic S. Self-ordered nanopore and nanotube platforms for drug delivery applications. Expert Opin Drug Deliv. 2009;6:1363–81.
- Mao YT, Hua HY, Zhang XG, et al. Ethosomes as delivery system for transdermal administration of vinpocetine. Pharmazie. 2013;68:381–2.
- Paleos CM, Tsiourvas D, Sideratou Z, Tziveleka LA. Drug delivery using multifunctional dendrimers and hyperbranched polymers. Expert Opin Drug Deliv. 2010;7:1387–98.
- Papasani MR, Wang G, Hill RA. Gold nanoparticles: the importance of physiological principles to devise strategies for targeted drug delivery. Nanomedicine. 2012;8:804–14.
- Patel VR, Agrawal YK. Nanosuspension: an approach to enhance solubility of drugs. J Adv Pharm Technol Res. 2011;2:81–7.
- Rouse JG, Yang J, Ryman-Rasmussen JP, et al. Effects of mechanical flexion on the penetration of fullerene amino acid-derivatized peptide nanoparticles through skin. Nano Lett. 2007;7:155–60.
- Safinya CR, Raviv U, Needleman DJ, et al. Nanoscale assembly in biological systems: from neuronal cytoskeletal proteins to curvature stabilizing lipids. Adv Mater. 2011;23:2260–70.
- Salmaso S, Caliceti P. Self assembling nanocomposites for protein delivery: supramolecular interactions of soluble polymers with protein drugs. Int J Pharm. 2013;440:111–23.
- Shakeel F, Baboota S, Ahuja A, et al. Skin permeation mechanism and bioavailability enhancement of celecoxib from transdermally applied nanoemulsion. J Nanobiotechnology. 2008;6:8.
- Shimkunas RA, Robinson E, Lam R, et al. Nanodiamond-insulin complexes as pH-dependent protein delivery vehicles. Biomaterials. 2009;30:5720–8.
- Siegwart DJ, Whitehead KA, Nuhn L, et al. Combinatorial synthesis of chemically diverse core-shell nanoparticles for intracellular delivery. Proc Natl Acad Sci U S A. 2011;108:12996–3001.
- Spyratou E, Mourelatou EA, Makropoulou M. Atomic force microscopy: a tool to study the structure, dynamics and stability of liposomal drug delivery systems. Expert Opin Drug Deliv. 2009;6:305–7.
- Steeland S, Vandenbroucke RE, Libert C. Nanobodies as therapeutics: big opportunities for small antibodies. Drug Discov Today. 2016;21:1076–113.
- Suri GS, Kaur A, Sen T. A recent trend of drug-nanoparticles in suspension for the application in drug delivery. Nanomedicine (Lond). 2016;11:2861–76.
- Swarnakar NK, Jain AK, Singh RP, et al. Oral bioavailability, therapeutic efficacy and reactive oxygen species scavenging properties of coenzyme Q10-loaded polymeric nanoparticles. Biomaterials. 2011;32:6860–74.
- Tang BC, Dawson M, Lai SK, et al. Biodegradable polymer nanoparticles that rapidly penetrate the human mucus barrier. Proc Natl Acad Sci U S A. 2009;106:19268–73.
- Tang BC, Fu J, Watkins DN, Hanes J. Enhanced efficacy of local etoposide delivery by poly(etheranhydride) particles against small cell lung cancer in vivo. Biomaterials. 2010;31:339–44.
- Torne S, Darandale S, Vavia P, et al. Cyclodextrin-based nanosponges: effective nanocarrier for Tamoxifen delivery. Pharm Dev Technol. 2013;18:619–25.
- Vaijayanthimala V, Lee DK, Kim SV, et al. Nanodiamond-mediated drug delivery and imaging: challenges and opportunities. Expert Opin Drug Deliv. 2015;12:735–49.
- Van Bockstaele F, Holz JB, Revets H. The development of nanobodies for therapeutic applications. Curr Opin Investig Drugs. 2009;10:1212–24.
- Vázquez E, Villaverde A. Microbial biofabrication for nanomedicine: biomaterials, nanoparticles and beyond. Nanomedicine. 2013;8:1895–8.
- Walrant A, Bechara C, Alves ID, Sagan S. Molecular partners for nanomedicine interaction and cell internalization of cell-penetrating peptides: how identical are they? Nanomedicine. 2012;7:133–43.
- Xing Y, Dai L. Nanodiamonds for nanomedicine. Nanomedicine (Lond). 2009;4:207-18.
- Yao L, Zhao X, Li Q, et al. In vitro and in vivo evaluation of camptothecin nanosuspension: a novel formulation with high antitumor efficacy and low toxicity. Int J Pharm. 2012;423:586–8.

Chapter 6 Role of Nanotechnology in Biological Therapies

Introduction

Biological therapies are playing an increasing role in modern medicine. This term includes recombinant human proteins, monoclonal antibodies (MAbs), vaccines, cell therapy, gene therapy, antisense and RNA interference (RNAi). Some technologies for cell and gene therapy are in themselves sophisticated methods of therapeutic delivery whereas others require special methods of delivery. Role of nanobiotechnology in delivery of biologicals will be discussed in this chapter. MAbs are considered along with drug delivery for cancer in Chap. 7.

Nanotechnology for Delivery of Proteins and Peptides

Industrial production of therapeutic peptides and proteins is now possible, but delivery of these molecules by the oral route, which is the most desirable route, remains a challenge. Injection has been the traditional method of administration of most peptides and proteins for systemic effect. Orally ingested proteins are rapidly converted to constituent amino acids before absorption. The aim is absorption of proteins and peptides in an intact state. Three main obstacles to oral delivery of proteins are:

- 1. Destruction of proteins by acid and proteolytic enzymes in the stomach
- 2. Difficulties of transporting molecules across the epithelial layer lining the intestine
- 3. Bioavailability is low

Nanotechnology-based methods have been explored for oral delivery of proteins. Advantages of delivery systems based on nanoparticles and cyclodextrins (CDs) are the protection of proteins from degradation, enhancement of absorption, targeting and controlling the release of the drug. Physicochemical characteristics of nanoparticles influence the ability to successfully entrap the intended drug. Biodistribution and safety issues need also to be considered once material from the delivery system is absorbed by the body and thus interacts with biological components. Microemulsions with flexible formulations have been used for the solubilization of peptides and proteins to design encapsulation processes for oral delivery of insulin nanoparticles 320–350 nm in size (Graf et al. 2008).

Nanobiotechnology for Vaccine Delivery

Nanomaterials are desirable vehicles for vaccine delivery via oral, mucosal, subcutaneous and transdermal. Advantages of nanoparticles-based vaccine delivery are stability, controlled delivery, enhanced vaccine uptake, reduction of vaccine dose, and co-delivery of antigen and adjuvant. Nanoparticle-based vaccines, so-called nanovaccines, enhance innate as well as adaptive immunity because nanoparticles are in the same size range as many pathogeneic organisms such as viruses (Seth et al. 2015). Polymeric nanoparticles such as PLGA (poly lactic-co-glycolic acid) and chitosan as well as metal nanoparticles such as gold have been used in nanovaccines. Virus-like particles (VLPs) are noninfectious viruses without genetic material. Nanoemulsions such as incomplete Fruend's adjuvant and nanobeads are used to enhance immunity.

Bacterial Spores for Delivery of Vaccines

Bacterial spores as described in Chap. 2 can be used for vaccine delivery. The spore coat can act as a vehicle for heterologous antigen presentation and protective immunization. Use of bacterial spores will solve the problem of stability and transport in the developing countries as they do not require refrigeration and the administration is needle free.

Dendrimer-RNA Nanoparticle Vaccines

Vaccines have had broad medical impact, but existing vaccine technologies and production methods are limited in their ability to respond rapidly to evolving and emerging pathogens, or sudden outbreaks. A rapid-response, fully synthetic, single-dose, adjuvant-free dendrimer nanoparticle vaccine platform has been developed wherein antigens are encoded by encapsulated mRNA replicons (Chahal et al. 2016). This is the first system capable of generating protective immunity against a broad spectrum of lethal pathogen challenges, including H1N1 influenza, *Toxoplasma gondii*, and Ebola virus. The vaccine can be formed with multiple

antigen-expressing replicons, and is capable of eliciting both CD8+ T-cell and antibody responses. This technology may enable rapid-response vaccines with broad efficacy that reduce the number and frequency of vaccinations, and healthcare worker burden.

Lipid Nanoparticles for Immunostimulatory RNA Delivery

Specific activation of Toll-like receptors (TLRs) is potentially useful for a variety of therapeutic indications including antiviral immunotherapy and as vaccine adjuvants. TLR7 and TLR 8 may be activated by their native ligands, ssRNA, or by small molecules of the imidazoquinoline family. However, the use of TLR7/8 agonists for in vivo therapy is limited by instability, in the case of RNA, or systemic biodistribution and toxicity in the case of small molecule agonists. Use of lipid-like materials, termed "lipidoids," has been explored to efficiently deliver immunostimulatory RNA (isRNA) to TLR-expressing cells to drive innate and adaptive immune responses (Nguyen et al. 2012). Lipidoid-isRNA nanoparticles, when tested in mice, stimulated strong IFN-α responses following subcutaneous injection, had robust antiviral activity that suppressed influenza virus replication. Certain materials were found to engage both TLR7-dependent and TLR7-independent activity in the mouse suggestive of cell-specific delivery. These lipidoid formulations, which are materials designed specifically for delivery of isRNA to TLRs, were superior to the commonly used N-[1-(2,3-dioleoyloxy)propyl]-N,N,Ntrimethylammonium methylsulfate-RNA delivery system and may provide new tools for the manipulation of TLR responses in vitro and in vivo.

Nanoparticles for DNA Vaccines

DNA vaccines, also referred to as genetic vaccines, are generating significant preclinical and clinical interest. It has been proven that the expression of an antigen or antigens from plasmid DNA (pDNA) may elicit both humoral and cellular immune responses. Therefore, DNA vaccines may have potential as new vaccines for important pathogens such as HIV, hepatitis C, tuberculosis, and malaria.

However, DNA vaccine delivery is not satisfactory. Relatively high doses of plasmid DNA (pDNA) are needed to elicit a response. The clinical results using "naked" pDNA have been disappointing in the breadth and depth of the immune response. Clinical trials with the gene gun have been promising, but it is unclear whether this technology will be commercially viable. Therefore, there is a need for new vaccine delivery systems that can be administered at low doses to elicit strong humoral and cellular immune responses. One promising approach is the development of microparticles and nanoparticles as delivery systems for DNA vaccines. Nanoemulsions or nanoparticle aerosol vaccines are also in development.

Nanoparticle-Based Adjuvants for Vaccines

For subunit vaccines, adjuvants play a key role in shaping immunological memory. NP delivery systems for antigens are promising adjuvants capable of promoting both cellular and humoral immune responses, but in most cases the mechanisms of action of these materials are poorly understood. A report has documented the immune response elicited by NPs composed of multilamellar "stapled" lipid vesicles carrying a recombinant Plasmodium vivax circumsporozoite antigen, VMP001, both entrapped in the aqueous core and anchored to the lipid bilayer surfaces (Moon et al. 2012). Immunization with NPs and monophosphoryl lipid A (MPLA), a FDAapproved immunostimulatory agonist for Toll-like receptor-4, promoted high-titer, high-avidity antibody responses against VMP001, lasting >1 y in mice at tenfold lower doses than conventional adjuvants. NPs promoted robust germinal center (GC) formation at low doses of antigen where no GC induction occurred with soluble protein immunization, and GCs nucleated near depots of NPs accumulating in the draining lymph nodes over time. In parallel, NP vaccination enhanced the expansion of antigen-specific follicular helper T cells, compared to vaccinations with soluble VMP001 or alum. Thus, NP vaccines may be a promising strategy to enhance the durability, breadth, and potency of humoral immunity by enhancing key elements of the B-cell response.

Although several adjuvants are currently approved for use in veterinary species, only alum has been widely used in humans. Although it induces strong antibody responses, cell mediated responses are often low and inflammatory reactions at the site of injection are common. In contrast to alum, antigen covalently coupled to nanobeads induces substantial cell-mediated responses along with moderate humoral responses. No adverse reactions were seen at the site of immunization in experimental animals. Thus, nanobead adjuvants may be useful for the induction of immunity to viral pathogens, in veterinary practice where a cell-mediated response is required. These observations also highlight the potential usefulness of nanobead vaccines for intracellular pathogens in humans. Most adjuvants only stimulate antibodies against a disease. The nanobead technology gives the immune system a further boost by producing T cells, which are needed to eliminate viruses or cancer. Nanobeads measure ~40 nm and this size is critical as it is similar to that of many viruses enabling abundant uptake by the immune system, which is tricked into producing high levels of many types of T cells.

Agonists of Toll-like receptors (TLRs) are potent activators of the innate immune system and hold promise as vaccine adjuvant and for anticancer immunotherapy. Unfortunately, in soluble form they readily enter systemic circulation and cause systemic inflammatory toxicity. A study has demonstrated that by covalent ligation of a small-molecule imidazoquinoline-based TLR7/8 agonist to 50 nm-sized degradable polymeric nanogels the potency of the agonist to activate TLR7/8 in in vitro cultured dendritic cells is largely retained (Nuhn et al. 2016). Importantly, imidazoquinoline-ligated nanogels focus the in vivo immune activation on the draining lymph nodes while dramatically reducing systemic inflammation.

Moreover, immunization studies in mice have shown that relative to soluble TLR7/8 agonist, imidazoquinoline-ligated nanogels induce superior antibody and T cell responses against a tuberculosis antigen. Nanoparticle ligation yields increased immune activation in the draining lymph nodes and results in strongly increased antibody titers and T cell responses against an admixed vaccine antigen. This approach opens up the possibilities of enhancing the therapeutic benefit of small-molecule TLR agonist for a variety of applications.

Nanospheres for Controlled Release of Viral Antigens

Aphios Corporation has developed an enhanced controlled release technology for nanoencapsulating potent viral antigens in biodegradable polymer nanospheres by utilizing SuperFluids, which are supercritical, critical or near-critical fluids with or without polar cosolvents. The use of SuperFluids reduces exposure of viral antigens such as HIV and influenza to potentially denaturing organic solvents such as methylene chloride and ethyl acetate, and improves the stability of protein antigens in the body at ambient temperature for long periods, thereby enhancing the capability of nanoencapsulated vaccine antigens to induce the production of protective and neutralizing antibodies. This controlled release vaccine delivery technology has the capability to deliver different types and combinations of HIV or influenza vaccine candidates including whole inactivated virus particles, DNA plasmids and/or subunit protein antigens. SuperFluids polymer nanoencapsulation technology will reduce cost by eliminating unnecessary processing steps while improving the manufacturing environment. Unlike currently available technologies, this technology is portable, inexpensive, and amenable to large-scale processing.

Nanotechnology for Oral Vaccines

Nanomaterials can protect biomolecules by encapsulating them and protecting them against the detrimental effects of pH and enzymes when administered orally. The oral nanoparticle vaccines can elicit localized immune response in colon by coating them with specific combination of pH responsive polymer Eudragit® (Evonik Industries). DNA molecules can also be successfully administered orally using nanoparticles. Orally administered chitosan nanoparticle encapsulating DNA for a food allergen can induce production of secretory IgA and serum IgG that can provide prophylaxis against food allergy. Nanoparticles aid in enhancement of uptake of antigen by the M cells in Payer's patch and gut associated lymphoid tissue and thereby contribute to enhanced immunity. M cells can be actively targeted using nanoparticles coated with specific ligands such as ulex europaeus 1 (UEA-1) lectin or arginylglycylaspartic acid for effective vaccine delivery.

ProteosomesTM as Vaccine Delivery Vehicles

Components of the immune system recognize particles more efficiently than soluble proteins. ProteosomesTM (GlaxoSmithKline) serve as vaccine delivery vehicles by their nanoparticulate nature, forming vesicles and vesicle clusters comparable to the size of small viruses. ProteosomeTM vaccine vesicles and vesicle clusters may range in size from 20 to 800 nm, depending on the type and amount of antigen formulated with the ProteosomesTM. The hydrophobic nature of the ProteosomeTM porin proteins also contributes to vaccine delivery capabilities by facilitating interaction of the vaccine particles with, and uptake of the vaccine by, cells that initiate immune responses. The fact that ProteosomesTM are effective nasal vaccines is particularly related to this enhanced recognition and uptake afforded by Proteosomes' particulate and hydrophobic nature. This technology is being applied to develop vaccines for influenza, allergy, plague, respiratory syncitial virus and Alzheimer's disease.

Targeted Synthetic Vaccine Particle (tSVPTM) Technology

Selecta's Biosciences' tSVP[™] platform creates fully-integrated synthetic nanoparticle vaccines engineered to mimic the properties of natural pathogens to elicit a maximal immune response. The tSVP vaccines are rationally designed to optimize the presentation of antigens to the immune system and ensure a focused and undistracted response. This is accomplished by delivering antigens and adjuvants, within the same biodegradable nanoparticle, directly to antigen-presenting cells. This approach maximizes the immune response while minimizing undesirable off-target effects. The tSVP platform includes a self-assembling nanoparticle platform that is synthetic, modular, and engineered for highly-effective targeting to immune cells. The tSVP vaccines incorporate only the essential elements required for a specific, robust immune response, based on precise engineering that is only possible with the proprietary nanoparticle self-assembly process.

Virus-Mimetic Nanovesicles as an Antigen-Delivery System

Virus-mimetic nanovesicles (VMVs) consist of phospholipid derived from mammalian cell plasma membrane, recombinant protein anchored to cell membrane via the route of signal peptide sorting, and surfactants capable of controlling the VMV size and strength, which enables the VMVs to display functional polypeptides or maintain the correct conformation of protein antigen (Zhang et al. 2015). The protein integrated into VMV by its hydrophobic transmembrane peptide has more modifications, such as glycosylation, than proteins in conventional subunit vaccines. Moreover, many viral envelope glycoproteins can be genetically engineered onto VMV liposomal surface to mimic the properties and conformational epitopes of natural virus. VMV provides an effective, straightforward, and tunable approach against a wide range of emerging enveloped viruses.

Nanobiotechnology for Cell Therapy

Cell therapy is the prevention or treatment of human disease by the administration of cells that have been selected, multiplied and pharmacologically treated or altered outside the body (ex vivo). The human body is made up of \sim 220 different kinds of specialized cells, which originate from stem cells. Stem cells are not specialized and but they can be induced to differentiate. The scope of cell therapy can be broadened to include methods, pharmacological as well as non-pharmacological, to modify the function of intrinsic cells of the body in vivo for therapeutic purposes. The aim of cell therapy is to replace, repair or enhance the function of damaged tissues or organs. The cells used can originate from the patient or from a donor or from another species. Other sources include cell lines and cell from patients' tumors to make cancer vaccines. Cells can be encapsulated in selectively permeable membranes that block entry of immune mediators but allow outward diffusion of active molecules produced by the cells. Genetic engineering of cells is part of ex vivo gene therapy. The cells may be introduced by various routes into the body and selectively implanted at the site of action. Cell therapies have now expanded to replace some conventional procedures. Bone marrow transplants are being replaced by peripheral blood stem cell transplants. Most of the current interest in cell therapy centers on stem cells. Cell therapy technologies are described in detail in a report on this topic (Jain 2017a).

In their natural environment in the body, stem cells transform into other cell types based on chemical triggers they receive from their surroundings. The nature and the location of these triggers are not known for most stem cells. The current ability to introduce specific chemicals at select locations on a cell is also very limited as one must bathe the entire surface of stem cells in various chemicals to search for a response. A nano lab has been used to experiment with individual adult stem cells. Each lab essentially consists of a capsule on a silicon chip, around which up to 1000 nanoreservoirs hold roughly a millionth of a billionth of a milliliter of liquid, comparable to the size of secretions cells use to communicate. This is an artificial cell-interface unit for a stem cell to establish chemical communication in much the same way real cells do. Nanotechnology is essential for this approach. Larger systems cannot provide the number of different reservoirs and chemicals within a space small enough to select different areas on a cell.

Nanobiotechnology by enabling us to manipulate materials, tissues, cells and DNA at the level of and within the individual cell, is well suited for optimizing the generally encouraging results already achieved in cell therapy. Role of combination of cell therapy with nanobiotechnology for tissue engineering is described in Chap. 7. Examples of applications of nanobiotechnology in cell therapy are:

- QDs serve as promising alternatives to organic dyes for cell labeling. Watersoluble biocompatible quantum rods are applied for nonspecific cell tracking as well as specific cellular targeting.
- Superparamagnetic iron oxide nanoparticles (SPIONs) are used with MRI to monitor the cells introduced therapeutically into the body.
- Delivery of gene therapy using genetically modified stem cells.
- Bone formation from mesenchymal stem cells (MSCs) is facilitated on a novel nanofibrous scaffold.
- Carbon nanotubes (CNTs) aid stem cell therapy of neurological disorders.

Nano-biocomposites Containing Living Cells

Study of individual cell behavior and applications of cells as biosensors, artificial organs, and vaccines requires their 3D encapsulation within nanostructured silica gels or matrices. A spray-drying process has been described that enables the large-scale production of functional nano-biocomposites (NBCs) containing living cells within ordered 3D lipid-silica nanostructures (Johnson et al. 2015). This process extends lipid fluidity and imparts high physical strength, which would prevent cell growth and force bacteria into viable but not culturable (VBNC) states. Although cellular ATP levels remain elevated, their ability to undergo resuscitation and enter growth phase greatly decreases with time in the VBNC state. The NBC platform for production of large quantities of VBNC cells is useful for research in bacterial persistence and screening of drugs targeting such cells. NBCs may also enable long-term preservation of living cells for applications in cell-based sensing and the packaging and delivery of live-cell vaccines.

Nanobiotechnology for Gene Therapy

Gene therapy is defined as the transfer of defined genetic material to specific target cells of a patient for the ultimate purpose of preventing or altering a disease state (Jain 2017b). It has three components; (1) identification of the gene that is mutated in the disease and obtaining a healthy copy of that gene; (2) carrier or delivery vehicle called vectors to deliver the healthy gene to a patient's cells; and (3) use of additional DNA elements that turn on the healthy gene in the right cells and at the right levels. As a broad term gene therapy covers some other biological therapies such as antisense, RNAi, gene editing and use of genetically modified or engineered cells.

Vectors used in the past were mostly viral but currently several nonviral techniques are being used as well. Genes and DNA are now being introduced without the use of vectors and various techniques are being used to modify the function of genes in vivo without gene transfer. Nanoparticles and other nanostructures can be used for gene delivery.

Nanoparticle-Mediated Gene Therapy

The success of the gene therapy for clinical applications, in part, would depend on the efficiency of the expression vector as determined by the level as well as the duration of gene expression. Although various cationic polymers and lipid-based systems are being investigated, most of these systems exhibit higher-level but transient gene expression. Most often, the emphasis is on the level of gene expression rather than on the duration of gene expression. In certain disease conditions, a relatively low level of gene expression (therapeutic level) but for a sustained duration may be more effective than higher-level but transient gene expression. Therefore, a gene expression system that can modulate the level as well as the duration of gene expression in the target tissue is desirable. Polymer-based sustained release formulations such as nanoparticles have the potential of developing into such a system.

Nanoparticles escape rapidly (within 10 min) from the endolysosomal compartment to the cytoplasmic compartment following their intracellular uptake via an endocytic process. The escape of nanoparticles is attributed to the reversal of their surface charge from anionic to cationic in the acidic pH of the endolysosomal compartment, causing nanoparticles to interact with the endolysosomal membrane and then escape into the cytoplasmic compartment. The rapid escape of nanoparticles from the endolysosomal compartment could protect nanoparticles as well as the encapsulated DNA from the degradative environment of the endolysosomes. Nanoparticles localized in the cytoplasmic compartment would release the encapsulated DNA slowly, thus resulting in sustained gene expression. Sustained gene expression could be advantageous, especially if the half-life of the expressed protein is very low and/or a chronic gene delivery is required for therapeutic efficacy.

Degradable nanoparticles are the only nonviral vectors that can provide a targeted intracellular delivery with controlled release properties. Furthermore, the potential advantage of degradable nanoparticles over their non-degradable counterparts is the reduced toxicity and the avoidance of accumulation within the target tissue after repeated administration. Modification of the surface of viral vectors with nanomaterials is a promising strategy to augment vector accumulation at the target tissue, circumvent host immune response, and avoid nonspecific interactions with the reticuloendothelial system. Some of the strategies to enhance virus vectors with nanobiotechnology are (Kasala et al. 2016):

- Encapsulation of viral vectors in hydrogels to induce prolonged and stable transgene expression in local tissue by protecting them from enzymatic degradation.
- Magnetic nanoparticle-coated viral vectors can be guided to and retained in target tissue by magnetic field exposure.
- PEGylation of viral vectors can enhance retention in blood and protect against host immune response.
- Active targeting by a nanocomplex leads to better intratumoral accumulation of the vector than EPR-mediated passive targeting.

Examples of application of nanoparticles for gene therapy are shown in Table 6.1 and some of these are described in the following text.

Calcium Phosphate Nanoparticles as Nonviral Vectors

Calcium phosphate nanoparticles present a unique class of nonviral vectors, which can serve as efficient and alternative DNA carriers for targeted delivery of genes. DNA-doped calcium phosphate nanoparticles approximately 80 nm in diameter has been synthesized. DNA encapsulated inside the nanoparticle is protected from the external DNase environment and could be transferred safely under in vitro or in vivo conditions. Moreover, the surface of these nanoparticles can be suitably modified by adsorbing a highly adhesive polymer like polyacrylic acid followed by conjugating the carboxylic groups of the polymer with a ligand such as p-amino-1-thio-beta-galactopyranoside using 1-ethyl-3-(3-dimethylaminopropyl)-carbodiimide hydrochloride as a coupling agent. These surface modified calcium phosphate nanoparticles can be used to target genes specifically to the liver.

Carbonate Apatite Nanoparticles for Gene Delivery

Biocompatible, inorganic nanoparticles of carbonate apatite have the unique features essentially required for smart delivery, as well as for the expression of genetic material in mammalian cells. The newly developed carbonate apatite, as with hydroxyapatite, adsorbs DNA, but, unlike the latter, it can prevent the growth of its crystals to a significant extent, enabling the synthesis of nanosized crystals to effectively carry the associated DNA across the cell membrane. It also possesses a high dissolution rate in endosomal acidic pH, leading to the rapid release of the bound DNA for a subsequent high level of protein expression. Carbonate apatite is a natural component of the body, and is usually found in the hard tissues, such as bone and teeth. Moreover, because of their nanosize dimensions and sensitivity to low pH, particles of carbonate apatite are quickly degraded when taken up by cells in their acidic vesicles, without any indication of toxicity. Apatite nanoparticles are promising candidates for nonviral gene delivery and are superior to polymer- or lipid-based systems that are generally non-biodegradable and inefficient.

Dendrimers for Gene Transfer

Dendrimers are nanoparticles ranging in size from 1 to 20 nm and can hold therapeutic substances such as DNA in their cavities. They are made up of precise 3D branches called dendrons, with structure that mimics the bifurcation of tree branches. The dendrimers are so close in shape and size to a histone cluster that DNA wraps around them as it does around the natural protein complex. Dendrimers show great

Nanoparticle	Application
Calcium phosphate nanoparticles.	Nonviral vectors for targeted gene therapy of liver.
Cationized gelatin nanoparticles.	Nonviral and non-toxic vectors for gene therapy.
Cochleate delivery system is based on interaction of cations with negatively charged phospholipids.	In vivo lipid-based delivery of DNA plasmids and antisense DNA.
Combination of a gene, nanoparticle and surfactant.	Facilitation of gene transfer in the brain across the blood-brain barrier.
Compacted DNA nanoparticles (20–25 nm): Each DNA molecule is wrapped in a coat of positively charged peptides.	Nanoparticles pass through a nuclear pore with thousands-fold enhancement of gene expression compared to naked DNA. Used for transnasal gene therapy in cystic fibrosis.
Fluorescently labeled organically modified silica nanoparticles as a nonviral vector.	For gene delivery and optical monitoring of intracellular trafficking and gene transfection.
Integrin-targeted nanoparticles	Site-specific delivery of anticancer genes
Intravenous liposomal DOTAP:Chol-FUS1 complex) of tumor suppressor gene FUS1.	Suppresses tumor growth and has led to tumor regression in mouse models of metastatic lung cancer.
L-tyrosine-based polyphosphate nanoparticle	Degradable nonviral gene delivery systems
Magnetic nanoparticles	Targeted gene delivery: viral and nonviral
Nanocomposites: nanoparticles of titanium dioxide combined with oligonucleotide DNA that can be activated by light or radiation.	Antisense genes can be delivered to a specific intracellular site in combination with radiotherapy for killing cancer cells in patients.
Nanoneedles with a tip diameter of 1 nm for delivery of genetic material into cells.	This method is next stage in the refinement of microneedles for injecting genetic material into cells.
Nanoparticles: EGF-PEG-biotin- streptavidin-PEI-DNA complexes.	Exhibit high transfection efficiency with no particle aggregation.
Nanorod binds plasmid DNA as well as proteins in spatially defined regions.	A versatile gene delivery system that increases the plasmid's cellular internalization and cytoplasmic release.
Nanotube spearing is based on the penetration of nickel-embedded nanotubes into cell membranes by magnetic field driving.	This technique may provide a powerful tool for highly efficient gene transfer into a variety of cells, especially the hard-to-transfect cells.
Nonionic polymeric micelles of poly(ethylene oxide)-poly(propylene oxide)-poly(ethylene oxide)	Stable gene transfer to the gastrointestinal tract can be achieved in mice by oral delivery
PAMAM dendrimers can hold DNA in cavities	Non-immunogenic vector for in vivo gene transfer.
Poly(D,L-lactide-co-glycolide) nanoparticles loaded with wild type p53 DNA.	Inhibition of cell proliferation in cancer due to sustained gene expression following intracellular release of p53.

 Table 6.1 Examples of application of nanoparticles for gene therapy

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Abbreviations: EGF Epidermal growth factor, PEI Polyethylenimine, PEG Polyethylene glycol

promise as DNA- and drug-delivery systems. The following factors, which drive the interest in use of dendrimers as gene, transfer vectors:

- 1. They can be produced as precise macromolecular structures.
- 2. They are composed of nanoscopic building blocks or modules.
- 3. They are non-immunogenic.

Activated polyamidoamine (PAMAM)-dendrimers provide a new technology for gene transfer that offers significant advantages over classical methods. QIAGEN reagents based on this technology provide high gene transfer efficiencies, minimal cytotoxicity, and can be used with a broad range of cell types. This technology could also be useful for in vivo gene transfer in gene therapy applications. Multifunctionalization of dendritic polymers provides gene vectors of low toxicity, significant transfection efficiency, specificity to certain biological cells and transport ability through their membranes (Paleos et al. 2009).

DNA Nanoparticles

Use of nanoparticles as nonviral vectors for gene therapy involves encapsulating snippets of therapeutic DNA within protective polymer coatings. The nanoparticles are designed to deliver their genetic payload only after they have moved through the blood circulation and entered the target cells where they degrade and release DNA. Using this DNA as a template, the cells can produce functional proteins that combat disease. Shapes of these nanocarriers may make a big difference in how well they work in treating cancer and other diseases. A study compared DNA nanoparticles in three shapes resembling worms, rods, and spheres, which mimic the shapes and sizes of viral particles (Jiang et al. 2013). Computer simulations and theoretical models provided helped in identifying what is responsible for this shape change so that the nanoparticle components can be chosen to obtain a certain shape. Worm-shaped particles resulted in 1600 times more gene expression in the liver cells than other shapes, which means that producing nanoparticles in this shape could be the most efficient way to deliver gene therapy to cells.

Gelatin Nanoparticles for Gene Delivery

Gelatin nanoparticles are biodegradable and desirable as alternative carriers to existing DNA delivery systems. To bind DNA by electrostatic interactions onto the surface of the gelatin nanoparticles, the quaternary amine cholamine is covalently coupled to the particles. The modified nanoparticles are loaded with different amounts of plasmid in varying buffers and compared to polyethyleneimine-DNA complexes (PEI polyplexes) as gold standard. In contrast to PEI polyplexes, cation-ized gelatin nanoparticles almost do not show any significant cytotoxic effects.

Cationized gelatin nanoparticles have the potential of being a new effective carrier for nonviral gene delivery. The major benefit of gelatin nanoparticles is not only the very low cell toxicity, but also their simple production combined with low costs and multiple modification opportunities offered by the matrix molecule.

The potential of engineered gelatin-based nanoparticles, nanovectors, has been investigated for delivery of therapeutic genes to human breast cancer tumors implanted in mice (Kommareddy and Amiji 2007). Plasmid DNA encoding for the soluble form of the extracellular domain of VEGF-R1 or sFlt-1 was encapsulated in the control and PEG-modified gelatin-based nanoparticles. Following intravenous administration in female Nu/Nu mice bearing orthotopic MDA-MB-435 breast adenocarcinoma xenografts, 15% of the dose found its way into the tumor. In vivo expression of sFlt-1 plasmid DNA was therapeutically active as shown by suppression of tumor growth and microvessel density measurements. The results of this study show that PEG-modified gelatin-based nanovectors can serve as a safe and effective systemically administered gene delivery vehicle for solid tumor. Clinical trials of this method are expected in the future.

Immunoliposomes for Delivery Anticancer Gene Therapy

Immunolipoplex-based gene transfer represents an advance over the viral vectors that have been used to deliver gene therapy, because these liposomes do not produce the immunologic response seen when disabled viruses are used to carry the payload. Tumor-directed gene delivery is of major interest in the field of cancer gene therapy. Varied functionalizations of non-viral vectors have been suggested to enhance tumor targetability. In one study, two different types of anti-EGF receptor (EGFR) immunonanoparticles containing pDNA, neutrally charged liposomes and cationic lipoplexes, were used for tumor-directed transfection of cancer therapeutic genes (Kim et al. 2016). Even though both anti-EGFR immunonanoparticles had a high binding affinity to the EGFR-positive cancer cells, the anti-EGFR immunolipoplex formulation exhibited ~100-fold higher transfection to the target cells than anti-EGFR immunoliposomes. The lipoplex formulation also showed a higher transfection to SK-OV-3. Thus, IL12 and/or salmosin genes were loaded in the anti-EGFR immunolipoplexes and intravenously administered to mice carrying SK-OV-3 tumors. Co-transfection of IL12 and salmosin genes using anti-EGFR immunolipoplexes to mice tumor xenografts significantly reduced tumor growth and pulmonary metastasis. Furthermore, combinatorial treatment with doxorubicin synergistically inhibited tumor growth. These results suggest that anti-EGFR immunolipoplexes containing pDNA encoding therapeutic genes could be utilized as a gene-transfer modality for cancer gene therapy. A phase II clinical trial in Switzerland is in progress to determine the efficacy of doxorubicin-loaded anti-EGFR immunoliposomes as first-line therapy in patients with advanced triple negative, EGFR positive breast cancer (ClinicalTrials.gov Identifier: NCT02833766).

Lipid Nanoparticles for Targeted Delivery of Nucleic Acids

Tekmira's delivery technology platform uses lipid nanoparticle (LNP), which fully encapsulate and systemically deliver a variety of nucleic acid molecules such as short interfering RNAs (siRNAs). Preclinical studies have shown them to be effective in delivering the drug to target organs and into cells where the nucleic acid-based drug can carry out its desired effect while minimizing systemic toxicity. LNP technology relies on enhanced permeability and retention effect, which occurs because these nucleic acid-containing particles have a long circulation time in the blood, resulting in increased accumulation at sites of vascular leak such as those found at sites of tumor cell growth, infection or inflammation. Once at the target site, cells take up the LNP through endocytosis and the nucleic acid payload is delivered inside the cell resulting in a high degree of potency. LPN technology is shown schematically in Fig. 6.1.

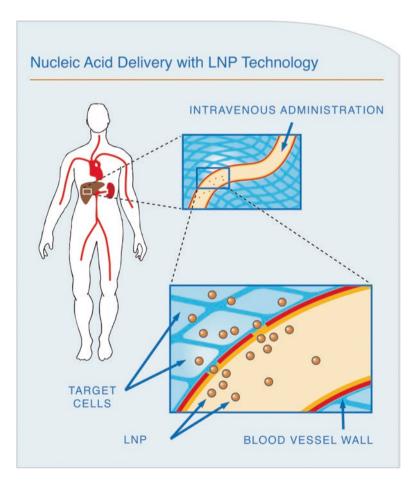


Fig. 6.1 Nucleic acid delivery with lipid nanoparticle (LPN) technology (Courtesy of Tekmira Pharmaceutical Corporation)

Magnetic Nanoparticles for Targeted Gene Delivery

Magnetic nanoparticles (MNPs) are usually based on magnetite core, and the mean diameter of different magnetic carriers varies from 100 to 500 nm. Both molecular linkers and physical interactions have been used to attach viral or nonviral vectors to MNPs. Significant improvement in transfection efficiency has been shown for several types of MNPs. Magnetic targeting is an effective strategy to decrease side effects of gene transfer, while increasing the selectivity and efficiency of the applied vector (Delyagina et al. 2011). As a nonviral method, targeted gene delivery with MNPs avoids the unwanted immune system responses that can occur when viruses are used to deliver genes. Although research, done in cell cultures, is in early stages, magnetically driven delivery systems have potential uses as vehicles for delivering drugs, genes or cells to a target organ. After preloading genetically engineered cells with nanoparticles, magnetic forces can be used to direct the cells to a target organ. Furthermore, nanoparticles may be delivered to magnetically responsive, removable stents in sites other than blood vessels, such as airways or parts of the gastrointestinal tract. After the MNPs have delivered enough genes, cells or other agents to have a long-lasting benefit, the stent could be removed.

Nanoparticles for Imaging and Intracellular Delivery of Nucleic Acids

Although materials have been developed and studied for polynucleotide transfer, the biological mechanisms and fate of the synthetic vehicle has remained elusive due to the limitations with current labeling technologies. Polymer beacons have been developed that enable the delivery of nucleic acids to be visualized at nanoscale (Bryson et al. 2009). The polycations have been designed to contain repeated oligoethyleneamines, for binding and compacting nucleic acids into nanoparticles, and lanthanide chelates (either luminescent europium Eu³⁺ or paramagnetic gadolinium Gd³⁺). The chelated Lns allow the visualization of the delivery vehicle both on the nm/µm scale via microscopy and on the sub-mm scale via MRI. These delivery beacons effectively bind and compact plasmid DNA (pDNA) into nanoparticles and protect nucleic acids from nuclease damage. These delivery beacons efficiently deliver pDNA into cultured cells and do not exhibit toxicity. Micrographs of cultured cells exposed to the nanoparticle complexes formed with fluorescein-labeled pDNA and the europium-chelated polymers reveal effective intracellular imaging of the delivery process. MRI of bulk cells exposed to the complexes formulated with pDNA and the gadolinium-chelated structures show bright image contrast, allowing visualization of effective intracellular delivery. Because of their versatility, these delivery beacons possess remarkable potential for tracking and understanding nucleic acid transfer in vitro, and have promise as in vivo vectors for gene therapy and agents for combining diagnostics and therapeutics.

Nanoparticles Linked to Viral Vectors for Photothermal Therapy

Hyperthermia can be produced by near-infrared laser irradiation of gold nanoparticles present in tumors and thus induce tumor cell killing via a bystander effect. However, selective delivery and physical targeting of gold nanoparticles to tumor cells are necessary to improve therapeutic selectivity. Covalent coupling of gold nanoparticles to retargeted adenoviral vectors enable selective delivery of the nanoparticles to tumor cells, thus facilitating hyperthermia and gene therapy as a combinatorial therapeutic approach. For this, sulfo-N-hydroxysuccinimide labeled gold nanoparticles have been linked to adenoviral vectors encoding a luciferase reporter gene driven by the cytomegalovirus promoter. The covalent coupling retains virus infectivity and ability to retarget tumor-associated antigens. These results show the feasibility of using adenoviral vectors as carriers for gold nanoparticles.

Nanoparticles for p53 Gene Therapy of Cancer

One of the important considerations in p53 gene delivery for tumor growth inhibition would be the sustained expression of the p53 protein in the target cells. A single-dose regimen results in only a weak and transient inhibition of cell proliferation. Multiple doses are required to obtain inhibition of cell proliferation comparable to that with viral vectors. Several mechanisms have been attributed to wt-p53 gene-mediated cancer therapy such as apoptosis of cancer cells, cell cycle arrest, and/or the antiangiogenic effect of the protein. Gene delivery with nanoparticles would require direct intratumoral injection in the case of a solid tumor or delivery via a catheter to an accessible diseased tissue. However, tumor targeting via intravascular administration would be possible if nanoparticle surface is modified to avoid extravasation by the reticuloendothelial system.

Nanoparticles with Virus-Like Function as Gene Therapy Vectors

Novel multifunctional DNA carriers (MDCs) have been described, which selfassemble with DNA to form structured nanoparticles that possess virus-like functions for cellular trafficking (Glover et al. 2009). The new gene therapy vectors use the same machinery that viruses use to transport their cargo into cells. To create the new gene therapy vector, the scientists used pieces of different genes to create a protein called a "modular DNA carrier," which can be produced by bacteria. This protein carries therapeutic DNA and delivers it to a cell's nucleus, where it reprograms a cell to function properly. In the laboratory, these carrier proteins were combined with therapeutic DNA and attached to cell membrane receptors and the nuclear import machinery of target cells. In turn, the packaged DNA moved into the cell through the cytoplasm and into the nucleus. The nanoparticles were internalized in cell-specific fashion and subsequently exited the endosome into the cytoplasm. The nanoparticles interact with cellular nuclear transport proteins and are actively trafficked into the cell nucleus of nondividing cells, resulting in 3fold to 4fold higher reporter gene expression in growth-arrested human embryonic kidney cells, as well as lower cytotoxicity, than lipid and polyethyleneimine vectors. MDCs that utilize cellular signaling pathways have enormous potential to safely and efficiently deliver therapeutic transgenes into the nucleus of nondividing cells.

Nanobiolistics for Nucleic Acid Delivery

Biolistic transfection using a gene gun is a method of incorporating DNA or RNA into cells that are difficult to transfect using traditional methods. Microparticles used in this technique are efficient at delivering DNA into cells, but cannot transfect small cells and may cause significant tissue damage, thus limiting their potential usefulness. Nanobiolistic by use of 40 nm diameter nanoparticles results in ~30% fewer damaged HEK293 cells following transfection and considerably enhances details of small cellular structures (O'Brien and Lummis 2011). The discovery that smaller projectiles are equally effective but cause less tissue damage could therefore have a significant impact on the feasibility of nanobiolistic transfection as a therapeutic technique. It may also be possible to modify the nanoparticles, e.g. with polyethyleneimine to create cationic gold particles, which have been shown to deliver increased amounts of DNA. The use of nanoparticles as efficient carriers of genetic material also enhances the prospects of efficiently transfecting smaller organisms or specific regions of cells such as dendritic spines.

Photo-Controlled in Vivo Activation of Biomolecules by Nanoparticles

Controlled activation or release of biomolecules in vivo is crucial for various biological applications. Activity of biomolecules has been controlled by light but the major hurdle in this process is that photoactivable compounds mostly respond to UV radiation and not to visible or near-infrared (NIR) light. The use of UV irradiation is limited by its toxicity and very low tissue penetration. A study has demonstrated the potential of NIR-to-UV upconversion nanoparticles (UCNs), which act as nanotransducers to absorb NIR light, have high tissue penetration power and negligible phototoxicity, and emit UV light locally, for photoactivation of caged compounds used for photo-controlled gene expression (Jayakumar et al. 2012). Both activation and knockdown of GFP was performed in both solution and cells, and patterned activation of GFP was achieved successfully by using upconverted UV light produced by NIR-to-UV UCNs. In-depth photoactivation through tissue phantoms and in vivo activation of caged nucleic acids were also accomplished. The success of this methodology has defined a unique level in the field of photo-controlled activation and in vivo delivery of biomolecules.

Silica Nanoparticles for Gene Delivery

Core shell silica particles with a diameter of 28 nm have been synthesized. Role of freeze-drying for the conservation of zwitterionic nanoparticles and the usefulness of different lyoprotective agents (LPA) DNA-binding capacity and transfection efficiency have been investigated. Of the various LPAs screened in the investigations, trehalose and glycerol were found to be well suited for conservation of cationically modified silica nanoparticles with simultaneous preservation of their DNA-binding and transfection activity.

Fluorescently labeled organically modified silica nanoparticles are useful as nonviral vectors for gene delivery as well as for optically monitoring intracellular trafficking and gene transfection. Highly monodispersed, stable aqueous suspensions of organically modified silica nanoparticles, encapsulating fluorescent dyes and surface functionalized by cationic-amino groups, are produced by micellar nanochemistry. Gel electrophoresis studies reveal that the particles efficiently complex with DNA and protect it from enzymatic digestion of DNase 1. The electrostatic binding of DNA onto the surface of the nanoparticles, due to positively charged amino groups, is also shown by intercalating an appropriate dye into the DNA and observing the fluorescence resonance energy transfer between the dye (energy donor) intercalated in DNA on the surface of nanoparticles and a second dye (energy acceptor) inside the nanoparticles. Imaging by fluorescence confocal microscopy shows that cells efficiently take up the nanoparticles in vitro in the cytoplasm, and the nanoparticles deliver DNA to the nucleus. This work shows that the nanomedicine approach, with nanoparticles acting as a drug delivery platform combining multiple optical and other types of probes, provides a promising direction for targeted therapy with enhanced efficacy as well as for real-time monitoring of drug action.

Capped mesoporous silica nanoparticle (MSN) materials have been designed as efficient stimuli-responsive controlled release systems with the advantageous 'zero premature release' property. A variety of internal and external stimuli for controlled release of different cargos, as well as the biocompatibility of MSN both in vitro and in vivo, indicate that these multifunctional materials will find a wide variety of applications for gene delivery (Zhao et al. 2010).

Cochleate-Mediated DNA Delivery

Cochleate, a lipid-based delivery system, is formed by interaction between cations, e.g. Ca²⁺ and negatively charged phospholipids such as phosphatidylserine. Cochleates are stable precipitates with a unique structure consisting of a large, continuous, solid, lipid bilayer sheet rolled up in spiral, with no internal aqueous space. They are non-toxic and non-inflammatory and have been used as vehicles for oral and parenteral delivery of protein and peptide antigens. Cochleate-mediated

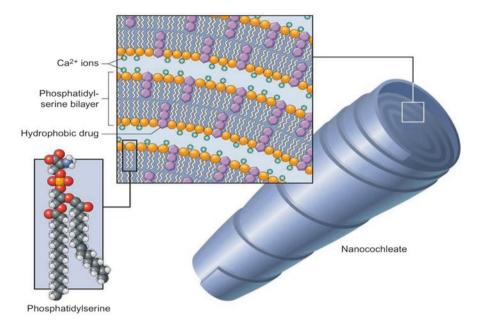


Fig. 6.2 Nanocochleate-mediated drug delivery (Courtesy of BioDelivery Sciences International Inc)

in vivo delivery of DNA plasmids and antisense DNA is under investigation. Protein and DNA cochleates are highly effective vaccines when given via mucosal or parenteral routes, including oral, intranasal, intramuscular, or subcutaneous. BioDelivery Sciences International Inc. is developing cochleate-based gene transfer as shown in Fig. 6.2.

Nanorod Gene Therapy

Gene therapy success has been limited in both viral and synthetic methods. In light of current gene-therapy challenges, synthetic transfection systems provide several advantages over viral methods including ease of production, as well as reduced risk of cytotoxicity and immune responses. The drawbacks of synthetic vectors greatly stem from difficulty of controlling the vectors' properties at the nanoscale. The nanorod greatly overcomes those drawbacks by binding plasmid DNA as well as a potential variety of proteins in spatially defined regions. The proteins the nanorod binds can increase the plasmid's cellular internalization, cytoplasmic release, and/or nuclear internalization. The nanorods can be further guided via their magnetic properties. The potential of this versatile gene delivery system with precise composition and size has been demonstrated in cell transfection studies.

Nanomagnets for Targeted Cell-Based Cancer Gene Therapy

Using human cells as delivery vehicles for anticancer gene therapy is a promising approach for treating cancer. Monocytes naturally migrate from the bloodstream into tumors and attempts have been made to use them to deliver therapeutic genes to these sites. However, transfected monocytes injected systemically fail to infiltrate tumors in large numbers. Therefore, nanoscale magnets have been developed to target cancer cells more effectively. The impact of gene therapy on cancer cells can be enhanced by 'magnetic targeting', i.e. inserting nanomagnets into cells carrying genes so that the number of cells successfully reaching and invading cancer can be increased. Systemic administration of such 'magnetic' monocytes to mice bearing solid tumors led to a marked increase in their extravasation into the tumor in the presence of an external magnet. Further studies are exploring the effectiveness of magnetic targeting in delivering a variety of cancer-fighting genes, including ones that could stop the spread of tumors. This technique could also be used to help deliver therapeutic genes in other diseases like arthritic joints or ischemic heart tissue.

NanoNeedles for Delivery of Genetic Material into Cells

Historically plasmid molecules have been introduced into the nuclei by pricking cells on the nuclei with microneedles. NanoNeedles for delivery of genetic material into cells have been developed by Hayashi Wang at Challentech International Inc. (Taiwan). Needles with diameter of 2 μ and height of 60 μ have a tip 1 nm in size can be used for injecting cells. A NanoNeedle chip has been used to deliver pCMV EGFP (enhanced green fluorescent protein) plasmids into primary cells or stem cells. These can be coated with tungsten for electroporation.

Application of Pulsed Magnetic Field and Superparamagnetic Nanoparticles

A simple approach to enhance gene delivery uses permanent and pulsating magnetic fields. DNA plasmids and novel DNA fragments (PCR products) containing sequence encoding for green fluorescent protein are coupled to polyethyleneimine coated superparamagnetic nanoparticles (SPIONs). The complexes are added to cells that are subsequently exposed to permanent and pulsating magnetic fields. Presence of these magnetic fields increases the transfection efficiency 40 times more than in cells not exposed to the magnetic field. The transfection efficiency is highest when the nanoparticles are sedimented on the permanent magnet before the application of the pulsating field, both for small (50 nm) and large (200–250 nm)

nanoparticles. The highly efficient gene transfer already within 5 min shows that this technique is a powerful tool for future in vivo studies, where rapid gene delivery is required before systemic clearance or filtration of the gene vectors occurs.

Nanobiotechnology for Antisense Drug Delivery

Antisense molecules are synthetic segments of DNA or RNA, designed to mirror specific mRNA sequences and block protein production. One way to target the genetic material is to block the messenger RNA (mRNA) by using 'antisense DNA,' which prevents the message from ever becoming a protein. The use of antisense drugs to block abnormal disease-related proteins is referred to as antisense therapeutics. Synthetic short segments of DNA or RNA are referred to as oligonucle-otides. Whereas typical drugs target the proteins, it is possible through antisense gene therapy to target the genetic material itself before it is ever made into copies of harmful proteins. Antisense drugs have the promise to be more effective than conventional drugs, but one of the problems with antisense therapy is delivery. The efficacy of antisense oligonucleotides is limited by the poor stability of the natural oligomers and the low efficacy of their cellular uptake. Nanotechnology has been used to improve this situation.

Antisense Nanoparticles

Gold nanoparticle-oligonucleotide complexes – antisense nanoparticles – have been used as intracellular gene regulation agents for the control of protein expression in cells (Rosi et al. 2006). Once inside cells, the DNA-modified nanoparticles act as mRNA "sponges" that bind to their targets and prevent them from being converted into proteins. By chemically tailoring the density of DNA bound to the surface of gold nanoparticles, they have demonstrated a tunable gene knockdown. In the future, this exciting new class of antisense material could be used for the treatment of cancer and other diseases that have a genetic basis. Advantages of attaching multiple strands of antisense DNA to the surface of a gold nanoparticle over conventional antisense oligonucleotides are:

- The DNA becomes more stable and can bind to the target mRNA more effectively than DNA that is not attached to a nanoparticle surface as in commercial agents such as Lipofectamine and Cytofectin.
- · They are less susceptible to degradation by nuclease activity
- They exhibit greater than 99% cellular uptake
- They can introduce oligonucleotides at a higher effective concentration than conventional transfection agents, and are nontoxic to the cells under the conditions studied.

Dendrimers for Antisense Drug Delivery

Polypropylenimine dendrimers have been used for delivering a 31 nt triplex-forming oligonucleotide (ODN) in breast, prostate and ovarian cancer cell lines, using 32P–labeled ODN. Dendrimers enhance the uptake of ODN by 14-fold compared with control ODN uptake. Dendrimers exert their effect in a concentration- and molecular weight-dependent manner, with generation 4 (G-4) dendrimer having maximum efficacy. The dendrimers have no significant effect on cell viability at concentrations at which maximum ODN uptake occurred. Gel electrophoretic analysis shows that ODN remains intact in cells even after 48 h of treatment. The hydrodynamic radii of nanoparticles formed from ODN in the presence of the dendrimers are in the range of 130–280 nm, as determined by dynamic laser light scattering. Taken together, these results indicate that polypropylenimine dendrimers might be useful vehicles for delivering therapeutic oligonucleotides in cancer cells.

Polymer Nanoparticles for Antisense Delivery System

ODNs have been shown to induce dystrophin expression in muscles cells of patients with Duchenne muscular dystrophy (DMD) and in the mdx mouse, the murine model of DMD. However, ineffective delivery of ODNs limits their therapeutic potential. Copolymers of cationic polyethylene imine (PEI) and non-ionic polyethylene glycol (PEG) form stable nanoparticles when complexed with AOs, but the positive surface charge on the resultant PEG-PEI-ODN nanoparticles limits their biodistribution. A modified double emulsion procedure for encapsulating PEG-PEI-ODN polyplexes into degradable PLGA nanospheres has been described (Sirsi et al. 2009). Formulation parameters were varied including PLGA molecular weight, ester end-capping, and sonication energy/volume. The results showed successful encapsulation of PEG-PEI-ODN within PLGA nanospheres with average diameters ranging from 215 to 240 nm. Encapsulation efficiency ranged from 60% to 100%, and zeta potential measurements confirmed shielding of the PEG-PEI-ODN cationic charge. PLGA showed a rapid burst release of about 20% of the PEG-PEI-ODN, followed by sustained release of up to 65% over 3 weeks. PEG-PEI-AO polyplexes were loaded into PLGA nanospheres using an ODN that is known to induce dystrophin expression in dystrophic mdx mice. Intramuscular injections of this compound into mdx mice resulted in over 300 dystrophin-positive muscle fibers distributed throughout the muscle cross-sections, approximately 3.4 times greater than for injections of ODN alone. It is concluded that PLGA nanospheres are effective compounds for the sustained release of PEG-PEI-ODN polyplexes in skeletal muscle and concomitant expression of dystrophin, and may have potential in treating DMD.

Nanoparticle-Mediated siRNA Delivery

Delivery of DNA and siRNA into mammalian cells is a powerful technique in treating various diseases caused by single gene defects. Potent sequence selective gene inhibition by short interferering RNA (siRNA) 'targeted' therapeutics promises the ultimate level of specificity, but siRNA therapeutics is hindered by poor intracellular uptake, limited blood stability and nonspecific immune stimulation. Use of viral vectors for siRNA delivery has also some problems. Nonviral carrier systems, especially nanoparticles, have been investigated extensively for siRNA delivery, and may be utilized in clinical applications in the future. So far, a few preliminary clinical trials of nanoparticles have produced promising results. However, further research is still required to pave the way to successful clinical applications. The most important issues that need to be focused on include encapsulation efficiency, formulation stability of siRNA, degradation in circulation, endosomal escape and delivery efficiency, targeting, toxicity and off-target effects (Yuan et al. 2011).

Chitosan-Coated Nanoparticles for siRNA Delivery

Overexpression of RhoA in cancer indicates a poor prognosis, because of increased tumor cell proliferation and invasion and tumor angiogenesis. Anti-RhoA siRNA inhibits aggressive breast cancer more effectively than conventional blockers of Rhomediated signaling pathways. Intravenous administration of encapsulated anti-RhoA siRNA in chitosan-coated polyisohexylcyanoacrylate (PIHCA) nanoparticles for xenografted aggressive breast cancers inhibits the growth of tumors and necrotic areas are observed in tumors, resulting from angiogenesis inhibition. Because of its efficacy and the absence of toxicity, it is suggested that this strategy of anti-RhoA siRNA holds significant promise for the treatment of aggressive cancers.

Delivery of siRNA by Nanosize Liposomes

siRNA incorporated into the neutral nanosize liposome 1,2-dioleoyl-sn-glycero-3phosphatidylcholine (DOPC) has been used for efficient in vivo siRNA delivery. Getting the siRNA to the targeted protein in tumor cells, focal adhesion kinase (FAK), is difficult as it located inside the cell, rather than on the cell surface where most proteins targeted by cancer drugs are found. FAK, which is difficult to target with a drug, can be attacked with the liposomal siRNA approach, which penetrates deeply into the tumor. In experimental studies, mice receiving the FAK-silencing liposome had significant reductions in mean tumor weight ranging. In addition to its anticancer effect, the therapeutic liposome also has an antiangiogenic effect when combined with chemotherapy. By inducing apoptosis among blood vessel cells, the treatment steeply reduces the number of small blood vessels feeding the tumor, cut the percentage of proliferating tumor cells and increases cell suicide among cancer cells. Two advantages of this approach are:

- 1. The FAK-targeting liposome ranges between 65 and 125 nm in diameter. Blood vessels that serve tumors are more porous than normal blood vessels, with pores of 100–780 nm wide. The liposomes do not enter the normal blood vessel, whose pores are 2 nm or less in diameter.
- 2. The liposome DOPC has no electrical charge. Its neutrality provides an advantage over positively or negatively charged liposomes when it comes to binding with and penetrating cells.

Animal experimental studies show the feasibility of siRNA as a clinically applicable therapeutic modality. The next step for the FAK siRNA-DOPC liposome is toxicity testing. In addition to ovarian cancer, FAK is overexpressed in colon, breast, thyroid, and head and neck cancers.

Delivery of Gold Nanorod-siRNA Nanoplex to Dopaminergic Neurons

A nanotechnology approach that uses gold nanorod-DARPP-32 siRNA complexes (nanoplexes) can target this dopaminergic signaling pathway in the brain (Bonoiu et al. 2009). The shift in the localized longitudinal plasmon resonance peak of gold nanorods was used to show their interaction with siRNA. Plasmonic enhanced dark field imaging was used to visualize the uptake of these nanoplexes in dopaminergic neurons in vitro. Gene silencing of the nanoplexes in these cells was evidenced by the reduction in the expression of key proteins (DARPP-32, ERK, and PP-1) belonging to this pathway, with no observed cytotoxicity. Moreover, these nanoplexes were shown to transmigrate across an in vitro model of the BBB. Therefore, these nanoplexes appear to be suited for brain-specific delivery of appropriate siRNA for therapy of drug addiction and other brain diseases.

Polymer-Based Nanoparticles for siRNA Delivery

Polyethylenimine Nanoparticles for siRNA Delivery

A highly efficient delivery system has been described using 1,4-butanediol diglycidyl ether (bisepoxide) crosslinked polyethylenimine (PEI) nanoparticles (Swami et al. 2007). The nanoparticle/DNA complexes (nanoplexes) exhibited approximately 2.5- to 5.0-fold gene transfer efficacy and decreased cytotoxicity in cultured cell lines, compared to the native PEI used as gold standard, and commercially available

transfection agents such as Lipofectamine 2000. The bisepoxide crosslinking results in change in amine ratio in PEI; however, it retains the net charge on nanoparticle unaltered. A series of nanoparticles obtained by varying the degree of crosslinking was found to be in the size range of 69–77 nm and the zeta potential varying from +35 to 40 mV. The proposed system was also found to deliver siRNA efficiently into HEK cells, resulting in approximately 70% suppression of the targeted gene for green fluorescent protein.

siRNA-PEG Nanoparticle-Based Delivery

Bioneer's patented siRNA-PEG nanoparticle-based delivery system has been developed to overcome many of the obstacles of siRNA delivery. In this novel and efficient delivery system, the synthetic siRNA is conjugated to polyethylene glycol (PEG) via a disulfide linkage. siRNA-PEG nanoparticles are then generated by adding a cationic core forming agent which interacts with negative-charged siRNA to form the core of a nanoparticle. The outer layer of PEG protects siRNA from degradation by ribonuclease in serum and thus significantly extends the circulation time of siRNA in blood.

The disulfide linkage between siRNA and PEG was introduced to be cleaved specifically in a reductive condition of the cytoplasm. Because the redox-potential of an intracellular environment is about two orders of magnitude lower than that of an extracellular environment, the intact form of siRNA is released in the cytoplasm after cellular uptake. Release of intact siRNA in the cytoplasm is essential for efficient gene silencing.

The efficiency of the siRNA-PEG nanoparticle formulation has been demonstrated by evaluating anticancer property of VEGF-siRNA in human prostate carcinoma. The results showed that VEGF siRNA-PEG nanoparticles almost completely inhibited the expression of secreted VEGF in a human prostate cancer cell line. More importantly, the tail vein injection of VEGF siRNA-PEG nanoparticles dramatically inhibited tumor growth in a PC3 tumor xenograft model, which demonstrated that siRNA-PEG nanoparticles are effective as a delivery vehicle for in vivo experiments.

The interaction between PEG-conjugated VEGF siRNA and PEI was shown to lead to the spontaneous formation of nanoscale polyelectrolyte complex (PEC) micelles (VEGF siRNA-PEG/PEI PEC micelles), having a characteristic siRNA/ PEI PEC inner core with a surrounding PEG shell layer (Kim et al. 2008). Intravenous as well as intratumoral administration of the PEC micelles significantly inhibited VEGF expression at the tumor tissue and suppressed tumor growth in an animal tumor model without showing any detectable inflammatory responses in mice. Following intravenous injection, enhanced accumulation of the PEC micelles was also observed in the tumor region. This study demonstrates the feasibility of using PEC micelles as a potential carrier for therapeutic siRNAs in local and systemic treatment of cancer.

Polycation-Based Nanoparticles for siRNA Delivery

Polycation-based nanoparticles (polyplexes) formed by self-assembly with RNA can be used to modulate pharmacokinetics and intracellular trafficking to improve the therapeutic efficacy of RNAi-based therapeutics (Howard 2009). Polyplexes can be used for extracellular and intracellular delivery of synthetic RNA molecules. Flexibility in design and a capability to introduce different functional groups into a wide range of polymer types, adds multifunctional properties needed to fulfill delivery requirements. Surface modification with PEG during polyplex self-assembly has been used for steric stabilization and results in 'stealth-like' nanoparticles that reduce serum protein interactions and capture by the mononuclear phagocyte system.

Endosomolytic and cleavable polymers can be built into the design of siRNA polyplexes to facilitate cytosolic release of siRNA needed to permit siRNA interaction with the intracellular target. Endosomal buffering, pH-activated polymers and membrane interactive peptides, which allow endosomal escape and transport to the cytosol, can be used to overcome capture within the endosomal-lysosomal pathway associated with cellular endocytosis of nanoparticles. The advent of bioresponsive nanoparticles whose function is triggered by biological conditions is a method used to control spatial delivery. Nanoparticles composed of reducible disulfide-linked polycations cleaved in response to intracellular redox conditions is an exciting strategy to install extracellular stability whilst allowing for intracellular breakdown and maximal release of the siRNA cargo.

Calando's Technology for Targeted Delivery of Anticancer siRNA

Calando Pharmaceuticals combines its proprietary technologies in targeted polymeric delivery systems and siRNA design to create effective therapeutics. Cyclodextrin-containing polymers form the foundation for a two-part siRNA delivery system. The first component is a linear, cyclodextrin-containing polycation that, when mixed with siRNA binds to the anionic "backbone" of the siRNA. The polymer and siRNA self-assemble into nanoparticles of approximately 50 nm diameter that fully protect the siRNA from nuclease degradation in serum. The cyclodextrin in the polymer enables the surface of the particles to be decorated by stabilizing agents and targeting ligands.

CALAA01 (Calando Pharmaceuticals) employs a novel nanoparticle delivery system containing non-chemically modified siRNA and a transferrin (Tf) protein targeting agent formulated with RONDELTM (RNA/Oligonucleotide Nanoparticle Delivery). The effects of administering escalating, intravenous (IV) doses of targeted nanoparticles CALAA01 targeting the M2 subunit of ribonucleotide reductase to nonhuman primates have been studied (Heidel et al. 2007a). The data show that multiple, systemic doses of targeted nanoparticles containing nonchemically modified siRNA can safely be administered to nonhuman primates. Further studies have shown that CALAA-01 exhibits significant antiproliferative activity in cancer cells of varying human type and species (mouse, rat, monkey); these findings

suggest that this duplex is a promising candidate for therapeutic development (Heidel et al. 2007b). Results from the initial phase I clinical trial where 24 patients with different cancers were treated with CALAA-01 were compared to data obtained from multispecies animal studies to provide a detailed example of translating this class of nanoparticles from animals to humans (Zuckerman et al. 2014). The pharmacokinetics of CALAA-01 in mice, rats, monkeys, and humans show IV administration correlates with body weight across all species. The safety profile of CALAA-01 in animals is similarly obtained in humans except that animal kidney toxicities are not observed in humans; this could be due to the use of a predosing hydration protocol used in the clinic. Taken in total, the animal models do appear to predict the behavior of CALAA-01 in humans.

Self-Assembling Nanoplatform for Delivery of siRNA

The NF-κB signaling pathway is implicated in various inflammatory diseases, including RA. Given that NF-kB signaling is critical for many immune cell functions, systemic blockade of this pathway may lead to detrimental side effects. siR-NAs coupled with a safe and effective delivery nanoplatform may afford the specificity lacking in systemic administration of small-molecule inhibitors. A melittin-derived cationic amphipathic peptide combined with siRNA targeting the p65 subunit of NF-kB (p5RHH-p65) noncovalently self-assemble into stable nanocomplexes that home to the inflamed joints in a murine model of RA (Zhou et al. 2014). Specifically, administration of p5RHH-p65 siRNA nanocomplexes abrogated inflammatory cytokine expression and cellular influx into the joints, protected against bone erosions, and preserved cartilage integrity. The p5RHH-p65 siRNA nanocomplexes potently suppressed early inflammatory arthritis without affecting p65 expression in off-target organs or eliciting a humoral response after serial injections. These data suggest that this self-assembling, largely nontoxic platform may have broad utility for the specific delivery of siRNA to target and limit inflammatory processes for the treatment of a variety of diseases. The nanoparticle formulation is critical for the success of the agent, because even though free siRNA localizes to the intended site (inflamed joints), it exhibits no gene silencing activity. This is likely because siRNA packaged as p5RHH nanocomplexes gained access to the cell cytoplasm through micropinocytosis, while the free siRNA could not. Taken together, these results suggest that this platform, with its relative site-specific gene silencing activity combined with minimal off-target toxicities, may have real translational potential for the treatment of many inflammatory processes beyond arthritis.

Topical Delivery of siRNA-Nanoparticle Conjugates

Topical application of nucleic acids offers many potential therapeutic advantages for suppressing genes in the skin, and potentially for systemic gene delivery. However, the epidermal barrier usually precludes entry of gene-suppressing therapy unless the barrier is disrupted. Spherical nucleic acid nanoparticle conjugates (SNA-NCs), gold cores surrounded by a dense shell of highly oriented, covalently immobilized siRNA, freely penetrate almost 100% of keratinocytes in vitro, mouse skin, and human epidermis within hours after application (Zheng et al. 2012). Significantly, these structures can be delivered in a commercial moisturizer or phosphate-buffered saline, and do not require barrier disruption or transfection agents, such as liposomes, peptides, or viruses. SNA-NCs targeting epidermal growth factor receptor (EGFR), an important gene for epidermal homeostasis, are >100-fold more potent and suppress longer than siRNA delivered with commercial lipid agents in cultured keratinocytes. Topical delivery of 1.5 uM EGFR siRNA for 3 week to hairless mouse skin almost completely abolishes EGFR expression, suppresses downstream ERK phosphorylation, and reduces epidermal thickness by almost 40%. Similarly, EGFR mRNA in human skin equivalents is reduced by 52% after 60 h of treatment with 25 nM EGFR SNA-NCs. Treated skin shows no clinical or histological evidence of toxicity. No cytokine activation in mouse blood or tissue samples is observed, and after 3 week of topical skin treatment, the SNA structures are virtually undetectable in internal organs. SNA-NC structure is highly tailorable and the gold core can serve as a scaffold for multicomponent functionalization, not just with siRNAs, but with targeting antibodies or peptides, and small molecule drugs as well. SNA conjugates may be promising agents for personalized, topically delivered gene therapy of cutaneous tumors, skin inflammation, and dominant negative genetic skin disorders.

Quantum Dots to Monitor RNAi Delivery

A critical issue in using RNA interference (RNAi) for identifying genotype/phenotype correlations is the uniformity of gene silencing within a cell population. Variations in transfection efficiency, delivery-induced cytotoxicity and 'off target' effects at high siRNA concentrations can confound the interpretation of functional studies. To address this problem, a method of monitoring siRNA delivery has been developed that combines unmodified siRNA with seminconductor quantum dots (QDs) as multi-color biological probes. siRNA is co-transfected with QDs using standard transfection techniques, thereby leveraging the photostable fluorescent nanoparticles to track delivery of nucleic acid, sort cells by degree of transfection and purify homogenously-silenced subpopulations. Compared to alternative RNAi tracking methods (co-delivery of reporter plasmids and end-labeling the siRNA), QDs exhibit superior photostability and tunable optical properties for an extensive selection of non-overlapping colors. This simple, modular system can be used for multiplexed gene knockdown studies, as demonstrated in a two-color proof-ofprinciple study with two biological targets. When the method is applied to investigate the functional role of T-cadherin (T-cad) in cell-cell communication, a subpopulation of highly silenced cells obtained by QD labeling is required to observe significant downstream effects of gene knockdown. QDs are compatible with a variety of transfection techniques (other reagents, electroporation and microinjection) and therefore amenable to nucleic acid monitoring in cells that are susceptible to liposome-triggered cytotoxicity. Primary cells may be particularly suited to benefit from this method, as nonviral delivery of siRNA has been technically difficult.

RNAi-Based Nanomedicines for Gene Silencing in Hematological Malignancies

Silence gene expression in leukocytes has great potential for identifying drug targets and for RNAi-based therapy for leukocyte diseases, but systemic siRNA delivery to leukocytes remains challenging. Both normal and malignant leukocytes are among the most difficult targets for siRNA delivery as they are resistant to conventional transfection reagents and are dispersed in the body. Down-regulation of cyclin D1 using RNAi is a potential therapeutic approach to this malignancy. Mantle cell lymphoma (MCL), an aggressive B-cell lymphoma that overexpresses cyclin D1 with relatively poor prognosis, was used as a prototypic blood cancer for validating a novel siRNA delivery strategy (Weinstein et al. 2016). The authors designed lipidbased nanoparticles (LNPs) coated with anti-CD38 MAbs that are specifically taken up by human MCL cells in the bone marrow of xenografted mice. When loaded with siRNAs against cyclin D1, CD38-targeted LNPs they induced gene silencing in MCL cells and prolonged survival of tumor-bearing mice with no observed adverse effects. These results highlight the therapeutic potential of cyclin D1 therapy in MCL and present a novel RNAi delivery system that opens new therapeutic opportunities for treating MCL and may be applied to other hematological malignancies.

Lipid Nanoparticles for mRNA Delivery

In vitro transcribed messenger RNA (mRNA) is a potential therapeutic platform but effective delivery of mRNA to specific cell types and tissues is needed. Lipid nanoparticles (LNPs) are efficient carriers for siRNAs and have entered clinical trials. However, little is known about the potential of LNPs to deliver mRNA. To investigate this mRNA-LNPs were generated by incorporating HPLC purified, 1-methylpseudouridine-containing mRNA comprising codon-optimized firefly luciferase into stable LNPs (Pardi et al. 2015). Mice were injected with 0.005–0.250 mg/kg doses of mRNA-LNPs by 6 different routes and high levels of protein translation could be measured using in vivo imaging. Subcutaneous, intramuscular and intradermal injection of the LNP-encapsulated mRNA translated locally at the site of injection for up to 10 days. High levels of protein production lasting several days could be achieved in the lung from the intratracheal administration of mRNA. Intravenous and intraperitoneal and to a lesser extent intramuscular and

intratracheal deliveries led to trafficking of mRNA-LNPs systemically resulting in active translation of the mRNA in the liver for 1–4 days. These results demonstrate that LNPs are appropriate carriers for mRNA in vivo and have the potential to become valuable tools for delivering mRNA encoding therapeutic proteins.

References

- Bonoiu AC, Mahajan SD, Ding H, et al. Nanotechnology approach for drug addiction therapy: gene silencing using delivery of gold nanorod-siRNA nanoplex in dopaminergic neurons. Proc Natl Acad Sci U S A. 2009;106:5546–50.
- Bryson JM, Fichter KM, Chu WJ, et al. Polymer beacons for luminescence and magnetic resonance imaging of DNA delivery. Proc Natl Acad Sci U S A. 2009;106:16913–8.
- Chahal JS, Khan OF, Cooper CL, et al. Dendrimer-RNA nanoparticles generate protective immunity against lethal Ebola, H1N1 influenza, and toxoplasma gondii challenges with a single dose. Proc Natl Acad Sci U S A. 2016;113:E4133–42.
- Delyagina E, Li W, Ma N, Steinhoff G. Magnetic targeting strategies in gene delivery. Nanomedicine (Lond). 2011;6(9):1593–604.
- Glover DJ, Ng SM, Mechler A, et al. Multifunctional protein nanocarriers for targeted nuclear gene delivery in nondividing cells. FASEB J. 2009;23:2996–3006.
- Graf A, Jack KS, Whittaker AK, et al. Protein delivery using nanoparticles based on microemulsions with different structure-types. Eur J Pharm Sci. 2008;33:434–44.
- Heidel JD, Yu Z, Liu J, et al. Administration in non-human primates of escalating intravenous doses of targeted nanoparticles containing ribonucleotide reductase subunit M2 siRNA. Proc Natl Acad Sci U S A. 2007a;104:5715–21.
- Heidel JD, Liu JY, Yen Y, et al. Potent siRNA inhibitors of ribonucleotide reductase subunit RRM2 reduce cell proliferation in vitro and in vivo. Clin Cancer Res. 2007b;13:2207–15.
- Howard KA. Delivery of RNA interference therapeutics using polycation-based nanoparticles. Adv Drug Deliv Rev. 2009;61:710–20.
- Jain KK. Cell therapy: technologies, markets & companies. Basel: Jain PharmaBiotech Publications; 2017a.
- Jain KK. Gene Therapy: technologies, markets and companies. Basel: Jain PharmaBiotech Publications; 2017b.
- Jayakumar MK, Idris NM, Zhang Y. Remote activation of biomolecules in deep tissues using nearinfrared-to-UV upconversion nanotransducers. Proc Natl Acad Sci U S A. 2012;109:8483–8.
- Jiang X, Qu W, Pan D. Plasmid-templated shape control of condensed DNA-block copolymer nanoparticles. Adv Mater. 2013;25:227–32.
- Johnson PE, Muttil P, MacKenzie D, et al. Spray-dried multiscale nano-biocomposites containing living cells. ACS Nano. 2015;9:6961–77.
- Kasala D, Yoon AR, Hong J, et al. Evolving lessons on nanomaterial-coated viral vectors for local and systemic gene therapy. Nanomedicine (Lond). 2016;11:1689–713.
- Kim SH, Jeong JH, Lee SH, et al. Local and systemic delivery of VEGF siRNA using polyelectrolyte complex micelles for effective treatment of cancer. J Control Release. 2008;129:107–16.
- Kim JS, Kang SJ, Jeong HY, et al. Anti-EGFR immunonanoparticles containing IL12 and salmosin genes for targeted cancer gene therapy. Int J Oncol. 2016;49:1130–8.
- Kommareddy S, Amiji M. Antiangiogenic gene therapy with systemically administered sFlt-1 plasmid DNA in engineered gelatin-based nanovectors. Cancer Gene Ther. 2007;14:488–98.
- Moon JJ, Suh H, Li AV, et al. Enhancing humoral responses to a malaria antigen with nanoparticle vaccines that expand Tfh cells and promote germinal center induction. Proc Natl Acad Sci U S A. 2012;109:1080–5.

- Nguyen DN, Mahon KP, Chikh G, et al. Lipid-derived nanoparticles for immunostimulatory RNA adjuvant delivery. Proc Natl Acad Sci U S A. 2012;109:E797–803.
- Nuhn L, Vanparijs N, De Beuckelaer A, et al. pH-degradable imidazoquinoline-ligated nanogels for lymph node-focused immune activation. Proc Natl Acad Sci U S A. 2016;113:8098–103.
- O'Brien JA, Lummis SC. Nano-biolistics: a method of biolistic transfection of cells and tissues using a gene gun with novel nanometer-sized projectiles. BMC Biotechnol. 2011;11:66.
- Paleos CM, Tziveleka LA, Sideratou Z, Tsiourvas D. Gene delivery using functional dendritic polymers. Expert Opin Drug Deliv. 2009;6:27–38.
- Pardi N, Tuyishime S, Muramatsu H, et al. Expression kinetics of nucleoside-modified mRNA delivered in lipid nanoparticles to mice by various routes. J Control Release. 2015;217:345–51.
- Rosi NL, Giljohann DA, Thaxton CS, et al. Oligonucleotide-modified gold nanoparticles for intracellular gene regulation. Science. 2006;312:1027–30.
- Seth A, Oh DB, Lim YT. Nanomaterials for enhanced immunity as an innovative paradigm in nanomedicine. Nanomedicine (Lond). 2015;10:959–75.
- Sirsi SR, Schray RC, Wheatley MA, Lutz GJ. Formulation of polylactide-co-glycolic acid nanospheres for encapsulation and sustained release of poly(ethylene imine)-poly(ethylene glycol) copolymers complexed to oligonucleotides. J Nanobiotechnology. 2009;7:1.
- Swami A, Kurupati RK, Pathak A, et al. A unique and highly efficient non-viral DNA/siRNA delivery system based on PEI-bisepoxide nanoparticles. Biochem Biophys Res Commun. 2007;362:835.
- Weinstein S, Toker IA, Emmanuel R, et al. Harnessing RNAi-based nanomedicines for therapeutic gene silencing in B-cell malignancies. Proc Natl Acad Sci U S A. 2016;113:E16–22.
- Yuan X, Naguib S, Wu Z. Recent advances of siRNA delivery by nanoparticles. Expert Opin Drug Deliv. 2011;8:521–36.
- Zhang P, Chen Y, Zeng Y, et al. Virus-mimetic nanovesicles as a versatile antigen-delivery system. Proc Natl Acad Sci U S A. 2015;112:E6129–38.
- Zhao Y, Vivero-Escoto JL, Slowing II, et al. Capped mesoporous silica nanoparticles as stimuliresponsive controlled release systems for intracellular drug/gene delivery. Expert Opin Drug Deliv. 2010;7:1013–29.
- Zheng D, Giljohann DA, Chen DL, et al. Topical delivery of siRNA-based spherical nucleic acid nanoparticle conjugates for gene regulation. Proc Natl Acad Sci U S A. 2012;109:11975–80.
- Zhou HF, Yan H, Pan H, et al. Peptide-siRNA nanocomplexes targeting NF-κB subunit p65 suppress nascent experimental arthritis. J Clin Invest. 2014;124:4363–74.
- Zuckerman JE, Gritli I, Tolcher A, et al. Correlating animal and human phase Ia/Ib clinical data with CALAA-01, a targeted, polymer-based nanoparticle containing siRNA. Proc Natl Acad Sci U S A. 2014;111:11449–54.

Chapter 7 Nanodevices and Techniques for Clinical Applications

Introduction

This chapter contains use of technologies for clinical applications in general. More detailed description of these technologies will be given in chapters dealing with special therapeutic areas.

Clinical Nanodiagnostics

Role of nanotechnology in molecular diagnostics was discussed in Chap. 4. This will have a tremendous impact on the practice of medicine. Biosensor systems based on nanotechnology could detect emerging disease in the body at a stage that may be curable. This is extremely important in management of infections and cancer. Some of the body functions and responses to treatment will be monitored without cumbersome laboratory equipment. Some examples are a radiotransmitter small enough to put into a cell and acoustical devices to measure and record the noise a heart makes.

Nano-endoscopy

Endoscopic microcapsules are being developed that can be ingested and precisely positioned in the gastrointestinal system by nanorobotic techniques. A control system allows a capsule to attach to the walls of the digestive tract and move within its lumen. Several different methods are being researched for the attachment of microcapsules including both dry and wet adhesion as well as mechanical methods such as a set of tripod legs with adhesive on feet. Simple models with surface characteristics like that of the digestive tract are being constructed to test these methods.

Precisely positioned microcapsules would enable physicians to view any part of the inside lining of the digestive tract in detail resulting in more efficient, accurate, and less invasive diagnosis. In addition, these capsules could be modified to include treatment mechanisms as well, such as the release of a drug or chemical near an abnormal area.

PillCam® capsule endoscope (Medtronic Inc), a tool to visualize small intestine abnormalities, was approved in 2001 and more than one million patients worldwide have benefited from PillCam capsule endoscopy. It is now the gold standard for small bowel visualization. Other companies are now producing ingestible capsules for this purpose. The patient ingests the capsule, which contains a tiny camera and intestinal peristalsis propels the capsule for approximately 8 h. During this time, the camera snaps the pictures and images that are transmitted to a data recorder worn by the patient. The physicians can review the images later to make the diagnosis. Controlling the positioning and movement on a nanoscale greatly improves the accuracy of this method. Video capsule endoscopy is a major innovation that provides high-resolution imaging of the entire small intestine in its entirety. Capsule endoscopy is the first-line investigation in patients with obscure gastrointestinal bleeding after a negative esophagogastroduodenoscopy and colonoscopy, and it has a positive impact on the outcome. Video capsule endoscopy is also useful in the evaluation of inflammatory and neoplastic disorders of the small bowel.

Colon Capsule Endoscopy represents a new diagnostic technology for colonic exploration and there are still some controversies. A conference has critically evaluated the available results obtained by Colon Capsule Endoscopy in clinical studies, to identify the proper test indications, and proposed a shared preparation protocol and Colon Capsule Endoscopy procedure (Spada et al. 2011).

The so called "gutbots" are based on nanotechnology including nanosensors and sticking devices. If such devices are successful, their use may be extended to the large intestine. Although colon is currently examined by colonoscopy, physicians might be interested in introducing a pill-sized camera through the anus to visualize the suspicious area. Similar nanorobots are under development for other parts of the body.

Application of Nanotechnology in Radiology

X-ray radiation is widely used in medical diagnosis. The basic design of the x-ray tube has not changed significantly in the last century. Now medical diagnostic x-ray radiation can be generated using CNT-based field emission cathode. The device can readily produce both continuous and pulsed X-rays with programmable wave form and repetition rate. The x-ray intensity is sufficient to image a human extremity. The CNT-based cold-cathode x-ray technology can potentially lead to portable and miniature X-ray sources for industrial and medical applications

Xintek Inc. (Research Triangle Park, NC) has invented a new X-ray device based on CNT that emits a scanning X-ray beam composed of multiple smaller beams while also remaining stationary. Therefore, the device can create images of objects from numerous angles and without mechanical motion, which is a distinct advantage for any machine since it increases imaging speed, can reduce the size of the device and requires less maintenance. This technology can lead to smaller and faster X-ray imaging systems for tomographic medical imaging such as CT scanners. Other advantages will be that scanners will be cheaper, use less electricity and produce higher-resolution images. This new technology enables the generation of digitized x-ray radiation with fine control of the spatial distribution of the x-ray pixels and temporal modulation of the radiation. The additional degrees of freedom in the source configuration will enable system vendors to design imaging systems with enhanced performance and new capabilities. The technology enables the design of stationary tomography imaging systems with faster scanning speed and potentially better imaging quality compared to currently available commercial scanners. Xintek's Field Emission X-ray technology is used for diagnostic medical imaging and in vivo imaging of small animal models for preclinical cancer studies.

High-Resolution Ultrasound Imaging Using Nanoparticles

Early diagnoses would involve using nanotechnology to improve the quality of images produced by one of the most common diagnostic tools used in physicians' offices – the ultrasound machine. In an experimental study, mice were injected intravenously with silica nanospheres (100 nm) in a suspension dispersed in agarose and imaged by a high-resolution ultrasound imaging system (Liu et al. 2006). B-mode images of the livers were acquired at different time points after particle injection. An automated computer program was used to quantify the grey scale changes. Ultrasonic reflections were observed from nanoparticle suspensions in agarose gels. The image brightness, i.e. mean grey scale level, increased with particle size and concentration. The mean grey scale of mouse livers also increased following particle administration. These results indicated that it is feasible to use solid nanoparticles as contrast enhancing agents for ultrasonic imaging. The long-term goal is to use this technology to improve the ability to identify very early cancers and other diseases. The aim is to identify disease at its cellular level, at its very earliest stage.

Another study has demonstrated improvement of a pulsed magneto-motive ultrasound (pMMUS) image quality by using large size superparamagnetic nanoclusters characterized by strong magnetization per particle (Mehrmohammadi et al. 2011). Water-soluble magnetic nanoclusters of two sizes (15 and 55 nm) were synthesized from 3 nm iron precursors in the presence of citrate capping ligand. The size distribution of synthesized nanoclusters and individual nanoparticles was characterized using dynamic light scattering analysis and TEM. Tissue mimicking phantoms containing single nanoparticles and two sizes of nanoclusters were imaged using a custom-built pMMUS imaging system. While the magnetic properties of citratecoated nanoclusters are identical to those of superparamagnetic nanoparticles, the magneto-motive signal detected from nanoclusters was larger, i.e. the same magnetic field produced larger magnetically induced displacement. Therefore, this study demonstrated that clusters of superparamagnetic nanoparticles result in pMMUS images with higher contrast and SNR.

Nanobiotechnology in Tissue Engineering

Tissue engineering is an interdisciplinary field, which applies the principles of engineering and the life sciences to the development of biological substitutes that restore, maintain or improve tissue function. Tissue engineering is an emerging field between traditional medical devices and regular pharmaceuticals. It faces many challenges and it is also a field that is extremely interdisciplinary requiring the efforts of physicians, cell biologists, material scientists, chemical engineers, and chemists. Apart from the use of nanoparticles for diagnostic and therapeutic purposes, nanotechnology has applications for the development of tissue engineering as indicated by some of the studies in life sciences.

The response of cell motility and metabolism to changes in substrates has been thoroughly studied in the past decade. Size, structure, geometry, integrin-binding and other factors have all been investigated. Various techniques have been employed to create micropatterned surfaces of different materials to study cell behavior. In the presence of patterned stripes of bovine serum albumin and laminin, Schwann cells aggregate preferentially on the laminin regions. Osteogenic cells have been cultured in 3D nanohydroxyapatite/collagen matrix, which is precipitated such a manner that hydroxyapatite crystals are uniformly distributed in a matrix of collagen, seemingly ideal for bone construction.

Microfluidic devices enable the study of methods for patterning cells, topographical control over cells and tissues, and bioreactors. They have not been used extensively in tissue engineering but major contributions are expected in two areas. The first is growth of complex tissue, where microfluidic structures ensure a steady blood supply, thereby circumventing the well-known problem of providing larger tissue structures with a continuous flow of oxygen as well as nutrition and removal of waste products. The second and probably more important function of microfluidics, combined with micro/nanotechnology, lies in the development of in vitro physiological systems for studying fundamental biological phenomena.

Nanoscale Surfaces for Stem Cell Culture

Adult stem cells spontaneously differentiate in culture, resulting in a rapid diminution of the multipotent cell population and their regenerative capacity. There is currently an unmet need for the supply of autologous, patient-specific stem cells for regenerative therapies in the clinic. MSC differentiation can be driven by the material/cell interface suggesting a unique opportunity for manipulating stem cells in the absence of complex soluble chemistries or cellular reprogramming. A nanostructured surface has been identified that retains stem-cell phenotype and maintains stem-cell growth over 8 weeks (McMurray et al. 2011). The authors had previously designed and produced a polycaprolactone-based support with nanoscale features that enabled osteogenesis from stem and progenitor mesenchymal populations cultured in osteogenic media. In the current study, by reduction of the level of offset to as close to zero as possible, the resulting nanotopography induced a switch from osteogenic stimulation to a surface conducive to MSC growth while allowing prolonged retention of MSC biomarkers and multipotency. The authors postulate that nanoscale modifications to surface topography alter the interaction of integrin receptors within cell adhesions, resulting in changes in intracellular tension. The demonstrable sensitivity of MSCs to materials, with <50 nm alterations in feature placement and the role of such defined topographies on cell fate and function, offers nanoscale patterning as a powerful tool for the noninvasive manipulation of stem cells. By incorporating nanoscale features into tissue-engineering scaffolds that support reservoirs of progenitor cells for a range of tissue-specific stem cell types, this approach can improve the regenerative capacity of in vitro-fabricated tissue and organs.

3D Nanofilament-Based Scaffolds

Ideally the tissue-engineering scaffolds should be analogous to native extracellular matrix (ECM) in terms of both chemical composition and physical structure. Polymeric nanofiber matrix is similar, with its nanoscaled nonwoven fibrous ECM proteins, and thus is a candidate ECM-mimetic material. Scaffolds for tissue engineering are typically solid or porous materials with isotropic characteristics and present regenerative cues such as growth factors or extracellular matrix proteins but these do not explicitly guide tissue regeneration. Novel 3D nanofilament-based scaffolds have been developed for tissue regeneration. This mimics the strategy used by collagen and other fibrillar structures to guide cell migration or tissue development and/or regeneration in a guided, direction-sensitive manner. The critical advantage of this technology is that it provides directional cues for cell and tissue regeneration. This strategy can be used to guide the migration of endogenous or transplanted cells and tissues to damaged tissues of the peripheral and central nervous systems to restore function, but could also be applied to tissue engineering.

The development of effective biological scaffold materials for tissue engineering and regenerative medicine applications hinges on the ability to present precise environmental cues to specific cell populations to guide their position and function. Natural extracellular matrices have an ordered nanoscale structure that can modulate cell behaviors critical for developmental control, including directional cell motility. A method has been described for fabricating fibrin gels with defined architecture on the nanometer scale in which magnetic forces are used to position thrombin-coated magnetic microbeads in a defined 2D array and thereby guide the self-assembly of fibrin fibrils through catalytic cleavage of soluble fibrinogen substrate (Alsberg et al. 2006). Time-lapse and confocal microscopy confirmed that fibrin fibrils nucleate near the surface of the thrombin-coated beads and extend out in a radial direction to form these gels. When controlled magnetic fields were used to position the beads in hexagonal arrays, the fibrin nanofibrils that polymerized from the beads oriented preferentially along the bead-bead axes in a geodesic (minimal path) pattern. These biocompatible scaffolds supported adhesion and spreading of human microvascular endothelial cells, which exhibited co-alignment of internal actin stress fibers with underlying fibrin nanofibrils within some membrane extensions at the cell periphery. This magnetically-guided, biologically-inspired microfabrication system is unique in that large scaffolds may be formed with little starting material, and thus it may be useful for in vivo tissue engineering applications in the future.

In addition to fabricating 3D microfabricated scaffolds as templates for cell aggregate formation nanoscale technologies can be used for controlling the features such as shape and pore architecture, as templates for microtissue formation, or as improved bioreactors. The nanoscale control of cellular environments can also be used to probe the influence of the spatial and temporal effects of specific cell-cell, cell-extracellular matrix, and cell-soluble factor interactions.

Electrospinning Technology for Nanobiofabrication

Jet-based technologies are increasingly being explored as potential high-throughput and high-resolution methods for the manipulation of biological materials. Previously shown to be of use in generating scaffolds from biocompatible materials, electrospinning technology has been used to deposit active biological threads and scaffolds comprised of living cells. This has been achieved by use of a coaxial needle arrangement where a concentrated living biosuspension flows through the inner needle and a medical-grade poly(dimethylsiloxane) medium with high viscosity and low electrical conductivity flows through the outer needle. Cells cultured after electrospinning were shown to be viable with no evidence of having incurred any cellular damage during the nanobiofabrication process. This demonstrates the feasibility of using coaxial electrospinning technology for biological and biomedical applications requiring the deposition of living cells as composite nanothreads for forming active biological scaffolds. The process could enable significant advances to be made in technologies ranging from tissue engineering to regenerative medicine. Perhaps in the future such living nanothreads might be spun directly into wounds.

Organogenesis Inc is developing electrospinning technology makes it possible to mimic the 3D architectural structure that is essential for the body's natural growth and repair processes to develop designer scaffolds for the purposes of regenerative. An implantable scaffold with the correct nanofiber diameter, orientation and architecture, is virtually indistinguishable from native tissue and is recognized as "self" by the body and facilitates regeneration. Electrospinning techniques have also been used to produce a variety of material, including vascular grafts, nerve guides, tendon and skin.

Nanomaterials for Tissue Engineering

Several nanomaterials, particularly nanofibers, have been investigated for use as scaffolds in tissue engineering. A naturally occurring nanofiber- and nanoparticlebased nanocomposite from the adhesive of Sundew can be used for tissue engineering, and opens the possibility for further examination of natural plant adhesives for biomedical applications (Zhang et al. 2010). Tissue engineering of skeletal muscle is a promising method for the treatment of soft tissue defects in reconstructive surgery. Nanomaterials are useful for this purpose.

Carbon Nanotubes for Artificial Muscles

Research on multiwalled CNTs (MWCNTs) could lead to new materials that will mimic biological tissues and artificial muscles. MWCNTs can withstand repeated stress and still can retain their structural and mechanical integrity, like the behavior of soft tissue. Under repeated high compressive strains, long, vertically aligned MWCNTs exhibit viscoelastic behavior like that observed in soft-tissue membranes. Under compressive cyclic loading, the mechanical response of the nanotube arrays shows preconditioning, characteristic viscoelasticity-induced rhysteresis, nonlinear elasticity and stress relaxation, and large deformations. Furthermore, no fatigue failure is observed at high strain amplitudes up to half a million cycles. This combination of soft-tissue-like behavior and outstanding fatigue resistance suggests that properly engineered nanotube structures could mimic artificial tissues, and that their good electrical conductivity could lead to their use as compliant electrical contacts in a variety of applications. The springiness is like real muscles' ability to return to their original shapes over a lifetime of perpetual extension and contraction. Because real muscles create a smoother motion than jerky electric motors or pneumatic devices, some of the new materials would be used to power robots and prosthetic limbs, as well as artificial tissue for implantation. MWCNTs are being combined with different polymers, which control when an artificial muscle gets stretched, to improve their resistance to fatigue.

Nanofibers for Tissue Engineering of Skeletal Muscle

Rapid lysis and contraction of pure collagen I- or fibrin-matrices have been a problem in the past efforts for tissue engineering of skeletal muscle. This problem could be overcome by combining both materials as significant proliferation of cultivated myoblasts has been detected in collagen-I-fibrin matrices and collagen nanofibers. Seeding cells on parallel orientated nanofibers results in strongly aligned myoblasts. Collagen I-fibrin mixtures as well as collagen nanofibers yield good proliferation rates and myogenic differentiation of primary rat myoblasts in vitro (Beier et al. 2009). In addition, parallel orientated electrospun nanofibers enable the generation of aligned cell layers and therefore represent the most promising step towards successful engineering of skeletal muscle tissue.

Nanofibrous Scaffolds for Stem Cell-Based Regenerative Therapies

Nanofibrous scaffolds are being developed for stem cells, which mimic the nanometer-scale fibers normally found in that matrix. These biodegradable scaffolds can nurture stem cells derived from adipose tissue. Preadipocytes grown on 3D matrices acquire morphology and biological features of mature adipocytes. This culture model has significant utility for in vitro studies of adipocyte cell biology and development. Other studies in animal models have established the ability to develop bone grafts on electrospun nanofibrous scaffolds in a well-vascularized site using MSCs.

A challenge in vascular tissue engineering is to develop optimal scaffolds and establish expandable cell sources for the construction of tissue-engineered vascular grafts that are nonthrombogenic and have long-term patency. Tissue-engineered vascular grafts have been used as a model to demonstrate the potential of combining nanofibrous scaffolds and bone marrow MSCs for vascular tissue engineering (Hashi et al. 2007). Biodegradable nanofibrous scaffolds with aligned nanofibers were used to mimic native collagen fibrils to guide cell organization in vascular grafts. The results from artery bypass experiments showed that nanofibrous scaffolds allowed efficient infiltration of vascular cells and matrix remodeling. Acellular grafts (without MSCs) resulted in significant intimal thickening, whereas cellular grafts (with MSCs) had excellent long-term patency and exhibited well organized layers of endothelial cells (ECs) and smooth muscle cells (SMCs), as in native arteries. Short-term experiments showed that nanofibrous scaffolds alone induced platelet adhesion and thrombus formation, which was suppressed by MSC seeding. In addition, MSCs, as ECs, resisted platelet adhesion in vitro, which depended on cellsurface heparan sulfate proteoglycans. These data, together with the observation on the short-term engraftment of MSCs, suggest that the long-term patency of cellular grafts may be attributed to the antithrombogenic property of MSCs. These results demonstrate several favorable characteristics of nanofibrous scaffolds, the excellent patency of small-diameter nanofibrous vascular grafts, and the unique antithrombogenic property of MSCs.

Nanomaterials for Combining Tissue Engineering and Drug Delivery

A variety of organic and inorganic nanostructures have been developed for scaffolds in tissue regeneration as well as drug delivery. These nanostructures provide favorable biological integration of implants and have applications in many areas, including orthopedics, cardiovascular medicine, and ophthalmology. Additionally, these nanostructures can deliver drugs in a localized and controlled manner, accounting for the short biological half-life, lack of long-term stability and tissue-selectivity, and potential toxicity of many therapeutic compounds. Elastin-like polypeptides (ELPs) are artificial polypeptides, derived from Val-Pro-Gly-Xaa-Gly (VPGXG) pentapeptide repeats found in human tropoelastin. The potential of ELPs to self-assemble into nanostructures in response to environmental triggers is another interesting feature of these polypeptides that promises to lead to a host of new applications. Genetically encodable ELPs are monodisperse, stimuli responsive, and biocompatible, properties that make them attractive for combining drug delivery and tissue engineering.

In sophisticated tissue engineering strategies, the biodegradable scaffold is preferred to serve as both a 3D substrate and a growth factor delivery vehicle to promote cellular activity and enhance tissue neogenesis. It is possible to fabricate tissue engineering scaffolds capable of controlled growth factor delivery whereby growth factor containing microspheres are incorporated into 3D scaffolds with good mechanical properties, well-interconnected macroporous and nanofibrous structures. The microspheres are uniformly distributed throughout the nanofibrous scaffold and their incorporation does not interfere the macro-, micro-, and nanostructures of the scaffold. The release kinetics of platelet-derived growth factor-BB (PDGF-BB) from microspheres and scaffolds has been investigated using PLGA50 microspheres. Incorporation of microspheres into scaffolds significantly reduces the initial burst release. Sustained release from several days to months has been achieved through different microspheres in scaffolds. Released PDGF-BB possesses biological activity as evidenced by stimulation of human gingival fibroblast DNA synthesis in vitro. The successful generation of 3D nanofibrous scaffold incorporating controlled-release factors indicates significant potential for more complex tissue regeneration.

Nanobiotechnology for Organ Replacement and Assisted Function

Several devices are used to repair, replace or assist the function of damaged organs such as kidneys. The technologies range from those for tissue repair to those for device to take over or assist the function of the damaged organs. The following sections include some examples of these applications.

Exosomes for Drug-Free Organ Transplants

Exosomes are nanovesicles shed by dendritic cells. They may hold the key to achieving transplant tolerance, i.e. the long-term acceptance of transplanted organs without the need for drugs. Exosomes are no larger than 65–100 nm; yet each contains a potent reserve of major histocompatibility complex (MHC) molecules – gene products that cells use to determine self from nonself. Millions of exosomes scurry about within the bloodstream, and while their function has been somewhat of a mystery, researchers are beginning to surmise that they play an important role in immune regulation and response.

Because certain dendritic cells have tolerance-enhancing qualities, several approaches under study involve giving recipients donor dendritic cells that have been modified in some way. The idea is that the modified donor cells would convince recipient cells that a transplanted organ from the same donor is not foreign. MHC-rich vesicles, siphoned from donor dendritic cells, are captured by recipient dendritic cells and processed in a manner important for cell-surface recognition. Thus, one can efficiently deliver donor antigen using the exosomes as a magic bullet. The exosomes that are caught by the dendritic cells of the spleen, the site where dendritic cells typically present antigens as bounty to T cells. However, these dendritic cells internalize the exosomes instead of displaying them to T cells despite the exosomes' rich endowment of donor MHC molecules. Once internalized, the exosomes are ushered inside larger vesicles, special endosomes called MHC-II enriched compartments, where they are processed with the dendritic cell's own MHC molecules. This hybrid MHC-II molecule, now loaded with a peptide of donor MHC, is then expressed on the cell's surface. As one family of MHC molecules, MHC-II serves as a beacon for a specific population of T cells called CD4+ T cells. Such cells are activated during chronic rejection in a process associated with the indirect pathway of immune recognition.

This finding is significant because current immunosuppression therapies used in the clinical setting are not able to efficiently prevent T cell activation via the indirect pathway. Perhaps the CD4+ T cells normally involved in this pathway would retreat from attack if they encountered a cell surface marker that is of both donor and recipient origin, such as that which is observed following the dendritic cell's internalization of the donor-derived exosomes. The process of internalizing the donor exosomes does not affect maturation of the dendritic cell. Only immature dendritic cells can capture antigens efficiently and are believed to participate in the induction of transplant tolerance. By contrast, once mature, dendritic cells can trigger T cell activation that leads to transplant rejection. Additional research will be required to determine whether donor-derived exosomes will enhance the likelihood that an organ transplant from the same donor will be accepted. Only a few research groups are engaged in active study of exosomes with most of the research taking place in Europe.

Nanobiotechnology and Organ-Assisting Devices

Organ assisting devices (OAD) is an emerging area for application of nanobiotechnology. This includes implants and other devices to assist or replace the impaired function of various organs. One example of this is restoration of function of the tympanic membrane of the ear by magnetically responsive nanoparticles. Other examples would be given in the later sections of this chapter.

Superparamagnetic iron oxide nanoparticles (SPIONs) composed of magnetite (Fe(3)O(4)) have been studied as vehicles for therapeutic molecule delivery to the inner ear and as a middle ear implant capable of producing biomechanically

relevant forces for auditory function. Magnetite SPIONs are synthesized, and then encapsulated in either silica or poly (D,L,-Lactide-co-glycolide) or obtained commercially with coatings of oleic acid or dextran. Permanent magnetic fields generate forces sufficient to pull them across tissue in several round window membrane models (in vitro cell culture, in vivo rat and guinea pig, and human temporal bone) or to embed them in middle ear epithelia. Biocompatibility has been investigated by light and electron microscopy, cell culture kinetics, and hair cell survival in organotypic cell culture and no measurable toxicity was found. A sinusoidal magnetic field applied to guinea pigs with SNP implanted in the middle ear resulted in displacements of the middle ear comparable to 90 dB SPL.

Nanosurgery

Miniaturization in Surgery

Historically surgery was macrosurgery and most of general surgery still involves gross manipulation of organs and tissues by human hands and hand-held instruments. Some branches of surgery such as ophthalmology and otorhinolaryngology started to miniaturize early and start using microsurgery. In the last quarter of twentieth century, miniaturization started to develop most branches of surgery. The basic feature was minimization of trauma to the body tissues during surgery. Trends were small incisions, laparoscopic surgery by fiberoptic visualization through tubular devices, vascular surgery by catheters and microsurgery under operating microscopes to refine the procedures and reduce trauma. Many of the devices such as robotics and implants will be a part of this miniaturization process.

Nanotechnology for Hemostasis During Surgery

There are few effective methods to stop bleeding during surgery without causing tissue damage. More than 57 million Americans undergo nonelective surgery each year, and as much as 50% of surgical time is spent working to control bleeding. Current tools used to stop bleeding include clamps, pressure, cauterization, vaso-constriction and sponges. Some simple liquids composed of peptides, when applied to open wounds in rodents, self-assemble into a nanoscale protective barrier gel that seals the wound and stop bleeding in less than 15 s. Once the injury heals, the non-toxic gel is broken down into molecules that cells can use as building blocks for tissue repair. The exact mechanism of the action of such solutions is still unknown, but one explanation is that the peptides interact with the extracellular matrix surrounding the cells. The hemostatic action has been demonstrated in open wounds in several different types of tissue: brain, liver, skin, spinal cord and intestine.

Minimally Invasive Surgery Using Catheters

Surgery is continuously moving towards more minimally invasive methods. The main driver of this technical evolution is patient recovery: the lesser the trauma inflicted on the patient, the shorter is the recovery period. Minimally invasive surgery, often performed by use of catheters navigating the vascular system, implies that the operator has little to no tactile or physical information about the environment near or at the surgical site. This information can be provided by biosensors implanted in the catheters. Verimetra Inc. is developing such devices. Minimally invasive and in vivo surgery is limited by the ability to provide controllable and powerful motion at scales appropriate for navigation within the human body. Nanotechnology will play an important role in the construction of miniaturized biosensing devices. These sensors improve outcomes, lower risk and help control costs by providing the surgeon with real-time data about:

- Instrument force and performance
- Tissue density, temperature or chemistry
- · Better or faster methods of preparing tissue or cutting tissue
- Extracting tissue and fluids

Examples of procedures and applications where such an approach would be useful are:

- Cardiovascular surgery
- Stent insertion
- · Percutaneous transluminal coronary angioplasty
- Coronary artery bypass graft (CABG)
- Atrial fibrillation
- Cardiac surgery in utero
- Cerebrovascular surgery
- Surgery of intracranial aneurysms
- · Embolization of intracranial vascular malformations

Nanorobotics

Robotics is already developing for applications in life sciences and medicine. Robots can be programmed to perform routine surgical procedures. A device is being developed for facilitating minimally invasive intrapericardial interventions on the beating-heart (Riviere et al. 2004). This is based on the concept of an endoscopic robotic device that adheres to the epicardium by suction and navigates by crawling like an inchworm to any position on the surface under the control of a surgeon. This approach obviates cardiac stabilization, lung deflation, differential lung ventilation, and reinsertion of laparoscopic tools for accessing different treatment sites, thus offering the possibility of reduced trauma to the patient. The device has a working channel through which various tools can be introduced for treatment. The current prototype demonstrated successful prehension, turning, and locomotion on beating hearts in a limited number of trials in a porcine model.

A motor for in vivo microbot propulsion has been constructed with a diameter of 250 μ m, demonstrating the potential to directly drive a flagellum for swimming at up to 1295 rpm with a torque of 13 nN m (Watson et al. 2009). The motor uses coupled axial-torsional vibration at 652–682 kHz in a helically cut structure excited by a thickness-polarized piezoelectric element. The motor was named the "Proteus motor" after the miniature submarine that traveled through the human body in the science fiction movie, "Fantastic Voyage." The output power is 4.25 μ W, on the order of what is necessary to navigate small human arteries. This micromotor, small enough to be injected into the human bloodstream, could be used for a range of complex surgical operations necessary to treat stroke victims, confront hardened arteries or address blockages in the bloodstream.

Bacteria are the microrobots of nature and provide an inspiration for building mobile microrobots that can navigate through confined heterogenous environments and perform minimally invasive environmental and biomedical operations. An origami-inspired rapid prototyping process has been developed for building selffolding, magnetically powered microrobots with complex body plans, reconfigurable shape and controllable motility (Huang et al. 2016). As a model, the authors used Trypanosoma brucei, which has a long and slender form with a flagellum that propels it in a corkscrew motion through bodily fluids to penetrate the blood vessel endothelium and invade extracellular tissue. When it enters the blood stream, it uses a quorum-sensing mechanism to change morphology into a shorter, stumpier conformation that allows it to hide from the host. It can change between these forms depending on the environment. Bacteria were recreated using hydrogel and magnetic nanoparticles, which give these microrobots their bacteria-like morphology and provide them with motility once an electromagnetic field is applied. The microrobots designed based upon the plasticity found in T. brucei are soft, flexible and motorless, unlike conventional robotics, and change between conformations when heat from a laser is applied.

Selective reprogramming of the mechanical design and magnetic anisotropy of body parts dynamically modulates the swimming characteristics of the microrobots. The authors found that tail and body morphologies together determine swimming efficiency and, unlike for rigid swimmers, the choice of magnetic field can subtly change the motility of soft microswimmers. These microrobots could deliver therapy to sites in the body as part of a noninvasive approach in surgery.

Nanobiotechnology introduces another dimension in microrobotics leading to the development of nanorobots also referred to as nanobots. Instead of performing procedures from outside the body, nanobots will be miniaturized for introduction into the body through the vascular system or at the end of catheters into various vessels and other cavities in the human body. Surgical nanobot, programmed by a human surgeon, could act as an autonomous on site surgeon inside the human body. Various functions such as searching for pathology, diagnosis and removal or correction of the lesion by nanomanipulation can be performed and coordinated by an on-board computer. Such concepts, once science fiction, are now considered to be within the realm of possibility. Nanorobots will have the capability to perform precise and refined intracellular surgery which is beyond the capability of manipulations by the human hand.

However, before these robots are built on nanoscale, engineers must ensure that the nanoparticles are biodegradable and can be accurately localized to target areas using electromagnetic fields. Nevertheless, it is quite feasible that such devices will be in clinical use in the next decade.

Nanoscale Laser Surgery

Scalpel and needle may remain adequate instruments for most surgery work and biological compounds may still be needed to prod cells to certain actions. Introduction of lasers in surgery more than a quarter of century ago has already refined surgery and experimental biological procedures to enable manipulations beyond the capacity of the human hand held instruments. Laser microsurgery was used both for ablation and repair of tissues (Jain 1983). Mechanical devices such as microneedles are too large for the cellular scale, while biological and chemical tools can only act on the cell as a whole rather than on any one specific mitochondrion or other structure. Further developments are leading to manipulation of cellular structures at the micrometer and nanometer scale. This is opening the field of nanoscale laser surgery.

Femtosecond (one millionth of a billionth of a second) laser pulses can selectively cut a single strand in a single cell in the worm and selectively knock out the sense of smell. One can target a specific organelle inside a single cell (a mitochondrion, e.g. or a strand on the cytoskeleton) and zap it out of existence without disrupting the rest of the cell. The lasers can neatly zap specific structures without harming the cell or hitting other mitochondria only a few 100 nm away. It is possible to carve channels slightly less than 1 micron wide, well within a cell's diameter of 10–20 microns. By firing a pulse for only 10–15 femtoseconds in beams only 1 micron wide, the density of photons crammed into each burst becomes incredibly intense: 100 quadrillion watts per square meter, 14 orders of magnitude greater than outdoor sunlight. That searing intensity creates an electric field strong enough to disrupt electrons on the target and create a micro-explosion. But because the pulse is so brief, the actual energy delivered into the cell is only a few nanojoules. To achieve that same intensity with nanosecond or millisecond pulses would require so much more energy the cell would be destroyed

That opens the door to researching how cytoskeletons give a cell its shape, or how organelles function independently from each other rather than a whole system. The technology might be scaled up to do surgery without scarring or perhaps to deliver drugs through the skin. Near-infrared femtosecond laser pulses have been applied in a combination of microscopy and nanosurgery on fluorescently labeled structures within living cells. Femtolasers are already in use in corneal surgery.

References

- Alsberg E, Feinstein E, Joy MP, et al. Magnetically-guided self-assembly of fibrin matrices with ordered nano-scale structure for tissue engineering. Tissue Eng. 2006;12:3247–56.
- Beier JP, Klumpp D, Rudisile M, et al. Collagen matrices from sponge to nano: new perspectives for tissue engineering of skeletal muscle? BMC Biotechnol. 2009;9:34.
- Hashi CK, Zhu Y, Yang GY, et al. Antithrombogenic property of bone marrow mesenchymal stem cells in nanofibrous vascular grafts. Proc Natl Acad Sci U S A. 2007;104:11915–20.
- Huang HW, Sakar MS, Petruska AJ, et al. Soft micromachines with programmable motility and morphology. Nat Commun. 2016;7:12263.
- Jain KK. Handbook of laser neurosurgery. Springfield: Charles C. Thomas; 1983.
- Liu J, Levine AL, Mattoon JS, et al. Nanoparticles as image enhancing agents for ultrasonography. Phys Med Biol. 2006;51:2179–89.
- McMurray RJ, Gadegaard N, Tsimbouri PM, et al. Nanoscale surfaces for the long-term maintenance of mesenchymal stem cell phenotype and multipotency. Nat Mater. 2011;10:637–44.
- Mehrmohammadi M, Yoon KY, Qu M, et al. Enhanced pulsed magneto-motive ultrasound imaging using superparamagnetic nanoclusters. Nanotechnology. 2011;22:045502.
- Riviere CN, Patronik NA, Zenati MA. Prototype epicardial crawling device for intrapericardial intervention on the beating heart. Heart Surg Forum. 2004;7:E639–43.
- Spada C, Hassan C, Sturniolo GC, et al. Literature review and recommendations for clinical application of Colon capsule endoscopy. Dig Liver Dis. 2011;43:251–8.
- Watson B, Friend J, Yeo L. Piezoelectric ultrasonic resonant motor with stator diameter less than 250 µm: the Proteus motor. J Micromech Microeng. 2009;19:022001.
- Zhang M, Lenaghan SC, Xia L. Nanofibers and nanoparticles from the insect-capturing adhesive of the sundew (Drosera) for cell attachment. J Nanobiotechnology. 2010;8:20.

Chapter 8 Nanooncology

Introduction

Biotechnologies are increasingly used in cancer research (Jain 2014). Application of nanotechnology in cancer can be termed nanooncology and includes both diagnostics and therapeutics (Jain 2008). Various applications in diagnosis and drug delivery for cancer are discussed in this chapter. Two nanotechnology-based products are already approved for the treatment of cancer – Doxil (a liposome preparation of doxorubicin) and Abraxane (paclitaxel in nanoparticle formulation). Approximately 150 drugs in development for cancer are based on nanotechnology. Some of the nanotechnologies and their applications in developing cancer therapies are described in this section. The most important factor in the fight against cancer, besides prevention, is early detection.

Nanobiotechnology for Detection of Cancer

Nanobiotechnology offers a novel set of tools for detection of cancer. It will contribute to early detection of cancer as follows:

- It can complement existing technologies and make significant contributions to cancer detection, prevention, diagnosis and treatment.
- It would be extremely useful in biomarker research and provide additional sensitivity in assays with relatively small sample volumes.
- Examples of applications of nanobiotechnology in cancer diagnostics include quantum dots and use of nanoparticles for tumor imaging.

Aptasensor for Electrochemical Detection of Exosomes

Exosomes are small (50–100 nm in diameter) vesicles secreted from various mammalian cells. Exosomes have been correlated with cancer antigens as well as anticancer immune responses and may represent cancer biomarkers. An aptamer-based electrochemical biosensor has been developed for quantitative detection of exosomes (Zhou et al. 2016). Aptamers specific to exosome transmembrane protein CD63 were immobilized onto gold electrode surfaces and incorporated into a microfluidic system. Probing strands pre-labeled with redox moieties were hybridized onto aptamer molecules anchored on the electrode surface. In the presence of exosomes these beacons released probing strands with redox reporters causing electrochemical signal to decrease. These biosensors could be used to detect as few as 1×10^6 particles/mL of exosomes, which represents 100-fold decrease in the limit of detection compared to commercial immunoassays relying on anti-CD63 antibodies. Given the importance of exosome-mediated signal transmission among cells, this study may represent an important step towards development of a simple biosensor that detects exosomes without washing or labeling steps in complex media.

Aptamer-Nanoparticle Combinations for Cancer Diagnostics and Therapeutics

Nanoparticles can be substantially improved when they are modified with aptamers, which are short RNA or DNA oligomers that can bind to a ligand with high affinity. Binding of the aptamer to its target "anchors" the aptamer nanoparticle conjugate at its site of action (Reinemann and Strehlitz 2014). Several aptamers show affinities comparable to those of MAbs with some advantages over MAbs because of their molecular nature. These include high stability, as well as low immunogenicity and toxicity. Furthermore, chemical modifications are possible to extend their lifetime in biological fluids, to immobilize them on surfaces, to attach them with biomarkers, and to "tune" their half-lives to match the indication. Aptamer-based molecular imaging agents have short circulating half-lives in the body, whereas MAb-based imaging agents may circulate for days to weeks. Antidotes can be rationally designed to reverse the effect of the aptamer molecules. The antidote can bind to the aptamer, disrupt its structure and cause its inactivation. Smaller size of aptamers enables access to epitopes that are unavailable to MAbs.

Aptamers-nanoparticle conjugates enable targeted drug delivery to the cancer cells because of their binding specificity. This can enhance therapeutic effects and reduce toxic effects on normal cells. Uses in bioanalysis include both in vitro detection of cancer cells and in vivo imaging. Simultaneous diagnosis and drug delivery enables personalized therapy of cancer. Despite of their advantages, only a limited number of aptamers are available for medically relevant target molecules. There is a need for the development of more aptamers that are specific for cancer cells or biomarker proteins.

Dendrimers for Sensing Cancer Cell Apoptosis

Poly(amidoamine) (PAMAM) dendrimers have been used as a platform for the targeted delivery of chemotherapeutic drugs in cancer. A PAMAM nanodevice can be used to monitor the rate and extent of cell-killing or apoptosis caused by the delivered chemotherapeutic drug, which is important for predicting clinical efficacy (Myc et al. 2007). Whereas other approaches to detect apoptosis rely on the human protein annexin V, which binds to a hidden cell membrane component revealed in the initial stages of apoptosis, this method detects caspase-3, an enzyme activated early in the apoptosis process. This enzyme cleaves the bond between two specific amino acids and this specificity has been exploited to design fluorescence resonance energy transfer (FRET)-based assays for caspase-3. The fluorescence appears only when caspase-3 breaks a valine-aspartic acid bond in a specially designed substrate for this enzyme. To create a tumor-specific apoptosis detector, folic acid and the caspase-3 substrate were attached to a PAMAM dendrimer. Folic acid acts as a tumor-targeting agent, binding to folic acid that many types of tumor cells produce in abundance. Apoptotic tumor cells bearing this folic acid receptor take up the dendrimer and fluoresce brightly. In contrast, apoptotic cells lacking the folic acid receptor do not fluoresce. An optical fiber device, capable of detecting FRET emissions in tumors, has been used to quantify apoptosis in live mice with tumors bearing the folic acid receptor.

Detection of Circulating Cancer Cells

During metastasis, some cancer cells escape from the primary tumor and enter the bloodstream to becoming circulating tumor cells (CTCs) in the peripheral blood stream. Some of these CTCs acquire the capability to establish secondary tumors in distant organs. Therefore, CTCs are important biomarkers for early diagnosis of cancer metastasis. Moreover, CTC enumeration is less invasive than biopsy, while providing a quantifiable method for cancer diagnosis and prognosis. Blood samples can be analyzed for CTCs by nucleic acid methods to isolate tumor-associated or tumor-specific mRNA. However, detection of CTCs in peripheral blood is difficult due to their low number. Currently, CellSearch® (Veridex) is the only FDA-approved method, and it relies on antibody-coated magnetic particles for isolation of CTCs from blood. One of its key drawbacks is low capture efficiency. Several biochip/ nanoparticle technologies have been used to refine capture of CTCs.

DNA Nanospheres for Isolation of CTCs

DNA nanospheres have been combined with microfluidics for CTC isolation (Sheng et al. 2013). Each nanosphere consists of a gold nanoparticle (AuNP) that is conjugated with several DNA aptamers forming AuNP-aptamers. Aptamers possess binding

capabilities comparable with that of MAbs, which are the capture agents most commonly used in CTC research. In contrast to antibodies, aptamers have the following advantages: complete engineering in test tubes rather than in animals; straightforward production by chemical synthesis through DNA synthesizers; and long-term stability during storage. Multiple aptamers on each AuNP can interact simultaneously with several receptors on a tumor cell, resulting in multivalent binding between AuNP-aptamers and the tumor cell. Binding affinity of AuNP-aptamers is 39-times higher than aptamers themselves alone. The capture efficiency of human acute leukemia cells increases from 49% using aptamers alone to 92% using AuNP-aptamers. Thus, combining DNA nanospheres with microfluidics is a promising platform for CTC isolation and cancer diagnosis.

Magnetic Nanoparticles for Capturing CTCs

A method has been described for magnetically capturing CTCs in the bloodstream of mice followed by rapid photoacoustic detection (Galanzha et al. 2009). Magnetic nanoparticles (MNPs), which were functionalized to target a receptor commonly found in breast cancer cells, bound and captured CTCs under a magnet. To improve detection sensitivity and specificity, gold-plated CNTs conjugated with folic acid were used as a second contrast agent for photoacoustic imaging. By integrating in vivo multiplex targeting, magnetic enrichment, signal amplification and multicolor recognition, this approach enables CTCs to be concentrated from a large volume of blood in the vessels of tumor-bearing mice, and has potential applications for the early diagnosis of cancer and the prevention of metastasis in humans.

Nano-velcro Technology for Capturing CTCs

A nano-Velcro technology, engineered into a 2.5×5 cm microfluidic chip is a second-generation CTC-capture technology, which is capable of highly efficient enrichment of rare CTCs captured in blood samples collected from prostate cancer patients (Wang et al. 2011a). It is based on the research team's earlier development of 'fly-paper' technology, that involves a nanopillar-covered silicon chip whose stickiness resulted from the interaction between the nanopillars and nanostructures on CTCs known as microvilli, creating an effect much like the top and bottom of Velcro. The new device adds an overlaid microfluidic channel to create a fluid flow path that increases mixing. In addition to the Velcro-like effect from the nanopillars, the mixing produced by the microfluidic channel's architecture causes the CTCs to have greater contact with the nanopillar-covered floor, further enhancing the device's efficiency. The device features high flow of the blood samples, which travel at increased speed, bouncing up and down inside the channel, get slammed against the surface, and get caught.

An affordable, nanoscale assay has been developed to quantify CTCs, which could improve cancer diagnosis and help understand how the disease spreads (Hou et al. 2013). This is a further development of the nanoscale velcro-like material that can capture CTCs. Simply capturing the cancer cell is not enough; it also needs to be analyzed against a panel of cancer biomarkers. The new method can release these cells, leaving them intact for further analysis such as genome sequencing. The technology is also cheaper, costing <\$50 to manufacture whereas comparable assays cost ~\$1000 per run. The device consisted of an array of silicon nanowires that are coated with antibodies, which bind to a protein that lines the outer membranes of some cancer cell types called EpCAM (Wang et al. 2009). This firstgeneration assay captured the targeted cells, but released only about half of them and of those, only ~10% of were viable, leaving the rest damaged. To improve on this, cell release was boosted by adding a temperature-sensitive polymer to the silicon nanowires. At 37 °C, the anti-EpCAM polymers grab tumor cells and at 4 °C they release them. Therefore, $\sim 90\%$ of the released cells are undamaged. Like the first-generation assay, the new device only separates them with 40-70% efficiency, but there is potential to boost efficiency further by adding a microfluidic component. The assay is being validated using patient samples and results are a clinical trial is planned. Purity of the cell population is being improved by isolating and running samples through two assays in succession, which takes ~1 h.

Gold Nanoparticles for Cancer Diagnosis

Gold nanoparticles conjugated to anti-epidermal growth factor receptor (anti-EGFR) monoclonal antibodies (MAbs) specifically and homogeneously bind to the surface of the cancer cells with 600% greater affinity than to the noncancerous cells. This specific and homogeneous binding is found to give a relatively sharper SPR absorption band with a red shifted maximum compared to that observed when added to the noncancerous cells. The particles that work the best are 35 nm in size. Thus, SPR scattering imaging or SPR absorption spectroscopy generated from antibody conjugated gold nanoparticles can be useful in molecular biosensor techniques for the diagnosis and investigation of living oral epithelial cancer cells in vivo and in vitro. Advantages of this technique are:

- It is not toxic to human cells. A similar technique with QDs uses semiconductor crystals to mark cancer cells, but the semiconductor material is potentially toxic to the cells and humans.
- It does not require expensive high-powered microscopes or lasers to view the results. All it takes is a simple, inexpensive microscope and white light.
- The results are instantaneous. If a cancerous tissue is sprayed with gold nanoparticles containing the antibody, the results can be seen immediately. The scattering is so strong that a single particle can be detected.

An animal study has successfully demonstrated the safety of diagnostic use of Raman-silica-gold-nanoparticles (R-Si-Au-NPs), which overcome the inherently weak nature of Raman effect by producing larger Raman signals through surfaceenhanced Raman scattering (Thakor et al. 2011). R-Si-Au-NPs were bound to PEG molecules to improve biological tolerance. Molecules that home in on cancer cells can be attached to PEG-R-Si-Au-NPs and the overall diameter is 100 nm. Photoimaging with these nanoparticles holds the promise of very early disease detection in colorectal cancer (CRC), even before any gross anatomical changes show up, without physically removing any tissue from the patient. Both rectal and intravenous administration of the particles did not show any systemic toxicity in experimental animals. Furthermore, the nanoparticles were quickly excreted. The intravenously administered nanoparticles were rapidly sequestered by scavenger cells resident in organs such as the liver and spleen. This opens the door to human tests of intravenous injections of these nanoparticles to search for tumors throughout the body. Molecules targeting breast, lung or prostate cancer can be attached to these nanoparticles. The investigators are now filing for FDA approval to proceed to clinical studies of the nanoparticles for the diagnosis of CRC.

Chemiluminescence resonance energy transfer (CRET) with gold nanoparticles (AuNPs) has been used as an efficient long-range energy acceptor in sandwich immunoassays. A CRET-based sandwich immunoassay has been developed for alpha fetoprotein (AFP) cancer biomarker (Huang and Ren 2011). In immunoassay, two antibodies (anti-AFP-1 and anti-AFP-2) are conjugated to AuNPs and horserad-ish peroxidase, respectively. The sandwich-type immunoreactions between the AFP (antigen) and the two different antibodies bridge the donors (luminol) and acceptors (AuNPs), which leads to the occurrence of CRET from luminol to AuNPs upon chemiluminescent reaction. We observed that the quenching of chemiluminescence signal depended linearly on the AFP concentration within a range of concentration from 5 to 70 ng mL⁻¹ and the detection limit of AFP was 2.5 ng mL⁻¹. This method was successfully applied for determination of AFP levels in sera from cancer patients, and the results were in good agreement with ELISA assays. This approach is expected to be extended to other assay designs, that is, using other antibodies, analytes, and chemiluminescent substance.

Gold nanoparticles can be heated rapidly whenever exposed to infrared light of the right wavelength. Heating of gold nanoparticles results in variations in pressure surrounding them, which in turn is expressed in the generation of ultrasound - a phenomenon called plasmon resonance. The shape of the particles determines the wavelength at which this happens. In this way, light from a laser results in sound. By attaching MAbs to gold nanoparticles or nanorods, which can recognize a specific cancer cell, the heating phenomenon can be used in cancer detection. This acoustic signal gives valuable information about the presence of cancer cells. Scientists at the University of Twente (UT) in the Netherlands expect better results with this approach than is currently possible with imaging techniques. The temperature rise can be up to 100 °C. Photothermal therapy would use the heated gold to destroy the tumor. Another option would be to include gold particles in capsules filled with cancer medication: the capsule attaches to the cancer cell, is heated and the medicine is released locally. Both diagnostic and therapeutic applications will be investigated by the UT scientists together with colleagues from the Erasmus Medical Center in Rotterdam and two companies: Esoate Europe and Luminostix.

Gold Nanorods for Detection of Metastatic Tumor Cells

Scientists at Purdue University have developed a technique for producing biocompatible gold nanorods of various sizes to which antibodies can be attached. Gold nanorods interact with light to produce plasmons, a wave-like motion of electrons on the surface of the nanorods. Depending on the ratio of a nanorod's length to its diameter, these plasmons trigger light emission at a specific frequency that is easily detected using SPR spectroscopy. An antibody that recognizes one specific cancer cell surface biomarker is attached to each nanorod of a given length and diameter. A gold nanorod-antibody construct that recognizes a biomarker found on all cell surfaces serves as an internal reference control that enables calculation of relative amounts of the various tumor biomarkers on a given cancer cell. Using a panel of three different antibody-labeled gold nanorods, it is possible to characterize breast tumors according to their cellular composition and correlate their findings to the metastatic potential of each given cell type. These results were validated using flow cytometry, the standard technique used to classify cells according to surface biomarkers. Gold nanorods enabled monitoring of as many as 15 different antibodynanorod constructs simultaneously.

Magnetoacoustic Detection of Cancer Using Superparamagnetic Nanoparticles

Magnetoacoustic detection is a method for the noninvasive, early detection of cancer. It uses specific superparamagnetic nanoparticles (NPs) that bind to tumor sites together with magnetic excitation and acoustic detection of the tumor-NPs complex (Steinberg et al. 2012). The method was demonstrated in a phantom by detecting a 5-mm diameter spherical tumor located 3 cm deep. A supporting localization algorithm can provide the clinician with essential tumor location data and could enable a sequential biopsy (Tsalach et al. 2014). It has been validated in both computerized simulations and in vitro experiments. It enables 3D tumor localization with an error of 2.14 mm and an overlapping volume of 84% of the actual tumor. Results are promising and show the feasibility of tumor localization using a time difference-of-arrival algorithm along with magnetoacoustic detection.

Nanosensors for Cancer Diagnosis

Differentiation Between Normal and Cancer Cells by Nanosensors

Rapid and effective differentiation between normal and cancer cells is an important challenge for the diagnosis and treatment of tumors. A nanoparticle array-based system has been described for identification of normal and cancer cells based on a

"chemical nose/tongue" approach that exploits subtle changes in the physicochemical nature of different cell surfaces (Bajaj et al. 2009). Differential interactions with functionalized nanoparticles are transduced through displacement of a multivalent polymer fluorophore that is quenched when bound to the particle and fluorescent after release. This sensing method can rapidly (min/s) and effectively distinguish (i) different cell types; (ii) normal, cancerous and metastatic human breast cells; and (iii) isogenic normal, cancerous and metastatic murine epithelial cell lines.

Implanted Biosensor for Cancer

An implant for biosensing of cancer, developed at the Massachusetts Institute of Technology (Cambridge, MA), contains nanoparticles that can be designed to test for different substances, including metabolites such as glucose and oxygen that are associated with tumor growth. It can also be used to test the effects of anticancer drugs in individual patients; the implant could reveal how much of a drug has reached the tumor. The nanoparticles are encased in a silicone delivery device, enabling their retention in patients' bodies for an extended period. The device can be implanted directly into a tumor, allowing a more direct look at what is happening in the tumor over time. The technique makes use of detection nanoparticles composed of iron oxide and coated with dextran. Antibodies specific to the target molecules are attached to the surface of the nanoparticles. When the target molecules are present, they bind to the particles and cause them to clump together. That clumping can be detected by MRI. The nanoparticles are trapped inside the silicone device, which is sealed off by a porous membrane. The membrane allows molecules smaller than 30 nm to get in, but the detection particles are too large to get out. In addition to monitoring the presence of chemotherapy drugs, the device could also be used to check whether a tumor is growing or shrinking, or whether it has spread to other locations, by sensing the amount and location of tumor biomarkers. Preclinical testing is being done for this device for human chorionic gonadotropin that can be considered a biomarker for cancer because it is produced by tumors but not normally found in healthy individuals except pregnant women.

Nanotubes for Detection of Cancer Proteins

Single-wall carbon nanotubes (SWCNTs) are being developing for monitoring cancer-specific-proteins. These are hundreds of times smaller than nanocantilevers, highly sensitive to single-protein binding events, and can be massively multiplexed with millions of tubes per chip for proteomic profiling. The tubes have extraordinary strength, unique electronic properties, and the ability to tag cancer-specific proteins to their surface. These tubes can be fabricated by decomposition of carbon-based gas in a furnace, using iron nanoparticles as catalyst material. With diameter of 1 nm and length of 1 μ m, these tubes are smaller than a single-strand of DNA.

In other words, such a tube is an atomic arrangement of one layer of carbon atoms, which are on the surface. Protein binding events occurring on the surface of these tubes produce a measurable change in the mechanical and electrical properties.

By coating the surfaces of SWCNTs MAbs, it is possible to detect circulating tumor cells (CTCs) in the blood. SWCNTs covered with MAbs, particularly those for insulin-like growth factor-1 receptor (IGF-1), which is commonly found at high levels on cancer cells, home in on target protein "antigens" on the surface of CTCs. This method can be used for detection of recurring CTCs or residual micrometastases from the originally treated tumor. The technique could be cost-effective and could diagnose whether cells are cancerous or not in seconds versus hours or days required for conventional histology examination. It will enable large scale production methods to make thousands of biosensors and have microarrays of these to detect the fingerprints of specific kinds of CTCs. Eventually it may be possible to design an assay that can detect CTCs on a hand-held device no bigger than a cell phone. Limitation of the technique is that it may not detect more than one antigen at a time on a single cell.

Nanobiochip Sensor Technique for Analysis of Oral Cancer Biomarkers

A pilot study has described a nanobiochip sensor technique for analysis of oral cancer biomarkers in exfoliative cytology specimens, targeting both biochemical and morphologic changes associated with early oral tumorigenesis (Weigum et al. 2010). Oral lesions from dental patients, along with normal epithelium from healthy volunteers, were sampled using a noninvasive brush biopsy technique. Specimens were enriched, immunolabeled, and imaged in the nanobiochip sensor according to previously established assays for the epidermal growth factor receptor (EGFR) biomarker and cytomorphometry. Four key parameters were significantly elevated in both dysplastic and malignant lesions relative to healthy oral epithelium, including the nuclear area and diameter, the nuclear-to-cytoplasmic ratio, and EGFR biomarker expression. Further examination using logistic regression and receiver operating characteristic curve analyses identified morphologic features as the best predictors of disease individually, whereas a combination of all features further enhanced discrimination of oral cancer and precancerous conditions with high sensitivity and specificity. Further clinical trials are necessary to validate the regression model and evaluate other potential biomarkers. Nanobiochip sensor technique is a promising tool for early detection of oral cancer, which could enhance patient survival.

Nanodots for Tracking Apoptosis in Cancer

Apoptosis is a hallmark effect triggered by anticancer drugs. Researchers at Seoul National University (Korea) have developed a biocompatible, fluorescent nanoparticle that could provide an early sign that apoptosis is occurring due to anticancer therapy (Yu et al. 2007). The team created their fluorescent surface enhanced Raman

spectroscopic (F-SERS) nanodots to boost the optical signal generated by typical, biocompatible fluorescent dyes. The nanodots consist of silver nanoparticles embedded in a silica sphere. Attached to the silica core are fluorescent dye molecules and molecules known as Raman labels that enhance the electronic interactions between the silver nanoparticles and the dye molecules. The researchers also linked annexin-V, a molecule that binds specifically to a chemical that appears on cells undergoing apoptosis, to the silica-silver nanoparticle construct. Toxicity tests showed that the silica-silver nanodots were not toxic to various human cells growing in culture. The investigators then added the nanodots to cells triggered to undergo apoptosis and could image those cells as they went through programmed cell death. Based on these results, the researchers prepared other nanodots containing antibodies that bind to other molecules involved in apoptosis. They then added these antibody-linked nanodots and the annexin-V-linked nanodots to cultured human lung cancer cells. The investigators could track the appearance of all three molecules simultaneously, which has been difficult to do using conventional cell staining techniques.

Nanolaser Spectroscopy for Detection of Cancer in Single Cells

Nanolaser scanning confocal spectroscopy can be used to identify a previously unknown property of certain cancer cells that distinguishes them with single cell resolution from closely related normal cells. This property is the correlation of light scattering and spatial organization of mitochondria; normally it is well scattered but in cancer cells, the mitochondria are disorganized and scatter light poorly. These optical methods are promising powerful tools for detecting cancer at an early stage.

Nanoparticles Designed for Dual-Mode Imaging of Cancer

The best characteristics of QDs and magnetic iron oxide nanoparticles have been combined to create a single nanoparticle probe that can yield clinically useful images of both tumors and the molecules involved in cancer. The method starts with synthesis of 30 nm diameter silica nanoparticles impregnated with rhodamine, a bright fluorescent dye, and 9 nm diameter water-soluble iron oxide nanoparticles. These two nanoparticles are then mixed with a chemical linker, yielding the dual-mode nanoparticle. On average, ten magnetic iron oxide particles link to a single dye-containing silica nanoparticle, and the resulting construct is ~45 nm in diameter. The combination nanoparticle performs better in both MRI and fluorescent imaging tests than the individual components. In MRI experiments, the combination nanoparticle generates an MRI signal that is over three-fold more intense than did the same number of iron oxide nanoparticles. Similarly, the fluorescent signal from the dual-mode nanoparticle is almost twice as bright as that produced by dye molecules linked directly to iron oxide nanoparticles. The dual-mode nanoparticles

are then labeled with an antibody that binds to molecules known as polysialic acids, which are found on the surface of certain nerve cell and lung tumors. These targeted nanoparticles are quickly taken up by cultured tumor cells and are readily visible using fluorescence microscopy.

Nanotechnology-Based Single Molecule Assays for Cancer

Information about the biological processes in living cells is required for the detection and diagnosis of cancer for the following reasons:

- To recognize the important changes, which occur when cells undergo malignant transformation.
- There are situations when primary cells from a surgical procedure cannot be propagated due to the type of cell or the low number of cells available.
- Detection of cancer at an early stage is a critical step for improving cancer treatment.

Early detection will require sensitive methods for isolating and interrogating individual cells with high spatial and temporal resolution without disrupting their cellular biochemistry. Probes designed to penetrate a cell and report on the conditions within that cell must be sufficiently small, exceedingly bright, and stable for a long time in the intracellular environment without disrupting the cell's normal biochemical functioning. A series of silver nanoparticles have been prepared that meet many of the criteria listed above. Although smaller than 100 nm in diameter, these particles are bright enough to be seen by eye using optical microscopy. Unlike fluorophores, fluorescent proteins, or quantum dots, silver nanoparticles do not photodecompose during extended illumination. Therefore, they can be used as a probe to continuously monitor dynamic events in living cells during studies that last for weeks or even months. Because the color of the scattered light from nanoparticles depends upon their size, they have been used to measure the change in single membrane pores in real time using dark-field optical microscopy. Intracellular and extracellular nanoparticles can also be differentiated by the intensity of light scattering. Next challenge is to develop methods for modifying the surface of the nanoparticles to make them more biocompatible, so that biological processes can be observed without disturbing or destroying the cell's intrinsic biochemical machinery. Ultimately, these probes may be combined to produce highly sensitive assays with high spatial and temporal resolution. This advance will enable researchers to study the interactions of multiple genes in the same cell simultaneously by using different colored reporter molecules. In addition to transcription and translation, similar live-cell single molecule assays will offer the prospect of studying more complex cellular processes, such as cell signaling. Continuous advances and evolution along these research fronts is necessary to unravel biochemical processes in vivo, and to develop tools that can be used to detect and diagnose cancer using only a single cell from the patient.

QDs for Detection of Tumors

QD bioconjugates that are highly luminescent and stable can be used for studying gene, and enable visualization of cancer cells in living animals. QDs can be combined with fluorescence microscopy to follow cells at high resolution in living animals. These offer considerable advantages over organic fluorophores for this purpose. QDs and emission spectrum scanning multiphoton microscopy have been used to develop a means to study extravasation of tumor cells in vivo.

QD-Based Test for DNA Methylation

DNA methylation contributes to carcinogenesis by silencing key tumor suppressor genes. An ultrasensitive and reliable nanotechnology assay, MS-qFRET (fluorescence resonance energy transfer), can detect and quantify DNA methylation (Bailey et al. 2009). Bisulfite-modified DNA is subjected to PCR amplification with primers that would differentiate between methylated and unmethylated DNA. QDs are then used to capture PCR amplicons and determine the methylation status via FRET. The specific target of the test is DNA methylation which occurs when methyl attaches to cytosine, a DNA building block. When this happens at specific gene locations it can stop the release of tumor-suppressing proteins; cancer cells then more easily form and multiply. The method involves singling out the DNA strands with methyl attachments through bisulfite conversion, whereby all non-methyl segments are converted into another nucleotide. Copies of the remaining DNA strands are made, two molecules (a biotin protein and a fluorescent dye) are attached at either end, and the strands are mixed with QDs that are coated with a biotin-attractive chemical. Up to 60 DNA strands are attracted to a single QD. An UV light or blue laser activates the QDs, which pass the energy to the fluorescent molecules on the DNA strands which then light up and are identifiable via a spectrophotometer, which both identifies and can count the DNA methylation.

Key features of MS-qFRET include its low intrinsic background noise, high resolution, and high sensitivity. This approach detects as little as 15 pg of methylated DNA in the presence of a 10,000-fold excess of unmethylated alleles, enables reduced use of PCR (as low as eight cycles), and allows for multiplexed analyses. The high sensitivity of MS-qFRET enables one-step detection of methylation at PYCARD, CDKN2B, and CDKN2A genes in patient sputum samples that contain low concentrations of methylated DNA, which normally would require a nested PCR approach.

The direct application of MS-qFRET on clinical samples offers great promise for its translational use in early cancer diagnosis, and prognostic assessment of tumor behavior, as well as monitoring response to therapeutic agents. Gene DNA methylation indicates a higher risk of developing cancer and is also seen as a warning sign of genetic mutations that lead to development of cancer. Moreover, since different cancer types possess different genetic markers, e.g. lung cancer biomarkers differ from those of leukemia, the test should identify which cancer a patient is at risk of developing. This test could be used for frequent screening for cancer and replacing traditionally invasive methods with a simple blood test. It could also help determine whether a cancer treatment is effective and thus enable personalized chemotherapy.

Spectral Imaging and CNTs in Malignant Tumors

Nanomaterials with luminescence in the short-wave infrared (SWIR) region are used for medical diagnostics because of favorable tissue transparency and low autofluorescence backgrounds in that region. SWCNTs with well-known sharp SWIR spectral signatures have potential for noninvasive detection and imaging of malignant tumors when linked to selective targeting agents such as antibodies. Spectral triangulation has been used for 3D localization using optical measurements made at the specimen surface (Lin et al. 2016). Structurally unsorted SWCNT samples emitting over a range of wavelengths are excited inside tissue phantoms by a light-emitting diodes (LED) matrix. A highly sensitive detector called an InGaAs (indium gallium arsenide) avalanche photodiode enables reading of faint signals from small concentrations of SWCNTs up to 2 cm deep in the simulated tissue used for laboratory tests. This has potential applications in diagnosis.

Nanobiotechnology for Early Detection of Cancer to Improve Treatment

Cancer cells themselves may be difficult to detect at an early stage but they leave a fingerprint, i.e. a pattern of change in biomarker proteins that circulate in the blood. There may be 20–25 biomarkers, which may require as many as 500 measurements, all of which should be made from a drop of blood obtained by pinprick. Thus, nanoscale diagnostics will play an important role in this effort. Nanowire sensors are in development at California Institute of Technology (Pasadena, CA) for very early diagnosis of cancer, when there are just a few thousand cells. Nanowires can electronically detect a few proteins molecules along with other biochemical markers that are early signs of cancer. Nanowires in a set are coated with several compounds, each of which binds to a specific biomarker, and changes the conductivity of the nanowire that can be measured. Thousands of such nanowires are combined on a single chip that enables identification of the type of cancer. Currently such a chip can detect between 20 to 30 biomarkers and is being used for the early diagnosis of brain cancer.

Cancer is easier to treat and less likely to develop drug resistance when treatment is started very early. Cancer cells in very early stages are less likely to have mutations that make them resistant to treatment.

An automated gold nanoparticle biobarcode assay probe has been described for the detection of prostate specific antigen (PSA) at 330 fg/mL, along with the results of a clinical pilot study designed to assess the ability of the assay to detect PSA in the serum of 18 men who have undergone radical prostatectomy for prostate cancer (Thaxton et al. 2009). Available PSA immunoassays are often not capable of detecting PSA in the serum of men after radical prostatectomy. This new bio-barcode PSA assay is approximately 300 times more sensitive than commercial immunoassays and all patients in this study had a measurable serum PSA level after radical prostatectomy. Because the patient outcome depends on the level of PSA, this ultrasensitive assay enables: (1) informing patients, who have undetectable PSA levels with conventional assays, but detectable and nonrising levels with the barcode assay, that their cancer will not recur; (2) earlier detection of recurrence earlier because of the ability to measure increasing levels of PSA before conventional tools can make such assignments; and (3) use of PSA levels, which would otherwise not be detectable with conventional assays, to follow the response of patients to treatment.

Nanobiotechnology-Based Drug Delivery in Cancer

Drug delivery in cancer is important for optimizing the effect of drugs and reducing toxic side effects. Several nanobiotechnologies, mostly based on nanoparticles, have been used to facilitate drug delivery in cancer. A classification of the nanotechnologies for drug delivery in cancer is shown in Table 8.1.

Approximately 150 drugs in development for cancer are based on nanotechnology. Those approved are listed in Table 8.2 and several more are in clinical trials.

Nanoparticle Formulations for Drug Delivery in Cancer

Anticancer Drug Particles Incorporated in Liposomes

Several injectable and biodegradable systems have been synthesized based on incorporation of anti-estrogens (AEs) in nanoparticles and liposomes. Both nano-spheres and nanocapsules (polymers with an oily core in which AEs were solubilized) incorporated high amounts of 4-hydroxy-tamoxifen (4-HT) or RU 58668. Liposomes containing various ratios of lipids enhanced the apoptotic activity of RU 58668 in several multiple myeloma cell lines tested by flow cytometry. These cell lines expressed both estrogen receptor alpha and beta subtypes. RU-loaded liposomes, administered intravenously in an animal model induce the arrest of tumor growth. Thus, the drug delivery of anti-estrogens enhances their ability to arrest the growth of tumors which express estrogen receptors and are of special interest for estrogen-dependent breast cancer treatment. In addition, it represents a new potent therapeutic approach for multiple myeloma.

SuperFluids[™] technology (Aphios Corporation) involves biodegradable polymer nanospheres utilizing supercritical, critical or near-critical fluids with or without polar cosolvents. These nanospheres are utilized to encapsulate proteins with

Table 5.1 Classification of nanobiotechnology approaches to drug derivery in cancer
Nanoparticles
Nanoparticle formulations of anticancer drugs, e.g. paclitaxel
Exosomes for cancer drug delivery
Nanoencapsulation and eclosure of anticancer drugs
Enclosing drugs in lipid nanocapsules
Encapsulating drugs in hydrogel nanoparticles
Micelles for drug delivery in cancer
Targeted delivery of anticancer therapy
Targeted drug delivery with nanoparticles
Pegylated nanoliposomal formulation
Folate-linked nanoparticles
Carbon magnetic nanoparticles for targeted drug delivery in cancer
Targeted drug delivery with nanoparticle-aptamer bioconjugates
Nanodroplets for site-specific cancer treatment
Lipid based nanocarriers
Targeted antiangiogenic therapy using nanoparticles
Nanoparticles for delivery of drugs to brain tumors
Combination of nanoparticles with radiotherapy
Combination with boron neutron capture therapy
Nanoengineered silicon for brachytherapy
Combination with physical modalities of cancer therapy
Combination with laser ablation of tumors
Combination with photodynamic therapy
Combination with thermal ablation
Combination with ultrasound
Nanoparticle-mediated gene therapy
p53 gene therapy of cancer
Immunolipoplex for delivery of p53 gene
Intravenous delivery of FUS1 gene
Strategies combining diagnostics and therapeutics
Nanoshells as adjuncts to thermal tumor ablation
Perfluorocarbon nanoparticles
Nanocomposite devices
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Table 8.1 Classification of nanobiotechnology approaches to drug delivery in cancer

controlled-release characteristics without usage of toxic organic solvent. The patented technology can be utilized to form stable biocompatible aqueous formulations of poorly soluble anticancer drugs such as paclitaxel and camptothecin. An improved process utilizing SuperFluidsTM results in the formation of small, uniform liposomes (nanosomes) to improve the delivery and therapeutic efficacy of poorly water-soluble drugs while reducing their toxicities. The process has been used for the nanoencapsulation of paclitaxel in a formulation called TaxosomesTM, which has been tested in nude mice with breast cancer xenografts. TaxosomesTM will lead to: (i) enhanced therapeutic efficacy; (ii) elimination of pre-medication to counteract

Trade name/compound	Manufacturer	Nanocarrier		
Abraxane/paclitaxel	Abraxis Biosciences	Albumin-bound paclitaxel		
Bexxar/anti-CD20 conjugated to iodine-131	Corixa/GlaxoSmithKline	Radio-immunoconjugate		
DaunoXome/daunorubicin	Diatos, available in France	Liposome		
Doxil/Caelyx/doxorubicin	Ortho Biotech	Liposome		
Myoset/doxorubicin	Cephalon, available in Europe	Non-pegylated liposome		
Oncaspar/PEG -L-asparaginase	Enzon	Polymer–protein conjugate		
Ontak/IL2 fused to diphtheria toxin	Eisai Inc	Immunotoxic fusion protein		
SMANCS/zinostatin	Yamanouchi Pharma	Polymer-protein conjugate		
Zevalin/anti-CD20 conjugated to yttrium-90	Cell Therapeutics Inc	Radio-immunoconjugate		
Zoladex/goserelin acetate	AstraZeneca	Polymer rods		

 Table 8.2
 Approved anticancer drugs using nanocarriers

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SMANCS styrene maleic anhydride neocarzinostatin

castor oil; (iii) reduction of drug toxicity side-effects; (iv) prolonged circulation time and therapeutic effect; and (v) improved quality of life.

The process has also been used for the nanoencapsulation of camptothecin, a potent and exciting anticancer agent, in a stable aqueous liposomal formulation called CamposomesTM. Water soluble derivatives of camptothecin, a unique topoisomerase 1 inhibitor, have recently been approved by the FDA for use in colorectal cancer. CamposomesTM have been shown to be very effective against lymphomas in nude mice.

Nanocapsules, which are small aggregates of cisplatin covered by a single lipid bilayer, have an unprecedented drug-to-lipid ratio and an in vitro cytotoxicity up to 1000-fold higher than the free drug. Analysis of the mechanism of nanocapsule formation suggests that the method may be generalized to other drugs showing low water solubility and lipophilicity.

In Protein Stabilized Liposome (PSLTM) nanotechnology of Azaya Therapeutics the liposome product is prepared in a single step that encapsulates the active drug Docetaxel (ATI-1123) in the lipid layer of the liposome while forming active nanoparticles in situ (100–130 nm). This process is geared toward the formulation of hydrophobic molecules that would otherwise have limited success as developmental drugs using traditional formulation methodologies. Azaya intends to use its PSL nanotechnology to improve the performance and reduce the nonspecific cytotoxicity of leading marketed chemotherapeutics such as Taxotere (docetaxel) and CAMPTOSAR®, as well as, several experimental drugs that have been withdrawn from development due to their non-specific cytotoxicity and formulation difficulties.

Cerasomes

Ceramide is a lipid molecule in plasma membrane of the cell and controls cell functions such as cell aging. Ceramide selectively kills cancer cells but is not toxic to normal cells. However, as a lipid, ceramide cannot be delivered effectively as a drug. To solve this limitation, cerasome is created to turn the insoluble lipid into a soluble form. Cerasomes are molecular-sized bubbles (size range 60–200 nm) filled with C6-ceramide for use as anticancer agents. Paclitaxel loaded cerasomes exhibit sophisticated controlled release behavior for drug delivery in cancer (Cao et al. 2010). Cerasomes have already been shown to effectively treat cellular and animal models of breast cancer and melanoma. Systemic administration of nanoliposomal C6-ceramide to mice engrafted with SK-HEP-1 tumors reduced tumor vascularization and proliferation, induced tumor cell apoptosis, decreased phosphorylation of AKT and ultimately blocked tumor growth (Tagaram et al. 2011). These studies show that nanoliposomal ceramide is an efficacious antineoplastic agent for the treatment of in vitro and in vivo models of human hepatocellular carcinoma.

Doxorubicin Nanocarriers

Resistance to anthracyclines and other chemotherapeutics due to P-glycoprotein (pgp)-mediated export is a frequent problem in cancer treatment. Iron oxidetitanium dioxide (TiO2) core-shell nanocomposites can serve as efficient carriers for doxorubicin to overcome this common mechanism of drug resistance in cancer cells (Arora et al. 2012). Doxorubicin nanocarriers (DNC) increased effective drug uptake in drug-resistant ovarian cells. Doxorubicin binds to the TiO2 surface by a labile bond that is severed upon acidification within cell endosomes. Upon its release, doxorubicin traverses the intracellular milieu and enters the cell nucleus by a route that evades P-gp-mediated drug export. Confocal and X-ray fluorescence microscopy and flow cytometry have been used to show the ability of DNCs to modulate transferrin uptake and distribution in cells. Increased transferrin uptake occurs through clathrin-mediated endocytosis, indicating that nanocomposites and DNCs may both interfere with removal of transferrin from cells. Together, these findings show that DNCs not only provide an alternative route of delivery of doxorubicin to pgp-overexpressing cancer cells but also may boost the uptake of transferrintagged therapeutic agents.

Chemical linkage of the anticancer drug doxorubicin onto squalene, a natural lipid precursor of the cholesterol's biosynthesis, led to the formation of squalenoyl doxorubicin (SQ-Dox) nanoassemblies of 130 nm mean diameter, with an original "loop-train" structure (Maksimenko et al. 2014). This unique nanomedicine demonstrates: (i) high drug payload, (ii) decreased toxicity of the coupled anticancer compound, (iii) improved therapeutic response, (iv) use of biocompatible transporter material, and (v) ease of preparation. These are not combined in the currently available nanodrugs. Cell culture viability tests and apoptosis assays showed that SQ-Dox nanoassemblies displayed better antiproliferative and cytotoxic effects

than the native doxorubicin because of the high activity of apoptotic mediators, such as caspase-3 and poly(ADP-ribose) polymerase. In vivo experiments have shown that the SQ-Dox nanomedicine dramatically improves the anticancer efficacy, compared to free doxorubicin. Lung cancer that did not respond to doxorubicin treatment was inhibited by 90% when treated with SQ-Dox nanoassemblies. – MiaPaCa-2 Pancreatic tumor xenografts in mice, treated with SQ-Dox nanoassembly, decreased by 95% compared with the tumors in the saline-treated mice, which was significantly higher than the 29% reduction achieved by native doxorubicin. showed A fiva-fold higher maximum dose of SQ-Dox nanoassembliescould be tolerated than the free drug. SQ-Dox nanoassemblies did not cause any myocardial lesions, such as those induced by the free doxorubicin treatment. These findings demonstrate that SQ-Dox nanoassemblies sensitize tumor cells to doxorubicin and reduce the cardiac toxicity, thus providing a remarkable improvement in the drug's therapeutic index.

Curcumin Nanoformulation as Cancer Therapeutics

Curcumin, an element found in the cooking spice turmeric has long been known to have potent anticancer properties as demonstrated in several human cancer cell line and animal carcinogenesis models. Nevertheless, widespread clinical application of this relatively efficacious agent in cancer and other diseases has been limited due to poor aqueous solubility, and consequently, minimal systemic bioavailability. Types of curcumin nanoformulation used in cancer therapeutics include. Curcumin has demonstrated efficacy as an anticancer agent, but a limiting factor is its extremely low aqueous solubility, which hampers its use as therapeutic agent. Therefore, several formulations have been developed to improve solibility and absorption. Nanoscale delivery systems for curcumin, include liposomes, polymer conjugates, polymer nanoparticle, solid nanoparticles, lipid nanoparticles, magnetic nanoparticles, and polymer micelles. The characteristics of these curcumin nanoformulations can be tailored according to the specific requirement for inducing cellular death by various mechanisms. Examples of commercially available curcumin nanoformulations are:

Curcumin nanoformulations significantly internalize in cancer cells through endocytosis or receptor-mediated pathways in the presence of endocytosis inhibitors and release curcumin in active form to induce its biological effects. Targeted delivery of curcumin using nanoparticles is advantageous as compared to conventional formulations. PSMA-targeted curcumin PLGA NPs specifically target PSMA overexpressing prostate cancer cells both in cell line and xenograft tumors (Yallapu et al. 2014).

One solution to the problem of curcumin delivery is by encapsulating free curcumin with a polymeric nanoparticle, creating nanocurcumin (Bisht et al. 2007). Furthermore, these authors showed that nanocurcumin's mechanisms of action on pancreatic cancer cells mirror that of free curcumin, including induction of cellular apoptosis, blockade of nuclear factor kappa B (NFkappaB) activation, and downregulation of steady state levels of multiple pro-inflammatory cytokines (IL-6, IL-8, and TNF α). Furthermore, curcumin nanoformulations retain molecular targeting effects, even though curcumin is encapsulated in nanoparticles or nanocarrier.

Curcumin nanoformulation	Bioavailability relevant to anticancer effect	Reference
CurcuEmulsome: solid tripalmitin core surrounded by phospholipid multilayers to enhances the poor water solubility of curcumin.	Curcumin is trapped in the inner core of CurcuEmulsome and has a prolonged release into the cell compared to emulsion formulations possessing a liquid core, resulting in prolonged cytotoxicity and cancer cell cycle arrest.	Ucisik et al. (2013)
Curcumin loaded chitosan nanoparticles (CLCsNPs)	Higher cytotoxicity effect of CLCsNPs may be due to their higher cellular uptake as compared to curcumin.	Khan et al. (2016)
Curcumin loaded nanosized polyelectrolyte complexes (PECs)	PECs significantly improved nuclear transport of curcumin in cancer cells, resulting in apoptosis.	Fatima et al. (2016)
Curcumin-loaded solid lipid nanoparticles (C-SLNs)	Curcumin levels in plasma were significantly increased	Kakkar et al. (2011)
Curcumin-loaded monomethoxy PEG poly(ɛ-caprolactone) micelles	I/V injection of aqueous formulation inhibits growth of colon carcinoma by anti-angiogenic effect and apoptosis.	Gou et al. (2011)
Curcumin-loaded PLGA-PEG- PLGA copolymeric micelles	Increased absorption with enhanced uptake by brain and lung which sparing liver and spleen.	Song et al. (2011)

 Table 8.3
 Bioavailability and anticancer effect of curcumin nanoformulations

Abbreviation: *PLGA* poly(d,l-lactide-co-glycolide), *PEG* poly(ethylene glycol)

Nanocurcumin provides an opportunity to expand the clinical repertoire of this efficacious agent by enabling ready aqueous dispersion. Future studies utilizing nanocurcumin are warranted in preclinical in vivo models of cancer and other diseases that might benefit from the effects of curcumin. Table 8.3 shows a selection of nanoformulations of curcumin with absorption characteristics, bioavailability, and anticancer effects.

Encapsulating Drugs in Hydrogel Nanoparticles

A versatile chemical technique has been developed for creating ultrafine nanosized hydrogels, essentially a network of polymer chains that absorb as much as 99% of their weight in water (Gao et al. 2007). Polyacrylamide was used to create nanoparticles of 2 nm diameter that have no charge on their surfaces. This lack of charge prevents blood proteins from sticking to the surface of the nanoparticles. Combined with the fact that these nanoparticles are too small to be recognized by the immune system, the result is a nanoscale drug delivery vehicle with the ability to remain in circulation long enough to reach and permeate tumors before being excreted through the kidneys. These nanoscale hydrogels were first tested as a drug delivery vehicle for a water-insoluble photosensitizer called meta-tetra(hydroxyphenyl) chlorin (mTHPC), which is approved in the European Union for use in treating head and neck cancer. mTHPC produces cell-killing reactive oxygen when irradiated with red light, but not without serious side effects resulting from the method now used to

deliver this drug to tumors. When added to the chemical mixture used to create the nanoparticles, mTHPC becomes trapped within the polymer framework. Characterization experiments showed that this photosensitizer does not escape from the nanoparticles, but is still capable of producing the same amount of reactive oxygen as if it were free in solution. When added to human brain cancer cells growing in culture and irradiated with red light, this formulation kills the cells rapidly. Empty nanoparticles had no effect on the cells. Neither did drug-loaded nanoparticles added to the cells that were kept in the dark.

Exosomes

Exosomes are small (50–100 nm), spherical vesicles produced and released by most cells to facilitate intercellular communication. These vesicles are of endosomal origin and are secreted in the extracellular milieu following fusion of late endosomal multive-sicular bodies with the plasma membrane. Exosomes have a defined protein composition, which confers specific biological activities contingent on the nature of the producing cell. Although exosomes express tumor antigens, leading to their proposed utility as tumor vaccines, they also can suppress T-cell signaling molecules and induce.

Exosomes produced by dendritic cells are called dexosomes and contain essential components to activate both adaptive and innate immune responses. Anosys is developing dexosome vaccines that use patient-specific dexosomes loaded with tumor antigen-derived peptides to treat cancer. Exosome research continues to reveal unique properties which broaden their fields of application. Anosys' Exosome Display Technology provides the ability to manipulate exosome composition and tailor exosomes with new desirable properties opening up opportunities in the field of recombinant vaccine and MAb preparation. This is achieved by generating genes coding for chimeric proteins linking an exosome addressing sequence to antigens or biologically active proteins. The resulting proteins are targeted to exosomal compartment and released in the extracellular milieu bound to exosomes.

Exosomes are emerging as novel approaches for cancer vaccine development. Safety of exosomes has been established in clinical trials that can be administered, but their potency for eliciting appropriate immune responses to kill cancer cells leaves much to be desired (Tan et al. 2010). Most of the investigational evidence is about solid tumors, and it has not been demonstrated that non-solid tumors (e.g. hematological malignancies) can be treated using exosome technology. Moreover, exosomal immunotherapy relies on the immune system and cancer patients, who are immuno-compromised and/or immunosuppressed due to chemotherapy and radiotherapy, might not be able to overcome cancer with their immune system alone.

Folate-Linked Nanoparticles

PEG-coated biodegradable nanoparticles can be coupled to folic acid to target the folate-binding protein; this molecule is the soluble form of the folate receptor that is overexpressed on the surface of many tumor cells. The specific interaction

between the conjugate folate-nanoparticles and the folate-binding protein has been evaluated by surface plasmon resonance and confirmed a specific binding of the folate-nanoparticles to the folate-binding protein. Thus, folate-linked nanoparticles represent a potential new drug carrier for tumor cell-selective targeting.

Ginger Nanoparticles for Delivery of Chemotherapy in Colorectal Cancer

Ginger-derived lipid nanoparticles can be used as a vector for delivery of the doxorubicin (DOX) for treatment of colon cancer. Nanoparticles created from ginger and their lipids were reassembled into ginger-derived nanovectors (GDNVs) that were taken up by colon cancer cells in an experimental study (Zhang et al. 2016). GDNVs showed better biocompatibility up to a concentration of 200 µmol/l as compared with cationic liposomes. DOX could be loaded in GDNVs with higher efficiency and showed a better pH-dependent drug-release profile than commercially available liposomal-DOX. Targeted delivery of DOX to Colon-26 tumors in vivo by GDNVs conjugated with the targeting ligand folic acid inhibited tumor more than free DOX. Such natural nanovectors avoid the undesirable effects of synthetic liposomes, such as cells stress and apoptosis.

Gold Nanoparticles Stabilized with Resveratrol

Synthesis of gold nanoparticles has stabilized by exploiting the antioxidant property of resveratrol and formation of resveratrol gold nanoparticles (R-GNPs) was confirmed by observation of the surface plasmon resonance band at 537 nm (Mohanty et al. 2014). The average size of R-GNPs produced in resveratrol medium was \sim 35 nm, geometrical shape was spherical and zeta potential was -21.2 mV. R-GNPs were biocompatible and showed excellent stability in saline and other buffers mimicking the physiological pH. The cytotoxic activity of doxorubicin loaded R-GNPs against glioma carcinoma cell line (LN 229), showed the suitability of R-GNPs as a carrier for anticancer drugs.

Iron Oxide Nanoparticles

A novel water-dispersible oleic acid (OA)-Pluronic-coated iron oxide magnetic nanoparticle formulation that can be loaded easily with high doses of water-insoluble anticancer agents (Jain et al. 2005). Drug partitions into the OA shell surrounding iron oxide nanoparticles, and the Pluronic that anchors at the OA-water interface confers aqueous dispersity to the formulation. Neither the formulation components nor the drug loading affects the magnetic properties of the core iron oxide nanoparticles. Sustained release of the incorporated drug is observed over 2 weeks under in vitro conditions. The nanoparticles have further demonstrated sustained intracellular drug retention relative to drug in solution and a dose-dependent antiproliferative

effect in breast and prostate cancer cell lines. This nanoparticle formulation can be used as a universal drug carrier system for systemic administration of water-insoluble drugs while simultaneously enabling magnetic targeting and/or imaging.

Lipid Based Nanocarriers

LiPlasome Pharma's proprietary prodrug and drug delivery technology is based on smart lipid based nanocarriers (LiPlasomes) that can be applied for targeted transport of anticancer drugs. The targeted drug delivery principle consists of long circulating nanoparticles such as liposomes or micelles that accumulate in porous cancer tissue with a high PLA2 activity. The carrier nanoparticles are composed of special prodrug lipids whose degradation products, after exposure to PLA2, are converted to active drugs such as anticancer lysolipids and/or fatty acid drug derivatives The PLA2 hydrolysis products will furthermore act as locally generated permeability enhancers that promote the absorption of the released drugs across the cancer cell membranes into putative intracellular target sites. This innovative prodrug and drug delivery concept allows for intravenous transport of high concentrations of anticancer drugs directly to the tumor target. It enables, without any prior knowledge of the position and size of the tumor, to release the anticancer drugs specifically at the tumor target site. The delivery system is formulated with PEG to prolong the serum half-life of the drugs and prodrugs and avoid the nanocarriers being removed by the reticuloendothelial system.

Micelles for Drug Delivery in Cancer

Block-copolymer micelles are spherical supramolecular assemblies of amphiphilic copolymers that have a core-shell-type architecture. The core is a loading space that can accommodate hydrophobic drugs, and the shell is a hydrophilic brush-like corona that makes the micelle water soluble, thereby allowing delivery of the poorly soluble contents (Fig. 8.1).

However, a key issue with the contained cytotoxic drugs is an understanding of how the micelle and the micelle-incorporated agent are distributed. By using fluorescently labeled polymer and organelle-specific dyes in combination with confocal microscopy, it has been shown that the micelles localize in several cytoplasmic organelles, including the mitochondria, but not the nucleus. Furthermore, the micelles increase the amount of a drug delivered to the cells, and have the potential to deliver drugs to certain subcellular targets. Antibodies can be attached to the polymers that make up the micelles. Administering immunomicelles loaded with the sparingly soluble anticancer drugs. Paclitaxel micelle, a tumor-targeted drug delivery system, has been investigated in clinical trials. Paclitaxel was shown to have remarkably prolonged blood circulation and effectively accumulate in solid tumors indicating a potential for the targeted therapy of solid tumors. A multicenter, open-label phase II treatment of advanced pancreatic cancer with paclitaxel loaded polymeric micelle

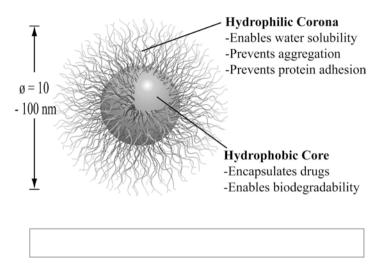


Fig. 8.1 Use of micelles for drug delivery (Source: Sutton et al. 2007)

showed that it was well tolerated and common toxicities were qualitatively like those seen with Cremophor-based paclitaxel (Saif et al. 2010). Overall survival and other efficacy parameters were preferable to that seen historically with gemcitabine. A phase II study of a cremophor-free, polymeric micelle formulation of paclitaxel for patients with advanced urothelial cancer after gemcitabine-cisplatin failure was generally well tolerated and showeded sufficient antitumor activity to warrant further development when used as second-line chemotherapy (Lee et al. 2012).

DACH-platin-PEG-polyglutamic acid (DACH Platin MedicelleTM) from NanoCarrier, based on MedicelleTM technology, has demonstrated enhanced permeability and retention of the compound in the tumor, leading to improved efficacy and toxicity profiles in animal experiments. The mechanism of action of MedicelleTM delivery system is based on the formation of micelles, including hydrophilic-hydrophobic block co-polymers, with a hydrophobic inner core and hydrophilic outer shell. This allows the chemical entrapment of various drugs into the micelles. The drugs are then released slowly into the organism. This product is being developed for clinical application.

Camptothecin (CPT) is a topoisomerase I inhibitor that is effective against cancer, but clinical application of CPT is limited by insolubility, instability, and toxicity problems. Biocompatible, targeted sterically stabilized micelles (SSM) have been used as nanocarriers for CPT (CPT-SSM). CPT solubilization in SSM is reproducible and is attributed to avoidance of drug aggregate formation. Furthermore, SSM composed of polyethylene glycol (PEGylated) phospholipids are attractive nanocarriers for CPT delivery because they are sufficiently small (~14 nm) to extravasate through the leaky microvasculature of tumor and inflamed tissues for passive targeting of solid cancers in vivo, resulting in high drug concentration in tumors and reduced drug toxicity to the normal tissues.

Stealth micelle formulations have stabilizing PEG coronas to minimize opsonization of the micelles and maximize blood circulation times. Clinical data have been reported on three stealth micelle systems: SP1049C, NK911, and Genexol-PM (Sutton et al. 2007). SP1049C is formulated as doxorubicin (DOX)-encapsulated pluronic micelles, NK911 is DOX-encapsulated micelles from a copolymer of PEG and DOX-conjugated poly(aspartic acid), and Genexol-PM is a paclitaxelencapsulated PEG-PLA micelle formulation. Polymer micelles are becoming a powerful nanotherapeutics platform that affords several advantages for targeted drug delivery in cancer, including increased drug solubility, prolonged circulation half-life, selective accumulation at tumor sites, and a decrease in toxicity.

A unique tumor-targeted micellar drug-delivery platform has been developed using paclitaxel as a model therapeutic. This nanopreparation is composed of a MMP2-sensitive self-assembly PEG 2000-paclitaxel conjugate (as a prodrug and MMP 2-sensitive moiety), transactivating transcriptional activator peptide-PEG1000-phosphoethanolamine (PE) as a cell-penetrating enhancer, and PEG1000-PE as a nanocarrier building block (Zhu et al. 2013). Several major drug delivery strategies, including self-assembly, PEGylation, the enhanced permeability and retention effect, stimulus sensitivity, a cell-penetrating moiety, and the concept of prodrug, were used in design of this nanoparticle in a collaborative manner. The nanopreparation enabled superior cell internalization, cytotoxicity, tumor targeting, and antitumor efficacy in vitro and in vivo as compared to its nonsensitive counterpart, free paclitaxel and conventional micelles. This nanoparticle construct has potential for effective intracellular delivery of drug into cancer cells.

Minicells for Targeted Delivery of Nanoscale Anticancer Therapeutics

Indiscriminate drug distribution and severe toxicity of systemic administration of chemotherapeutic agents can be overcome through encapsulation and cancer cellspecific targeting of chemotherapeutics in 400 nm minicells (EnGeneIC Delivery Vehicle). Targeted minicells enter the cancer cells via receptor-mediated endocytosis while the bacteria carrying nanoparticles enter the mammalian cells in a nonspecific manner, i.e. via phagocytosis. Scientists at EnGeneIC discovered that minicells can be packaged with therapeutically significant concentrations of chemotherapeutics of differing charge, hydrophobicity, and solubility (MacDiarmid et al. 2007). Targeting of minicells via bispecific antibodies to receptors on cancer cell membranes results in endocytosis, intracellular degradation, and drug release. Doses of drugs delivered via minicells are ~1000 times less than the dose of the free drug required for equivalent or better tumor shrinkage It produces significant tumor growth inhibition and regression in mouse xenografts and lymphoma in dogs despite administration of minute amounts of drug and antibody; a factor critical for limiting systemic toxicity that should allow the use of complex regimens of combination chemotherapy. Phase I clinical trials are in progress for various cancers.

In a further study, minicells were shown to specifically and sequentially deliver to tumor xenografts siRNAs or shRNA-encoding plasmids to counteract drug resistance by knocking down a multidrug resistance protein (MacDiarmid et al. 2009). Subsequent administration of targeted minicells containing cytotoxic drugs eliminate formerly drug-resistant tumors. The dual sequential treatment, involving minicells loaded with both types of payload, enable complete survival without toxicity in mice with tumor xenografts, while involving several thousand-fold less drug, siRNA and antibody than needed for conventional systemic administration of cancer therapies.

Targeted minicells loaded with doxorubicin were safely administered to dogs with late stage spontaneous brain cancer and clinical activity was observed (MacDiarmid et al. 2016). These findings demonstrate the strong potential for clinical applications of targeted, doxorubicin-loaded minicells for the effective treatment of patients with brain cancer. On this basis, a phase I clinical study of EGFR-targeted, doxorubicin-loaded minicells (EnGeneIC's Cerebral EDVTM) for effective treatment of human patients with recurrent glioblastoma was completed in Australia and is in progress in the USA.

Nanoconjugates for Subcutaneous Delivery of Anticancer Drugs

Most of the anticancer drugs are administered intravenously. Nanoformulation of anticancer drugs are being developed for subcutaneous delivery of existing and new chemotherapeutics. Subcutaneous nanocarrier delivery of hyaluronan-conjugated doxorubicin or cisplatin has demonstrated significantly improved efficacy with decreased toxicity compared with standard agent combination therapy at all doses tested, achieving complete pathologic tumor response in mice implanted with human tumors (Cohen et al. 2011). Advantages of subcutaneous anticancer drug delivery are:

- Avoids complicated and expensive intravenous infusions.
- Improves safety and efficacy for existing chemotherapy drugs.
- Highly localized drug delivery to primary tumor sites to prevent recurrence.
- Enables development of multi-drug combinations to overcome drug resistance.
- Incorporation of imaging agents to monitor penetration of the drug into tumor.

Nanomaterials for Delivery of Poorly Soluble Anticancer Drugs

Nanomaterials have been successfully manipulated to create a new drug-delivery system that can solve the problem of poor water solubility of most promising currently available anticancer drugs and thereby increase their effectiveness. The poorly soluble anticancer drugs require the addition of solvents for them to be easily absorbed into cancer cells. Unfortunately, these solvents not only dilute the potency of the drugs but create toxicity as well. A novel approach has been devised using silica-based nanoparticles to deliver the anticancer drug camptothecin and other water-insoluble drugs into human cancer cells (Lu et al. 2007). The method incorporates a hydrophobic anticancer drug camptothecin into the pores of fluorescent

mesoporous silica nanoparticles and delivers the particles into a variety of human cancer cells to induce cell death. The results suggest that the mesoporous silica nanoparticles might be used as a vehicle to overcome the insolubility problem of many anticancer drugs.

Nanoparticle Formulation for Enhancing Anticancer Efficacy of Cisplatin

Cisplatin is a first line chemotherapy for most types of cancer. However, its use is dose-limited due to severe nephrotoxicity. Rational engineering of a novel nanoplatinate has been reported, which self-assembles into a nanoparticle at unique platinum to polymer ratio, and releases cisplatin in a pH-dependent manner (Paraskar et al. 2010). The nanoparticles are rapidly internalized into the endolysosomal compartment of cancer cells, and exhibit an IC50 comparable to that of free cisplatin and superior to carboplatin. The nanoparticles showed significantly improved anticancer efficacy in terms of tumor growth delay in breast and lung cancers. Furthermore, the nanoparticle treatment resulted in reduced systemic and nephrotoxicity, validated by decreased biodistribution of platinum to the kidney. Given the need for a better platinate, this coupling of nanotechnology and structure-activity relationship to rationally reengineer cisplatin is anticipated to have a major impact on the treatment of cancer.

Nanoparticle Formulations of Paclitaxel

Paclitaxel is active and widely used to treat multiple types of solid tumors. The commercially available paclitaxel formulation uses Cremophor/ethanol (C/E) as the solubilizers. Other formulations including nanoparticles have been introduced. A study evaluated the effects of nanoparticle formulation of paclitaxel on its tissue distribution in experimental animals (Yeh et al. 2005). The nanoparticle and C/E formulations showed significant differences in paclitaxel disposition; the nanoparticles yielded 40% smaller area under the blood concentration-time curve and faster blood clearance of total paclitaxel concentrations (sum of free, protein-bound, and nanoparticle-entrapped drug). Tissue specificity of the two formulations was different. The nanoparticles showed longer retention and higher accumulation in organs and tissues, especially in the liver, small intestine, and kidney. The most striking difference was an eight-fold greater drug accumulation and sustained retention in the kidney. These data indicate that nanoparticulate formulation of paclitaxel affects its clearance as well as distribution in tissues with preferential accumulation in the liver, spleen, small intestine, and kidney. Solid tumors have unique features, such as leaky tumor blood vessels and defective lymphatic drainage, that promote the delivery and retention of macromolecules or particles, a phenomenon recognized as the enhanced permeability and retention effect. Tissue specificity of the gelatin nanoparticles warrants further investigations before using nanoparticle formulations of anticancer drugs for tumors in various organs.

Gold nanoparticles (2 nm) have been covalently functionalized with paclitaxel (Gibson et al. 2007). The synthetic strategy involves the attachment of a flexible hexaethylene glycol linker at the C-7 position of paclitaxel followed by coupling of the resulting linear analogue to phenol-terminated gold nanocrystals. The reaction yields the product with a high molecular weight, while exhibiting an extremely low polydispersity index. The organic shell of hybrid nanoparticles contains 67% by weight of paclitaxel, which corresponds to ~70 molecules of the drug per 1 nanoparticle. High-resolution TEM was employed for direct visualization of the inorganic core of hybrid nanoparticles, which were found to retain their average size, shape, and high crystallinity after multiple synthetic steps and purifications. The interparticle distance substantially increases after the attachment of paclitaxel as revealed by lowmagnification TEM, suggesting the presence of a larger organic shell. Thus, organic molecules with exceedingly complex structures can be covalently attached to gold nanocrystals in a controlled manner and fully characterized by traditional analytical techniques. In addition, this approach gives a rare opportunity to prepare hybrid particles with a well-defined amount of drug and offers a new alternative for the design of nanosized drug-delivery systems. Follow-up studies will determine the potency of the paclitaxel-loaded nanoparticles. Since each ball is loaded with a uniform number of drug molecules, it will be relatively easy to compare the effectiveness of the nanoparticles with the effectiveness of generally administered paclitaxel. This technique could help to deliver more of the drug directly to the cancer cells and reduce the side effects of chemotherapy. The aim is to improve the effectiveness of the drug by increasing its ability to stay bound to microtubules within the cell.

Albumin nanoparticle technology enables the transportation of hydrophobic drugs such as paclitaxel without the need of potentially toxic solvents. Nab-paclitaxel can be administered without premedication, in a shorter infusion time and without the need for a special infusion set. Moreover, this technology allows the selective delivery of larger amounts of anticancer drug to tumors, by exploiting endogenous albumin pathways. Nab-paclitaxel is approved for the treatment of metastatic breast cancer, after the failure of first-line standard therapy, when anthracyclines are not indicated. Efficacy and safety data, along with a more convenient administration, confirm the potential for nab-paclitaxel to become a reference taxane in breast cancer treatment (Guarneri et al. 2012).

Nanoparticles Containing Albumin and Antisense Oligonucleotides

Nanoparticles consisting of human serum albumin (HSA) and containing different antisense oligonucleotides (ASO) have been used for drug delivery to tumors. The preparation process has been optimized regarding the amount of solving agent, stabilization conditions as well as nanoparticle purification. The glutaraldehyde crosslinking procedure of the particle matrix is a crucial parameter for biodegradability and drug release of the nanoparticles. The drug loading efficiency increases with longer chain length and employment of a phosphorothioate backbone. The resulting nanoparticles can be tested in cell cultures for cytotoxicity and cellular uptake. All cell lines show a significant cellular uptake of HSA nanoparticles. The entrapment of a fluorescent labeled oligonucleotide within the particle matrix can be used for the detection of the intracellular drug release of the carrier systems. Confocal laser scanning microscopy reveals that nanoparticles cross-linked with low amounts of glutaraldehyde, rapidly degrade intracellularly, leading to a significant accumulation of the ASO in cytosolic compartments of the tumor cells.

Niosomes for Anticancer Drug Delivery

Several modifications of niosomes have been used to improve cancer drug delivery. An efficient tumor-targeted niosomal delivery system for the delivery of doxorubicin as an anticancer agent was designed and transferrin was conjugated to niosomes to produce transferrin (Tf) niosomes (Tavano et al. 2013). Niosome-Tf conjugates demonstrated far greater extents of cellular uptake by cancer cells, suggesting that they were mainly taken up by transferrin receptor-mediated endocytosis. Doxorubicin-loaded niosome anticancer activity was demonstrated against MCF-7 and MDA-MB-231 tumor cell lines and a significant reduction in viability in a dose-and time-related manner was observed.

Pegylated Nanoliposomal Formulation

PEG-coated nanoparticles remain in the tumors and bloodstream longer compared to gelatin nanoparticles. The coating prevents the nanoparticles from removal by the reticuloendothelial system. This property has led to more effective nanoparticles with tumor-targeting properties.

Ceramide, an antimitogenic and proapoptotic sphingolipid, accumulates in cancer tissues and helps to kill cancer cells when patients undergo chemotherapy and radiation. Although the mechanism remains unknown, ceramide is inherently attracted to tumor cells. In vitro tumor cell culture models have shown the potential therapeutic utility of raising the intracellular concentration of ceramide. However, therapeutic use of systemically delivered ceramide is limited by its inherent insolubility in the blood as it is a lipid as well as its toxicity when injected directly into the bloodstream. Packaging ceramide in nanoliposome capsules allows them to travel through the bloodstream without causing toxicity and release the ceramide in the tumor. Systemic intravenous delivery of C6-ceramide (C6) in a pegylated liposomal formulation significantly limited the growth of solid tumors in a syngeneic BALB/c mouse tumor model of breast adenocarcinoma (Stover et al. 2005). A pharmacokinetic analysis of systemic liposomal-C6 delivery showed that the pegylated liposomal formulation follows first-order kinetics in the blood and achieves a steady-state concentration in tumor tissue. Intravenous liposomal-C6 administration was also shown to diminish solid tumor growth in a human xenograft model of breast cancer. In this study in mice, the ceramide bundles targeted and destroyed only breast cancer cells, sparing the surrounding healthy tissue. Together, these results indicate that bioactive ceramide analogues can be incorporated into pegylated liposomal vehicles for improved solubility, drug delivery, and antineoplastic efficacy. The next step is to explore how additional chemotherapeutic agents could be incorporated into the liposomes for a more lasting effect.

Peptide-Linked Nanoparticle Delivery

The coupling chemistry and surface charge effects of peptide labeling in nanoparticle drug delivery strategies are more difficult to control than using folate. Chemical conjugation to peptides reduces colloidal stability, which is a limiting factor in the development of targeting nanoparticles. However, the successful peptide targeting of structural, hormonal, cytokine and endocrine receptors in the delivery of therapeutic and diagnostic radionuclides provides justification for finding methods to synthesize peptide-targeted nanoparticles (Franzen 2011). Although most of the work so far has been done using gold nanoparticles, biological and polymer nanoparticles are more colloidally stable and present enormous opportunities for coupling to peptides. Further studies are needed to develop peptide targeting for nanoparticles to rival the selectivity that has been achieved with the small molecule folate.

Hydrogel nanoparticles (HNPs), based on aromatic dipeptide N-fluorenylmethoxycarbonyl-diphenylalanine (Fmoc-FF) that self-assembles to produce peptide nanofibrils, have been for delivery of chemotherapeutic agents (Ischakov et al. 2013). Doxorubicin (DOX) and 5-fluorouracil (5-FU) were incorporated into the HNPs to determine how release rates differed owing to differences in the drugs' molecular weight, hydrophobicity and chemical structures. It was found that 50% of 5-FU was released from HNPs after 5 h, and the kinetic release reached a plateau after 12 h. In comparison, 50% of DOX was released after 20 h and 80% released within 55 h. This difference in release rate may be explained by DOX possessing an aromatic moiety, and, therefore, it may interact more with the Fmoc-FF structure and hydrogen bonds between the peptides in the HNPs resulting in slower release than 5-FU. Although Fmoc-FF-based HNPs show potential for use in delivering therapeutic agents, the hydrogel may need to be tailored to suit the release rate of the drug in question. The use of peptide-based hydrogels is better than polymer-based hydrogels as fabrication does not require the use of extreme pH and temperature, which can affect biocompatibility.

Poly-2-hydroxyethyl Methacrylate Nanoparticles

Poly-2-hydroxyethyl methacrylate nanoparticles can potentially be used for the controlled release of the anticancer drug doxorubicin and reduction of its toxicity (Chouhan and Bajpai 2009). Suspension polymerization of 2-hydroxyethyl methacrylate (HEMA) results in the formation of swellable nanoparticles of defined

composition. Release profiles of doxorubicin can be greatly modified by varying the experimental parameters such as percent loading of doxorubicin and concentrations of HEMA, cross-linker and initiator. Swelling of nanoparticles and the release of doxorubicin increases with the increase in percentage loading of drug. Absorption spectra of doxorubicin do not change following its capture and release form the nanoparticles, indicating that chemical structure of the drug is likely to be unaffected by the procedure.

Polypeptide-Doxorubicin Conjugated Nanoparticles

Artificial recombinant chimeric polypeptides (CPs), produced from genetically altered E. coli, have been shown to spontaneously self-assemble into 50 nm nanoparticles on conjugation with various chemotherapeutics regardless of their water solubility (MacKay et al. 2009). CPs contain a biodegradable polypeptide that is attached to a short Cys-rich segment. Covalent modification of the Cys residues with a structurally diverse set of chemotherapeutics, leads to spontaneous formation of nanoparticles over a range of CP compositions and molecular weights. Attachment to one of CPs induces characteristics that the drug alone does not possess. Most chemotherapeutics do not dissolve in water, which limits their ability to be taken in by cells, but attachment to a nanoparticle makes the drug soluble. When used to deliver chemotherapeutics to a murine cancer model, CP nanoparticles have a fourfold higher maximum tolerated dose than free drug, and induce nearly complete tumor regression after a single dose. After delivering the drug to the tumor, the delivery vehicle breaks down into harmless byproducts, markedly decreasing the toxicity for the recipient. This simple as well as inexpensive strategy can promote co-assembly of drugs, imaging agents and targeting moieties into multifunctional nanomedicines. Since blood vessels supplying tumors are more porous, or leaky, than normal vessels, the nanoformulation can more easily enter and accumulate within tumor cells. This means that higher doses of the drug can be delivered, increasing its anticancer effects while decreasing the side effects associated with systematic chemotherapy.

Porous Silicon Nanoparticles for Cancer Drug Delivery

Conjugation of methotrexate (MTX) to porous silicon (PSi) nanoparticles (MTX-PSi) with positively charged surface can improve the cellular uptake of MTX and inhibit the proliferation of cancer cells. In an experimental study, MTX-PSi conjugates sustained the release of MTX up to 96 h, and the released fragments including MTX were confirmed by mass spectrometry (Wang et al. 2015). Finally, the porous structure of MTX-PSi enabled a successful concomitant loading of an anti-angiogenic hydrophobic drug, sorafenib, and considerably enhanced the dissolution rate of sorafenib. Dual drug delivery of antiangiogenic and chemotherapeutic agents can enhance anticancer therapeutic effect.

Protosphere Nanoparticle Technology

Protosphere[™] nanoparticle technology (Abraxis Bioscience Inc), also referred to as nanoparticle albumin-bound or nab[™] technology, was used to integrate biocompatible proteins with drugs to create the nanoparticle form of the drug having a size of about 100–200 nm. SPARC (secreted protein acidic and rich in cysteine), a protein overexpressed and secreted by cancer cells, binds albumin to concentrate albumin-bound cytotoxic drugs at the tumor.

The product Abraxane (ABI-007) is a patented albumin-stabilized nanoparticle formulation of paclitaxel (nab-paclitaxel) designed to overcome insolubility problems encountered with paclitaxel. The solvent Cremophor-EL, used previously in formulations of paclitaxel, causes severe hypersensitivity reactions. To reduce the risk of allergic reactions when receiving Taxol, patients must undergo premedication using steroids and antihistamines and be given the drug using slow infusions. The active component (paclitaxel) can be delivered into the body at a 50% higher dose over 30 min. This contrasts with Taxol infusions, which can take up to 3 h. Because Abraxane is solvent-free, solvent-related toxicities are eliminated, premedication is not required and administration can occur more rapidly. Abraxane also has a different toxicity profile than solvent-based paclitaxel, including a lower rate of severe neutropenia. In a randomized phase III trial, the response rate of Abraxane was almost twice that of the solvent-containing drug Taxol. Because Abraxane does not contain solvents, higher doses of paclitaxel could be given which may account in part for its increased anticancer activity. In addition, albumin is a protein that normally transports nutrients to cells and has been shown to accumulate in rapidly growing tumors. Therefore, Abraxane's increased effectiveness may also be due to preferential delivery of albumin-bound paclitaxel to cancer cells. In addition to the standard infusion formulation of Abraxane, oral and pulmonary delivery formulations are also being investigated.

A randomized controlled phase III clinical trial compared the safety and efficacy of 260 mg/m² of Abraxane to 175 mg/m² of Taxol administered every 3 weeks in patients with metastatic breast cancer (Gradishar et al. 2005). Abraxane was infused over 30 min without steroid pretreatment and at a higher dose than Taxol, which requires steroid therapy and infusion over 3 h Abraxane was found to be superior to Taxol on lesion response rate as well as on tumor progression rate. In 2005, the FDA approved Abraxane for the treatment of metastatic breast cancer. Abraxane also is being evaluated in non-small cell lung, ovarian, melanoma and cervical cancers.

siRNA Delivery in Combination with Nanochemotherapy

Use of anticancer drugs in combination with siRNAs is promising for knockout of drug resistance genes as well as for restoration of the sensitivity of resistant tumors to anticancer therapy. Nanotechnology-based approach can protect siRNA against RNAse degradation as well as prevent off-target effects, which would optimize delivery in combination chemotherapeutic drugs to treat resistant tumors (Tekade et al. 2016). Several nanovectors have been used in animal experimental

studies including dendrimers, micelles, polymersomes, lipidic nanoparticles, liposomes, and lipoplexes. However, further research is still required to develop an ideal vector for the simultaneous delivery of siRNA and anticancer drug.

Zinc Oxide Nanoparticles for Drug Delivery in Cancer

Zinc oxide (ZnO) nanomaterials provide versatile platforms for biomedical applications and therapeutic intervention and recent studies demonstrate that they hold considerable promise as anticancer agents. Several of these are under development at the experimental, preclinical and clinical stages. Through a better understanding of the mechanisms of action and cellular consequences resulting from nanoparticles interactions with cells, the inherent toxicity and selectivity of ZnO nanoparticles against cancer may be improved further to make them attractive new anticancer agents (Rasmussen et al. 2010).

Nanoparticles for Targeted Delivery of Anticancer Therapeutics

Nanosystems are emerging that may be very useful for tumor-targeted drug delivery: novel nanoparticles are pre-programmed to alter their structure and properties during the drug delivery process to make them most effective for the different extraand intracellular delivery steps. This is achieved by the incorporation of molecular sensors that can respond to physical or biological stimuli, including changes in pH, redox potential or enzymes. Tumor-targeting principles include systemic passive targeting and active receptor targeting. Physical forces (e.g. electric or magnetic fields, ultrasound, hyperthermia or light) may contribute to focusing and triggered activation of nanosystems. Biological drugs delivered with programmed nanosystems also include plasmid DNA, siRNA and other therapeutic nucleic acids.

Drug delivery systems are being developed that attempt to destroy tumors more effectively by using synthesized smart nanoparticles that target and kill cancer cells while sparing healthy cells. Such particles can be injected intravenously into the blood circulation. Nanoparticle-based therapy relies on enhanced permeability and retention effect to localize in solid tumors and not healthy tissue. Each particle, chemically programmed to have an affinity for the cell wall of tumor, can recognize the cancer cell, anchor itself to it, and diffuse inside the cell. Once inside, the particle promptly disintegrates and releases the drug precisely where it is needed. To be effective, the nanoparticles must evade the body's immune system, penetrate the cancer cells, and discharge the drugs before being recognized by the cancer cells. Advantages of such systems are:

- They can fool cancer cells, which are very good at detecting and rejecting drugs.
- Provide rapid drug delivery at sufficiently high concentration that can overwhelm the cancer cell's resistance mechanisms.
- Reduction of side effects because the cancer cells are targeted selectively, sparing the normal cells.

Another approach is use a nanoparticle made of a hydrogen and carbon polymer with anticancer drug bound up in its fabric and attached to a substance that targets cancer cells. Following intravenous injection, the polymer would gradually dissolve on reaching the target and gradually release the drug. One limitation of systemic introduction of such nanoparticles, unless properly targeted, is that they may end up in the liver and spleen. This is an unwanted side effect because once the nanoparticles dissolve in those organs, they release toxic levels of chemotherapy in healthy tissues.

Aptamer Nanoformulations for Targeted Anticancer Therapy

Role of aptamers in combination of cancer diagnosis with therapy has been described earlier in this chapter. The small size of aptamers, low immunogenicity and stability facilitate the development of aptamer-based nanoformulations suitable for drug delivery systems. Examples of the anticancer potential of aptamers and their application for active drug targeting are shown in Table 8.4.

Design of a self-assembled aptamer-micelle nanostructure has been reported that achieves selective and strong binding of otherwise low-affinity aptamers at physio-logical conditions (Wu et al. 2009). Specific recognition ability is directly built into the nanostructures. The attachment of a lipid tail onto the end of nucleic acid aptamers provides these unique nanostructures with an internalization pathway. Other merits include: extremely low off rate once bound with target cells, rapid recognition ability with enhanced sensitivity, low critical micelle concentration values, and dual-drug delivery pathways. To prove the potential detection/delivery application of this aptamer–micelle in biological living systems, the authors mimicked a tumor site in the blood stream by immobilizing tumor cells onto the surface of a flow channel device. Flushing the aptamer–micelles through the channel demonstrated their selective recognition ability under flow circulation in human whole-blood sample.

Type of aptamer	Nanoformulation	Indication	Reference
Anti-HER2 aptamer (HApt)	Gold nanoparticles	HER-2 positive breast cancer	Lee et al. (2015)
CD133 aptamer	Salinomycin-loaded PEGylated PLGA nanoparticles	Osteosarcoma	Ni et al. (2015)
CD133 aptamers A15 and EGFR aptamers CL4	Salinomycin-loaded PLGA nanoparticles	Hepatocellular carcinoma	Jiang et al. (2015)
EGFR-targeting aptamers	Triple-functional pRNA-3WJ nanoparticles	Triple-negative breast cancer	Shu et al. (2015)
EpCAM aptamer	Doxorubicin-loaded PEG- PLGA nanoparticles	Non-small cell lung cancer	Alibolandi et al. (2015)
Mucin 1 aptamer	Gold nanoparticle-hybridized graphene oxide	Breast cancer	Yang et al. (2015)

 Table 8.4
 Aptamer-based nanoformulations for targeted anticancer therapy

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The aptamer–micelles show great dynamic specificity in flow channel systems that mimic drug delivery in the blood system. Therefore, DNA aptamer-micelle assembly has shown high potential for cancer cell recognition and for targeted in vivo drug delivery applications.

Use of DNA aptamers with doxorubicin-encapsulated DOTAP/DOPE nanoparticles significantly suppress the tumor growth and increased the survival rate in animal models with breast cancer xenografts (Song et al. 2015).

Nanoformulations presented by based on Fe3O4-saturated lactoferrin (Fe3O4-bLf) nanocarriers with locked nucleic acid (LNA) modified aptamers, improve the survival rate in the triple positive xenograft colon cancer model (EpCAM, CD133, CD44), due to phosphorylation of p53, induction of apoptosis and mitochondrial depolarization (Roy et al. 2015). A complete regression of tumor was observed in 70% of mice. In addition to anticancer properties, these multifunctional nanosystems may be used in near-infrared (NIR), MRI and CT imaging.

Bacteriophage Capsid-Based Nanoparticles for Targeted Cell-Delivery

The importance of bacteriophage capsid-based NPs as cell-delivery vehicles is now being recognized. The bacteriophage T4 capsid $(100 \times 70 \text{ nm})$ is well suited for this purpose, because it can hold a single long DNA or multiple short pieces of DNA up to 170 kb packed together with >1000 protein molecules. Virtually any specific protein and nucleic acid can be encapsidated together into a phage T4 capsid that can display surface-binding ligands for tissue targeting. T4 NPs packed in vivo with active cyclic recombination (Cre) recombinase and in vitro with fluorescent mCherry expression plasmid DNA have been delivered into cancer cells (Liu et al. 2014). When released into cells together, the packaged active Cre recombinase within the capsid circularizes the packaged DNA of the linear expression plasmid, enhancing the expression of the mCherry gene. The efficient and specific packaging and unpackaging of DNA and active protein together into targeted cells has potential applications in targeted gene therapy and cancer therapy.

Canine Parvovirus as a Nanocontainer for Targeted Drug Ddelivery

The canine parvovirus (CPV) utilizes transferrin receptors (TfRs) for binding and cell entry into canine as well as human cells. TfRs are over-expressed by a variety of tumor cells and are widely being investigated for tumor-targeted drug delivery. To explore the natural tropism of CPV to TfRs for targeting tumor cells, CPV virus-like particles (VLPs) produced by expression of the CPV-VP2 capsid protein in a baculo-virus expression system have been examined for attachment of small molecules and delivery to tumor cells. Structural modeling suggested that six lysines per VP2 subunit are presumably addressable for bioconjugation on the CPV capsid exterior. Between 45 and 100 of the possible 360 lysines/particle can be routinely derivatized with dye molecules depending on the conjugation conditions. Dye conjugation also

demonstrates that the CPV-VLPs could withstand conditions for chemical modification on lysines. Attachment of fluorescent dyes neither impairs binding to the TfRs nor affects internalization of the 26 nm-sized VLPs into several human tumor cell lines. CPV-VLPs therefore exhibit highly favorable characteristics for development as a novel nanomaterial for tumor targeting.

Carbon Nanotubes for Targeted Drug Delivery to Cancer Cells

CNTs with DNA and RNA wrapped around them to make them biocompatible can be targeted towards cancer cells by attaching additional molecules. Such CNT composites, in combination with laser treatment, may be used to destroy the cancer cells. An improved delivery scheme for intracellular tracking and anticancer therapy uses a novel double functionalization of a CNT delivery system containing antisense oligodeoxynucleotides as a therapeutic gene and CdTe QDs as fluorescent labeling probes via electrostatically layer-by-layer assembling (Jia et al. 2007).

Chemically functionalized SWCNTs have shown promise in tumor-targeted accumulation in mice and exhibit biocompatibility, excretion, and little toxicity. The anticancer drug paclitaxel (PTX) has been conjugated to branched PEG chains on SWCNTs via a cleavable ester bond to obtain a water-soluble SWCNT-PTX conjugate (Liu et al. 2008). SWCNT-PTX is more efficient in suppressing tumor growth than Taxol in a murine 4 T1 breast cancer model, owing to prolonged blood circulation and ten-fold higher tumor PTX uptake by SWCNT delivery, likely through enhanced permeability and retention. Drug molecules carried into the reticuloendothelial system are released from SWCNTs and excreted via biliary pathway without toxic effects on normal organs. Thus, CNT drug delivery is promising for enhancing treatment efficacy and minimizing side effects of cancer therapy by use of low drug doses. Water-dispersed carbon nanohorns, prepared by adsorption of polyethylene glycol-doxorubicin conjugate (PEG-DXR) onto oxidized single-wall carbon nanohorns, have been shown to be effective anticancer drug delivery carriers when administered intratumorally to human NSCLC-bearing mice (Murakami et al. 2008). There was significant retardation of tumor growth associated with prolonged DXR retention in the tumor.

Although considerable further work is required before any new drugs based on CNTs are developed, it is hoped that it will eventually lead to more effective treatments for cancer. However, it is too early to claim whether carbon-based nanomaterials will become clinically viable tools to combat cancer, although there is a definite role for them in complementing existing technologies.

Carbon Magnetic Nanoparticles for Targeted Drug Delivery in Cancer

The high surface area of CNTs enables efficient drug loading as well as bioconjugation and makes them the ideal platforms for decoration with magnetic nanoparticles (MNPs), which are important because of their broad range of potential applications in non-invasive tumor imaging and drug delivery (Quyen Chau et al. 2015). The remarkable characteristics of CNTs and MNPs can be combined leading to CNT/MNP hybrids which offer numerous advantages in comparison to the use of either material alone.

A nanocomposite drug delivery system, Chelerythrine and Fe3O4 loaded MWNTs, can target hepatocytes when treating malignant tumors (Cao et al. 2016). Cytotoxicity and anti-proliferation effect from the prepared nanocomposites were tested in vitro on human hepatocarcinoma HepG2 and normal liver LO2 cell lines. The results showed an efficient inhibition rate to HepG2 cell line and low cytotoxicity to LO2 cell line making the nanocomposites promising candidate for anticancer therapy of malignant tumors. Anticancer drugs such as doxorubicin can be incorporated in carbon MNPs.

Chitosan Nanoparticles for Targeted Anticancer Drug Delivery

Chitosan-based NPs are one of the most promising delivery vehicles for cancer chemotherapy and diagnosis due to their unique characteristics such as biodegradability, biocompatibility, remarkable cell membrane penetrability, high drug-carrying capacities, pH-dependent therapeutic unloading, ability to have a multi-functionality and prolonged circulating time (Prabaharan 2015). Grafting cancer-specific ligands onto the Chitosan NPs, which leads to ligand-receptor interactions, has been successfully developed for active targeting. Chitosan-conjugated components also respond to external or internal physical and chemical stimulus in targeted delivery to tumors (Ghaz-Jahanian et al. 2015).

CRLX101 for Targeted Anticancer Drug Delivery

CRLX101 (Cerulean Pharma Inc) is a nanoparticle consisting of a cyclodextrincontaining polymer conjugate of the anticancer drug camptothecin (CPT). The individual polymer strands self-assemble into nanoparticles (~5 strands) of ~20–30 nm diameter and 10 wt% CPT by multiple, interstrand, inclusion complex formation between cyclodextrin and the CPT molecules. CRLX101 has been evaluated in clinical trials on patients with relapsed or refractory cancer following chemotherapy. These combined phase I/IIa data demonstrate encouraging safety, pharmacokinetic, and efficacy results (Weiss et al. 2013). CRLX101 is currently in phase II trials for human cancers.

Tumor and nonneoplastic tissue biopsies from cancer patients, who have been administered CRLX101, show that the intact nanoparticles localize in human tumors and not in adjacent tissues (Clark et al. 2016). Sufficient concentrations reach the tumors to cause down-regulation of tumor biomarkers such as topoisomerase I and carbonic anhydrase IX. These results will aid in better understanding how nanoparticle therapeutics function in humans and how to improve design of future cancer therapeutics.

Cyclosert System for Targeted Delivery of Anticancer Therapeutics

Cyclosert[™] (Calando Pharmaceuticals) is the first nanoparticle drug transport platform to be designed de novo and synthesized specifically to overcome limitations in existing technologies used for the systemic transport of therapeutics to targeted sites within the body. Based on small cyclic repeating molecules of glucose called cyclodextrins, Cyclosert promotes the ability of cytotoxic drugs to inhibit the growth of human cancer cells while reducing toxicity and remaining non-immunogenic at therapeutic doses. The system is particularly designed to reduce the toxicity of the drugs until they reach the targeted tumor cells where the active drug is released in a controlled fashion. Animal studies have shown that the Cyclosert system can safely deliver tubulysin A, a potent, but highly toxic, antitumor agent. In vitro studies have shown the tubulysin-Cyclosert conjugate to be effective against multiple human cancer cell lines. The conjugate is stable and 100 times more water soluble than the free drug. Calando is developing CALAA01, a siRNA, for anticancer use using Cyclosert as a delivery system.

Fullerenes for Enhancing Tumor Targeting by Antibodies

Although it was previously possible to attach drug molecules directly to antibodies, scientists have not been able to attach more than a handful of drug molecules to an antibody without significantly changing its targeting ability. That happens, in large part, because the chemical bonds that are used to attach the drugs – strong, covalent bonds – tend to block the targeting centers on the antibody's surface. If an antibody is modified with too many covalent bonds, the chemical changes will destroy its ability to recognize the cancer it was intended to attack.

To overcome this limitation, a new class of anticancer compounds have been created that contain both tumor-targeting antibodies and nanoparticles called fullerenes (C60), which can be loaded with several molecules of anticancer drugs like Taxol®. It is possible to load as many as 40 buckyballs into a single skin-cancer antibody called ZME-018, which can be used to deliver drugs directly into melanoma tumors. Certain binding sites on the antibody are hydrophobic (water repelling), and attract the hydrophobic fullerenes in large numbers so multiple drugs can be loaded into a single antibody in a spontaneous manner. No covalent bonds are required, so the increased payload does not significantly change the targeting ability of the antibody. The real advantage of fullerene immunotherapy over other targeted therapeutic agents is likely to be the fullerene's potential to carry multiple drug payloads, such as Taxol plus other chemotherapeutic drugs. Cancer cells can become drug resistant, and one can cut down on the possibility of their escaping treatment by attacking them with more than one kind of drug at a time. The first fullerene immunoconjugates have been prepared and characterized as an initial step toward the development of fullerene immunotherapy.

Gold Nanoparticles for Targeted Drug Delivery in Cancer

Gold and silica composite nanoparticles have been investigated as nanobullets for cancer. Gold atoms bind to silicon atoms with dangling bonds and serve as seeds for the growth of Au islands. The large electron affinity of gold causes a significant change in the electronic structure of silica resulting in a substantial reduction in the highest occupied and the lowest unoccupied molecular orbital and the optical gap, thus allowing it to absorb near infrared radiation. This suggests that a small cluster can have a similar effect in the treatment of cancer as the large size nanoshell, but with a different mechanism.

The unique chemical properties of colloidal gold make it a promising targeted delivery approach for drugs or genes to specific cells. The physical chemical properties of colloidal gold permit more than one protein molecule to bind to a single particle of colloidal gold. Cytimmune Sciences Inc. has shown that tumor necrosis factor (TNF) can be bound to gold nanocrystals and delivered safely and effectively to tumor-burdened mice and dogs. Cytimmune scientists have characterized and modified the colloidal gold (cAu) particles to optimize binding of TNF to the nanocrystals and the targeting of the particles to the tumor. The therapeutic compounds that CytImmune is developing are new formulations of the TNF- α , which causes the death of tumors but is toxic to healthy organs. Coupling TNF- α to colloidal gold is expected to improve the safety and effectiveness of anticancer therapy. Specifically, two drugs are in development: Aurimune-T and AuriTax. Aurimune-T is manufactured by covalently linking molecules of TNF- α and Thiol-derivatized polyethylene glycol (PEG-THIOL) onto the surface of 25 nm colloidal gold. Intravenously administered Aurimune-T rapidly accumulates in solid tumors implanted in mice and shows little to no accumulation in the reticuloendothelial system or in other healthy organs. Coincident with the sequestration of gold is a ten-fold accumulation of TNF- α in the tumor when compared to animals treated with native TNF- α . By getting more TNF- α to the tumor Aurimune-T improves the safety and efficacy of TNF-α treatment since maximal tumor responses were achieved at lower doses of the drug. The second nanoparticle drug, AuriTax, consists of TNF- α , a chemotherapeutic (paclitaxel), and PEG-THIOL, which are bound to the same cAu nanoparticle. Like Aurimune-T, AuriTax delivers ten-fold more TNF- α and paclitaxel to the solid tumor when compared to each drug alone. These results support the continued development of the colloidal gold platform for cancer therapy and TNF- α as a tumor targeting ligand.

Biocompatible and nontoxic pegylated gold nanoparticles with surface-enhanced Raman scattering have been used for in vivo tumor targeting and detection (Qian et al. 2008). Colloidal gold has been safely used to treat rheumatoid arthritis for 50 years, and has recently been found to amplify the efficiency of Raman scattering by 14–15 orders of magnitude. It has been shown that large optical enhancements can be achieved under in vivo conditions for tumor detection in live animals. An important finding is that small-molecule Raman reporters such as organic dyes are not displaced but were stabilized by thiol-modified polyethylene glycols. These pegylated SERS nanoparticles are considerably brighter than semiconductor QDs with light emission

in the near-infrared window. When conjugated to tumor-targeting ligands such as single-chain variable fragment antibodies (ScFv), the conjugated nanoparticles are able to target tumor biomarkers such as EGFRs on human cancer cells and in xenograft tumor models. ScFv peptides bind cancer cells and the gold particles latch onto tumors after their injection into a mouse. When illuminated with a laser beam, the tumor-bound particles emit a signal that is specific to the dye. The signal from the dye tags is very bright and the distinct peaks in the dye signal mean several different probes could be used at the same time. The tags' rich spectroscopic signatures provide the capability of using several probes at once, but that will require more sophisticated computational tools. The authors are developing data processing tools and making them available to the NCI's caBIG (cancer biomedical informatics grid) so that the research community can use them. Compared with QDs, the gold particles are more than 200 times brighter on a particle-to-particle basis, although they are about 60 times larger by volume. Covered with a non-toxic polymer, the gold particles are about 60-80 nanometers in diameter. That's 150 times smaller than a typical human cell and thousands of times smaller than a human hair. The researchers could detect human cancer cells injected into a mouse at a depth of 1-2 cm. That makes the gold particles especially appropriate tools for gathering information about head or neck tumors, which tend to be more accessible. The technology will need further adaptation for use with abdominal or lung cancers deep within the body.

PEGylated gold nanoparticles are decorated with various amounts of human transferrin (Tf) to give a series of Tf-targeted particles with near-constant size and electrokinetic potential. Studies in experimental animals with tumors show that quantitative biodistribution of the nanoparticles 24 h after intravenous injections results in their accumulations in the tumors and other organs independent of Tf (Choi et al. 2010a). However, the nanoparticle localization within a specific organ is influenced by the Tf content. In tumor tissue, the content of targeting ligands significantly influences the number of nanoparticles localized within the cancer cells. In liver tissue, high Tf content leads to small amounts of the nanoparticles residing in hepatocytes, whereas most nanoparticles can provide greater intracellular delivery of therapeutic agents to the cancer cells within solid tumors than their nontargeted analogs.

Selective transport of gold nanoparticles to the nuclei of cancer cells has been achieved by properly conjugating them with specific peptides (Kang et al. 2010). Localization of gold nanoparticles at the nucleus of a cancer cell damages the DNA resulting in double-strand breaks. Dark-field imaging of live cells in real time revealed that the nuclear targeting of gold nanoparticles specifically induces cytokinesis arrest in cancer cells leading apoptosis.

Prostate tumor specific epigallocatechin-gallate (EGCg) functionalized radioactive gold nanoparticles (AuNPs), when delivered intratumorally, circumvent transport barriers, resulting in targeted delivery of therapeutic payloads. Gold nanoparticles derived from the Au-198 isotope with therapeutic range of 11 mm in tissue have been developed, which is sufficiently long to provide cross-fire effects of a radiation dose delivered to cells within the prostate gland and short enough to minimize the

radiation dose to critical tissues near the periphery of the capsule. The formulation of biocompatible 198Au nanoparticles utilizes the redox chemistry of prostate tumor specific phytochemical EGCg as it converts gold salt into gold nanoparticles and selectively binds with excellent affinity to Laminin67R receptors, which are over expressed in prostate tumor cells. Therapeutic studies showed 80% reduction of tumor volumes in PC-3 xenograft SCID mice after 28 d demonstrating significant inhibition of tumor growth compared to controls (Shukla et al. 2012). This innovative nanotechnological approach serves as a basis for designing biocompatible target specific antineoplastic agents. This novel intratumorally injectable 198AuNP-EGCg nanotherapeutic agent may provide significant advances in oncology for use as an effective treatment for prostate and other solid tumors.

Hepatic Artery Infusion of LDL-DHA Nanoparticles for Liver Cancer

Dietary intake of the natural omega-3 fatty acid docosahexaenoic acid (DHA) has been shown to protecting patient with viral hepatitis B or C from developing hepatocellular carcinoma (HCC). A low-density lipoprotein-based nanoparticle that acts as a transporter for unesterified DHA (LDL-DHA) is a selectively cytotoxic for HCC cells. In one experimental study, a single hepatic artery injection of nanoparticles loaded with LDL-DHA in rats with orthotopic hepatomas led to three-fold reduction of size of the tumors with necrosis without any histologic or biochemical evidence of injury to liver tissue surrounding the tumors (Wen et al. 2016). LDL-DHA selectively deregulated redox reactions in tumor tissues by increasing levels of reactive oxygen species as well as lipid peroxidation, depleting and oxidizing glutathione and nicotinamide adenine dinucleotide phosphate, and significantly down-regulating the antioxidant enzyme glutathione peroxidase-4. The redox balance in the surrounding liver was not disrupted.

Hyaluronic Acid Nanocarriers for Targeted Anticancer Therapeutics

Hyaluronic acid (HA), a natural polysaccharide, has been used the development of anticancer therapies due to its ability to target cancer cells. It is biocompatibile, nontoxic and biodegradable. HA can be conjugated with nanoparticles such as micelles, nanocapsules, liposomes, and polyplexes as nanocarriers for cytostatic drugs, proteins, polynucleotides, immunomodulators and imaging agents used in the management of cancer. HA nanocarriers can be used for passive as well as active targeting because of the binding capacity of HA to specific cancer cell surface receptors, such as CD44, which is involved in tumor progression as well as in the metastatic process. (Cadete and Alonso 2016). Ability to combine different nanoparticles for remote-controlled drug delivery to tumors and combination of diagnostic imaging with therapeutics provides an opportunity for targeted personalized therapy for cancer.

Different types of HA-modified lipid nanoparticles, mostly liposomes, have been investigated for delivering active compounds to CD44-overexpressing cells. Surface

modification by HA improves in vivo stability of liposomes and improve pharmacokinetics to increase their blood circulation time (Nascimento et al. 2016).

Magnetic Nanoparticles for Remote-Controlled Drug Delivery to Tumors

Remotely controlled nanoparticles, when pulsed with an electromagnetic field, can release anticancer drugs into tumors. This technology could lead to the improved diagnosis and targeted treatment of cancer. In an earlier work, injectable multifunctional nanoparticles were designed to flow through the bloodstream, home to tumors and clump together. Clumped particles help visualization of tumors by MRI. The system that makes it possible consists of particles that are superparamagnetic, a property that causes them to give off heat when they are exposed to a magnetic field. Tethered to these particles are active molecules, such as anticancer drugs. Exposing the particles to a low-frequency electromagnetic field causes the particles to radiate heat, which melts the tethers and releases the drugs. The waves in this magnetic field have frequencies between 350 and 400 kilohertz -the same range as radio waves. These waves pass harmlessly through the body and heat only the nanoparticles. The tethers in the system consist of strands of DNA. Two strands of DNA link together through hydrogen bonds that break when heated. In the presence of the magnetic field, heat generated by the nanoparticles breaks these, leaving one strand attached to the particle and allowing the other to float away with its cargo. One advantage of a DNA tether is that its melting point is tunable. Longer strands and differently coded strands require different amounts of heat to break. This heatsensitive tuneability makes it possible for a single particle to simultaneously carry many different types of cargo, each of which can be released at different times or in various combinations by applying different frequencies or durations of electromagnetic pulses. To test the particles, the researchers implanted mice with a tumor-like gel saturated with nanoparticles. They placed the implanted mouse into the well of a cup-shaped electrical coil and activated the magnetic pulse. The results confirm that without the pulse, the tethers remain unbroken. With the pulse, the tethers break and release the drugs into the surrounding tissue. The experiment is a proof of principal demonstrating a safe and effective means of tunable remote activation. However, work remains to be done before such therapies become viable in the clinic.

Coated magnetic nanoparticles are very useful for delivering chemotherapeutic drugs. Magnetic carriers have been synthesized by co-precipitation of iron oxide followed by coating with polyvinyl pyrrolidone (PVP) and characterization was performed using X-ray diffraction, TEM, TGA, FTIR and UV-vis spectroscopy (Arsula Rose et al. 2013). Magnetite (Fe3O4) remained as the core of the carrier. The amount of PVP bound to the iron oxide nanoparticles was estimated by thermo-gravimetric analysis and the attachment of PVP to the iron oxide nanoparticles was confirmed by FTIR analysis. The loading efficiency of epirubicin hydrochloride onto the PVP coated and uncoated iron oxide nanoparticles was measured at intervals by UV-Vis Spectroscopy. The binding of epirubicin hydrochloride to the PVP coated and uncoated iron oxide nanoparticles were confirmed by FTIR analysis.

The drug displayed increased cell cytotoxicity at lower concentrations when conjugated with the nanoparticles than being administered conventionally as individual drugs indicating potential of epirubicin loaded PVP-coated iron oxide nanoparticles for magnetically targeted drug delivery.

Mesoporous Silica Nanoparticles

Mesoporous silica nanoparticles (MSNs) have a considerable potential for drug delivery applications due to their flexibility and high drug load potential. MSNs are biodegradable and mostly eliminated through renal clearance. Although numerous reports demonstrate sophisticated drug delivery mechanisms in vitro, the therapeutic benefit of these systems for in vivo applications has been uncertain in the past. Recent preclinical data has demonstrated that MSNs are safe and a biocompatible technology platform for targeted drug delivery, passive as well as folate-directed, in cancer. MSNs medical applicability in vivo has been demonstrated for both drug delivery and diagnostics. Therapeautic efficacy of MSNs has been shown in vivo following oral, local, subcutaneous or intravenous administration and MSNs have been approved for clinical trials. Incorporation of multiple therapeutic and diagnostic agents into MSNs is feasible and this will enable diagnostic-guided therapy. There are still several issues to be considered before MSNs can be used in clinical practice (Rosenholm et al. 2012).

Monitoring of Targeted Delivery by Nanoparticle-Peptide Conjugates

Tryptophan-phenylalanine dipeptide nanoparticles (DNPs) can shift the peptide's intrinsic fluorescent signal from the ultraviolet to the visible range. DNPs are photostable, biocompatible and have a narrow emission bandwidth and visible fluorescence properties. DNPs functionalized with the MUC1 aptamer and doxorubicin can target cancer cells and can be used to image and monitor drug release in real time (Fan et al. 2016). In the body or tissue of an animal or person, it would be possible to watch the fluorescent signal with an optical detection system. This method has applications in targeted drug delivery for personalized management of cancer. Initial studies were done with doxorubicin but it can be applied to other anticancer agents.

Nanobees for Targeted Delivery of Cytolytic Peptide Melittin

The in vivo application of cytolytic peptides for cancer therapeutics is hampered by toxicity, nonspecificity, and degradation. A specific strategy was developed to synthesize a nanoscale delivery vehicle for cytolytic peptides by incorporating the synthetic version of a toxin called melittin that is found in bees into the outer lipid monolayer of a perfluorocarbon (PFC) nanoparticle. The composite structures, called nanobees, are engineered to travel directly to tumor cells without harming any others.

They spare the healthy cells but attach to tumor blood vessels, which express a specific protein to which a substance on the nanobees has a chemical affinity. Melittin, which would destroy red blood cells and other normal tissues if it is delivered intravenously, is completely safe when carried on a nanoparticle. Favorable pharmacokinetics of this nanocarrier have been demonstrated, which allow accumulation of melittin in murine tumors in vivo and a dramatic reduction in tumor growth without any apparent signs of toxicity (Soman et al. 2009). Furthermore, direct assays demonstrated that molecularly targeted nanocarriers selectively delivered melittin to multiple tumor targets, including endothelial and cancer cells, through a hemifusion mechanism. In cells, this hemifusion and transfer process did not disrupt the surface membrane but did trigger apoptosis and in animals caused regression of precancerous dysplastic lesions. Collectively, these data suggest that the ability to restrain the wide-spectrum lytic potential of a potent cytolytic peptide in a nanovehicle, combined with the flexibility of passive or active molecular targeting, represents an innovative molecular design for chemotherapy with broad-spectrum cytolytic peptides for the treatment of cancer at multiple stages. So far nanobees have been tested only on mice, with promising results, but what works in mice does not always work in humans. If proven to be effective in humans, this therapy could become widely available in about 5-10 years.

Nanobody-Shell Polymeric Micelles for Targeted Drug Delivery

PEG-b-poly[N-(2-hydroxypropyl) methacrylamide-lactate] crosslinked thermosensitive biodegradable polymeric micelles suitable for active tumor targeting, have been developed by coupling the anti-EGFR EGa1 nanobody to their surface (Talelli et al. 2011). The micellar conjugates were characterized using SDS-PAGE and gel permeation chromatography. The conjugation was successful as demonstrated by western blot and dot blot analysis. Rhodamine labeled EGa1-micelles showed substantially higher binding as well as uptake by EGFR over-expressing cancer cells than untargeted rhodamine labeled micelles. No binding was observed of the nanobody micelles to EGFR negative cells as well as to 14C cells in the presence of an excess of free nanobody. This demonstrates that the binding of the nanobody micelles is by interaction with the EGF receptor. These polymeric micelles are highly promising systems for active drug targeting.

Nanoformulations of Monoclonal Antibodies for Targeted Drug Delivery

MAbs are used as the homing ligands used in the design of anticancer formulations targeted to receptors on tumor cells and improve intracellular uptake. MAbs act through induction of antibody-dependent cellular cytotoxicity and complement dependent cytotoxicity. Rituximab, an IgG1 antibody, binds to the CD20 receptor, which is present on the cells of most B cell neoplasms (Fan et al. 2014). There is a significant improvement in the cellular uptake and cytotoxic effect of PLA-conjugated

rituximab as compared to non-targeted counterparts (Popov et al. 2011). Limitations of development of MAb-based nanotherapeutics include, large size, immunogenic properties, sensitivity to environmental factors, and high cost of synthesis. Much has been learned since the commercialization of the first-generation nanomedicines including DOXIL® and Abraxane® to improve our understanding of targeted as well as non-targeted nanoparticles that are under various stages of development as anticancer therapeutics.

Immobilization of antibodies onto a surface of gold-coated nanoparticles significantly decreases the ability of cetuximab to initiate a cytotoxic response in EGFRexpressing tumor xenografts (Ahmed et al. 2015). In contrast, cetuximab and its fragment were employed in synthesis of oxaliplatin-loaded EGFR-targeted liposomes tested for treatment of EGFR-positive colon cancer. Co-treatment with receptor-targeted antibodies and liposomes as drug delivery nanoformulations results in increased cytotoxic activity against cancer cells (Zalba et al. 2015). Enhanced permeability and retention effect (EPR) may occur in the tumor, whether using active targeting of nanoparticles, binding of drugs to their tumoral targets or the presence of tumor associated macrophages. Antibody fragments enable high antigen binding specificity with smaller size of synthetized nanoformulations and less immunogenicity (Bertrand et al. 2014). Dimercaptosuccinic acid-modified iron oxide magnetic nanoparticles (MNPs) co-loaded with anti-CD22 antibodies and doxorubicin (anti-CD22-MNPs-DOX) may be used as drug nanocarriers in the treatment of non-Hodgkin's lymphoma due to increased uptake of DOX and induction of apoptosis (Sun et al. 2015).

In the nab-paclitaxel formulation of paclitaxel, Abraxane, hydrophobic paclitaxel is suspended in 130-nm albumin nanoparticles and thus made water-soluble. Abraxane nanoparticle has been noncovalently coated with recombinant MAbs (anti-VEGF, bevacizumab) to guide Abraxane delivery into tumors. The chemotherapy agent retains its cytotoxic effect, while the antibody maintains the ability to bind its ligand when the two are present in a single nanoparticle (AB160), and the nanoformulation yields improved antitumor efficacy in a preclinical human melanoma xenograft model (Nevala et al. 2016). Further data suggest that numerous therapeutic monoclonal IgG1 antibodies may be utilized in this platform, which has implications for many solid and hematologic malignancies. A phase II clinical trial is testing the efficacy of pertuzumab, trastuzumab, and paclitaxel albumin-stabilized nanoparticle formulation in treating patients with HER2-positive advanced breast cancer (ClinicalTrials.gov Identifier: NCT01730833).

Nanogel-Based Stealth Cancer Vaccine Targeting Macrophages

A subset of macrophages only found deep inside lymph nodes play a major role in slowing cancer, but existing therapeutic cancer vaccines provide only a limited clinical benefit as the vaccine nanoparticles are gobbled up by the macrophages and dendritic cells circulating in the body. To overcome this problem, a nanoparticulate cancer vaccine was developed by encapsulating a synthetic long peptide antigen within an immunologically inert nanoparticulate hydrogel (nanogel) of cholesteryl pullulan (Muraoka et al. 2014). After subcutaneous injection to mice, the nanogelbased vaccine was efficiently transported to the draining lymph node, and was preferentially engulfed by medullary macrophages but was not sensed by other macrophages and dendritic cells because of "immunologically stealth mode". These macrophages effectively cross-primed the vaccine-specific CD8+ T cells in the presence of a Toll-like receptor (TLR) agonist as an adjuvant. The nanogel-based vaccine inhibited in vivo tumor growth more than another vaccine formulation using a conventional adjuvant delivery system. Lymph node macrophages were highly responsive to TLR stimulation, which may underlie the potency of the macrophage-oriented, nanogel-based vaccine. These results indicate that targeting medullary macrophages using the immunologically stealth nanoparticulate delivery system is an effective vaccine strategy.

Nanovehicles for Targeted Delivery of Paclitaxel

Nanoparticles have been used to deliver paclitaxel, an antitumor drug, directly to tumors for targeted anticancer treatment. The nanoparticles were loaded with paclitaxel and then mixed with lipids to form nanoparticle-like clusters, which were then coated with a glycosaminoglycan (GAG). The nanovehicle was formed of clusters of loaded nanoparticles then coated with a GAG. When these clusters come into contact with cancerous cells the paclitaxel is released from the individual nanoparticles directly into the cancerous cell. This targeted release allows the treatment to be focused to the cancerous cells, reducing the negative effects of the chemotherapy treatment.

The ability of the nanovehicles to specifically target the cancerous cells is due to the specific GAG used in the coating of the clusters. The researchers use hyaluronan, a sugar that is recognized by receptors on many different types of cancer cell. When the nanovehicle interacts with the cancer cell the sugar is recognized by the receptors, triggering a structural change and the subsequent release of the paclitaxel directly into the cell. The release of the paclitaxel directly into the target cell also overcomes the issues associated with the solubility of the drug (Rivkin et al. 2010). The vehicle is similar to a cluster bomb, when the delivery vehicle, comprising of multiple nanoparticles, comes into contact with cancer cells it releases the chemotherapeutic payload directly into the cell. Peer also mentions that the device can be used to treat a variety of cancers, such as blood, colon, breast, pancreatic, ovarian and several types of brain cancer. The ability of the nanovehicle to be recognized by the cancer cells means that it increases the effectiveness of the treatment while healthy cells are unaffected by the treatment. Tests on tumor-bearing mice have demonstrated that the nanoclusters are more effective when compared with free paclitaxel and other albumin nanoparticles containing paclitaxel. The nanoclusters also demonstrated a high safety profile and a high level of accumulation within tumors.

The fabrication of the nanovehicles means that the treatment may potentially be safer than alternative current therapies. The nanocluster is formed of the naturally occurring lipid hyaluronan, a lipid that decomposes in the body once the nanoparticles have delivered the paclitaxel. The researchers hope that GAGs may provide vehicles for other chemotherapy drugs, such as taxanes, and may also be used as carriers for other therapeutic applications.

Nanocell for Targeted Drug Delivery to Tumor

Simultaneous delivery of chemotherapeutic and antiangiogenic drugs is clearly beneficial, but because chemotherapy is blood-borne, shutting down the tumor's blood supply with antiangiogenic drugs may decrease the delivery of drugs designed to kill the tumor cells. A more effective strategy would be to use a delivery vehicle that became concentrated in tumors before the vasculature shuts down, and allows the staged release of the two drugs. The delivery of the antiangiogenic factor could lead to a collapse of the vascular network and imprison the vehicle, which would still be carrying its second payload of chemotherapeutic drug, inside the tumor. The subsequent release of the latter drug within the tumor would kill the cancer cells. For example, a composite nanocell can be constructed with a solid biodegradable polymer core surrounded by a lipid membrane in which the outer membrane is loaded with the antiangiogenic drug combretastatin and the inner membrane with the chemotherapy drug doxorubicin. The nanocells are small enough to pass through tumor blood vessels, but they are too large to pass through the pores of normal vessels. Once inside the tumor, the nanocell's outer membrane can disintegrate, releasing the antiangiogenic drug and causing the collapse of the blood vessels feeding the tumor. The collapsed blood vessels trap the nanocell inside the tumor. The nanocell can then slowly release the chemotherapy drug. Although the effect of the sequential delivery of these two drugs on tumor growth is dramatic, these results can not be quickly translated into therapy for humans. There is a concern that antiangiogenic drugs may promote the spread of tumors to other tissues. Also, in contrast to combretastatin, many antiangiogenic drugs require prolonged tissue exposure to shut down the vasculature, and so may not be amenable to this approach with a short exposure time.

Nanodiamonds for Local Delivery of Chemotherapy at Site of Cancer

Nanodiamonds (NDs) with diameter of 2–8 nm, physically bind with doxorubicin and sandwich between a base and thin layer of polymer parylene, to enable extended targeted and controlled release at diseased areas in cancer, viral infection, and inflammation. A substantial amount of drug can be loaded onto clusters of nanodiamonds, which have a high surface area. Nanodiamonds have many other advantages for drug delivery. They can be functionalized with nearly any type of therapeutic. They can be suspended easily in water, which is important for biomedical applications. They are very scalable and can be produced in large quantities. In control experiments, where the drug was administered without the nanodiamonds, virtually the whole drug was released within 1 day. By adding the drug-laden nanodiamonds to the device, drug release was instantly lengthened to the months-long timescale. The FDA-approved polymer parylene displayed the stable and continuous slow-release of drug for at least 1 month due to the powerful sequestration abilities of the DOX-ND complex. The device also avoids the massive initial release of the drug, which is a disadvantage of conventional therapy.

The nanodiamonds are quite economical and have already been mass-produced as lubrication components for automobiles and for use in electronics. Because the fabrication process is devoid of any destructive steps, the DOX-ND conjugates are unaffected and unaltered. The flexible microfilm device resembles a piece of plastic wrap and can be customized easily into different shapes. It can transform conventional treatment strategies and reduce patients' unnecessary exposure to toxic drugs. The biocompatible and minimally invasive device could be used to deliver chemotherapy drugs locally to sites where malignant tumors have been surgically removed.

Nanoimmunoliposome-Based System for Targeted Delivery of siRNA

Low transfection efficiency, poor tissue penetration, and nonspecific immune stimulation by in vivo administered siRNAs have delayed their therapeutic applications. Their potential as anticancer therapeutics hinges on the availability of a vehicle that can be systemically administered, safely and repeatedly, and will deliver the siRNA specifically and efficiently to both primary tumors and metastases. A nanosized immunoliposome-based delivery complex (scL) has been developed that, will preferentially target and deliver molecules including plasmid DNA and antisense oligonucleotides, to tumor cells following systemic administration (Pirollo et al. 2007). This tumor-targeting nanoparticle delivery vehicle can also deliver siRNA to both primary and metastatic disease. The efficiency of this complex has been enhanced by the inclusion of a pH-sensitive histidine-lysine peptide in the complex (scL-HoKC) and by delivery of a modified hybrid (DNA-RNA) anti-HER-2 siRNA molecule. Scanning probe microscopy confirms that this modified complex maintains its nanoscale size. More importantly, this nanoimmunoliposome anti-HER-2 siRNA complex can sensitize human tumor cells to chemotherapeutics, silence the target gene, affect its downstream pathway components in vivo, and significantly inhibit tumor growth in a pancreatic cancer model. This complex has the potential to help translate the potent effects of siRNA into a clinically viable anticancer therapeutic.

Nanoparticle-Mediated Targeting of MAPK Signaling Pathway

The MAPK signal transduction cascade is dysregulated in a majority of human tumors and nanoparticle-mediated targeting of this pathway can optimize cancer chemotherapy. Nanoparticles engineered from a polymer that is chemically conjugated to a selective MAPK inhibitor, PD98059, are taken up by cancer cells through endocytosis and demonstrate sustained release of the active agent, resulting in the

inhibition of phosphorylation of downstream extracellular signal regulated kinase (Basu et al. 2009). Modification of the polymer, which is biocompatible as well as biodegradable and approved by the FDA, leads to a 20-fold increase in drug loading capacity. Nanoparticle-mediated targeting of MAPK has been shown to inhibit the proliferation of melanoma and lung carcinoma cells and induce apoptosis in vitro. Administration of the PD98059-nanoparticles in melanoma-bearing mice inhibits tumor growth and enhances the antitumor efficacy of cisplatin chemotherapy. This study shows the nanoparticle-mediated delivery of signal transduction inhibitors is a potentially effective method of cancer chemotherapy

Nanoparticles for Targeted Antisense Therapy of Cancer

Antisense oligonucleotides (ASO) against specific molecular targets (e.g. Bcl-2 and Raf-1) are important reagents in cancer biology and therapy. Phosphorothioate modification of the ASO backbone has resulted in an increased stability of ASO in vivo without compromising, in general, their target selectivity. Although the power of antisense technology remains unsurpassed, dose-limiting side effects of modified ASO and inadequate penetration into the tumor tissue have necessitated further improvements in ASO chemistry and delivery systems. Oligonucleotide delivery systems may increase stability of the unmodified or minimally modified ASO in plasma, enhance uptake of ASO by tumor tissue, and offer an improved therapy response. An overview of ASO design and in vivo delivery systems with focus on preclinical validation of a liposomal nanoparticle containing minimally modified raf antisense oligodeoxynucleotide (LErafAON) has been published (Zhang et al. 2009). Intact rafAON (15-mer) is present in plasma and in normal and tumor tissues of athymic mice systemically treated with LErafAON. Raf-1 expression is decreased in normal and tumor tissues of LErafAON-treated mice. Therapeutic benefit of a combination of LErafAON and radiation or an anticancer drug exceeds radiation or drug alone against human prostate, breast, and pancreatic tumors grown in athymic mice. Further improvements in ASO chemistry and nanoparticles are promising avenues in antisense therapy of cancer.

Nanoparticles for Delivery of Suicide DNA to Prostate tumors

A prostate-specific, locally delivered gene therapy has been developed for the targeted killing of prostate cells using C32/DT-A, a degradable polymer a nanoparticulate system, to deliver a diphtheria toxin suicide gene (DT-A) driven by a prostate specific promoter to cells (Peng et al. 2007). These nanoparticles were directly injected to the normal prostate and to prostate tumors in mice. Nearly 50% of normal prostates showed a significant reduction in size, attributable to cellular apoptosis, whereas injection with naked DT-A-encoding DNA had little effect. A single injection of C32/DT-A nanoparticles triggered apoptosis in 80% of tumor cells present in the tissue. It is expected that multiple nanoparticle injections would trigger a greater percentage of prostate tumor cells to undergo apoptosis. These results suggest that local delivery of polymer/DT-A nanoparticles may have application in the treatment of benign prostatic hypertrophy and prostate cancer.

Nanoparticles for Targeted Delivery of Concurrent Chemoradiation

The development of chemoradiation – the concurrent administration of chemotherapy and radiotherapy – has led to significant improvements in local tumor control and survival. However, it is limited by its high toxicity. A novel NP therapeutic, ChemoRad NP, has been developed, which can deliver biologically targeted chemoradiation (Wang et al. 2010). This is a biodegradable and biocompatible lipid-polymer hybrid NP that is capable of delivering both chemotherapy and radiotherapy. Using docetaxel, indium¹¹¹ and yttrium⁹⁰ as model drugs, ChemoRad NP was shown to encapsulate chemotherapeutics (up to 9% of NP weight) and radiotherapeutics (100 mCi of radioisotope per gram of NP) efficiently and deliver both effectively. Targeted delivery of ChemoRad NPs and high therapeutic efficacy of ChemoRad NPs was demonstrated using prostate cancer as a disease model. ChemoRad NP represents a new class of therapeutics that holds great potential to improve cancer treatment.

Nanoparticle-Based Therapy Targeted to Cancer Metastases

Early detection of metastases plays an important role in the management of metastatic cancer. In patients with prostate cancer who undergo surgical lymph-node resection or biopsy, MRI with lymphotropic superparamagnetic nanoparticles can correctly identify all patients with nodal metastases. This diagnosis is not possible with conventional MRI alone and has implications for the management of men with metastatic prostate cancer, in whom adjuvant androgen-deprivation therapy with radiation is the mainstay of management.

Nanoparticle formulations of anticancer drugs may be more effective against cancer metastases. Nanoparticles can transport complex molecular cargoes to the major sites of metastasis, such as the lungs, liver and lymph nodes, as well as targeting to specific cell populations within these organs (Schroeder et al. 2012). Oral administration of alpha-TEA formulated in liposome or biodegradable poly(D, L-lactide-coglycolide) nanoparticle has been shown to significantly reduce tumor burden in a mammary cancer mouse model. Both formulations reduce lymph node and lung micrometastatic tumor foci, but nanoparticle formulation is more effective in reducing metastases. Tumor targeting with nanoparticles facilitates systemic delivery of immunomodulatory cytokine genes to remote sites of cancer metastasis. Targeted delivery and localized expression of the intravenously administered nanoparticles bearing the gene encoding granulocyte/macrophage colony-stimulating factor was confirmed in a patient with metastatic cancer, as was the recruitment of significant tumor-infiltrating lymphocytes (Gordon et al. 2008).

Nanoparticle-Mediated Delivery of Multiple Anticancer Agents

Concomitant delivery of the multiple anticancer agents by nanocarriers is expected to enhance the synergistic effects for the following reasons (Mi et al. 2012):

- Nanocarriers can encapsulate large quantities of the therapeutic agents.
- Cellular uptake of the nanocarriers is efficient due to internalization by endocytosis.
- Nanocarriers 100–200 nm in diameter with a surface coating such as PEG or vitamin E TPGS can escape elimination by macrophages and enable sustained delivery.
- Nanocarriers may provide high oral bioavailability of the formulated agents.

Nanostructured Hyaluronic Acid for Targeted Drug Delivery in Cancer

Active targeting of bioactive molecules by nanoparticulate delivery systems that include hyaluronic acid (HA) in their structures is an attractive approach to drug delivery because HA is biocompatible, nontoxic and noninflammatory. To make HA useful as an intravenous targeting carrier, strategies s1hould be devised to reduce its clearance from the blood; suppress its uptake by liver and spleen; and provide tumor-triggered mechanisms of release of an active drug from the HA carrier (Ossipov 2010).

HA nanoparticles (HA-NPs), which are formed by the self-assembly of hydrophobically modified HA derivatives, have been tested for their physicochemical characteristics and fates in tumor-bearing mice after systemic administration (Choi et al. 2010b). Irrespective of the particle size, significant amounts of HA-NPs circulated for 2 days in the bloodstream and selectively accumulated into the tumor. The smaller HA-NPs could reach the tumor more effectively than larger HA-NPs. The concentration of HA-NPs in the tumor site was dramatically reduced when mice were pretreated with an excess of free HA. These results indicate that HA-NPs can accumulate into the tumor site by a combination of passive and active targeting mechanisms.

Perfluorocarbon Emulsion for Targeted Chemotherapeutic Delivery

Kereos Inc's emulsion particles consist of a perfluorocarbon core surrounded by a lipid monolayer, which stabilizes the particle in addition to providing a virtually unlimited number of anchoring sites for targeting ligands and payload molecules. The result is an oil-in-water emulsion of particles with an average size of approximately 250 nm, referred to as "targeted nanoparticles." Delivered by injection, this approach offers the following advantages:

- High molecular specificity of MAbs, small-molecule ligands and other targeting ligands for disease biomarkers translates directly into high specificity of the emulsion particles for disease sites.
- Although only 10–100 targeting ligand molecules are needed to direct and securely bind an individual emulsion particle to the disease site, each particle can

carry 100,000 or more payload molecules. This "signal amplification" opens up opportunities not otherwise possible.

• Both in terms of size and composition, the emulsion particles are designed to be both safe and effective, and to avoid potential problems with distribution, metabolism or excretion

Polymer Nanoparticles for Targeted Drug Delivery in Cancer

Cerulean Nanopharmaceuticals' CRLX101 (formerly IT-101), a cyclodextrin polymer-based nanoparticle containing camptothecin, is in phase IIa clinical development for the treatment of cancer. PET data from ⁶⁴Cu-labeled CRLX101 to quantify the in vivo biodistribution in mice bearing tumors shows that ~8% of the injected dose is rapidly cleared as a low-molecular-weight fraction through the kidneys and the remaining material circulates in plasma with a terminal half-life of 13.3 h (Schluep et al. 2009). A 3-compartment model is used to determine vascular permeability and nanoparticle retention in tumors, and accurately represents the experimental data. The calculated tumor vascular permeability indicates that most of nanoparticles stay intact in circulation and do not disassemble into individual polymer strands. A key assumption to modeling the tumor dynamics is that there is a sink for the nanoparticles within the tumor. Histological measurements using confocal microscopy show that CRLX101 localizes within tumor cells and provides the sink in the tumor for the nanoparticles.

Several mechanisms have been proposed to explain nanoparticle retention in tumors:

- 1. Dextran-coated iron oxide nanoparticles accumulate in the interstitial fluid and are taken up by tumor vascular endothelial cells, which observed mostly in areas of neovascularization whereas intracellular concentrations are highest in tumor cells.
- Long circulating liposomes accumulate predominantly in tumor stroma, either in the extracellular space or in tumor-associated macrophages in a breast cancer tumor model. A Her2-targeted version of the same liposomes achieves the same over all tumor concentration but more internalization by cancer cells through endocytosis is observed.
- 3. Cyclodextrin-based polymers (CDP) conjugates have been shown to be avidly taken up by cancer cells. This result may be a function of the unique surface characteristics of CDP nanoparticles, which contain hydrophobic pockets within the cyclodextrin molecules that have been shown to interact with lipid rafts of cell membranes.

Scientists at the MIT-Harvard Center for Cancer Nanotechnology Excellence (Cambridge, MA) have studied the effects of altering nanoparticle polymer composition, drug loading, and solvents on the ability of the resulting nanoparticles to target and deliver drugs to tumors. As a targeting agent for all the polymer nanoparticles studied, they used a molecule that recognizes the prostate-specific membrane antigen. The aim of this study was to develop formulation parameters that would control the size of the resulting polymer nanoparticles, which the investigators believe play a major role in optimizing tumor targeting. Nanoparticles were prepared from a biocompatible material. Experimenting with a variety of polymer concentrations and solvent mixtures, they found that they could systematically control the size of the resulting polymers. The results were so consistent that the investigators believe that they may have developed a broadly applicable approach to reproducibly tuning the size of polymer nanoparticles during their formulation. In a final experiment, the researchers added the targeting agent to their optimized nanoparticles. The targeted nanoparticles can significantly increase drug delivery to human prostate tumors growing in mice.

Accurins are polymeric nanoparticles that incorporate a therapeutic payload and are designed to have prolonged circulation within the bloodstream, enable targeting of the diseased tissue or cells, and provide for the controlled and timely release of the therapeutic payload. Accurins are designed with specific pharmaceutical properties intended to target tumors at three levels: tissue, cellular and molecular. Tissue targeting is achieved by engineering the physical and chemical properties – size, shape and surface properties – of the Accurin to allow it to escape through gaps in the blood vessels surrounding tumors and other disease sites. Cellular targeting is achieved using proprietary targeting ligands on the surface of the Accurin that binds to specific cell surfaces or tissue markers. The specific characteristics of the therapeutic payload may enable molecular targeting within the diseased cells.

Polylactide nanoparticles (NPs) loaded with doxorubicin (DOX) and coated with bone-seeking pamidronate (Pam) have been developmed for the targeted treatment of malignant osteolysis associated with inoperable primary bone tumors and multifocal skeletal metastases, which is a challenge in management of these patients (Yin et al. 2016). In vivo biodistribution of radiolabeled targeted Pam-NPs demonstrated enhanced bone tumor accumulation and prolonged retention compared with nontargeted NPs. In a murine model of focal malignant osteolysis, Pam-functionalized, DOX-loaded NPs (Pam-DOX-NPs) significantly attenuated localized osteosarcoma (OS) progression compared with nontargeted DOX-NPs. Evaluation of repeat dosing with Pam-DOX-NPs in dogs with OS, which possess tumors of anatomic size and physiology comparable to those in humans, showed that the treatment was well tolerated with no hematologic or cardiac toxicity. Biodistribution of Pam-DOX-NPs demonstrated by nuclear scintigraphy showed malignant bone-targeting capability with measurable anticancer activity as confirmed with percent tumor necrosis on histopathology assessment.

Polymersomes for Targeted Cancer Drug Delivery

Polymersomes, hollow shell nanoparticles, have unique properties of that allow them to deliver two distinct drugs, paclitaxel and doxorubicin directly to tumors implanted in mice. Loading, delivery, and cytosolic uptake of drug mixtures from degradable polymersomes are shown to exploit both the thick membrane of these block copolymer vesicles and their aqueous lumen as well as pH-triggered release within endolysosomes. Drug-delivering polymersomes break down in the acidic environment of the cancer cells resulting in targeted release of these drugs within tumor cells. While cell membranes and liposomes (vesicles often used for drugdelivery) are created from a double layer of fatty molecules called phospholipids, a polymersome is comprised of two layers of synthetic polymers. The individual polymers are degradable and considerably larger than individual phospholipids but have many of the same chemical features. The large polymers making up the shell allow paclitaxel, which is water-insoluble, to embed within the shell. Doxorubicin, which is water-soluble, stays within the interior of the polymersome until it degrades. The polymersome and drug combination is self-assembling the structure spontaneously forms when all components are suitably mixed together. Recent studies have shown that cocktails of paclitaxel and doxorubicin lead to better tumor regression than either drug alone, but previously there was no carrier system that could carry both drugs as efficiently to a tumor. Polymersomes get around those limitations.

Another approach is by assembling diverse bioactive agents, such as DNA, proteins, and drug molecules into core-shell multifunctional polymeric nanoparticles (PNPs) that can be internalized in human breast cancer cells (Bertin et al. 2006). Using ring-opening metathesis polymerization, block copolymers containing smallmolecule drug segments (>50% w/w) and tosylated hexaethylene glycol segments were prepared and assembled into PNPs that allowed for the surface conjugation of single-stranded DNA sequences and/or tumor-targeting antibodies. The resulting antibody-functionalized particles were readily uptaken by breast cancer cells that overexpressed the corresponding antigens.

Quantum Dots and Quantum Rods for Targeted Drug Delivery in Cancer

A single-particle QD conjugated with a tumor-targeting MAb (anti-HER2) has been tracked in tumors of live mice (Tada et al. 2007). The researchers used a dorsal skinfold chamber and a high-speed confocal microscope with a high-sensitivity camera to track the antibody-labeled QDs and made 30-frame-per-second movies of these nanoparticles (NPs) as they traveled through the bloodstream. The HER2 MAb binds to a protein found on the surface of certain breast and other tumors. This was injected, conjugated to the QDs, into mice with HER2-overexpressing breast cancer to analyze the molecular processes of its mechanistic delivery to the tumor. The investigators identified six distinct 'stop-and-go' steps in the process involved in the antibody-labeled QDs traveling from the injection site to the cell where they bind HER2: within a blood vessel in the circulation, during extravasation, in the extracellular region, binding HER2 on the cell membrane, moving into the perinuclear region and within the perinuclear region. The image analysis of the delivery processes of single particles in vivo thus provides valuable information on antibody-conjugated therapeutic nanoparticles, which will be useful in increasing therapeutic efficacy.

Water-soluble CdSe/CdS/ZnS quantum rods (QRs) have been developed as targeted probes for imaging cancer cell lines using two-photon fluorescence imaging. The researchers first developed a new method of creating QRs that would remain well dispersed in water and then refined the technique to allow the attachment of targeting molecules (in this case, transferrin, which binds to a receptor that is over-expressed in many types of cancer cells) to the QR surface. QRs, similar to the spherical QDs, fluoresce and can be made to fluoresce in a range of colors. However, since QRs have larger dimensions than QDs, they are easier to excite with incoming light than QDs. This research showed that the QRs were only taken up by targeted transferrin-positive cells and accumulated within these cells, being easily visible using low-intensity near-infrared light, which helps to protect cell integrity. If future research can further our understanding of QDs and QRs following these studies, it is hoped that we could then improve the ability of NPs to deliver drugs specifically to tumors, thus resulting in improved cancer diagnostics and therapeutics.

Remote Controlled Drug Delivery from Magnetic Nanocrystals

Combination of magnetic nanocrystals with ability to exhibit hyperthermic effects when placed in an oscillating magnetic field and mesoporous silica nanoparticles that can contain and release drug cargos could provide a unique drug delivery system for cancer. A nanosystem that incorporates zinc-doped iron oxide nanocrystals within a mesoporous silica framework that has been surface-modified with pseudorotaxanes (Thomas et al. 2010). Upon application of an AC magnetic field, the nanocrystals generate local internal heating, causing the molecular machines to disassemble and allowing the drug cargos to be released. Breast cancer cell (MDA-MB-231) death was achieved in vitro when doxorubicin-loaded particles were exposed to an AC field. This material has potential as a noninvasive, externally controlled drug delivery system with cancer-killing properties.

Targeted Delivery of Nanoparticulate Drugs into Lymphatic System

The lymphatic system plays a major role in the defense cancer and is one of the main pathways for the metastasis of tumors. The regional lymph nodes, when invaded by cancer cells, act as reservoirs from where these cells spread to other parts of the body. The lymphatic system is not easily accessible by conventional intravenous infusion of chemotherapeutics, thus limiting the amount of drug that reaches lymphatic tissues including lymph node metastases. The lymphatics, however, can be exploited as a route for drug delivery as these channels can transport certain lipophilic compounds and chemotherapeutics.

Nanoparticles can be effectively taken up into lymphatics as well as retained in lymph nodes for several days, and without using any specific targeting ligand, they are internalized exclusively by nodal resident dendritic cells (DCs) and other antigen presenting cells. Animal studies have demonstrated that nanoparticles made of natural or synthetic polymers and liposomal carriers have higher accumulation in the lymph nodes and surrounding lymphatics compared to conventional intravenous therapies (Xie et al. 2009). In vivo studies have shown that up to 40–50% of resident lymph node DCs internalize nanoparticles, further supporting the feasibility of this delivery strategy. Bio-availability and bio-distribution can be controlled easily by varying the size of nanoparticles. Biodegradable nanoparticles of 20–45 nm have shown the potential for immunotherapeutic applications that specifically target DCs in lymph nodes, e.g. targeted delivery of immunomodulating formulations and vaccines. This can diminish toxicity of highly toxic active drugs.

Targeted Drug Delivery with Nanoparticle-Aptamer Bioconjugates

Nucleic acid ligands (aptamers) are potentially well suited for the therapeutic targeting of drug encapsulated controlled release polymer particles in a cell- or tissuespecific manner. Scientists at the Massachusetts Institute of Technology (Cambridge, MA) have synthesized poly(lactic acid)-block-polyethylene glycol (PLA-PEG) copolymer with a terminal carboxylic acid functional group (PLA-PEG-COOH), and encapsulated rhodamine-labeled dextran (as a model drug) within PLA-PEG-COOH nanoparticles. These nanoparticles have the following desirable characteristics:

- Negative surface charge, which may minimize nonspecific interaction with the negatively charged nucleic acid aptamers
- Carboxylic acid groups on the particle surface for potential modification and covalent conjugation to amine-modified aptamers
- Presence of PEG on particle surface, which enhances circulating half-life while contributing to decreased uptake in nontargeted cells.

Nanoparticle-aptamer bioconjugates were generated with RNA aptamers that bind to the prostate-specific membrane antigen (PSMA), a well-known prostate cancer tumor marker that is overexpressed on prostate acinar epithelial cells. These bioconjugates could efficiently target and get taken up by the prostate epithelial cells, which express the PSMA protein. The uptake of these particles was not enhanced in cells that do not express the prostate-specific membrane antigen protein. This represents the first report of targeted drug delivery with nanoparticleaptamer bioconjugates.

Numerous investigators have used aptamers as replacements for antibodies in various therapeutic and diagnostic applications. A DNA-protein nanoengine can be programmed to release therapeutically useful molecules in response to a programmed molecular signal. A drug molecule, or even a therapeutic gene, can be linked to this piece of DNA, and the combination is called the "output." When the output piece of DNA is then mixed with the aptamer, the two bind to one another until the aptamer comes in contact with the input signal. The aptamer folds around the input signal, causing it to release its cargo, the output DNA-drug molecule combination.

Use of T Cells for Delivery of Gold Nanoparticles to Tumors

Gold nanoparticles (AuNPs) are injected intravenously and accumulate within the tumor via the enhanced permeability and retention (EPR) effect. Although reliance on the EPR effect for tumor targeting has proven adequate for vascularized tumors in small animal models, the efficiency and specificity of tumor delivery in vivo, particularly in tumors with poor blood supply, may not be adequate. Human T cells, loaded with 45 nm gold colloid nanoparticles, can be used as cellular delivery vehicles for AuNP transport into tumors, without affecting viability or function (e.g. migration and cytokine production). Using a human tumor xenograft mouse model, it was demonstrated that AuNP-loaded T cells retain their capacity to migrate to tumor sites in vivo (Kennedy et al. 2011). In addition, the efficiency of AuNP delivery to tumors in vivo is increased by more than four-fold compared to injection of free PEGylated AuNPs and the use of the T cell delivery system also dramatically alters the overall nanoparticle biodistribution. Thus, the use of T cell chaperones for AuNP delivery could enhance the efficacy of nanoparticle-based therapies and imaging applications by increasing AuNP tumor accumulation. This could also be used for thermal destruction of tumor by application of NIR laser.

Dendrimers for Anticancer Drug Delivery

Earlier studies of dendrimers in drug delivery systems focused on their use for encapsulating drug molecules. However, it was difficult to control the release of the drug. One solution to this problem involves the use of dendrimers with pH-sensitive hydrophobic acetal groups on the dendrimer periphery. Loss of acetal group at mildly acidic pH triggers the disruption of micelles and release of the drug. Another approach is to attach the drug to the periphery of the dendrimer so that the release of the drug can be controlled by incorporating a degradable linkage between the drug and the dendrimer. Dendrimers have been used to facilitate boron neutron capture therapy as well as photodynamic therapy of cancer.

Developments in polymer and dendrimer chemistry have provided a new class of molecules called 'dendronized polymers', i.e. linear polymers that bear dendrons at each repeat unit. Their behavior differs from that of linear polymers and provides drug delivery advantages because of their longer circulation time and numerous possibilities for peripheral attachments of drugs.

Another approach is to attach the drug to the periphery of the dendrimer so that the release of the drug can be controlled by incorporating a degradable linkage between the drug and the dendrimer. New developments in polymer and dendrimer chemistry have provided a new class of molecules called 'dendronized polymer', i.e. linear polymer that bear dendrons at each repeat unit. Their behavior differs from that of linear polymers and provides drug delivery advantages because of their longer circulation time and numerous possibilities peripheral attachments of drugs. Modified PAMAM dendritic polymers <5 nm in diameter have been used as drug carriers. They are conjugated to folic acid as a targeting agent and then coupled to methotrexate and injected intravenously into animals bearing tumor that overexpress the folate receptor. Folate molecules bind to receptors on tumor cell membranes and facilitate the transport of methotrexate to inside of the tumor cell.

Doxorubicin (DOX) has been conjugated to a biodegradable dendrimer with optimized blood circulation time through size and molecular architecture, drug loading through multiple attachment sites, solubility through PEGylation, and drug release through pH-sensitive hydrazone linkages. Dendrimer-DOX is >10 times less toxic than free DOX toward colon carcinoma cells in culture. Following intravenous administration to tumor-bearing mice, tumor uptake of dendrimer-DOX is nine-fold higher than intravenous free DOX and causes complete tumor regression. No cures are achieved in tumor-implanted mice treated with free DOX, drug-free dendrimer, or dendrimer-DOX in which the DOX is attached by means of a stable carbamate bond. The antitumor effect of dendrimer-DOX is like that of an equimolar dose of liposomal DOX (Doxil). The remarkable antitumor activity of dendrimer-DOX results from the ability of the dendrimer to favorably modulate the pharmacokinetics of attached DOX.

Application of Dendrimers in Boron Neutron Capture Therapy

Boron neutron capture therapy (BNCT) offers a potential method for localized destruction of tumor cells. The technology is based on the nuclear reaction between thermal neutrons and boron-10 (10B) to yield alpha particles and lithium-7 nuclei. The destructive effect of this reaction is limited to a range of about the diameter of a single cell. For BNCT to be effective in cancer therapy, there must be selective delivery of an adequate concentration of 10B to tumors. Various types of antibodies as well as epidermal growth factor have been utilized to investigate receptor-mediated boron delivery, however in vivo studies have demonstrated only a small percentage of the total administered dose accumulates in tumors while high concentrations end up in the liver.

In normal as well as cancer cells, the low molecular weight vitamin, folic acid, is required for several enzymatic pathways. Cell membrane receptors mediating endocytic transport of folic acid into cells are expressed in elevated levels in a variety of human tumors. Folic acid conjugates with macromoledules such as toxins, enzymes, antibodies, genes, and liposomes have been shown to be internalized into tumor cells overexpressing folate receptors. These strategies have been employed to enhance the effect of BNCT. The use of dendrimers as boron carriers for antibody conjugation is based on their well-defined structure and multivalency

The use of dendrimers as boron carriers for antibody conjugation is based on their well-defined structure and multivalency. Boronated PAMAM dendrimers have been designed to target the epidermal growth factor receptor, a cell surface receptor that is frequently overexpressed in brain tumor cells.

Preclinical evaluation has been described of a multipurpose STARBURST PAMAM (polyamidoamine) dendrimer prototype (Dendritic Nanotechnologies Inc) that exhibits properties suitable for use as: (i) targeted, diagnostic MRI/NIR (near-IR) contrast agents, (ii) and/or for controlled delivery of cancer therapies (Tomalia et al. 2007). The lead candidate is 1,4-diaminobutane, a dendritic nanostructure ~5 nm diameter, which was selected because of a very favorable biocompatibility profile on in vitro studies, i.e. benign and non-immunogenic. The expectation is that it will exhibit desirable mammalian kidney excretion properties and demonstrated targeting features.

Application of Dendrimers in Photodynamic Therapy

Photodynamic therapy (PDT) uses light-activated drugs called photosensitizers to treat a range of diseases characterized by rapidly growing tissue, including the formation of abnormal blood vessels, such as cancer and age-related macular degeneration. The more traditional name for this therapy is photoradiation therapy. Treatment with PDT consists of a two-step process that starts with administration of the drug, or photosensitizer, by intravenous injection. Once the drug enters the bloodstream, it attaches itself to low-density lipoproteins already circulating. As cells undergoing rapid growth require an above-average supply of lipoproteins, the drug reaches these types of cells more quickly and in higher concentrations. Once the necessary level of concentration is attained, the second step is to activate the drug with a specific dose of light of a specific wavelength. This causes the conversion of normal oxygen found in tissue to a highly-energized form called singlet oxygen, which in turn, disrupts normal cellular functions. Neither the drug nor the light exerts any effect until combined.

Numerous studies have used liposomes, oils and polymeric micelles as encapsulation methods, with some success. However, all techniques suffer from one unpleasant side effect: after controlled release and photosensitization, the drug is free to circulate the body, accumulating in the eyes and skin. This leads to phototoxic side effects, rendering the patient highly sensitive to light. A further disadvantage is that liposomes can be engulfed and destroyed by cells of the reticuloendothelial system. Such problems have limited the emerging field of PDT, but combination of this technique with nanotechnology is promising.

The possibility of improving dendrimers through appropriate functionalization of their periphery makes them promising carriers of PDT. The use of 5-aminolevulinic acid (ALA) is one approach to PDT based on dendrimers. ALA is a natural precursor of the photosensitizer protoporphyrin IX (PIX) and its administration increases the cellular concentrations of PIX. Cellular uptake of the dendrimer occurs through endocytic routes predominantly via a macropinocytosis pathway. A dendrimer conjugate, which incorporated 18 aminolaevulinic acid residues attached via ester linkages to a multipodent aromatic core, has been investigated (Battah et al. 2007). The ability of the dendrimer to deliver and release 5-ALA intracellularly for metabolism to the photosensitizer, protoporphyrin IX, was studied in the transformed PAM 212 murine keratinocyte and A431 human epidermoid carcinoma cell lines. The macromolecular dendritic derivatives were shown to deliver 5-ALA efficiently to cells for sustained porphyrin synthesis.

Another approach to deep tissue penetration is based on two-photon excitation with near-infrared lasers. Multivalent aspects of dendrimer scaffold can be used to conjugate several 2-photon absorbing chromophores to the porphyrin core. Such a system can generate singlet oxygen efficiently on light irradiation at 780 nm wavelength.

Dendrimer-Based Synthetic Vector for Targeted Cancer Gene Therapy

A synthetic vector system based on polypropylenimine dendrimers has the desired properties of a systemic delivery vehicle and mediates efficient transgene expression in tumors after intravenous administration. Specifically, the systemic injection of dendrimer nanoparticles containing a TNF- α expression plasmid regulated by telomerase gene promoters (hTR and hTERT) leads to transgene expression, regression of remote xenograft murine tumors, and long-term survival of up to 100% of the animals. The combination of pharmacologically active synthetic transfection agent and transcriptionally targeted antitumor gene creates an efficacious gene medicine for the systemic treatment of experimental solid tumors. The promising results of these experiments could make it possible to treat inaccessible tumors in humans using gene therapy in the future. This new treatment can selectively target cancer cells, without causing damage to surrounding healthy cells.

Poly-L-lysine Dendrimer as Antiangiogenetic Agent

Poly-L-lysine (PLL) sixth generation (G6) dendrimer molecules exhibit systemic antiangiogenic activity that could lead to arrest of growth of solid tumors. Intravenous administration of the PLL-dendrimer molecules into C57BL/6 mice inhibits vascularization of tumors grown within dorsal skinfold window chambers as demonstrated by intravital microscopy (Al-Jamal et al. 2010). The in vivo toxicological profile of the PLL-dendrimer molecules is shows that it is safe at the dose regime studied. The antiangiogenic activity of the PLL dendrimer is further shown to be associated with significant suppression of B16F10 solid tumor volume and delayed tumor growth. Enhanced apoptosis/necrosis within tumors of PLL-dendrimer-treated animals only and reduction in the number of CD31 positive cells are observed in comparison to protamine treatment. This study suggests that PLL-dendrimer molecules can exhibit a systemic antiangiogenic activity that may be used for therapy of solid tumors, and in combination with their capacity to carry other therapeutic or diagnostic agents may potentially offer capabilities combining diagnosis with therapy.

RNA Nanotechnology for Delivery of Cancer Therapeutics

RNA has immense promise as a therapeutic agent against cancer but the problem has been to have an efficient system to bring multiple therapeutic agents directly into specific cancer cells where they can perform different tasks. The 25-nm RNA

nanoparticles enable repeated long-term administration and avoid the problems of short retention time of small molecules and the difficulties in the delivery of particles larger than 100 nm. Nanoparticles, which are assembled from three short pieces of RNA and resemble miniature triangles, possess both the right size to enter cells and the right structure to carry other therapeutic strands of RNA inside with them, where they can halt viral growth or cancer's progress. RNA molecules come in many variant forms, and the one mimicked from the phi29 virus – called pRNA – also can be linked to other types of RNA to form longer, hybrid strands with properties that could be assigned. Incubation of cancer with the pRNA dimer, one subunit of which harbored the receptor-binding moiety and the other harboring the gene-silencing molecule, resulted in their binding and entry into the cells, and subsequent silencing of anti/proapoptotic genes. The chimeric pRNA complex was found to be processed into functional double-stranded siRNA by Dicer (RNA-specific endonuclease). Animal studies have confirmed the suppression of tumorigenicity of cancer cells by ex vivo delivery.

RNA nanotechnology has been used to engineer both therapeutic siRNA and a receptor-binding RNA aptamer into individual pRNAs of phi29's motor. The RNA building block harboring siRNA or other therapeutic molecules is subsequently incorporated in a trimer through the interaction of engineered right and left interlocking RNA loops. The incubation of the protein-free nanoscale particles containing the receptor-binding aptamer or other ligands results in the binding and co-entry of the trivalent therapeutic particles into cells, which can modulate the apoptosis of cancer cells as shown in animal studies. The use of such antigenicity-free 20–40 nm particles holds promise for the repeated long-term treatment of cancer and other chronic diseases.

Delivery of siRNAs for Cancer

Targeted delivery of siRNAs is a safer and more effective therapy for cancer. Although macromolecules accumulate nonspecifically in tumors through the enhanced permeability and retention (EPR) effect, previous studies using nanoparticles to deliver siRNA demonstrated that attachment of cell-specific targeting ligands to the surface of nanoparticles leads to enhanced potency relative to non-targeted formulations. Although both nontargeted and transferrin-targeted siRNA nanoparticles exhibit similar biodistribution and tumor localization by PET, transferrin-targeted siRNA nanoparticles reduce tumor luciferase activity by ~50% relative to nontargeted siRNA nanoparticles 1 day after injection. Compartmental modeling is used to show that the primary advantage of targeted nanoparticles is associated with processes involved in cellular uptake in tumor cells rather than overall tumor localization. Optimization of internalization may, therefore, be a key to the development of effective nanoparticle-based targeted siRNA therapeutics.

Combination Delivery Systems for Nanoparticle Penetration into Tumor Tissue

Current approved cancer nanotherapeutics, which passively accumulate around leaky regions of the tumor vasculature because of an enhanced permeation and retention (EPR) effect, provide only modest survival benefits. This suboptimal outcome is likely due to physiological barriers that hinder delivery of the nanotherapeutics throughout the tumor. The tumor microenvironment has elevated interstitial fluid pressure and deregulated extracellular matrix components, which disfavor the EPR effect. Effectiveness of nanomedicines in cancer is limited in part by inadequate delivery and transport in tumor interstitium. Tumor priming to overcome these limitations includes measures for extravasation and interstitial transport of nanomedicines in solid tumors include normalization of tumor vasculature, interstitial fluid pressure modulation, enzymatic extracellular matrix degradation, and apoptosis-inducing tumor priming technology, which is exemplified by enhancement of delivery and efficacy of liposomal doxorubicin.

Many of the cancer nanotherapeutics are ≈ 100 nm in diameter and exhibit enhanced accumulation around the leaky regions of the tumor vasculature, but their large size hinders penetration into the dense collagen matrix. Therefore, a multistage system has been proposed in which nanoparticles disintegrate from 100 to 10-nm size after they extravasate from leaky regions of the tumor vasculature and are exposed to the tumor microenvironment (Wong et al. 2011). The smaller nanoparticles can more readily diffuse throughout the tumor's interstitial space. This size change is triggered by proteases such as MMP-2 that are highly expressed in the tumor microenvironment and degrade the cores of 100-nm gelatin nanoparticles, releasing smaller 10-nm nanoparticles from their surface. Quantum dots (QD) were used as a model system for the 10-nm particles because their fluorescence can be used to demonstrate the validity of this approach. In vitro MMP-2 activation of the multistage nanoparticles revealed that the size change was efficient and effective in the enhancement of diffusive transport. In vivo circulation half-life and intratumoral diffusion measurements indicate that multistage nanoparticles exhibit both the long circulation half-life necessary for the EPR effect and the deep tumor penetration required for delivery into the tumor's dense collagen matrix.

Other approaches utilize external stimuli to promote the vascular supply, increase perfusion and permeability of nanoparticles using methods such as hyperthermia and radiation therapy. Combination therapies have also been explored with nanomedicine in which a therapy primes the tumor region for nanoparticles by targeting cancer cells in the perivascular region which are a barrier to nanoparticle penetration. Photoimmunotherapy has been targeted to destroy perivascular cancer cells prior to injection of nanoparticles resulting in an enhanced uptake of nanoparticles in the tumor and distribution of the nanoparticle throughout the tumor (Sano et al. 2013).

Nanotechnology-Based Cancer Therapy

Devices for Nanotechnology-Based Cancer Therapy

Convection-Enhanced Delivery with Nanoliposomal CPT-11

Combination of convection-enhanced delivery (CED) with a novel, highly stable nanoparticle/liposome containing CPT-11 (nanoliposomal CPT-11) is a potential dual drug delivery strategy for brain tumor treatment. Following CED in rat brains, tissue retention of nanoliposomal CPT-11 was shown to be greatly prolonged, with >20% injected dose remaining at 12 days (Noble et al. 2006). In contrast, CED of free CPT-11 resulted in rapid drug clearance. At equivalent CED doses, nanoliposomal CPT-11 increased area under the time-concentration curve by 25-fold and tissue t1/2 by 22-fold over free CPT-11; CED in intracranial U87 glioma xenografts showed even longer tumor retention. Plasma levels were undetectable following CED of nanoliposomal CPT-11. Importantly, prolonged exposure to nanoliposomal CPT-11 resulted in no measurable CNS toxicity at any dose tested, whereas CED of free CPT-11 induced severe CNS toxicity. In the intracranial U87 glioma xenograft model, a single CED infusion of nanoliposomal CPT-11 resulted in significantly improved median survival compared with CED of control liposomes. The study concluded that CED of nanoliposomal CPT-11 greatly prolonged tissue residence while also substantially reducing toxicity, resulting in a highly effective treatment strategy in preclinical brain tumor models.

Nanoengineered Silicon for Brachytherapy

BrachySilTM (³²P BioSilicon, pSivida Corporation) is a nanoparticle in which the isotope 32-phosphorus is immobilized. It demonstrates a very high degree of isotope retention following injection into the liver, thus reducing the risk of soluble radioactive material affecting healthy hepatic tissue, or entering the circulation and causing systemic toxicity. Unlike titanium seeds, which remain forever in the body, phosphorus seeds degrade over time and enable repetition of treatment if necessary. Other treatments for primary liver cancer include a variety of embolization and radio frequency ablation techniques. BrachySil offers a more versatile and safer product for the treatment of such tumors. The procedure is undertaken without surgery under local anesthetic and patients can be discharged the following day. A phase IIa trial in primary liver cancer has shown that it is safe and effective in tumor regression with increased efficacy. An efficacy/safety study for the treatment of 309 days.

Anticancer Effect of Nanoparticles

Antiangiogenic Therapy Using Nanoparticles

Integrin-targeted nanoparticles can be used for site-specific delivery of a therapeutic payload. Selective targeting of upregulated $\alpha_v\beta_3$ and Flk-1 on the neovasculature of tumors is a novel antiangiogenesis strategy for treating a wide variety of solid tumors. Targeted radiotherapy works using different targeting agents on a NP, to target both the integrin $\alpha_v\beta_3$ and the vascular endothelial growth factor receptor. This provides a rationale for the potential therapeutic efficacy of the IA-NP-90Y and anti-Flk-1 MAb-NP-90Y complexes as novel therapeutic agents for the treatment of a variety of tumor types.

The mechanism of inhibition of the function of pro-angiogenic heparin-binding growth factors (HB-GFs), such as vascular endothelial growth factor 165 (VEGF165) and basic fibroblast growth factor (bFGF) by gold nanoparticles (GNPs) has been investigated (Arvizo et al. 2011). It was shown that a naked GNP surface is required and core size plays an important role to inhibit the function of HB-GFs and subsequent intracellular signaling events. The authors also demonstrated that the inhibitory effect of GNPs is due to the change in HB-GFs conformation/configuration (denaturation) by the NPs, whereas the conformations of non-HB-GFs remain unaffected. This study will help structure-based design of therapeutic NPs.

Cytotoxic Effects of Cancer Nanoparticles

Nanoparticles may have a direct cytotoxic effect on cancer cells by various mechanisms. DNA degradation and anticancer activity of copper nanoparticles of 4–5 nm size have been reported, e.g. dose-dependent degradation of isolated DNA molecules by copper nanoparticles through generation of singlet oxygen. Singlet oxygen scavengers such as sodium azide and Tris [hydroxyl methyl] amino methane could prevent the DNA degradation (Jose et al. 2011). Additionally, it was observed that the copper nanoparticles exert cytotoxic effect towards U937 and Hela cells of human histiocytic lymphoma and human cervical cancer origins, respectively by inducing apoptosis.

Gold Nanoparticles for Inhibiting Tumor Growth

A study has demonstrated that unmodified gold nanoparticles (AuNPs) inhibit the proliferation of cancer cells in a size- and concentration-dependent manner by abrogating MAPK-signaling (Arvizo et al. 2013). In addition, these AuNPs reverse epithelial-mesenchymal transition (EMT) in cancer cells by reducing secretion of a number of proteins involved in EMT, up-regulating E-Cadherin, and down-regulating Snail, N-Cadherin, and Vimentin. Inhibition of MAPK signaling and reversal of EMT upon AuNP treatment inhibits tumor growth and metastasis in two separate

orthotopic models of ovarian cancer. Western blot analyses of tumor tissues reveal upregulation of E-Cadherin and down-regulation of Snail and phospho-MAPK, confirming the reversal of EMT and inhibition of MAPK signaling with AuNP treatment. The ability of a single self-therapeutic nanoparticle to abrogate signaling cascades of multiple growth factors is distinctive and has potential medical applications as an antitumor/antimetastatic agent.

Nanoshell-Based Cancer Therapy

Nanoshells may be combined with targeting proteins and used to ablate target cells. This procedure can result in the destruction of solid tumors or possibly metastases not otherwise observable by the oncologist. In addition, Nanoshells can be utilized to reduce angiogenesis present in cancer. Experiments in animals, in vitro and in tissue demonstrate that specific cells (e.g. cancer cells) can be targeted and destroyed by an amount of infrared light that is otherwise not harmful to surrounding tissue. This procedure may be performed using an external (outside the body) infrared laser. Prior research has indicated the ability to deliver the appropriate levels of infrared light at depths of up to 15 cm, depending upon the tissue. Photo-thermal tumor ablation in mice has been achieved by using near infrared-absorbing nanoparticles. The advantages of Nanoshell-based tumor cell ablation include:

- Targeting to specific cells and tissues to avoid damage to surrounding tissue
- Superior side effect profile than targeted chemotherapeutic agents or photodynamic therapy
- Repeatability because of:
 - No "tissue memory" as in radiation therapy
 - Biocompatibility
 - Ability to treat metastases, and inoperable tumors
- Nanoshells enable a seamless integration of cancer detection and therapy.

Nanobody-Based Cancer Therapy

A nanobody with subnanomolar affinity for the human tumor-associated carcinoembryonic antigen (CEA) was conjugated with *Enterobacter cloacae* beta-lactamase, and its site-selective anticancer prodrug activation capacity was evaluated. The conjugate was readily purified in high yields without aggregation or loss of functionality of the constituents. In vitro experiments showed that the nanobody-enzyme conjugate effectively activated the release of phenylenediamine mustard from the cephalosporin nitrogen mustard prodrug 7-(4-carboxybutanamido) cephalosporin mustard at the surface of CEA-expressing LS174T cancer cells. In vivo studies demonstrated that the conjugate had an excellent biodistribution profile and induced regressions and cures of established tumor xenografts. The easy generation and manufacturing yield of nanobody-based conjugates together with their potent antitumor activity make nanobodies promising vehicles for new generation cancer therapeutics.

Nanosecond Pulsed Electric Fields for Cancer Therapy

Nanosecond pulsed electric fields (nsPEFs) has been proven effective in treating several murine tumors. A series of intense electric pulses is used to overcome the barriers of the cell membrane, which is termed as electroporation. Combined with chemotherapy, electroporation can be used to treat skin tumors with reduced dose of chemotherapeutic drugs, which is termed as electrochemotherapy. With increasing the field intensity of the above electric pulses, irreversible breakdown of the plasma membrane can be achieved, which is termed as irreversible electroporation (IRE). Now, IRE has been

To get in vivo evidences of nsPEF for skin tumor treatment, tumor models in 10 female BALB/c nude mice were established by inoculating them with human melanoma cells A375 (Guo et al. 2014). These mice were randomly divided into treated group (exposed to nsPEF with intensity of 20 kV/cm and duration of 300 ns) and control group equally. Five days post-nsPEF treatment, tumor growth in the treated group was effectively inhibited, typical apoptotic characteristics were observed by terminal deoxynucleotidyl transferase dUTP nick end labeling (TUNEL), and significant increases in Bax and decreases in Bcl-2, micro-vessel density, VEGF and proliferating cell nuclear antigen were observed by IHC. These experimental results indicate that in vivo tumor growth can be effectively inhibited by nsPEF, which activates two targets, initiates apoptosis and inhibits angiogenesis.

To determine if nsPEFs is equally effective in treatment of human breast cancer, 30 human breast cancer tumors transplants in mice were exposed to 720 pulses of 100 ns duration, at 4 pulses/sec and 30 kV/cm (Wu et al. 2014). Two weeks after treatment, the growth of treated tumors was inhibited by 79%. MRI showed morphological changes in tumors. Pulsed tumors exhibited apoptosis evaluated by TUNEL staining, inhibition in Bcl-2 expression and decreased blood vessel density. Notably, CD34, VEGF and VEGFR expression in treated tumors were strongly suppressed. To evaluate any adverse effects, normal skin was treated in the same way as tumors, and pulsed skin showed no permanent damages. The results suggest that nsPEFs can inhibit human breast cancer development and suppress tumor blood vessel growth, indicating its potential as a novel therapy for breast cancer.

Nanoparticles Combined with Physical Agents for Tumor Ablation

Several physical agents have been used for ablation of tumors. Nanoparticles can be comined with these techniques and some examples are shown here.

Boron Neutron Capture Therapy Using Nanoparticles

Boron carbide nanoparticles have been used for T cell-guided boron neutron capture therapy. Nanoparticles are produced by ball milling in various atmospheres of commercially available boron carbide. The physical and chemical properties of the particles are investigated using TEM, photon correlation spectroscopy, X-ray photoelectron spectroscopy, X-ray diffraction, vibrational spectroscopy, gel electrophoresis and chemical assays and revealing profound changes in surface chemistry and structural characteristics. In vitro thermal neutron irradiation of B16 melanoma cells incubated with sub-100 nm nanoparticles induces complete cell death. The nanoparticles alone induce no toxicity.

A cancer therapeutic plus diagnostic has been developed that is a variation of BNCT using radio-activate boron-nitride (BN) nanotubes. BNs are covalently bound to tumor-cloned antibodies or immunoglobulins (IgGs) to deliver intense, short-lived, therapeutic doses of radiation specifically to active tumor sites. The therapy involves activation of the BN nanotubes with a neutron beam (as in BNCT) once the IgG carrier molecules reach their target tissue. In contrast to conventional BNCT, instant BN nanotubes can deliver significant numbers of boron atoms (100–1000s) specifically to the tumor site while avoiding exposures to surrounding tissue. BNCT is a technique that relies on (non-radioactive) 10B delivery specifically to a tumor site and then activating it using an accurate beam of epithermal neutrons (low energy neutrons with velocities adjusted to penetrate tissue to the specific tumor depth where the 10B has lodged). BN nanotube structure is like the "rolled-up-graphite" structure of a CNT, six member rings but with boron atoms bound to three surrounding nitrogen atoms, and the nitrogen atoms bound to surrounding boron atoms (no conjugation). Thus, each BN nanotube is composed of a substantial number of boron atoms, e.g. 50%, meaning hundreds to thousands for each nanotube. Boron has a relatively large radioactive cross section and can be easily made radioactive in a neutron flux.

Gold Nanoparticles Combined with Radiation Therapy

High atomic number metals, such as gold, preferentially absorb much more X-ray energy than soft tissues, and thus augment the effect of ionizing radiation when delivered to cells. Proteins that regulate poly-SUMO (small ubiquitin-like modifier) chain conjugates play important roles in cellular response to DNA damage, such as those caused by cancer radiation therapy. A study has demonstrated that conjugation of a weak SUMO-2/3 ligand to gold nanoparticles (AuNPs) facilitates selective multivalent interactions with poly-SUMO-2/3 chains leading to efficient inhibition of poly-SUMO-chain-mediated protein-protein interactions (Li et al. 2012). The ligand-gold particle conjugate significantly sensitized cancer cells to radiation but was not toxic to normal cells. This study demonstrates a viable approach for selective targeting of poly-Ubl chains through multivalent interactions created by nanoparticles that can be chosen based on their properties, such as abilities to augment radiation effects.

A method for the targeting of gold nanoparticles to a tumor in a mouse model is based on the use of the pH Low Insertion Peptide (pHLIP), which delivers various imaging agents to acidic tumors (Yao et al. 2013). Compare of tumor targeting by nonfunctionalized nanogold particles with nanogold-pHLIP conjugates, where nanogold is covalently attached to the N terminus of pHLIP, shows that both intratumoral

and IV administration demonstrated a significant enhancement of tumor uptake of gold nanoparticles conjugated with pHLIP. Statistically significant reduction of gold accumulation was observed in acidic tumors and kidney when pH-insensitive K-pHLIP was used as a vehicle, suggesting an important role of pH in the pHLIP-mediated targeting of gold nanoparticles. pHLIP technology can substantially improve delivery of gold nanoparticles to tumors by providing specificity of targeting, enhancing local concentration in tumors, and distributing nanoparticles throughout the tumor mass where they remain for an extended period, which can facilitate imaging as well as thermolysis or radiation of tumors. Anticancer drugs may be attached to gold nanoparticle conjugates for delivery.

Laser-Induced Cancer Destruction Using Nanoparticles

Laser is a form of photothermal therapy used for destruction of cancer cells. Biological systems are known to be highly transparent to 700-1100-nm NIR light. It is shown here that the strong optical absorbance of SWCNTs in this special spectral window, an intrinsic property of CNTs, can be used for optical stimulation of nanotubes inside living cells to enable multifunctional nanotube biological transporters. Oligonucleotides transported inside living cells by nanotubes can translocate into cell nucleus upon endosomal rupture triggered by NIR laser pulses. Continuous NIR radiation can cause cell death because of excessive local heating of CNTs in vitro. Selective cancer cell destruction can be achieved by functionalization of CNTs with a folate moiety, selective internalization of CNTs inside cells labeled with folate receptor tumor markers, and NIR-triggered cell death, without harming receptor-free normal cells. Thus, the transporting capabilities of CNTs combined with suitable functionalization chemistry and their intrinsic optical properties can lead to new classes of novel nanomaterials for drug delivery and cancer therapy. One example for application is lymphoma as lymphoma cells have well-defined surface receptors that recognize unique antibodies. When attached to a CNT, the antibody would play the role of a Trojan horse. This approach is being tested in laboratory mice with lymphoma. The researchers want to determine if shining NIR on the animal's skin will destroy lymphatic tumors, while leaving normal cells intact. CNTs also can be delivered to diseased cells by direct injection. The idea is to use the nanotube to deliver therapeutic molecules of DNA, RNA or protein directly into the cell nucleus to fight various infections and diseases.

Plasmon-resonant gold nanorods, which have large absorption cross sections at near-infrared frequencies, are excellent candidates as multifunctional agents for image-guided therapies based on localized hyperthermia. The controlled modification of the surface chemistry of the nanorods is of critical importance, as issues of cell-specific targeting and nonspecific uptake must be addressed prior to clinical evaluation. Nanorods coated with cetyltrimethylammonium bromide (a cationic surfactant used in nanorod synthesis) are internalized within hours into cancer cells by a nonspecific uptake pathway, whereas the careful removal of cetyltrimethylammonium bromide from nanorods functionalized with folate results in their accumulation on the cell surface over the same time interval. Thus the nanorods render the tumor cells highly susceptible to photothermal damage when irradiated at the nanorods' longitudinal plasmon resonance, generating extensive blebbing of the cell membrane at laser fluences as low as 30 J/cm2 (Huff et al. 2007).

A light-controlled delivery system that can be tailored to release nonbiological molecules into living cells can be remotely controlled and can release quantifiable amounts on demand. The technique utilizes gold nanoparticles, in the form of nanoshells, to transport the target molecule into the cell, where it can subsequently be released. dsDNA-nanoshells can be loaded with molecules, which are associated with the DNA; these molecules can be released inside the cell when triggered by light (Huschka et al. 2010). The research describes how the nanoshell complexes were loaded with 4,6-diamino-2-phenylindole (DAPI), a fluorescent blue dye that can reversibly bind to DNA. The nanoshells were then introduced to cancer cells, and once uptake of the nanoparticles by the cells was confirmed, the cells were illuminated using a continuous wave laser at a specified wavelength. The wavelength of the laser excitation is tailored to the specific DNA, the Plasmon resonance wavelength dehybridizes the DNA, causing the release of the DAPI molecule. The DAPI molecule is released from the nanoshell and diffuses through the cytoplasm into the cell nucleus. The diffusion of the DAPI molecule into the cell nucleus was confirmed by the staining of the nuclear DNA. The ability of DAPI to reversibly stain DNA fluorescent blue allowed the intracellular release process to be easily visualized. The research concluded that the light-triggered release of DAPI using a laser did not have an adverse effect on the cells, due to the low power of the laser and the minimal irradiation times required to stimulate the release of the molecule. The researchers also discerned that the uptake of the nanoshells had no adverse effects on the living cells.

Poly(lactic-co-glycolic acid) nanoparticles can be used to encapsulate the photosensitizer meso-tetraphenylporpholactol and are stable as well as nonphototoxic when administered systemically. Upon cellular internalization, the photosensitizer is released from the nanoparticle and becomes highly phototoxic. Irradiation with visible light results in cell-specific killing of several cancer cell lines. In vivo experiments have shown complete eradication of cancers in mouse models. The concept of photosensitizers with selective phototoxicity should have widespread applications in cancer therapy.

A nanocarrier consisting of polymeric micelles of diacylphospholipidpoly(ethylene glycol) (PE-PEG) coloaded with the photosensitizer drug 2-[1-hexyloxyethyl]-2-devinyl pyropheophorbide-a (HPPH), and magnetic Fe3O4 nanoparticles has been used for guided drug delivery together with light-activated photodynamic therapy for cancer. The nanocarrier shows excellent stability and activity over several weeks. The loading efficiency of HPPH is practically unaffected upon coloading with the magnetic nanoparticles, and its phototoxicity is retained. The magnetic response of the nanocarriers was demonstrated by their magnetically directed delivery to tumor cells in vitro. The magnetophoretic control on the cellular uptake provides enhanced imaging and phototoxicity. These multifunctional nanocarriers demonstrate the exciting prospect offered by nanochemistry for targeting photodynamic therapy. In a novel nanoformulation of for PDT of cancer, the photosensitizer molecules are covalently incorporated into organically modified silica (ORMOSIL) nanoparticles (Ohulchanskyy et al. 2007). The incorporated photosensitizer molecules retain their spectroscopic and functional properties and can robustly generate cytotoxic singlet oxygen molecules upon photoirradiation. The synthesized nanoparticles are of ultralow size (~20 nm) and are highly monodispersed and stable in aqueous suspension. The advantage offered by this covalently linked nanofabrication is that the drug is not released during systemic circulation, which is often a problem with physical encapsulation. These nanoparticles are also avidly taken up by tumor cells and demonstrate phototoxic action, thereby improving the diagnosis as well as PDT of cancer.

A single-particle PET-based platform has been developed to quantitatively correlate the heat generation of plasmonic nanoparticles with their potential as cancer killing agents by using a temperature sensitive lipid-based assay and comparison with their theoretically predicted photo-absorption. In vivo, the heat generation of irradiated nanoparticles was evaluated in human tumor xenografts in mice using ¹⁸F-FDG PET imaging (Jørgensen et al. 2016). To validate the use of this platform, the authors quantified the photothermal efficiency of NIR resonant silica-gold nanoshells (AuNSs) and benchmarked this against the heating of colloidal spherical, solid gold nanoparticles (AuNPs). As expected, both in vitro and in vivo the heat generation of the resonant AuNSs was more as compared to the non-resonant AuNPs. Furthermore, the results showed that PET imaging could be reliably used to monitor early response to photothermal treatment. This approach provides a much needed platform to benchmark the emerging plethora of novel plasmonic nanoparticles for their potential for photothermal cancer therapy. The next stage of research will be injecting nanoparticles into the circulation where they end up in the tumors that may have metastasized. The tumors can be localized with PET scans and irradiated with lasers, while also effectively assessing how well the treatment has worked shortly after the irradiation. In addition, the nanoparticles can be coated with chemotherapy, which is released by the heat and will also help kill the cancer cells.

Nanoparticle-Mediated Thermal Ablation of Cancer

Thermal ablation of cancer is a recognized technique and is involved in laser ablation of cancer as well. Hyperthermia is the gentle heating of tissue below ablation temperatures, typically <5 °C above normal body temperature. Clinical studies have demonstrated hyperthermia can more than double the efficacy of radiation therapy in select tumors, without an increase in toxicity, and can enhance the efficacy of several chemotherapeutic agents for many types of solid tumors. Thermal ablation of cancer has been refined by use of nanoparticles. Some examples are given in this section and further examples are given in following sections where combination of imaging with thermolysis is described.

An experimental procedure for the treatment of breast cancer is called magnetic thermal ablation. Magnetic nanoparticles are promising tools for the minimal invasive elimination of small tumors in the breast using magnetically-induced heating.

The approach complies with the increasing demand for breast conserving therapies and has the advantage of offering a selective and refined tuning of the degree of energy deposition allowing an adequate temperature control at the target.

Anti-HER2 antibody can induce antitumor responses, and can be used in delivering drugs to HER2-overexpressing cancer. Anti-HER2 immunoliposomes containing magnetite nanoparticles, which act as tumor-targeting vehicles, have been used to combine anti-HER2 antibody therapy with hyperthermia in experimental studies. SWCNTs emit heat when they absorb energy from NIR light. Tissue is relatively transparent to NIR, which suggests that targeting SWCNTs to tumor cells, followed by noninvasive exposure to NIR light, will ablate tumors within the range of NIR. One study has demonstrated the specific binding of MAb-coupled SWCNTs to tumor cells in vitro, followed by their highly specific ablation with NIR light (Chakravarty et al. 2008). Only the specifically targeted cells were killed after exposure to NIR light.

Targeted nanotherapeutics (TNT) system is an innovation of thermal ablation of cancer that bonds iron nanoparticles and MAbs into bioprobes. The magnetic field energy is converted to lethal heat by the particles causing a rapid temperature increase to more than 170 °C. at the surface of the cancer cells, killing them and their blood supply with negligible damage to surrounding healthy tissues. To evaluate the potential of TNT for in vivo tumor targeting, efficacy, and predictive radionuclide-based heat dosimetry were studied using ¹¹¹In-ChL6 bioprobes (ChL6 is chimeric L6) in a human breast cancer xenograft model (Denardo et al. 2007). Mice in the study received a series of alternating magnetic field (AMF) bursts in a single 20-min treatment. Dosing was calculated using an equation that included tumor concentration of bioprobes, heating rate of particles at different amplitudes, and the spacing of AMF bursts. MAb-guided bioprobes (iron oxide nanoparticles) effectively targeted the tumors without causing particle-related toxicity. Tumor total heat dose, calculated using empirically observed ¹¹¹In-bioprobe tumor concentration and in vitro nanoparticle heat induction by AMF, correlated with tumor growth delay. The biggest problem of thermotherapy of cancer has been how to apply it to the tumor alone, how to predict the amount needed and how to determine its effectiveness. By combining nanotechnology, focused AMF therapy and quantitative molecular imaging techniques, a safe technique has been developed that could be considered for clinical use as a treatment for breast and other cancers.

Metal nanoshells belong to a class of nanoparticles with tunable optical resonances that have been used for thermal ablative therapy for cancer. Nanoshells can be tuned to strongly absorb light in the NIR, where optical transmission through tissue is optimal. Nanoshells placed at depth in tissues can be used to deliver a therapeutic dose of heat by using moderately low exposures of extracorporeally applied NIR. In vivo studies under MRI guidance have revealed that exposure to low doses of NIR in solid tumors treated with metal nanoshells reach temperatures capable of inducing irreversible tumor destruction within min. Gold nanoshells are ~120 nm in diameter and a cancer cell is 170 times bigger. Therefore, nanoshells can penetrate the tumor capillaries and lodge in the tumor. Application of NIR light, which passes through the skin harmlessly, heats the nanoshells and kills the tumor cells. Since no drug is used, the cancer cells are unlikely to develop drug resistance.

The ability to control both wavelength-dependent scattering and absorption of nanoshells offers the opportunity to design nanoshells which provide both diagnostic and therapeutic capabilities in a single nanoparticle. A nanoshell-based alloptical platform technology can integrate cancer imaging and therapy applications. Immunotargeted nanoshells, engineered to both scatter light in the near infrared range enabling optical molecular cancer imaging and to absorb light, enable selective destruction of targeted carcinoma cells through photothermal therapy. In a proof of principle experiment, dual imaging/therapy immunotargeted nanoshells were used to detect and destroy breast carcinoma cells that overexpress HER2, a clinically relevant cancer biomarker. This approach has some significant advantages over alternatives that are under development. For example, optical imaging is much faster and less expensive than other medical imaging techniques. Gold nanoparticles are also more biocompatible than other types of optically active nanoparticles, such as QDs.

Nanospectra Biosciences Inc. is already developing nanoshells for the targeted destruction of various cancers using Nanoshells (AuroShellTM). AuroLaseTM Cancer Therapy combines the unique physical and optical properties of AuroShellTM microparticles with a near infrared laser source to thermally destroy cancer cells without significant damage to surrounding tissue. AuroShellTM microparticles are injected intravenously and specifically collect in the tumor through the associated leaky vasculature (the Enhanced Permeability and Retention effect, or EPR). After the particles accumulate in a tumor, the area is illuminated with a near-infrared laser at wavelengths chosen to allow the maximum penetration of light through tissue. Unlike solid metals and other materials, AuroShellTM microparticles are designed to specifically absorb this wavelength, converting the laser light into heat. This results in the rapid destruction of the tumor along its irregular boundaries. The basics of this approach have been tested experimentally.

The blood vessels inside tumors develop poorly, allowing small particles like nanoshells to leak out and accumulate inside tumors. An animal trial involved 25 mice with tumors ranging in size from 3 to 5.5 mm. The mice were divided into three groups. The first group was given no treatment. The second received saline injections, followed by 3 min exposure to near-infrared laser light. The final group received nanoshell injections and laser treatments. In the test, researchers injected nanoshells into the mice, waited 6 h to give the nanoshells time to accumulate in the tumors and then applied a 5 mm laser beam on the skin above each tumor. Surface temperature measurements taken during the laser treatments showed a marked increase that averaged about 46 °F (7.7 °C) for the nanoshells group. There was no measurable temperature increase at the site of laser treatments in the saline group. Likewise, sections of laser-treated skin located apart from the tumor sites in the nanoshells group also showed no increase in temperature, indicating that the nanoshells had accumulated as expected within the tumors. All signs of tumors disappeared in the nanoshells group within 10 days. These mice remained cancer-free after treatment. Tumors in the other two test groups continued to grow rapidly. All mice in these groups were euthanized when the tumors reached 10 millimeters in size. The mean survival time of the mice receiving no treatment was 10.1 days; the mean survival time for the group receiving saline injections and laser treatments was 12.5 days. The advantages of Nanoshell-based tumor cell ablation include:

- · Targeting to specific cells and tissues to avoid damage to surrounding tissue
- Less adverse effects than targeted chemotherapeutic agents or photodynamic therapy
- Repeatability because of lack of "tissue memory" as in radiation therapy and biocompatibility
- Ability to treat malignancies such as glioblastoma multiforme, metastases and inoperable tumors.

Thermosensitive liposomes have been used as vehicles for the delivery and release of drugs to tumors. To improve the targeting efficacy for breast cancer treatment, a HER2-specific affibody molecule was conjugated to the surface of thermosensitive small unilamellar liposomes of measuring 80–100 nm refered to as "Affisomes", to study effects of this modification on physical characteristics and stability of the resulting preparation (Puri et al. 2008). Affisomes released calcein, a water-soluble fluorescent probe, in a temperature-dependent manner, with optimal leakage (90–100%) at 41 °C. Affisomes, when stored at room temperature, retained >90% entrapped calcein up to 7 days. Affisomes are promising candidates for targeted thermotherapy of breast cancer.

Siennova® (Endomagnetics Inc) therapeutic hyperthermia system uses externally generated magnetic energy to heat magnetic nanoparticles embedded in or adjacent to tumors that in combination with radiation, chemotherapy, or immunotherapy produces a therapeutic benefit. It is in development for the treatment of non-muscle invasive bladder cancer initially and has yet to receive regulatory approval.

Temperature-Sensitive Liposomes for Cancer Destruction

Temperature-sensitive liposomes (TSLs) can be modified to be leaky and explode upon landing on tumor hotspots. At 37 °C, the normal body temperature, the watertight TSLs are chemically and thermally stable. However, at 42°C, the drugs are released. Upon exposure to 1 h of mild heating at 42°C there is significant enhancement of cytotoxic activity in human melanoma cancer cells. The effects of the TSLs also carry in animal studies has shown improved survival of mice carrying tumor transplants. If 5° degrees of difference in temperature is sufficient to discriminate between healthy and cancer cells, the aim should be to raise temperature of only the tumors and not the whole body. For tumors near the body surface, such as head, neck, and skin, a simple heating pad would be sufficient. Internally located tumors would require use of a heat probe or ultrasound.

Ultrasound Radiation of Tumors Combined with Nanoparticles

Nanoparticles have been introduced in tumors followed by ultrasound-induced cavitation for safe and efficient drug and gene delivery. Acoustic cavitation plays a key role both in achieving targeted drug release and enhanced extravasation at modest pressure amplitudes and acoustic energies, as well as in enabling real-time monitoring of the drug delivery process (Mo et al. 2012). Nanoparticle delivery from ultrasoundactivated composite agents may improve tumor treatment by offering a combination of better targeting, enhanced payload delivery, and controlled local drug release (Burke et al. 2014). The next challenge in ultrasound-enhanced drug delivery will thus be to develop a new generation of drug-carrying nanoparticles, which are of the right size range for delivery to tumors, and capable of achieving cavitation as well as drug release at modest acoustic pressures and energies that are safe for the patient.

Nanomedicines Combined with Molecular Targeted Anticancer Therapeutics

Nanomedicines that preferentially deploy cytotoxic agents to tumors and molecular targeted therapeutics that inhibit specific aberrant oncogenic drivers are emerging as the new paradigm for the management of cancer. Some studies are exploring the combination of nanomedicines with molecular targeted therapeutics and the sequence of applications. A supramolecular cis-platinum nanoparticle has been engineered, which induced apoptosis in breast cancer cells, and elicited prosurvival signaling via an EGF receptor/phosphoinositide 3-kinase (PI3K) pathway (Pandey et al. 2014). Combination of mathematical modeling and in vitro and in vivo validation using a pharmacologic inhibitor of PI3K, PI828, demonstrated that administration of PI828 following treatment with the supramolecular cis-platinum nanoparticle results in enhanced antitumor efficacy in breast cancer as compared with when the sequence is reversed or when the two treatments are administered simultaneously. This study shows the importance of drug sequencing when using a combination of a nanomedicine and a targeted therapeutic. The results also indicate that a rational combination of cis-platinum nanoparticles and a PI3K-targeted therapeutic can emerge as a potential therapy for breast cancer.

Impact of Nanotechnology-Based Imaging in Management of Cancer

The role of nanotechnology in diagnostic imaging of cancer, particularly MRI, has already been described earlier in this Chapter. Nanotechnology-based cancer imaging will lead to sensitive and accurate detection of early stage cancer. Nanoparticleenabled imaging can help accurate delivery of cancer therapy.

Cornell Dots for Cancer Imaging

Cornell dots (C dots) are ultrasmall, cancer-targeted, multimodal silica nanoparticles <7 nm in diameter, which have been surface functionalized with cyclic arginineglycine-aspartic acid peptide ligands and radioiodine. C dots exhibit high-affinity binding, favorable tumor-to-blood residence time ratios, and enhanced tumorselective accumulation in avß3 integrin-expressing melanoma xenografts in mice (Benezra et al. 2011). The silica shell, essentially glass, is chemically inert and small enough to pass through the body and out in the urine. Coating the dots by PEGylation further protects them from being recognized by the body as foreign substances, giving them more time to find targeted tumors. The outside of the shell can also be coated with organic molecules that can attach to desired targets on tumor surfaces or within tumors. C dots fulfill a need because clinical translation of nanoparticle probes, including QDs, has not kept pace with the accelerated growth in minimally invasive surgical tools that rely on optical imaging agents. The cluster of dye molecules in a single dot fluoresces under NIR much more brightly than single dye molecules, and the fluorescence identifies malignant cells, showing a surgeon exactly what needs to be cut out and helping ensure that all malignant cells are found. C dots can reveal the extent of a tumor's blood vessels, cell death, treatment response and invasive or metastatic spread to lymph nodes and distant organs.

The FDA has approved the first clinical trial in humans of C dots that can light up cancer cells in PET-optical imaging. The trial was conducted at Memorial Sloan-Kettering Center, New York. C dots were labeled with ¹²⁴I for PET imaging and modified with cRGDY peptides, which contain the dye Cy5 for molecular targeting, rendering them inherently fluorescent (Phillips et al. 2014). The safety, pharmacokinetics, clearance properties, and radiation dosimetry of ¹²⁴I-cRGDY-PEG-C dots were assessed by serial PET and CT after intravenous administration in patients. Metabolic profiles and laboratory tests of blood and urine specimens, obtained before and after particle injection, were monitored over a 2-week interval. Findings are consistent with a well-tolerated inorganic particle tracer exhibiting in vivo stability and distinct, reproducible pharmacokinetic signatures defined by renal excretion. No toxic or adverse events attributable to the particles were observed. Coupled with preferential uptake and localization of the probe at sites of disease, these firstin-human results suggest safe use of these particles in human cancer diagnostics. The technology aims to safely show surgeons extent of tumors in human organs. Although this trial provides estimation of nanoparticle dose requirements, future studies will be needed in larger cohorts of patients, to evaluate nonspecific localization of C dots due to enhanced permeability and retention effects in the tumor tissue, as well as functionalization with other targeting ligands tailored for personalized cancer imaging. This study has achieved translation of inorganic, cancer-targeted nanoparticles from bench to bedside, but there will be many years before such nanoparticle-based imaging agents will be approved by the FDA for routine clinical diagnosis. Commercial development will continue in collaboration with Hybrid Silica Technologies Inc.

Nanoparticles and Optoacoustic Imaging in Management of Cancer

Optoacoustic imaging combines the rich contrast of optical methods with the resolution of ultrasound imaging and can therefore deliver optical visualization of cancer far deeper in tissue than optical microscopy and other conventional optical imaging methods (Taruttis et al. 2015). Multispectral optoacoustic tomography (MSOT) provides spectral detection of absorption contrast to visualize several endogenous tissue components that are relevant to cancer including hemoglobin oxygenation and volume as well as a range of exogenous contrast agents, e.g. approved optical dyes and a rapidly growing toolbox of light-absorbing nanoparticles. Different materials that absorb light, such as gold or silver nanoparticles, carbon nanotubes, or iron-oxide particles, have been investigated in optoacoustic imaging studies.

Nanoparticles offer promising characteristics over organic dyes in terms of their absorption and photostability and offer an alternative for optoacoustic contrast generation. Gold nanoparticles have been shown to generate strong optoacoustic signals due to plasmon resonance and can offer a tunable absorption spectrum based on their shape. Imaging of gold nanorods that accumulate in the tumor due to enhanced permeability and retention has been demonstrated, whereas gold nanospheres conjugated to anti-EGFR have been investigated in the context of tumor targeting. Other examples include in vivo brain tumor contrast enhancement by gold nanospheres coated with gadolinium and a Raman-molecular tag to enable trimodal visualization by MRI, optoacoustics, and Raman imaging (Kircher et al. 2012). Silver nanoplates with absorption peaks around 800 nm functionalized with antibodies for EGFR targeting have been also been considered for imaging pancreatic cancer (Homan et al. 2012).

MSOT can provide imaging biomarkers of cancer that are useful for personalized management of cancer. Noninvasive imaging of the breast, lymph nodes and the skin as well as endoscopic imaging of the gastrointestinal tract are the most likely applications of optoacoustic visualization of cancer to be investigated in clinical trials in the future.

Nanoparticle-MRI for Tracking Dendritic Cells in Cancer Therapy

Several techniques have been developed that allow an effective cellular internalization of clinical SPIO formulations without affecting cell proliferation, differentiation, and function, with "magnetoelectroporation" being the most recent labeling paradigm. Animal studies have shown that the MR distribution pattern is reliable when cells have limited cell division, as validated by conventional histological techniques. Magnetically labeled stem cells are not yet in clinical use due to safety concerns about the in vivo behavior of stem cells. A phase I trial has shown the feasibility and safety of imaging autologous dendritic cells that were labeled with a clinical superparamagnetic iron oxide formulation or ¹¹¹In-oxine and were co-injected intranodally in melanoma patients under ultrasound guidance. In contrast to scintigraphic imaging, MRI allowed assessment of the accuracy of dendritic cell delivery and of inter- and intra-nodal cell migration patterns MRI cell tracking using iron oxides appears clinically safe and well suited to monitor cellular therapy in humans. It is believed that MRI cell tracking will become an important technique that someday may become routine in standard radiological practice once stem cell therapy enters clinical practice.

Nanoparticle-CT Scan

Use of nanomaterials for one of the most common imaging techniques, computed tomography (CT), has remained unexplored. Current CT contrast agents are based on small iodinated molecules. They are effective in absorbing X-rays, but nonspecific distribution and rapid pharmacokinetics have rather limited their microvascular and targeting performance. While most of the nanoparticles are designed to be used in conjunction with MRI, bismuth sulfide (Bi₂S₃) nanoparticles naturally accumulate in lymph nodes containing metastases and show up as bright white spots in CT images. A polymer-coated Bi₂S₃ nanoparticle preparation has been proposed as an injectable CT imaging agent. This preparation demonstrates excellent stability at high concentrations, high X-ray absorption (fivefold better than iodine), very long circulation times (>2 h) in vivo and an efficacy/safety profile comparable to or better than iodinated imaging agents. The utility of these polymer-coated Bi₂S₃ nanoparticles for enhanced in vivo imaging of the vasculature, the liver and lymph nodes has been demonstrated in mice. These nanoparticles and their bioconjugates are expected to become an important adjunct to in vivo imaging of molecular targets and pathological conditions. Tumor-targeting agents are now being added to the surfaces of these polymer-coated Bi₂S₃ nanoparticles.

Nanosensor Device as an Aid to Cancer Surgery

Scientists at the University of Nebraska-Lincoln have developed a high-resolution touch sensor, one that uses a self-assembling nanoparticle device and acts much like a human finger. The self-assembly process developed by the research team involves no complex lithography, thus proving to be cost-effective and would be relatively easy to reproduce. This device can sense texture by touch, which is vital for surgeons who need the "touch sensation" in order to operate with precision and accuracy, such as when it comes to detecting and removing cancer cells from the body. One of the most important applications of this newly created sensor is the potential it holds for cancer surgeons, who are faced with the difficult task of knowing where to stop cutting when removing cancer cells in the body. In the development of artificial skin, the nano device structure can attain resolution of ~20 microns or even less. As this dimension is comparable to single cell dimension, one can hope to "see" a single cancer cell in a tissue. The next goal is "to make a high resolution thermal imaging device, and develop an ultra sound detector with a much better image resolution to enable detection of malignant tumors at early stages.

Nanoparticle-Based Imaging in Oncology Clinical Trials

Currently CT scans are used as surrogate end points in cancer clinical trials. The size of the tumor gives only limited information about the effectiveness of therapy. New imaging agents could speed the clinical trials process in two ways; (1) better imaging data could help oncologists better select which therapies to use on a certain patient; and (2) and increasingly sensitive and specific imaging agents will be able to provide real-time information about whether a therapy is working. Currently, oncologists and their patients must wait months to determine if a given therapy is working. Shorter clinical trials would mean that effective new drugs would reach patients quicker and ineffective drugs would be dropped from clinical trials sooner, allowing drug discoverers to better focus their efforts on more promising therapies.

QDs Aid Lymph Node Mapping in Cancer

An improved method for performing sentinel lymph node (SLN) biopsy, which depends on illuminating lymph nodes during cancer surgery, has been developed using QDs that emit NIR light, a part of the spectrum that is transmitted through biological tissue with minimal scattering. SLN mapping is a common procedure used to identify the presence of cancer in a single, "sentinel" lymph node, thus avoiding the removal of a patient's entire lymph system. SLN mapping relies on a combination of radioactivity and organic dyes but the technique is inexact during surgery, often leading to removal of much more of the lymph system than necessary, causing unwanted trauma. QD technique is a significant improvement over the dye/radioactivity method currently used to perform SLN mapping. The imaging system and QDs allowed the pathologist to focus on specific parts of the SLN that would be most likely to contain malignant cells, if cancer were present.

Different varieties of PEG-coated QDs have been injected directly into tumors in mouse models of human cancer and their course tracked through the skin using NIR fluorescence microscopy to image and map SLNs (Ballou et al. 2007). In tumors that drained almost immediately to the SLNs, the QDs were confined to the lymphatic system, mapping out the connected string of lymph nodes. This provided easy tagging of the SLNs for pathology and there was little difference in results among the different QD types used. Examination of the SLNs identified by QD localization showed that at least some contained metastatic tumor foci. The animals used in this study were followed for >2 years, with no evidence of toxicity, even though QDs could still be observed within the animals. SLN mapping has already revolutionized cancer surgery. NIR QDs have the potential to improve this important technique even further. Because the QDs in the study are composed of heavy metals, which can be toxic, they have not yet been approved for clinical use until safety has been established.

Single Wall Carbon Nanotubes for Targeted Imaging of Tumors

Detection of small, deep tumors for early diagnosis and surgical interventions remains a challenge for conventional imaging modalities. Second-window near-infrared light (NIR2, 950–1400 nm) is promising for in vivo fluorescence imaging due to deep tissue penetration and low tissue autofluorescence. With their intrinsic fluorescence in the NIR2 regime and lack of photobleaching, SWCNTs are attractive contrast agents for detecting tumors. Targeted M13 virus-stabilized SWCNTs were used to visualize deep tumors in vivo (Ghosh et al. 2014). The targeted nanoprobe, which uses M13 bacteriophage to stably display both tumor-targeting peptides and an SWCNT imaging probe, has excellent tumor-to-background uptake and exhibits higher signal-to-noise performance compared with visible and NIR1 dyes for delineating tumor nodules. Detection and excision of tumors by a gynecological surgeon was shown to improve with SWCNT image guidance and led to the identification of submillimeter tumors. This approach is useful for guiding surgical interventions where deep tissue molecular imaging is informative.

Nanoparticles for Targeted Therapy of Tumors

Nanoparticles can deliver chemotherapy drugs directly to tumor cells and then give off a signal after the cells are destroyed. Drugs delivered this way are 100 times more potent than standard therapies. Gold nanoparticles can help X-rays kill cancerous cells more effectively in experimenats on mice. Combination of nanoparticles followed by X-ray treatment reduced the size of the tumors, or completely eradicated them, whereas tumors that had received only X-ray therapy continued to grow. The gold nanoparticles had no therapeutic effect on their own. The technique works because gold, which strongly absorbs X-rays, selectively accumulates in tumors. This increases the amount of energy that is deposited in the tumor compared with nearby normal tissue.

Efficient conversion of strongly absorbed light by plasmonic gold nanoparticles to heat energy and their easy bioconjugation suggest their use as selective photothermal agents in molecular cancer cell targeting. Oral squamous carcinoma cell lines have been incubated with anti-epithelial growth factor receptor (EGFR) antibody conjugated gold nanoparticles and then exposed to continuous visible argon ion laser at 514 nm. Malignant cells required less than half the laser energy to be killed than the benign cells after incubation with anti-EGFR antibody conjugated Au nanoparticles. No photothermal destruction was observed for all types of cells in the absence of nanoparticles at four times energy required to kill the malignant cells with anti-EGFR/Au conjugates bonded. Au nanoparticles thus offer a novel class of selective photothermal agents using a CW laser at low powers. The ability of gold nanoparticles to detect cancer was demonstrated previously. Now it will be possible to design an 'all in one' active agent that can be used to noninvasively find the cancer and then destroy it. This selective technique has a potential in molecularly targeted photothermal therapy in vivo.

Nanocarriers with TGF- β Inhibitors for Targeting Cancer

TGF-β inhibitors can prevent the growth and metastasis of certain cancers. However, there may be adverse effects caused by TGF- β signaling inhibition, including the induction of cancers by the repression of TGF-B-mediated growth inhibition. Application of a short-acting, small-molecule TGF- β type I receptor (TR-I) inhibitor at a low dose has been shown to be effective in treating several experimental intractable solid tumors, including pancreatic adenocarcinoma and diffuse-type gastric cancer, characterized by hypovascularity and thick fibrosis in tumor microenvironments. Low-dose TR-I inhibitor alters neither TGF-B signaling in cancer cells nor the number of fibrotic components. However, it decreases pericyte coverage of the endothelium without reducing endothelial area specifically in tumor neovasculature and promotes accumulation of macromolecules, including anticancer nanocarriers, in the tumors. Compared with the absence of TR-I inhibitor, anticancer nanocarriers exhibit potent growth-inhibitory effects on these cancers in the presence of TR-I inhibitor. The use of TR-I inhibitor combined with nanocarriers may thus be of significant clinical and practical importance in treating intractable solid cancers.

Nanobombs for Cancer

Nanobombs are nanoscale bombs, which infiltrate into tumors in a minimally invasive manner and then explode on exposure to physical or chemical triggers. Various nanomaterials have been used for the construction of nanobombs including gold and silica nanoparticles as well as carbon nanotubes. Nanobombs are effective anticancer agents as the shock waves that are generated after local explosion inside the tumor kill cancer cells and disrupt cancer pathways so that the effect spreads beyond the area of explosion.

Temperature change can be used to trigger explosion. Nanogels fabricated by light cross-linking exhibit abrupt volume expansion upon exposure to sudden temperature change, causing cell death (Lee et al. 2009). In another approach, Nanoclusters (gold nanobombs) can be activated in cancer cells only by confining near-infrared laser pulse energy within the critical mass of the nanoparticles in the nanocluster. Once the nanobombs are exploded and kill cancer cells, macrophages can effectively clear the cell debris and the exploded nanotube along with it.

Blending of supramolecular chemistry and mechanostereochemistry with mesoporous silica nanoparticles has led to a new class of materials that are biological nanoscale bombs with the potential to infiltrate cells and explode upon the pulling of a chemical trigger. The triggers are initiated by changes in pH, light and redox potentials, in addition to enzymatic catalysis. This approach has been tried in "in vitro" experiments where loaded mechanized silica nanoparticles are endocytosed selectively by cancer cells and an intracellular trigger causes release of a cytotoxin, effectively leading to apoptosis.

Nanoparticle-Based Anticancer Drug Delivery to Overcome MDR

Although multidrug resistance (MDR) is known to develop through a variety of molecular mechanisms within the tumor cell, many tend to converge toward the alteration of apoptotic signaling. The enzyme glucosylceramide synthase (GCS), responsible for bioactivation of the proapoptotic mediator ceramide to a nonfunctional moiety glucosylceramide, is overexpressed in many MDR tumor types and has been implicated in cell survival in the presence of chemotherapy.

A study investigated the therapeutic strategy of coadministering ceramide with paclitaxel in an attempt to restore apoptotic signaling and overcome MDR in the human ovarian cancer cell line using modified poly(epsilon-caprolactone) (PEO-PCL) nanoparticles to encapsulate and deliver the therapeutic agents for enhanced efficacy (van Vlerken et al. 2007). Results show that indeed the complete population of MDR cancer cells can be eradicated by this approach. Moreover, with nanoparticle drug delivery, the MDR cells can be resensitized to a dose of paclitaxel near the IC50 of non-MDR (drug sensitive) cells, indicating a 100-fold increase in chemosensitization via this approach. Molecular analysis of activity verified the hypothesis that the efficacy of this therapeutic approach is idue to a restoration in apoptotic signaling, although the beneficial properties of PEO-PCL nanoparticle delivery enhanced the therapeutic success even further, showing the promising potential for the clinical use of this therapeutic strategy to overcome MDR. Besides MDR, this novel paclitaxel-ceramide nanoparticle therapy also shows great potential for use in the treatment of non-MDR cancer types, in which therapeutic efficacy of paclitaxel is also enhanced.

Nanotechnology, used in conjunction with existing therapies, such as gene therapy and P-glycoprotein inhibition, has been shown to improve the reversal of drug resistance. The mechanisms involved include specific targeting of drugs, enhanced cellular uptake of drugs, and improved bioavailability of drugs. Important strategies in the reversal of drug resistance include (Palakurthi et al. 2012):

- · A multifunctional nanoparticulate system
- · Therapeutics to kill resistant cancer cells and cancer stem cells
- Release of encapsulated cytotoxic therapeutics in a stimuli-responsive tumor microenvironment

Time-Delayed, Dual-Drug Nanoparticle Delivery System

Cancer patients are routinely given two or more different chemotherapy drugs in the hope that a multipronged attack will be more successful than a single drug. Although many studies have identified drugs that work well together, it is now shown that the timing of drug administration can dramatically influence the outcome. A time-delayed, dual-drug nanoparticle delivery system for treating cancer has been developed (Morton et al. 2014). Nanoparticles contain two drugs (one in the membrane and one

in the center of each nanoparticle) and are coated to target them to cancer cells. Cancer cells take up the nanoparticles. The first drug quickly escaped the nanoparticle, sensitizing the cells to the second drug, which escaped more slowly. In mice, tumors from cells that respond to the first drug are reduced when the mice are treated with the dual-drug nanoparticles, but the tumors continue to grow in mice receiving only single-drug therapy. This time-delayed, nanoparticle-mediated drug delivery may avoid the resistance that cancer cells develop to chemotherapy. In this study the cancer cells were weakened by administering the drug erlotinib, which shuts down one of the pathways that promote uncontrolled tumor growth. These pretreated tumor cells were much more susceptible to treatment with a DNA-damaging drug called doxorubicin than cells given the two drugs simultaneously.

Erlotinib, which targets EGFR found on tumor cell surfaces, is approved for treatment of pancreatic and lung cancers. Doxorubicin is used to treat many cancers, including leukemia, lymphoma, and bladder, breast, lung, and ovarian tumors. The combination of these two drugs proved particularly powerful against triple-negative breast cancer, which does not have overactive estrogen, progesterone, or HER2 receptors, account for ~16% of breast cancer cases, are much more aggressive than other types and tend to strike younger women. To deliver the combination, the authors designed liposomes to carry doxorubicin inside the particle's core, with erlotinib embedded in the outer layer. PEG coating protects the particles them from being broken down in the body or filtered out by the liver and kidneys. Another tag, folate, helps direct the particles to tumor cells, which express high quantities of folate receptors. Once the particles reach a tumor and are taken up by cells, the particles start to break down. Erlotinib, carried in the outer shell, is released first, but doxorubicin release is delayed and takes more time to seep into cells, giving erlotinib time to weaken the cells' defenses. There is a lag between 4–24 h between the erlotinib and doxorubicin peaks of effectiveness. As a next step before possible clinical trials in human patients, the researchers are now testing the particles in genetically programmed mice that develop tumors on their own, instead of having human tumor cells implanted in them.

The time-staggered delivery could also improve other types of chemotherapy. They authors have devised several combinations involving cisplatin, a commonly used DNA-damaging drug, and are working on other combinations to treat prostate, head and neck, and ovarian cancers. At the same time, they are working on more complex nanoparticles to enable more precise loading of the drugs and fine-tuning of their staggered release.

Combination of Diagnostics and Therapeutics for Cancer

Aptamer Conjugated Magnetic Nanoparticles

Magnetic nanoparticles have shown promise for targeted drug delivery, hyperthermia and MRI imaging in cancer. Aptamer conjugated magnetic nanoparticles controlled by an externally applied 3-D rotational magnetic field have been developed as a nanosurgical approach for the removal of cancerous cells selectively from the interior of an organ or tissue without any collateral damage (Nair et al. 2010). This system could be upgraded for the selective removal of complex cancers from diverse tissues by incorporating various target specific ligands on magnetic nanoparticles.

Biomimetic Nanoparticles Targeted to Tumors

Nanoparticle-based diagnostics and therapeutics hold great promise because multiple functions can be built into the particles. One such function is an ability to home to specific sites in the body, e.g., biomimetic particles. One homing system is based on a peptide that recognizes clotted plasma proteins and selectively homes to tumors, where it binds to vessel walls and tumor stroma. Iron oxide nanoparticles and liposomes coated with this tumor-homing peptide accumulate in tumor vessels, where they induce additional local clotting, thereby, producing new binding sites for more particles. The system mimics platelets, which also circulate freely but accumulate at a diseased site and amplify their own accumulation at that site. The self-amplifying homing is a novel function for nanoparticles. The clotting-based amplification greatly enhances tumor imaging, and the addition of a drug carrier function to the particles is envisioned.

Dendrimer Nanoparticles for Targeting and Imaging Tumors

Dendrimer nanoparticles have been used to entrap metal nanoparticles, a combination that could serve as a potent imaging and thermal therapy agent for tumors if it were not for associated toxicity issues. To eliminate the toxicity associated with dendrimer-metal nanoparticle combinations, methods have been developed for modifying the surface of dendrimers laden with gold nanoparticles. This chemical treatment greatly reduces the toxicity of the hybrid nanoparticle without changing its size. Construction of novel dendrimers with biocompatible components, and the surface modification of commercially available dendrimers by PEGylation, acetylation, glycosylation, and amino acid functionalization have been proposed to solve the safety problem of dendrimer-based nanotherapeutics (Cheng et al. 2011). There are several opportunities and challenges for the development of dendrimer-based nanoplatforms for targeted cancer diagnosis and therapy.

Gold Nanoparticle Plus Bombesin for Imaging and Therapy of Cancer

Bombesin (BBN) peptides have demonstrated high affinity toward gastrin-releasing peptide (GRP) receptors in vivo that are overexpressed in prostate, breast, and small-cell lung carcinoma. In vivo studies using gold nanoparticles (AuNPs)-BBN and its radiolabeled surrogate ¹⁹⁸AuNP-BBN constructs are GRP-receptor-specific showing accumulation with high selectivity in GRP-receptor-rich prostate tumors implanted

in severe combined immunodeficient mice (Chanda et al. 2010). The intraperitonel mode of delivery was found to be efficient as AuNP-BBN conjugates showed reduced RES organ uptake with concomitant increase in uptake at tumor targets. The selective uptake of this new generation of GRP-receptor-specific AuNP-BBN peptide analogs have clinical potential in molecular imaging using CT techniques as the contrast numbers in prostate tumor sites are severalfold higher as compared to the pretreatment group. They also provide synergistic advantages by combining molecular imaging with therapy of cancer.

Gold Nanorods for Diagnosis Plus Photothermal Therapy of Cancer

Photothermal therapy is based on the enhancement of electromagnetic radiation by noble metal nanoparticles due to strong electric fields at the surface. The nanoparticles also absorb laser light more easily, so that the coated malignant cells only require half the laser energy to be killed compared to the benign cells. This makes it relatively easy to ensure that only the malignant cells are being destroyed. These unique properties provide the potential of designing novel optically active reagents for simultaneous molecular imaging and photothermal cancer therapy. Gold nanorods with suitable aspect ratios (length divided by width) can absorb and scatter strongly in the NIR region (650–900 nm). Changing the spheres into rods lowers the frequency to which the nanoparticles respond from the visible light spectrum used by the nanospheres to the NIR spectrum. Since these lasers can penetrate deeper under the skin than lasers in the visible spectrum, they can reach tumors that are inaccessible to visible lasers.

In vitro studies have demonstrated that gold nanorods are novel contrast agents for both molecular imaging and photothermal cancer therapy. Nanorods are synthesized and conjugated to anti-epidermal growth factor receptor (anti-EGFR) monoclonal antibodies (MAbs) and incubated in cancer cell cultures. The anti-EGFR antibody-conjugated nanorods bind specifically to the surface of the malignant-type cells with a much higher affinity due to the overexpressed EGFR on the cytoplasmic membrane of the malignant cells. As the strongly scattered red light from gold nanorods in dark field is observed througha laboratory microscope, the malignant cells are clearly visualized and differentiated from the nonmalignant cells. After exposure to continuous red laser at 800 nm, malignant cells require about half the laser energy to be photothermally destroyed than the nonmalignant cells. Thus, both efficient cancer cell diagnostics and selective photothermal therapy are realized at the same time.

Gold Nanotubes for Diagnosis Plus Photothermal Therapy of Cancer

High recurrence rates of tumors after surgical removal remain a formidable challenge in cancer therapy. Chemo- or radiotherapy is often given following surgery to prevent this, but these treatments cause serious side effects. Gold nanotubes (AuNTs) have the potential to enhance the efficacy of these conventional treatments by integrating diagnosis and therapy in one single system, e.g. by high-resolution imaging, as cancer drug delivery vehicles, and as therapeutics for destroying cancer cells (Ye et al. 2015).

A length-controlled synthesis was developed to fabricate AuNTs with well-defined shape, i.e. inner void and open ends, high crystallinity, and tunable NIR surface plasmon resonance. By controlling the length, the researchers could produce AuNTs with the right dimensions to absorb near infrared light. By adjusting the brightness of the laser pulse, the researchers control control whether the AuNTs were in cancer-destruction mode, or ready to image tumors. A new type of imaging technique, multispectral optoacoustic tomography, was used to visualize the AuNTs in mice, in which AuNTs had been injected intravenously. Polysodium 4-styrenesulfonate (PSS)-coated AuNTs were shown to achieve the following ideal attributes for development as effective and safe in vivo imaging nanoprobes, photothermal conversion agents, and drug delivery vehicles:

- Cellular uptake by colorectal cancer cells and macrophage cells.
- · Ablation of cancer cells using single wavelength pulse laser irradiation.
- Accumulate at the tumor site and generate excellent in vivo photoacoustic signals.
- AuNTs were excreted from the body by hepatobiliary clearance within 72 h post-intravenous injection and therefore are unlikely to cause toxic effects.

Magnetic Nanoparticles for Imaging as Well as Therapy of Cancer

Several multifunctional nanoparticles are being developing s for simultaneous imaging and therapeutic applications in cancer. Tumor-targeting dendrimers can contain an imaging as well as a delivery agent for drugs, genetic materials. A dendrimer linked to a fluorescent imaging agent and paclitaxel can identify tumor cells and kill them simultaneously.

In ovarian cancer, metastasis occurs when cells slough off the primary tumor and float free in the abdominal cavity. If one could use the magnetic nanoparticles to trap drifting cancer cells and pull them out of the abdominal fluid, it may be possible to predict and perhaps prevent metastasis. With this aim, magnetic cobalt spinel ferrite nanoparticles, which have cobalt-spiked magnetite at their core, were coated with biocompatible polygalacturonic acid and functionalized with ligands specific for targeting expressed EphA2 receptors on ovarian cancer cells (Scarberry et al. 2008). By using such magnetic nanoparticle-peptide conjugates, targeting and extraction of malignant cells were achieved with a magnetic field. The particles, which are just 10 nm or less in diameter, are not magnetic most of the time, but when a magnet is present, they become strongly attracted to it. Targeting ovarian cancer cells with receptor specific peptide-modified magnetic nanoparticles resulted in cell capture from a flow stream in vitro and from the peritoneal cavity of mice in vivo. Successful removal of metastatic cancer cells from the abdominal cavity and from circulation using magnetic nanoparticle conjugates indicate the feasibility of a dialysis-like treatment and may improve long-term survival rates of ovarian cancer patients. This approach can be applied for treating other cancers, such as leukemia, once the receptors on malignant cells are identified and the efficacy of targeting ligands is established. This technique will provide a way to test for and even treat metastatic ovarian cancer. Although the nanoparticles were tested inside the bodies of mice, it is possible to construct an external device that would remove a patient's abdominal fluid, magnetically filter out the cancer cells, and then return the fluid to the body. After surgery for removal of the primary tumor, a patient would undergo such a treatment to remove any residual cancer cells. The researchers are currently developing such a filter and testing it on abdominal fluid from human ovarian cancer patients.

Micelles for Targeted Drug Delivery and PET Imaging in Cancer

H40-DOX-cRGD, a multifunctional unimolecular micelle made of a hyperbranched amphiphilic block copolymer with attached doxorubicin (DOX), was tested for targeted anticancer drug delivery and PET imaging in tumor-bearing mice (Xiao et al. 2012). A uniform size distribution and pH-sensitive drug release behavior was observed. There was a much higher cellular uptake in U87MG human glioblastoma cells due to integrin $\alpha\nu\beta3$ -mediated endocytosis than non-targeted unimolecular micelles (i.e., H40-DOX), thereby leading to a significantly higher cytotoxicity. Thus, unimolecular micelles formed by hyperbranched amphiphilic block copolymers integrate passive and active tumor-targeting abilities with pH-controlled drug release. Simultaneous PET imaging for diagnosis provides the basis for personalized cancer therapy.

Nanobialys for Combining MRI with Delivery of Anticancer Agents

Although gadolinium has been the dominant paramagnetic metal for MRI contrast, the recent association of this lanthanide with nephrogenic systemic fibrosis, an untreatable disease, has spawned renewed interest in alternative metals for molecular MRI. Manganese was one of the first examples of a paramagnetic contrast material studied in cardiac and hepatic MRI because of efficient site-specific MR T1-weighted molecular imaging. Similar to Ca2+ and unlike the lanthanides, manganese is a natural cellular constituent, and often a cofactor for enzymes and receptors. Mangafodipir trisodium, a manganese blood pool agent, has been approved as a hepatocyte-specific contrast agent with transient side-effects due to de-chelation of manganese from the linear chelate. A self-assembled, manganese(III)-labeled nanobialys MRI nanoparticle, has been developed for combined diagnosis and delivery of a chemotherapeutic agent (Pan et al. 2008). The 'bialy' shape affords increased stability. Nanobialys nanoparticles have been characterized for targeted detection of fibrin, a major biochemical feature of thrombus. A complementary ability of nanobialys to incorporate anticancer compounds with greater than 98%

efficiency and to retain more than 80% of these drugs after infinite sink dissolution, point to the potential of this platform technology to combine a therapeutic agent with a diagnostic agent.

Nanoparticles, MRI and Thermal Ablation of Tumors

Nanostructures with surface-bound ligands can be used for the targeted delivery and ablation of colorectal cancer (CRC), the third most common malignancy and the second most common cause of cancer-related mortality in the US. Normal colonic epithelial cells as well as primary CRC and metastatic tumors all express a unique surface-bound guanylyl cyclase C (GCC), which binds the bacterial heat-stable enterotoxin (ST) -a peptide. This makes GCC a potential target for metastatic tumor ablation using ST-bound nanoparticles in combination with thermal ablation with near-infrared or radiofrequency energy absorption. Furthermore, the incorporation of iron or iron oxide nanoparticles into such structures would provide advantages for MRI.

Gold nanoshell-based, targeted, multimodal contrast agents in the near infrared (NIR) are fabricated and utilized as a diagnostic and therapeutic probe for MRI, fluorescence optical imaging, and photothermal cancer therapy of breast carcinoma cells in vitro (Bardhan et al. 2009). This may enable diagnosis as well as treatment of cancer during one hospital visit.

In future, it may be possible for a patient to be screened for breast cancer using MRI techniques with engineered enhanced ferrites as the MRI contrast agent. Enhanced ferrites are a class of ferrites that are specially engineered to have enhanced magnetic or electrical properties and are created by core-shell morphology. Magnetic nanoparticles are coupled to the radio frequency of the MRI, which converts the radio frequency into heat. If a tumor is detected, the physician could increase the power to the MRI coils and localized heating would destroy the tumor without damage to the surrounding healthy cells. The only hinderance to the development of enhanced ferrites for 100 megahertz applications is a lack of understanding of the growth mechanisms and synthesis-property relationships of these nanoparticles. By studying the mechanism for the growth of the enhanced ferrites, it will be possible to create shells that help protect the metallic core from oxidation in biologically capable media.

pHLIP Nanotechnology for Detection and Targeted Therapy of Cancer

The pH-selective insertion and folding of a membrane peptide, pHLIP (pH low insertion peptide), can be used to target acidic tissue in vivo, including acidic foci in tumors. pHLIP nanotechnology is a promising approach for mapping areas of elevated acidity in the body. The peptide has three states: soluble in water, bound to the surface of a membrane, and inserted across the membrane. At physiological pH, the equilibrium is toward water, which explains its low affinity for cells in healthy tissue; at acidic pH, the equilibrium shifts toward membrane insertion and tissue

accumulation. This peptide acts like a nanosyringe to deliver tags or therapy to cells. Tumors can be detected by labeling pHLIP peptide with Cy5.5 and imaging by use of NIR fluorescence with wavelengths in the range of 700–900 nm. In a mouse breast adenocarcinoma model, fluorescently labeled pHLIP detects solid acidic tumors with high accuracy and accumulates in them even at a very early stage of tumor development (Andreev et al. 2007). The fluorescence signal is stable and is approximately five times higher in tumors than in healthy counterpart tissue. Tumor targeting is based on the finding that most tumors, even very small ones, are acidic because of the way they grow, known as the Warburg effect. Tumors may be treated by attaching and delivering anticancer agents with pHLIP.

QD Conjugates Combine Cancer Imaging, Therapy and Sensing

The specificity and sensitivity of a QD-aptamer-doxorubicin (QD-Apt-Dox) conjugate as a targeted cancer imaging, therapy, and sensing system has been shown in vitro. By functionalizing the surface of fluorescent QD with a RNA aptamer, which recognizes the extracellular domain of the prostate specific membrane antigen (PSMA), the system is capable of differential uptake and imaging of prostate cancer cells that express the PSMA. The intercalation of Dox, an anticancer drug with fluorescent properties, in the double-stranded stem of the aptamer results in a targeted conjugate with reversible self-quenching properties based on a Bi-FRET mechanism. A donoracceptor model FRET between QD and Dox and a donor-quencher model FRET between Dox and aptamer result when Dox is intercalated within the aptamer. This simple multifunctional nanoparticle system can deliver Dox to the targeted prostate cancer cells and sense the delivery of Dox by activating the fluorescence of QD, which concurrently images the cancer cells.

Silica Nanoparticles for Combining Diagnosis with Cancer Therapy

Hybrid mesoporous silica nanoparticles (hMSNs) can combine therapeutic and diagnostic functions to create smart nanocarriers that use diagnostic information to control therapeutic action (Baleizão and Farinha 2015). The benefits of hMSNs in drug delivery applications stem from their large surface area and pore volume. These properties enable the materials to accommodate large amounts of payload molecules, protect them from premature degradation, and promote controlled and fast release (Xu et al. 2013).

Squalene-Based Nanocomposites for Tumor Imaging and Therapy

Nanocomposites, constructed of magnetite nanocrystals into NPs by self-assembling molecules of the squalenoyl gemcitabine (SQgem) bioconjugated, are characterized by an unusually high drug loading, a significant magnetic susceptibility, and a low burst release. When injected into a subcutaneous mice tumor model, these

magnetite/SQgem NPs were magnetically guided, and displayed considerably greater anticancer activity than other anticancer treatments including nonmagnetically guided magnetite/SQgem NPs (Arias et al. 2011). The histology and immunohistochemistry investigation of the tumor biopsies clearly evidenced the therapeutic superiority of the magnetically guided nanocomposites, while Prussian blue staining confirmed their accumulation at the tumor periphery. The superior therapeutic activity and enhanced tumor accumulation has been successfully visualized using T2-weighted MRI imaging. This concept was further enlarged by (i) the design of squalene-based NPs containing the T1 Gd3+ contrast agent instead of magnetite and (ii) the application to other anticancer squalenoyls, such as, cisplatin, doxorubicin, and paclitaxel. This nanotechnology platform is expected to have important applications in imaging-guided cancer therapy.

Radiolabeled Carbon Nanotubes for Tumor Imaging and Targeting

SWCNTs with covalently attached multiple copies of tumor-specific MAbs, radiometal-ion chelates, and fluorescent probes can target lymphomas and deliver both imaging and therapeutic molecules to these tumors (McDevitt et al. 2007). Each nanotube, which contained approximately six antibody molecules and 114 radioactive atoms, proved to be stable in human plasma for at least 96 h and could bind to targeted tumor cells. Most importantly, the chemical linkages binding the radioactive element indium-111 was completely stable in human plasma for the entire 4-day experiment. Tests using a mouse model of human lymphoma showed that the nanotube construct successfully targeted tumors while avoiding healthy cells. The ability to specifically target tumor with prototype-radiolabeled or fluorescent-labeled, antibody-appended SWCNT constructs was encouraging and suggested further investigation of these as diagnostic combined with drug delivery for cancer.

Ultrasonic Tumor imaging and Targeted Chemotherapy by Nanobubbles

Ultrasound has been used in the past in combination with microbubbles, micron-sized spherical gas-filled structures stabilized by a shell, which amplifies the biophysical effects of the ultrasound. Nanobubbles, defined nanometer size bubbles, were designed to obtain more efficient drug delivery systems. Their small sizes allow extravasation from blood vessels into surrounding tissues and ultrasound-targeted site-specific release with minimal invasiveness (Cavalli et al. 2016). Additionally, nanobubbles might improved stability of the drug and longer residence time in systemic circulation.

Drug delivery in polymeric micelles combined with tumor irradiation by ultrasound results in effective drug targeting, but this technique requires prior tumor imaging. A targeted drug delivery method uses ultrasound to image tumors, while also releasing the drug from nanobubbles into the tumor (Rapoport et al. 2007). Mixtures of drug-loaded polymeric micelles and perfluoropentane (PFP) nanobubbles stabilized

by the same biodegradable block copolymer were prepared. Size distribution of nanoparticles was measured by dynamic light scattering. Cavitation activity (oscillation, growth, and collapse of microbubbles) under ultrasound was assessed based on the changes in micelle/nanobubble volume ratios. The effect of the nanobubbles on the ultrasound-mediated cellular uptake of doxorubicin (Dox) in MDA MB231 breast tumors in vitro and in vivo (in mice bearing xenograft tumors) was determined by flow cytometry. Phase state and nanoparticle sizes were sensitive to the copolymer/perfluorocarbon volume ratio. At physiologic temperatures, nanodroplets converted into nanobubbles. Doxorubicin was localized in the nanobubble walls formed by the block copolymer. Upon intravenous injection into mice, Dox-loaded micelles and nanobubbles extravasated selectively into the tumor interstitium, where the nanobubbles coalesced to produce microbubbles. When exposed to ultrasound, the bubbles generated echoes, which made it possible to image the tumor. The sound energy from the ultrasound popped the bubbles, releasing Dox, which enhanced intracellular uptake by tumor cells in vitro to a statistically significant extent relative to that observed with unsonicated nanobubbles and unsonicated micelles and resulted in tumor regression in the mouse model. In conclusion, multifunctional nanoparticles that are tumor-targeted drug carriers, long-lasting ultrasound contrast agents, and enhancers of ultrasound-mediated drug delivery have been developed and deserve further exploration as cancer therapeutics.

Role of Nanobiotechnology in Cancer Immunology

It is now recognized that many cancer patients have tumor-specific T cell and antibody responses. Most antitumor responses are directed against non-mutated selfantigens. Cellular immunotherapy consists of giving the patient cells that stimulate antitumor activity in the patient (tumor and dendritic cell vaccines) or that have intrinsic antitumor activity (autologous and allogeneic lymphocytes). The aim is to harness potent immunological weapons to destroy cancer cells. Immunotherapy of cancer is an approach that is more specific and less toxic than chemotherapy and radiation (Jain 2014). Tumors may induce tolerance, and it may not suffice to only activate the immune system against a tumor associated antigen, but the elimination of immune tolerance is of equal importance (Grabbe et al. 2016). Nanobiotechnology plays an important role in cancer immunology.

Cell types such as dendritic cells (DCs), regulatory T cells (Tregs), macrophages and myeloid-derived suppressor cells (MDSC) that generate an immunosuppressive tumor microenvironment and promote tumor growth as well as metastases are a major barrier for cancer immune therapy. Most of these cell types except Treg derive from myeloid bone marrow progenitors that differentiate into the different suppressor cell lineages, mainly driven by the cancer cells themselves.

DCs are derived from bone marrow progenitors and circulate in the blood as immature precursors prior to migration into peripheral tissues. Within different tissues, DCs differentiate and become active in the taking up and processing of antigens, and their subsequent presentation on the cell surface linked to major histocompatibility (MHC) molecules. Upon appropriate stimulation, DCs undergo further maturation and migrate to secondary lymphoid tissues where they present antigens to T cells and induce an immune response. DCs have the capacity to prime tumor-specific T cell responses and are potentially effective vaccines for immunotherapy of cancer. Nanoparticle-based antigen delivery systems have been identified as an innovative strategy to improve the efficacy of subunit vaccines targeted to DCs. Among them, self-assembled micellar nanoparticles have emerged as promising candidates for vaccine delivery (Trimaille and Verrier 2015). A review of various nanoparticle-based adjuvants for anticancer vaccines has pointed out the need for further understanding of differences of uptake and intracellular for every nanocarrier how and how this influences the success for its use as a nanocarrier for vaccination (Tonigold and Mailänder 2016).

The maintenance of immune homeostasis requires Tregs. Given their intrinsic selfreactivity, Tregs must stably maintain a suppressive phenotype to avoid autoimmunity. Treg cell-mediated immune suppression is a significant barrier to effective anticancer immune responses. Aim of the current approaches is to eliminate Tregs, and thereby increase anticancer immunity. However, DC-based immunotherapies have limited success in clinical trials due to suppression of tumor antigen-specific T cell responses by Treg cells. Nanoparticles are expected to improve immunotherapy by enabling targeted antigen loading to activate DC in vivo and transient circumvention of Treg cell activity, but Treg cells represent a very difficult target because they lack cell-specific surface molecules for selective particle targeting (Jonuleit et al. 2016).

Macrophage-targeting or depleting chemotherapies are limited by off-target side effects, general toxicity or drug resistance. Targeted therapies using nanoparticle mediated delivery of drugs or small molecules has potential for increased specificity, higher efficacy and fewer side effects (Tuettenberg et al. 2016). Such delivery can improve both organ- and cell-specific targeting.

Nanorobotics for Management of Cancer

It is within the realm of possibility to use molecular tools to design a miniature device, such as a nanobot that can be introduced in the body, can locate and identify cancer cells, and finally destroy them. The device would have a biosensor to identify cancer cells and a supply of anticancer substance that could be released on encountering cancer cells. A small computer could be incorporated to program and integrate the combination of diagnosis and therapy and provide the possibility to monitor the in vivo activities by an external device. Since there is no universal anticancer agent, the computer program could match the type of cancer to the most appropriate agent. Such a device could be implanted as a prophylactic measure in persons who do not any obvious manifestations of cancer. It would circulate freely and could detect and treat cancer at the earliest stage. Such a device could be reprogrammed through remote control and enable change of strategy if the lesion encountered is other than cancer.

Bacterial Nanorobots for Targeting Cancer

Flagellated nanomotors combined with the nanometersized magnetosomes of a single magnetotactic bacterium (MTB) can be used as an effective integrated propulsion and steering system for devices such as nanorobots designed for targeting locations only accessible through the smallest capillaries in humans while being visible for tracking and monitoring purposes using modern medical imaging modalities such as MRI (Martel et al. 2009). Through directional and magnetic field intensities, the displacement speeds, directions, and behaviors of swarms of these bacterial actuators can be controlled from an external computer. Such a device can be used for diagnosis as well as therapy of cancer.

DNA Robots for Targeting Cancer

DNA nanotechnology is widely investigated for its potential to deliver drugs and molecular signals to cells in the body because DNA is a biocompatible and biodegradable material. However, opinions differ as about the best nanorobot design, i.e. the ideal structure to load, transport, and deliver molecules. Various designs include a spider-like robot that moves along a chemical track, a nanofactory with mobile robotic walkers and molecular forklifts, and DNA tweezers that open and close to grasp and release molecules.

An autonomous DNA nanorobot has been described that can transpor molecular payloads to cells, sense cell surface inputs for conditional, trigger activation, and reconfigure its structure for payload delivery (Douglas et al. 2012). The nanorobot, constructed using a computer-aided design tool called DNA origami, is a hexagonal barrel, 35 nm in diameter and opens like a clam shell. The device can be loaded with a variety of materials and is controlled by an aptamer-encoded logic gate, enabling it to respond to a wide array of cues that have demonstrated their efficacy in selective regulation of nanorobot function. This barrel-shaped DNA nanorobot seeks out cancer cells and delivers self-destruct instructions. It can successfully deliver antibodies fragments to surfaces of cancer cells to kill them and bacterial proteins to activate T cells.

Fullerenes for Protection Against Chemotherapy-Induced Cardiotoxicity

Therapeutic use doxorubicin as an anticancer drug is limited due to its cardiotoxicity. Generation of free radicals plays an important role in the mechanism of doxorubicininduced cardiotoxicity. There is significant evidence indicating that mitochondria are the principal targets in this pathological process. Efficacy of fullerenol ($C_{60}OH_{24}$) in preventing single, high-dose doxorubicin-induced cardiotoxicity has been investigated in rats with malignant neoplasm (Injac et al. 2008). Study was performed on adult female Sprague Dawley rats with chemically induced mammary carcinomas. The animals were sacrificed 2 days after the application of doxorubicin and/or fullerenol, and the serum activities of cardiac enzymes were determined. The results obtained showed that the administration of a single dose of 8 mg/kg in all treated groups induces statistically significant cardiotoxicity. There were significant changes in the enzymes lactate dehydrogenase and creatine kinase and increase in level of tissue malondialdehyde (MDA), a product of lipid peroxidation, after intraperitoneal administration of doxorubicin. The results revealed that doxorubicin induced oxidative damage and that the fullerenol antioxidant effect caused significant changes in the levels of biomarker MDA in the heart. Thus, fullerenol may have an important role as for cardioprotection in doxorubicin-treated individuals.

Concluding Remarks and Future of Nanooncology

The rationale for using nanobiotechnology in oncology is that nanoparticles have optical, magnetic, or structural properties that are not available from larger molecules or bulk solids. When linked with tumor targeting ligands such as MAbs, peptides, or small molecules, nanoparticles can be used to target tumor antigens (biomarkers) as well as tumor vasculatures with high affinity and specificity. In the size range of 5–100 nm diameter, nanoparticles have large surface areas and functional groups for conjugating to multiple diagnostic and therapeutic anticancer agents. Recent advances have led to bioaffinity nanoparticle probes for molecular and cellular imaging, targeted nanoparticle drugs for cancer therapy, and integrated nanodevices for early cancer detection and screening. These developments have provided opportunities for personalized oncology in which biomarkers are used to diagnose and treat cancer based on the molecular profiles of individual patients.

Nanoparticles have shown promise for incorporating multiple functions including diagnosis and therapy of cancer. Most of the work done in this area is still experimental and some challenges need to resolved before clinical applications. These include the following:

- Preventing capture/removal by the reticuloendothelial system.
- Difficulties in selective targeting as well as penetration of tumor by systemic administration of anticancer nanostructures, which requires identification of receptors unique to a specific cancer.
- · Investigation of long-term fate and toxicity concerns of nanoparticles.

Efforts are being made to use nanostructures to develop anticancer treatment strategies based on various mitochondrial targets that play vital roles in cancer development and progression. Cancer mitochondria-targeted multifunctional compounds have been identified that could provide an alternative strategy for the development of novel solutions for cancer diagnosis and therapy (Zhang et al. 2011).

References

- Ahmed M, Pan DW, Davis ME. Lack of in vivo antibody dependent cellular cytotoxicity with antibody containing gold nanoparticles. Bioconjug Chem. 2015;26:812–6.
- Alibolandi M, Ramezani M, Abnous K, et al. In vitro and in vivo evaluation of therapy targeting epithelial-cell adhesion-molecule aptamers for non-small cell lung cancer. J Control Release. 2015;209:88–100.
- Al-Jamal KT, Al-Jamal WT, Akerman S, et al. Systemic antiangiogenic activity of cationic poly-L-lysine dendrimer delays tumor growth. Proc Natl Acad Sci U S A. 2010;107:3966–71.
- Andreev OA, Dupuy AD, Segala M, et al. Mechanism and uses of a membrane peptide that targets tumors and other acidic tissues in vivo. Proc Natl Acad Sci U S A. 2007;104:7893–8.
- Arias JL, Reddy LH, Othman M, et al. Squalene based nanocomposites: a new platform for the design of multifunctional pharmaceutical theragnostics. ACS Nano. 2011;5:1513–21.
- Arora HC, Jensen MP, Yuan Y, et al. Nanocarriers enhance doxorubicin uptake in drug-resistant ovarian cancer cells. Cancer Res. 2012;72:769–78.
- Arsula Rose P, Praseetha PK, Bhagat M, et al. Drug embedded PVP coated magnetic nanoparticles for targeted killing of breast cancer cells. TRCT. 2013;12:463–72.
- Arvizo RR, Rana S, Miranda OR, et al. Mechanism of anti-angiogenic property of gold nanoparticles: role of nanoparticle size and surface charge. Nanomedicine. 2011;7:580–7.
- Arvizo RR, Saha S, Wang E, et al. Inhibition of tumor growth and metastasis by a self-therapeutic nanoparticle. Proc Natl Acad Sci U S A. 2013;110:6700–5.
- Bailey VJ, Easwaran H, Zhang Y, et al. MS-qFRET: a quantum dot-based method for analysis of DNA methylation. Genome Res. 2009;19:1455–61.
- Bajaj A, Miranda OR, Kim IB, et al. Detection and differentiation of normal, cancerous, and metastatic cells using nanoparticle-polymer sensor arrays. Proc Natl Acad Sci U S A. 2009;106:10912–6.
- Baleizão C, Farinha JP. Hybrid smart mesoporous silica nanoparticles for theranostics. Nanomedicine (Lond). 2015;10:2311–4.
- Ballou B, Ernst LA, Andreko S, et al. Sentinel lymph node imaging using quantum dots in mouse tumor models. Bioconjug Chem. 2007;18:389–96.
- Bardhan R, Chen W, Perez-Torres C, et al. Nanoshells with targeted simultaneous enhancement of magnetic and optical imaging and photothermal therapeutic response. Adv Funct Mater. 2009;19:3901–9.
- Basu S, Harfouche R, Soni S, et al. Nanoparticle-mediated targeting of MAPK signaling predisposes tumor to chemotherapy. Proc Natl Acad Sci U S A. 2009;106:7957–61.
- Battah S, Balaratnam S, Casas A, et al. Macromolecular delivery of 5-aminolaevulinic acid for photodynamic therapy using dendrimer conjugates. Mol Cancer Ther. 2007;6:876–85.
- Benezra M, Penate-Medina O, Zanzonico PB, et al. Multimodal silica nanoparticles are effective cancer-targeted probes in a model of human melanoma. J Clin Invest. 2011;121:2768–80.
- Bertin PA, Gibbs JM, Shen CK, et al. Multifunctional polymeric nanoparticles from diverse bioactive agents. J Am Chem Soc. 2006;128:4168–9.
- Bertrand N, Wu J, Xu X, Kamaly N, Farokhzad OC. Cancer nanotechnology: the impact of passive and active targeting in the era of modern cancer biology. Adv Drug Deliv Rev. 2014;66:2–25.
- Bisht S, Feldmann G, Soni S, et al. Polymeric nanoparticle-encapsulated curcumin (nanocurcumin): a novel strategy for human cancer therapy. J Nanobiotechnology. 2007;5:3.
- Burke CW, Alexander E, Timbie K, et al. Ultrasound-activated agents comprised of 5FU-bearing nanoparticles bonded to microbubbles inhibit solid tumor growth and improve survival. Mol Ther. 2014;22:321–8.
- Cadete A, Alonso MJ. Targeting cancer with hyaluronic acid-based nanocarriers: recent advances and translational perspectives. Nanomedicine (Lond). 2016;11:2341–57.
- Cao L, Liang Y, Zhao F, et al. Chelerythrine and Fe3O4 loaded multi-walled carbon nanotubes for targeted cancer therapy. J Biomed Nanotechnol. 2016;12:1312–22.
- Cao Z, Ma Y, Yue X, et al. Stabilized liposomal nanohybrid cerasomes for drug delivery applications. Chem Commun (Camb). 2010;46:5265–7.

- Cavalli R, Soster M, Argenziano M. Nanobubbles: a promising efficient tool for therapeutic delivery. Ther Deliv. 2016;7:117–38.
- Chakravarty P, Marches R, Zimmerman NS, et al. Thermal ablation of tumor cells with antibodyfunctionalized single-walled carbon nanotubes. Proc Natl Acad Sci U S A. 2008;105:8697–702.
- Chanda N, Kattumuri V, Shukla R, et al. Bombesin functionalized gold nanoparticles show in vitro and in vivo cancer receptor specificity. Proc Natl Acad Sci U S A. 2010;107:8760–5.
- Cheng Y, Zhao L, Li Y, Xu T. Design of biocompatible dendrimers for cancer diagnosis and therapy: current status and future perspectives. Chem Soc Rev. 2011;40:2673–703.
- Choi CH, Alabi CA, Webster P, Davis ME. Mechanism of active targeting in solid tumors with transferrin-containing gold nanoparticles. Proc Natl Acad Sci U S A. 2010a;107:1235–40.
- Choi KY, Chung H, Min KH, et al. Self-assembled hyaluronic acid nanoparticles for active tumor targeting. Biomaterials. 2010b;31:106–14.
- Chouhan R, Bajpai AK. Real time in vitro studies of doxorubicin release from PHEMA nanoparticles. J Nanobiotechnol. 2009;7:5.
- Clark AJ, Wileya DT, Zuckerman JE, et al. CRLX101 nanoparticles localize in human tumors and not in adjacent, nonneoplastic tissue after intravenous dosing. Proc Natl Acad Sci U S A. 2016;113:3850–4.
- Cohen SM, Mukerji R, Cai S, et al. Subcutaneous delivery of nanoconjugated doxorubicin and cisplatin for locally advanced breast cancer demonstrates improved efficacy and decreased toxicity at lower doses than standard systemic combination therapy in vivo. Am J Surg. 2011;202:646–53.
- Denardo SJ, Denardo GL, Natarajan A, et al. Thermal dosimetry predictive of efficacy of 111In-ChL6 nanoparticle AMF-induced thermoablative therapy for human breast cancer in mice. J Nucl Med. 2007;48:437–44.
- Douglas SM, Bachelet I, Church GM. A logic-gated nanorobot for targeted transport of molecular payloads. Science. 2012;335:831–4.
- Fan L, Lou D, Zhang Y, Gu N. Rituximab-Au nanoprobes for simultaneous dark-field imaging and DAB staining of CD20 over-expressed on Raji cells. Analyst. 2014;139:5660–3.
- Fan Z, Sun L, Huang Y, et al. Bioinspired fluorescent dipeptide nanoparticles for targeted cancer cell imaging and real-time monitoring of drug release. Nat Nanotechnol. 2016;11:388–94.
- Fatima MT, Chanchal A, Yavvari PS, et al. Cell permeating nano-complexes of amphiphilic polyelectrolytes enhance solubility, stability, and anti-cancer efficacy of curcumin. Biomacromolecules. 2016;17:2375–83.
- Franzen S. A comparison of peptide and folate receptor targeting of cancer cells: from single agent to nanoparticle. Expert Opin Drug Deliv. 2011;8:281–98.
- Galanzha EI, Shashkov EV, Kelly T, et al. In vivo magnetic enrichment and multiplex photoacoustic detection of circulating tumour cells. Nat Nanotechnol. 2009;4:855–60.
- Gao D, Xu H, Philbert MA, et al. Ultrafine hydrogel nanoparticles: synthetic approach and therapeutic application in living cells. Angew Chem Int Ed Engl. 2007;46:2224–7.
- Ghaz-Jahanian MA, Abbaspour-Aghdam F, Anarjan N, et al. Application of chitosan-based nanocarriers in tumor-targeted drug delivery. Mol Biotechnol. 2015;57:201–18.
- Ghosh D, Bagley AF, Deep NYJ, et al. Noninvasive imaging and surgical guidance of submillimeter tumors using targeted M13-stabilized single-walled carbon nanotubes. Proc Natl Acad Sci U S A. 2014;111:13948–53.
- Gibson JD, Khanal B, Zubarev E. Paclitaxel-functionalized gold nanoparticles. J Am Chem Soc. 2007;129:11653–61.
- Gordon EM, Levy JP, Reed RA, et al. Targeting metastatic cancer from the inside: a new generation of targeted gene delivery vectors enables personalized cancer vaccination in situ. Int J Oncol. 2008;33:665–75.
- Gou M, Men K, Shi H, et al. Curcumin-loaded biodegradable polymeric micelles for colon cancer therapy in vitro and in vivo. Nanoscale. 2011;3:1558–67.
- Grabbe S, Landfester K, Schuppan D, et al. Nanoparticles and the immune system: challenges and opportunities. Nanomedicine. 2016;11:2723–34.

- Gradishar WJ, Tjulandin S, Davidson N, et al. Superior efficacy of albumin-bound paclitaxel, ABI-007, compared with polyethylated castor oil-based paclitaxel in women with metastatic breast cancer: results of a Phase III trial. J Clin Oncol. 2005;23:7794–803.
- Guarneri V, Dieci MV, Conte PF. Enhancing intracellular taxane delivery: current role and perspectives of nanoparticle albumin-bound paclitaxel in the treatment of advanced breast cancer. Expert Opin Pharmacother. 2012;13:395–406.
- Guo F, Yao C, Li C, et al. In vivo evidences of nanosecond pulsed electric fields for melanoma malignancy treatment on tumor-bearing BALB/c nude mice. Technol Cancer Res Treat. 2014;13:337–44.
- Homan KA, Souza M, Truby R, et al. Silver nanoplate contrast agents for in vivo molecular photoacoustic imaging. ACS Nano. 2012;6:641–50.
- Hou S, Zhao H, Zhao L, et al. Capture and stimulated release of circulating tumor cells on polymer grafted silicon nanostructures. Adv Mater. 2013;25:1547–51.
- Huang X, Ren J. Gold nanoparticles based chemiluminescent resonance energy transfer for immunoassay of alpha fetoprotein cancer marker. Anal Chim Acta. 2011;686:115–20.
- Huff TB, Tong L, Zhao Y, et al. Hyperthermic effects of gold nanorods on tumor cells. Nanomedicine. 2007;2:125–32.
- Huschka R, Neumann O, Barhoumi A, Halas NJ. Visualizing light-triggered release of molecules inside living cells. Photodynamic therapy of cancer using nanoparticles. Nano Lett. 2010;10:4117–22.
- Injac R, Perse M, Boskovic M, et al. Cardioprotective effects of fullerenol C60(Oh)24 on a single dose doxorubicin-induced cardiotoxicity in rats with malignant neoplasm. Technol Cancer Res Treat. 2008;7:15–26.
- Ischakov R, Adler-Abramovich L, Buzhansky L, et al. Peptide-based hydrogel nanoparticles as effective drug delivery agents. Bioorg Med Chem. 2013;21:3517–22.
- Jain KK. Applications of biotechnology in oncology. New York: Springer; 2014.
- Jain KK. Recent advances in nanooncology. TCRT. 2008;7:1-13.
- Jain TK, Morales MA, Sahoo SK, et al. Iron oxide nanoparticles for sustained delivery of anticancer agents. Mol Pharm. 2005;2:194–205.
- Jia N, Lian Q, Shen H, et al. Intracellular delivery of quantum dots tagged antisense oligodeoxynucleotides by functionalized multiwalled carbon nanotubes. Nano Lett. 2007;7:2976–80.
- Jiang J, Chen H, Yu C, et al. The promotion of salinomycin delivery to hepatocellular carcinoma cells through EGFR and CD133 aptamers conjugation by PLGA nanoparticles. Nanomedicine (Lond). 2015;10:1863–79.
- Jonuleit H, Bopp T, Becker C. Treg cells as potential cellular targets for functionalized nanoparticles in cancer therapy. Nanomedicine (Lond). 2016;11:2699–709.
- Jørgensen JT, Norregaard K, Tian P, et al. Single particle and PET-based platform for identifying optimal plasmonic nano-heaters for photothermal cancer therapy. Sci Rep. 2016;6:30076.
- Jose GP, Santra S, Mandal SK, Sengupta TK. Singlet oxygen mediated DNA degradation by copper nanoparticles: potential towards cytotoxic effect on cancer cells. J Nanobiotechnol. 2011;9:9.
- Kakkar V, Singh S, Singla D, Kaur IP. Exploring solid lipid nanoparticles to enhance the oral bioavailability of curcumin. Mol Nutr Food Res. 2011;55:495–503.
- Kang B, Mackey MA, El-Sayed MA. Nuclear targeting of gold nanoparticles in cancer cells induces DNA damage, causing cytokinesis arrest and apoptosis. J Am Chem Soc. 2010;132:1517–9.
- Kennedy LC, Bear AS, Young JK, et al. T cells enhance gold nanoparticle delivery to tumors in vivo. Nanoscale Res Lett. 2011;6:283.
- Khan MA, Zafaryab M, Mehdi SH, et al. Characterization and anti-proliferative activity of curcumin loaded chitosan nanoparticles in cervical cancer. Int J Biol Macromol. 2016;93(Pt A):242–53.
- Kircher MF, de la Zerda A, Jokerst JV, et al. A brain tumor molecular imaging strategy using a new triple-modality MRI-photoacoustic-Raman nanoparticle. Nat Med. 2012;18:829–34.

- Lee H, Dam DH, Ha JW, et al. Enhanced human epidermal growth factor receptor 2 degradation in breast cancer cells by lysosome-targeting gold nanoconstructs. ACS Nano. 2015;9:9859–67.
- Lee JL, Ahn JH, Park SH, et al. Phase II study of a cremophor-free, polymeric micelle formulation of paclitaxel for patients with advanced urothelial cancer previously treated with gemcitabine and platinum. Investig New Drugs. 2012;30:1984–90.
- Lee Y, Park SY, Kim C, Park TG. Thermally triggered intracellular explosion of volume transition nanogels for necrotic cell death. J Control Release. 2009;135:89–95.
- Li YJ, Perkin AL, Su Y, et al. Gold nanoparticles as a platform for creating a multivalent poly-SUMO chain inhibitor that also augments ionizing radiation. Proc Natl Acad Sci U S A. 2012;109:4092–7.
- Lin CW, Bachilo SM, Vu M, et al. Spectral triangulation: a 3D method for locating single-walled carbon nanotubes in vivo. Nanoscale. 2016;8:10348–57.
- Liu JL, Dixit AB, Robertson KL, et al. Viral nanoparticle-encapsidated enzyme and restructured DNA for cell delivery and gene expression. Proc Natl Acad Sci U S A. 2014;111:13319–24.
- Liu Z, Chen K, Davis C, et al. Drug delivery with carbon nanotubes for in vivo cancer treatment. Cancer Res. 2008;68:6652–60.
- Lu J, Liong M, Zink JI, Tamanoi F. Mesoporous silica nanoparticles as a delivery system for hydrophobic anticancer drugs. Small. 2007;3:1341–6.
- MacDiarmid JA, Amaro-Mugridge NB, Madrid-Weiss J, et al. Sequential treatment of drugresistant tumors with targeted minicells containing siRNA or a cytotoxic drug. Nat Biotechnol. 2009;27:643–51.
- MacDiarmid JA, Langova V, Bailey D, et al. Targeted doxorubicin delivery to brain tumors via minicells: proof of principle using dogs with spontaneously occurring tumors as a model. PLoS One. 2016;11:e0151832.
- MacDiarmid JA, Mugridge NB, Weiss JC, et al. Bacterially derived 400 nm particles for encapsulation and cancer cell targeting of chemotherapeutics. Cancer Cell. 2007;11:431–45.
- MacKay JA, Chen M, McDaniel JR, et al. Self-assembling chimeric polypeptide-doxorubicin conjugate nanoparticles that abolish tumours after a single injection. Nat Mat. 2009;8:993–9.
- Maksimenko A, Dosio F, Mougin J, et al. A unique squalenoylated and nonpegylated doxorubicin nanomedicine with systemic long-circulating properties and anticancer activity. Proc Natl Acad Sci U S A. 2014;111:E217–26.
- Martel S, Mohammadi M, Felfoul O, et al. Controlled MRI-trackable propulsion and steering systems for medical nanorobots operating in the human microvasculature. Int J Robot Res. 2009;28:571–82.
- McDevitt MR, Chattopadhyay D, Kappel BJ, et al. Tumor targeting with antibody-functionalized, radiolabeled carbon nanotubes. J Nucl Med. 2007;48:1180–9.
- Mi Y, Guo Y, Feng SS. Nanomedicine for multimodality treatment of cancer. Nanomedicine. 2012;7:1791–4.
- Mo S, Coussios CC, Seymour L, Carlisle R. Ultrasound-enhanced drug delivery for cancer. Expert Opin Drug Deliv. 2012;9:1525–38.
- Mohanty RK, Kumar R, Thennarasu S, Mandala AB. Resveratrol stabilized gold nanoparticles enable surface loading of doxorubicin and anticancer activity. Colloids Surf B Biointerfaces. 2014;114:138–43.
- Morton SW, Lee MJ, Deng ZJ, et al. A nanoparticle-based combination chemotherapy delivery system for enhanced tumor killing by dynamic rewiring of signaling pathways. Sci Signal. 2014;7:ra44.
- Murakami T, Sawada H, Tamura G, et al. Water-dispersed single-wall carbon nanohorns as drug carriers for local cancer chemotherapy. Nanomedicine. 2008;3:453–63.
- Muraoka D, Harada N, Hayashi T, et al. Nanogel-based immunologically stealth vaccine targets macrophages in the medulla of lymph node and induces potent antitumor immunity. ACS Nano. 2014;8:9209–18.
- Myc A, Majoros IJ, Thomas TP, Baker Jr JR. Dendrimer-based targeted delivery of an apoptotic sensor in cancer cells. Biomacromolecules. 2007;8:13–8.

- Nair BG, Nagaoka Y, Morimoto H, et al. Aptamer conjugated magnetic nanoparticles as nanosurgeons. Nanotechnology. 2010;21:455102.
- Nascimento TL, Hillaireau H, Vergnaud J, Fattal E. Lipid-based nanosystems for CD44 targeting in cancer treatment: recent significant advances, ongoing challenges and unmet needs. Nanomedicine (Lond). 2016;11:1865–87.
- Nevala WK, Buhrow SA, Knauer DJ, et al. Antibody-targeted chemotherapy for the treatment of melanoma. Cancer Res. 2016;76:3954–64.
- Ni M, Xiong M, Zhang X, et al. Poly(lactic-co-glycolic acid) nanoparticles conjugated with CD133 aptamers for targeted salinomycin delivery to CD133+ osteosarcoma cancer stem cells. Int J Nanomedicine. 2015;10:2537–54.
- Noble CO, Krauze MT, Drummond DC, et al. Novel nanoliposomal CPT-11 infused by convectionenhanced delivery in intracranial tumors: pharmacology and efficacy. Cancer Res. 2006;66:2801–6.
- Ohulchanskyy TY, Roy I, Goswami LN. Organically modified silica nanoparticles with covalently incorporated photosensitizer for photodynamic therapy of cancer. Nano Lett. 2007;7:2835–42.
- Ossipov DA. Nanostructured hyaluronic acid-based materials for active delivery to cancer. Expert Opin Drug Deliv. 2010;7:681–703.
- Palakurthi S, Yellepeddi VK, Vangara KK. Recent trends in cancer drug resistance reversal strategies using nanoparticles. Expert Opin Drug Deliv. 2012;9:287–301.
- Pan D, Caruthers SD, Hu G, et al. Ligand-directed nanobialys as theranostic agent for drug delivery and manganese-based magnetic resonance imaging of vascular targets. J Am Chem Soc. 2008;130:9186–7.
- Pandey A, Kulkarni A, Roy B, et al. Sequential application of a cytotoxic nanoparticle and a PI3K inhibitor enhances antitumor efficacy. Cancer Res. 2014;74:675–85.
- Paraskar AS, Soni S, Chin KT, et al. Harnessing structure-activity relationship to engineer a cisplatin nanoparticle for enhanced antitumor efficacy. Proc Natl Acad Sci U S A. 2010;107:12435–40.
- Peng W, Anderson DG, Bao Y, et al. Nanoparticulate delivery of suicide DNA to murine prostate and prostate tumors. Prostate. 2007;67:855–62.
- Phillips E, Penate-Medina O, Zanzonico PB, et al. Inorganic nanoparticles for first-in-human molecular imaging of cancer. Sci Transl Med. 2014;6:260ra149.
- Piktel E, et al. Recent insights in nanotechnology-based drugs and formulations designed for effective anti-cancer therapy. J Nanobiotechnol. 2016;14:39.
- Pirollo KF, Rait A, Zhou Q, et al. Materializing the potential of small interfering RNA via a Tumortargeting nanodelivery system. Cancer Res. 2007;67:2938–43.
- Popov J, Kapanen AI, Turner C, et al. Multivalent rituximab lipid nanoparticles as improved lymphoma therapies: indirect mechanisms of action and in vivo activity. Nanomedicine (Lond). 2011;6:1575–91.
- Prabaharan M. Chitosan-based nanoparticles for tumor-targeted drug delivery. Int J Biol Macromol. 2015;72:1313–22.
- Puri A, Kramer-Marek G, et al. HER2-specific affibody-conjugated thermosensitive liposomes (Affisomes) for improved delivery of anticancer agents. J Liposome Res. 2008;18:293–307.
- Qian X, Peng XH, Ansari DO, et al. In vivo tumor targeting and spectroscopic detection with surface-enhanced Raman nanoparticle tags. Nat Biotechnol. 2008;26:83–90.
- Quyen Chau ND, Ménard-Moyon C, Kostarelos K, Bianco A. Multifunctional carbon nanomaterial hybrids for magnetic manipulation and targeting. Biochem Biophys Res Commun. 2015;468:454–62.
- Rapoport N, Gao Z, Kennedy A. Multifunctional nanoparticles for combining ultrasonic tumor imaging and targeted chemotherapy. JNCI. 2007;99:1095–106.
- Rasmussen JW, Martinez E, Louka P, Wingett DG. Zinc oxide nanoparticles for selective destruction of tumor cells and potential for drug delivery applications. Expert Opin Drug Deliv. 2010;7:1063–77.
- Reinemann C, Strehlitz B. Aptamer-modified nanoparticles and their use in cancer diagnostics and treatment. Swiss Med Wkly. 2014;144:w13908.

- Rivkin I, Cohen K, Koffler J, et al. Paclitaxel-clusters coated with hyaluronan as selective tumortargeted nanovectors. Biomaterials. 2010;31:7106–14.
- Rosenholm JM, Mamaeva V, Sahlgren C, Lindén M. Nanoparticles in targeted cancer therapy: mesoporous silica nanoparticles entering preclinical development stage. Nanomedicine (Lond). 2012;7:111–20.
- Roy K, Kanwar RK, Kanwar JR. LNA aptamer based multi-modal, Fe3O4-saturated lactoferrin (Fe3O4-bLf) nanocarriers for triple positive (EpCAM, CD133, CD44) colon tumor targeting and NIR, MRI and CT imaging. Biomaterials. 2015;71:84–99.
- Saif MW, Podoltsev NA, Rubin MS, et al. Phase II clinical trial of paclitaxel loaded polymeric micelle in patients with advanced pancreatic cancer. Cancer Investig. 2010;28:186–94.
- Sano K, Nakajima T, Choyke PL, Kobayashi H. Markedly enhanced permeability and retention effects induced by photo-immunotherapy of tumors. ACS Nano. 2013;7:717–24.
- Scarberry KE, Dickerson EB, McDonald JF, et al. Magnetic nanoparticle peptide conjugates for in vitro and in vivo targeting and extraction of cancer cells. J Am Chem Soc. 2008;130:10258–62.
- Schluep T, Hwang J, Hildebrandt IJ, et al. Pharmacokinetics and tumor dynamics of the nanoparticle IT-101 from PET imaging and tumor histological measurements. Proc Natl Acad Sci U S A. 2009;106:11394–9.
- Schroeder A, Heller DA, Winslow MM, et al. Treating metastatic cancer with nanotechnology. Nat Rev Cancer. 2012;12:39–50.
- Sheng W, Chen T, Tan W, Fan ZH. Multivalent DNA nanospheres for enhanced capture of cancer cells in microfluidic devices. ACS Nano. 2013;7:7067–76.
- Shu D, Li H, Shu Y, et al. Systemic delivery of anti-miRNA for suppression of triple negative breast cancer utilizing RNA nanotechnology. ACS Nano. 2015;9:9731–40.
- Shukla R, Chanda N, Zambre A, et al. Laminin receptor specific therapeutic gold nanoparticles (198AuNP-EGCg) show efficacy in treating prostate cancer. Proc Natl Acad Sci U S A. 2012;109:12426–31.
- Soman NR, Baldwin SL, Hu G, et al. Molecularly targeted nanocarriers deliver the cytolytic peptide melittin specifically to tumor cells in mice, reducing tumor growth. J Clin Invest. 2009;119:2830–42.
- Song X, Ren Y, Zhang J, et al. Targeted delivery of doxorubicin to breast cancer cells by aptamer functionalized DOTAP/DOPE liposomes. Oncol Rep. 2015;34:1953–60.
- Song Z, Feng R, Sun M, et al. Curcumin-loaded PLGA-PEG-PLGA triblock copolymeric micelles: Preparation, pharmacokinetics and distribution in vivo. J Colloid Interface Sci. 2011;354:116–23.
- Steinberg I, Ben-David M, Gannot I. A new method for tumor detection using induced acoustic waves from tagged magnetic nanoparticles. Nanomedicine. 2012;8:569–79.
- Stover TC, Sharma A, Robertson GP, Kester M. Systemic delivery of liposomal short-chain ceramide limits solid tumor growth in murine models of breast adenocarcinoma. Clin Cancer Res. 2005;11:3465–74.
- Sun M, Wang J, Lu Q, et al. Novel synthesizing method of pH-dependent doxorubicin-loaded anti-CD22-labelled drug delivery nanosystem. Drug Des Devel Ther. 2015;9:5123–33.
- Sutton D, Nasongkla N, Blanco E, Gao J. Functionalized micellar systems for cancer targeted drug delivery. Pharm Res. 2007;24:1029–46.
- Tada H, Higuchi H, Wanatabe TM, Ohuchi N. In vivo real-time tracking of single quantum dots conjugated with monoclonal anti-HER2 antibody in tumors of mice. Cancer Res. 2007;67:1138–44.
- Tagaram HR, Divittore NA, Barth BM, et al. Nanoliposomal ceramide prevents in vivo growth of hepatocellular carcinoma. Gut. 2011;60:695–701.
- Talelli M, Rijcken CJ, Oliveira S, et al. Nanobody-shell functionalized thermosensitive corecrosslinked polymeric micelles for active drug targeting. J Control Release. 2011;151:183–92.
- Tan A, De La Peña H, Seifalian AM. The application of exosomes as a nanoscale cancer vaccine. Int J Nanomedicine. 2010;5:889–900.

- Taruttis A, van Dam GM, Ntziachristos V. Mesoscopic and macroscopic optoacoustic imaging of cancer. Cancer Res. 2015;75:1548–59.
- Tavano L, Muzzalupo R, Mauro L, et al. Transferrin-conjugated pluronic niosomes as a new drug delivery system for anticancer therapy. Langmuir. 2013;29:12638–46.
- Tekade RK, Tekade M, Kesharwani P, D'Emanuele A. RNAi-combined nano-chemotherapeutics to tackle resistant tumors. Drug Discov Today. 2016;21:1761–74.
- Thakor AS, Luong R, Paulmurugan R, et al. The fate and toxicity of Raman-active silica-gold nanoparticles in mice. Sci Transl Med. 2011;3:79ra33.
- Thaxton CS, Elghanian R, Thomas AD, et al. Nanoparticle-based bio-barcode assay redefines "undetectable" PSA and biochemical recurrence after radical prostatectomy. Proc Natl Acad Sci U S A. 2009;106:18437–42.
- Thomas CR, Ferris DP, Lee JH, et al. Noninvasive remote-controlled release of drug molecules in vitro using magnetic actuation of mechanized nanoparticles. J Am Chem Soc. 2010;132:10623–5.
- Tomalia DA, Reyna LA, Svenson S. Dendrimers as multi-purpose nanodevices for oncology drug delivery and diagnostic imaging. Biochem Soc Trans. 2007;35(Pt 1):61–7.
- Tonigold M, Mailänder V. Endocytosis and intracellular processing of nanoparticles in dendritic cells: routes to effective immunonanomedicines. Nanomedicine (Lond). 2016;11:2625–30.
- Trimaille T, Verrier B. Micelle-based adjuvants for subunit vaccine delivery. Vaccines (Basel). 2015;3:803–13.
- Tsalach A, Steinberg I, Gannot I. Tumor localization using magnetic nanoparticle-induced acoustic signals. IEEE Trans Biomed Eng. 2014;61:2313–23.
- Tuettenberg A, Steinbrink K, Schuppan D. Myeloid cells as orchestrators of the tumor microenvironment: novel targets for nanoparticular cancer therapy. Nanomedicine (Lond). 2016;11:2735–51.
- Ucisik MH, Küpcü S, Schuster B, Sleytr UB. Characterization of CurcuEmulsomes: nanoformulation for enhanced solubility and delivery of curcumin. J Nanobiotechnology. 2013;11:37.
- van Vlerken LE, Duan Z, Seiden MV, Amiji MM. Modulation of intracellular ceramide using polymeric nanoparticles to overcome multidrug resistance in cancer. Cancer Res. 2007;67:4843–50.
- Wang CF, Mäkilä EM, Kaasalainen MH, et al. Dual-drug delivery by porous silicon nanoparticles for improved cellular uptake, sustained release, and combination therapy. Acta Biomater. 2015;16:206–14.
- Wang S, Liu K, Liu J, et al. Highly efficient capture of circulating tumor cells by using nanostructured silicon substrates with integrated chaotic micromixers. Angew Chem Int Ed Engl. 2011a;50:3084–8.
- Wang J, Lu Z, Gao Y, et al. Improving delivery and efficacy of nanomedicines in solid tumors: role of tumor priming. Nanomedicine (Lond). 2011b;6:1605–20.
- Wang S, Wang H, Jiao J, et al. Three-dimensional nanostructured substrates toward efficient capture of circulating tumor cells. Angew Chem Int Ed Engl. 2009;48:8970–3.
- Wang AZ, Yuet K, Zhang L, et al. ChemoRad nanoparticles: a novel multifunctional nanoparticle platform for targeted delivery of concurrent chemoradiation. Nanomedicine (Lond). 2010;5:361–8.
- Weigum SE, Floriano PN, Redding SW, et al. Nano-bio-chip sensor platform for examination of oral exfoliative cytology. Cancer Prev Res. 2010;3:518–28.
- Weiss GJ, Chao J, Neidhart JD, et al. First-in-human phase 1/2a trial of CRLX101, a cyclodextrincontaining polymer-camptothecin nanopharmaceutical in patients with advanced solid tumor malignancies. Investig New Drugs. 2013;31:986–1000.
- Wen X, Reynolds L, Mulik RS, et al. Hepatic arterial infusion of low-density lipoprotein docosahexaenoic acid nanoparticles selectively disrupts redox balance in hepatoma cells and reduces growth of orthotopic liver tumors in rats. Gastroenterology. 2016;150:488–98.
- Wong C, Stylianopoulos T, Cui J, et al. Multistage nanoparticle delivery system for deep penetration into tumor tissue. Proc Natl Acad Sci U S A. 2011;108:2426–31.
- Wu S, Wang Y, Guo J, et al. Nanosecond pulsed electric fields as a novel drug free therapy for breast cancer: an in vivo study. Cancer Lett. 2014;343:268–74.

- Wu Y, SefahK LH, et al. DNA aptamer–micelle as an efficient detection/delivery vehicle toward cancer cells. Proc Natl Acad Sci U S A. 2009;107:5–10.
- Xiao Y, Hong H, Javadi A, et al. Multifunctional unimolecular micelles for cancer-targeted drug delivery and positron emission tomography imaging. Biomaterials. 2012;33:3071–82.
- Xie H, Li YF, Kagawa HK, et al. An intrinsically fl uorescent recognition ligand scaffold based on chaperonin protein and semiconductor quantum-dot conjugates. Small. 2009;5:1036–42.
- Xu W, Riikonen J, Lehto VP. Mesoporous systems for poorly soluble drugs. Int J Pharm. 2013;453:181–97.
- Yallapu MM, Khan S, Maher DM, et al. Anti-cancer activity of curcumin loaded nanoparticles in prostate cancer. Biomaterials. 2014;35:8635–48.
- Yang L, Tseng YT, Suo G, et al. Photothermal therapeutic response of cancer cells to aptamer-gold nanoparticle-hybridized graphene oxide under NIR illumination. ACS Appl Mater Interfaces. 2015;7:5097–106.
- Yao L, Danniels J, Moshnikova A, et al. pHLIP peptide targets nanogold particles to tumors. Proc Natl Acad Sci U S A. 2013;110:465–70.
- Ye S, Marston G, McLaughlan JR, et al. Engineering gold nanotubes with controlled length and near-infrared absorption for theranostic applications. Adv Funct Mater. 2015;25:2117–27.
- Yeh TK, Lu Z, Wientjes MG, Au JL. Formulating paclitaxel in nanoparticles alters its disposition. Pharm Res. 2005;22:867–74.
- Yin Q, Tang L, Cai K, et al. Pamidronate functionalized nanoconjugates for targeted therapy of focal skeletal malignant osteolysis. Proc Natl Acad Sci U S A. 2016;113:E4601–9.
- Yu KN, Lee SM, Han JY, Park H, et al. Multiplex targeting, tracking, and imaging of apoptosis by fluorescent surface enhanced raman spectroscopic dots. Bioconjug Chem. 2007;18:1155–62.
- Zalba S, Contreras AM, Haeri A, Ten Hagen TL, Navarro I, Koning G, Garrido MJ. Cetuximaboxaliplatin-liposomes for epidermal growth factor receptor targeted chemotherapy of colorectal cancer. J Control Release. 2015;210:26–38.
- Zhang C, Newsome JT, Mewani R, et al. Systemic delivery and pre-clinical evaluation of nanoparticles containing antisense oligonucleotides and siRNAs. Methods Mol Biol. 2009;480:65–83.
- Zhang E, Zhang C, Su Y, et al. Newly developed strategies for multifunctional mitochondriatargeted agents in cancer therapy. Drug Discov Today. 2011;16:140–6.
- Zhang M, Xiao B, Wang H, et al. Edible ginger-derived nano-lipids loaded with doxorubicin as a novel drug-delivery approach for colon cancer therapy. Mol Ther. 2016;24:1783–96.
- Zhou Q, Rahimian A, Son K, et al. Development of an aptasensor for electrochemical detection of exosomes. Methods. 2016;97:88–93.
- Zhu L, Wang T, Perche F, et al. Enhanced anticancer activity of nanopreparation containing an MMP2-sensitive PEG-drug conjugate and cell-penetrating moiety. Proc Natl Acad Sci U S A. 2013;110:17047–52.

Chapter 9 Nanoneurology

Introduction

Neurology deals with study and management of disorders of the nervous system. Considerable research is in progress in basic neurosciences and clinical neurology. The management is mostly medical. Many neurological disorders require surgical intervention and the closely related specialty of surgical neurology or neurosurgery will also be considered in this chapter. New technologies are being used for research in neurosciences, neuropharmacology and clinical neurology (Jain 2013). There is a considerable scope for application of nanobiotechnology in neurology and hence the term nanoneurology (Jain 2009). Nanobiotechnology has been applied for neurophysiological studies, diagnosis, neuropharmacology and refinement of surgical tools. Neuroprotection is an important objective in treatment of diseases of the central nervous system (CNS).

Nanobiotechnology for Neurophysiological Studies

Nanoelectrodes in Neurophysiology

Insulated microelectrodes are used in neurophysiological studies since 1950s with minor modifications. Single large neuron recordings are possible with electrodes in μ m diameter range. It is worthwhile to have electrodes with nanoscale tips for recording from small neurons. It is now possible to grind the bare tip of a tungsten microelectrode down to 100–1000 nm and remove the insulation at the tip. An electrode with 700 nm tip can record well-isolated action potentials extracellularly from single visual neurons in vivo.

Chronic EEG Recording

A CNT/adhesive polydimethylsiloxane (aPDMS) composite-based dry EEG electrode has been developed for capacitive measuring of EEG signals (Lee et al. 2016). As research related to brain-computer interface applications has advanced, the presence of hairs on a patient's scalp presents an obstacle to recording EEG signals using dry electrodes. The CNT/aPDMS electrode is elastic, highly conductive, selfadhesive, and capable of making conformal contact with and attaching to a hairy scalp. Hundreds of conductive pillars coated with Parylene C insulation layer were fabricated on to the conductive disk. The top of disk is solderable, which enables the electrode to connect with a variety of commercial EEG recording systems. The performance of the electrodes has been evaluated by recording EEGs, including alpha rhythms, auditory-evoked potentials, and steady-state visually-evoked potentials. The results revealed that the electrode provided a high signal-to-noise ratio with good tolerance for motion. Almost no leakage of current was observed. Although preamplifiers with ultrahigh input impedance were previously considered to be essential for capacitive electrodes, the EEGs were recorded with CNT/aPDMS by directly connecting a commercially available EEG acquisition system to the electrode to yield high-quality signals comparable to those obtained using conventional wet electrodes.

Nanoscale Devices for Network-Level Electrophysiology

Transistor arrays of silicon nanowires with diameter of 30 nm and fabricated on transparent substrates can be reliably interfaced to acute brain slices (Qing et al. 2010). These can record across a wide range of length scales, whereas the transparent device chips only provide imaging of individual cell bodies. Combination of arrays with patch clamp studies enables identification of action potential signals. The result is a recording with high temporal and spatial resolution, as well as mapping of functional connectivity. This provides a powerful platform for studying neural circuits in the brain.

Nanostructured arrays enable long-term monitoring of intracellular electrical signals from multiple cells simultaneously their small size. They are less damaging to the cells than conventional μ m-sized pipettes. There are two examples of these:

- 1. Rat neurons were cultured on a vertical array of 150 nm diameter silicon wires capped by a conducting metal tip. They were used for stimulating and recording of intracellular action potentials as well as mapping of synaptic connections in the cultures (Robinson et al. 2012).
- 2. In another study, arrays of similar-sized 'nanopillars' were built using platinum. These were used to culture mouse cardiomyocytes and study changes in the intracellular action potentials induced by drugs (Xie et al. 2012).

To get the nanowires efficiently into cells, both studies used membrane electroporation by applying small electrical currents through the nanoelectrodes themselves.

Chronic Subcellular Recording from Implanted Electrodes

Experimental studies have shown that sub-100 nm silicon nanowires can be integrated into live cells without causing detrimental effects (Kim et al. 2007). Subcellularsized chronically implanted recording electrodes have demonstrated significant improvement in single unit (SU) yield over larger recording probes. Additional work has expanded this initial success by combining the subcellular fiber-like lattice structures with the design space versatility of silicon microfabrication to further improve the signal-to-noise ratio, density of electrodes, and stability of recorded units over months to years. However, ultrasmall microelectrodes present very high impedance, which must be lowered for SU recordings. While poly(3,4ethylenedioxythiophene) (PEDOT) doped with polystyrene sulfonate (PSS) coating have demonstrated great success in acute to early-chronic studies for lowering the electrode impedance, concern exists over long-term stability. A new blend of PEDOT doped with carboxyl functionalized multiwalled carbon nanotubes (CNTs) shows dramatic improvement over the traditional PEDOT/PSS formula (Kozai et al. 2016). PEDOT/CNT-coated subcellular electrodes demonstrated significant improvement in chronic spike recording stability over 4 months compared to PEDOT/PSS recording sites. High-density ultrasmall nanoelectrodes combined with advanced electrode surface modification are likely to make significant contributions to the development of long-term (permanent), high quality, and selective neural interfaces.

Nanowires for Monitoring Brain Activity Via Blood Vessels

Electrical recording from spinal cord vascular capillary bed has been achieved demonstrating that the intravascular space may be used to record brain activity without violating the brain parenchyma. It is feasible to use blood vessels as conduits to guide the platinum nanowires for detecting activity of individual neurons lying adjacent to the blood vessels. This can provide an understanding of the brain at the neuron-to-neuron interaction level with non-intrusive, biocompatible and biodegradable nanoprobes. This technique may enable monitoring of individual brain cells and perhaps provide new treatments for neurological diseases. Because nanowires can deliver electrical impulses as well as receive them, the technique has potential as a treatment for Parkinson's disease (PD). It has already been demonstrated that patients with PD can experience significant improvement from direct stimulation of

the affected area of the brain. But the stimulation is currently carried out by inserting wires through the skull and into the brain that can cause scarring of the brain tissue. By stimulating the brain with nanowires threaded through blood vessels, patients can receive benefits of the treatment without the damaging side effects. The challenge is to precisely guide the nanowire probes to a predetermined spot through the thousands of branches in the brain's vascular system. One solution is to replace the platinum nanowires with new conducting polymer nanowires. Not only do the polymers conduct electrical impulses, they change shape in response to electrical fields, which would allow the researchers to steer the nanowires through the brain's circulatory system. Polymer nanowires have the added benefit of being 20 to 30 times smaller than the platinum ones used in the reported laboratory experiments. They are biodegradable and therefore suitable for short-term brain implants.

Gold Nanoparticles for In Vivo Study of Neural Function

As a novel in vivo method to study interactions between gold nanoparticles AuNPs and the nervous system, negatively charged AuNPs, 50 nm in diameter, were injected into the CNS of a cockroach (Rocha et al. 2011). The charged nanoparticles affected the insect's locomotion and behavior but no significant effect on the life expectancy of the cockroach after 2 months of observation, apparently due to the encapsulation of AuNPs inside the insect's brain. This inexpensive method offers an opportunity to further understand how nanoparticles affect neural communication by monitoring insect activity and locomotion.

Nanodiagnosis and Nanoparticle-Based Brain Imaging

Nanodiagnostic technologies described in Chap. 4 are applicable to neurological disorders. Relation of various technologies to diagnosis of neurological disorders is shown in Fig. 9.1.

Applications of Nanotechnology in Molecular Imaging of the Brain

Some of the applications of nanobiotechnology in brain imaging are:

- Tracking of stem cells by tagging with nanoparticles such as SPIONs so they can be detected with MRI
- QDs for molecular imaging in cerebrovascular disorders.
 - early aneurysm detection and guide endovascular intervention
 - imaging of vessels prone to spasm

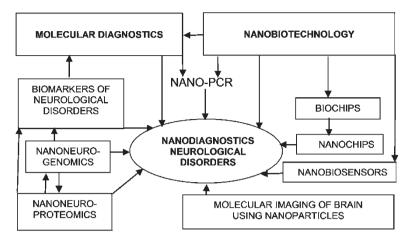


Fig. 9.1 Nanodiagnostics for neurological disorders

- to distinguish penumbra from infarction
- to identify unstable arterial plaques for targeted intervention
- Early diagnosis of neurodegenerative disorders
- Early diagnosis of brain tumors

Nanoparticles and MRI for Macrophage Tracking in the CNS

Activated macrophages, acting in concert with other immune competent cells, are an index of inflammatory/ immune reaction in CNS disorders such as multiple sclerosis, ischemic stroke lesions, and tumors. The MRI detection of brain macrophages defines precise spatial and temporal patterns of macrophage involvement that helps to characterize individual neurological disorders. Macrophage tracking by magnetic MRI with iron oxide nanoparticles has been developed during the last decade for numerous diseases of the CNS. Experimental studies on animal models were confirmed by clinical applications of MRI technology of brain macrophages. This approach is being explored as an in vivo biomarker for the clinical diagnosis of cerebral lesion activity, in experimental models for the prognosis of disease development, and to determine the efficacy of immunomodulatory treatments under clinical evaluation (Petry et al. 2007). Comparative brain imaging follow-up studies of blood-brain barrier leakage by MRI with gadolinium-chelates, microglia activation by PET with radiotracer ligand PK11195 and MRI detection of macrophage infiltration provide more precise information about the pathophysiological cascade of inflammatory events in cerebral diseases. Such multimodal characterization of the inflammatory events should help in the monitoring of patients, in defining precise time intervals for therapeutic interventions, and in developing and evaluating new therapeutic strategies.

Nanoparticles for Tracking Stem Cells for Therapy of CNS Disorders

Cellular MRI using superparamagnetic iron oxide nanoparticles (SPION) can visualize and track cells in living organisms. MRI studies have been conducted in rat models of CNS injury and stroke to track stem cells that were either grafted intracerebrally, contralaterally to a cortical photochemical lesion, or injected intravenously (Sykova and Jendelova 2007). ESCs and MSCs were labeled with iron oxide nanoparticles (Endorem®) and human CD34⁺ cells were labeled with magnetic MicroBeads (Miltenyi). During the first post-transplantation week, grafted MSCs or ESCs migrated to the lesion site in the cortex as well as in the spinal cord and were visible in the lesion on MRI as a hypointensive signal, persisting for more than 30 days. In rats with an SCI, an increase in functional recovery was noted after the implantation of MSCs or after an injection of granulocyte colony stimulating factor (G-CSF). Morphometric measurements in the center of the lesions showed an increase in white matter volume in cell-treated animals. Prussian blue staining confirmed numerous iron-positive cells, and the lesions were considerably smaller than in control animals. To obtain better results with cell labeling, new polycation-bound SPION (PC-SPION) were developed. In comparison with Endorem, PC-SPION demonstrated a more efficient intracellular uptake into MSCs, with no decrease in cell viability. These studies demonstrate that MRI of grafted adult as well as ESCs labeled with iron oxide nanoparticles is a useful method for evaluating cellular migration toward a lesion site.

Autologous bone marrow CD34+ cells labeled with magnetic nanoparticles have been delivered into the spinal cord via lumbar puncture in a study on patients with chronic SCI (Callera and de Melo 2007). One group received their own labeled-CD34+ cells whereas the others received an injection containing only magnetic nanoparticles without stem cells to serve as controls. CD34+ cells were labeled with magnetic nanoparticles coated with a monoclonal antibody specific for the CD34 cell membrane antigen. MRI showed that magnetically labeled CD34+ cells were visible at the lesion site as hypointense signals following transplantation, but these signals were not visible in any patient in the control group. This study shows that autologous bone marrow CD34+ cells labeled with magnetic nanoparticles, when delivered intrathecally migrate into the site of injury in patients with chronic SCI and can be tracked by MRI. This shows the feasibility of treatment of SCI with intrathecal cell therapy.

Multifunctional NPs for Diagnosis and Treatment of Brain Disorders

Multifunctional NPs (MFNPs) are particularly suited for combining diagnostics with therapeutics of brain disorders. Tailoring the size, contents, and surface electronic properties through chemistry and physical methods within sub-200 nm

nanoparticles will be key factors for using MFNPS (Suh et al. 2009). Functions such as directing neuronal growth and influencing stem cell differentiation for brain repair seem to be the next logical step in nanobiotechnology utilizing MFNPS. Studies involving stem cell differentiation and transplantation, neural implants, targeted drug delivery with real-time monitoring capabilities, and in vivo RNAi will be of great interest. Advances in neuroscience will arise from systematic investigations starting from synthesis to application where the efforts are focused on probing and understanding events occurring at the nano – bio interface.

Nanotechnology-Based Drug Delivery to the CNS

Delivery of drugs to CNS is a challenge and the basics as well as various strategies are discussed in a special report on this topic (Jain 2017). Molecular motors, operating at nanoscale, can deliver drugs to the CNS by peripheral muscle injection. An advantage is the use of nanomotors in native environment for intraneural drug delivery. The disadvantages are that this approach requires engineered molecular motors for use in cells and neurotoxicity may be a problem.

Nanotechnology-Based Drug Delivery for Neurodegenerative Disorders

Nanoencapsulation for Delivery of Vitamin E for Alzheimer Disease

Vitamin E is used for the treatment of neurological disorders, particularly those where oxidative stress plays a role. Oxidative stress is an early hallmark of affected neurons in Alzheimer's disease (AD). The antioxidant vitamin E provides limited neuroprotection in AD, which may have derived from its lipophilic nature and resultant inability to quench cytosolic reactive oxygen species (ROS), including those generated from antecedent membrane oxidative damage. Encapsulation into polyethylene glycol (PEG)-based nanospheres enables entery into the cytosol and improve the efficacy of vitamin E against $A\beta$ -induced ROS. These findings suggests suggests that nanosphere-mediated delivery methods may be a useful adjunct for antioxidant therapy in AD.

Selegiline-PEG Nanoparticles Targeting Aß Fibrils in Alzheimer Disease

Deposition of the A β proteins (senile plaques) in the extracellular synaptic spaces of the neocortex is plays a role in progress of AD. The increased activity of monoamine oxidase-B (MAO-B) in AD brains causes oxidative damage, and MAO-B inhibitors have been reported to inhibit the neuronal degeneration. Destabilizing effect of selegiline, a selective MAO-B inhibitor, on A β -fibrils has been investigated in vitro by conjugating it with poly (lactic-co-glycolic acid)-poly (ethylene glycol) (PLGA-PEG) nanoparticles (Baysal et al. 2013). Results show that selegiline-loaded PLGA-PEG nanoparticles are a promising drug carrier for destabilizing the $A\beta$ fibrils in AD patients.

Nanoparticles for Drug Delivery Across BBB

Currently most of the strategies are directed at overcoming the blood brain barrier (BBB). Role of nanobiotechnology in overcoming BBB is described elsewhere (Jain 2012). Very small nanoparticles may just pass through the BBB but this uncontrolled passage is not desirable. Most of the strategies described in this report for passage of drugs across the BBB can be enhanced by nanotechnology and some examples are:

- Nanoparticles open the tight junctions between endothelial cells and enable the drug to penetrate the BBB either in free form or together with the nanocarrier.
- Nanoparticles are transcytosed through the endothelial cell layer and allow the direct transport of their therapeutic cargo.
- Nanoparticles are endocytosed by endothelial cells and release the drug inside the cell, as a precursor step to the transport of active ingredients, which occurs by exocytosis at the abluminal side of the endothelium.
- Nanoparticles, which combine an increased retention at the brain capillaries with adsorption onto the capillary walls, improve delivery to the brain by creating a concentration gradient that promotes transport across the endothelial cell layer.
- Drug transport is enhanced by the solubilization of the endothelial cell membrane lipids by surfactant, which leads to membrane fluidization (surfactant effect).
- Coating agents (such as polysorbates) inhibit the transmembrane efflux systems, i.e. P-glycoprotein.
- Nanoparticles induce local toxic effects at the brain vasculature, which leads to a limited permeabilization of the brain endothelial cells.

BBB represents an insurmountable obstacle for many drugs, including antibiotics, antineoplastic agents, and a variety of CNS-active drugs, especially neuropeptides. One of the possibilities to overcome this barrier is a drug delivery to the brain using nanoparticles. Drugs that have successfully been transported into the brain using this carrier include the hexapeptide dalargin, the dipeptide kytorphin, loperamide, tubocurarine, the NMDA receptor antagonist MRZ 2/576, and doxorubicin.

The use of NPs to deliver drugs to the brain across the BBB may provide a significant advantage to current strategies. The primary advantage of NP carrier technology is that NPs mask the BBB limiting characteristics of the therapeutic drug molecule. Furthermore, this system may slow drug release in the brain, decreasing peripheral toxicity. Various factors that influence the transport include the type of polymer or surfactant, NP size, and the drug molecule. Use of metallic NPs such as AuNPs is associated with risk of neurotoxicity and special precautions such as coating of NPs are required to prevent this. Other nanomaterials used for delivery across BBB include carbon nanotubes, dendrimers, lipid NPs, liposomes, micelles, nanogels, PLGA, poly- ε -caprolactone, and polymeric NPs.

Carbon Nanotubes for Drug Delivery to the CNS

Suitability of functionalized carbon nanotubes (fCNTs) for drug delivery to the CNS has been investigated. fCNTs can directly penetrate cell membranes in an energyindependent manner possibly due to their 'needle-like' structure. SWCNTs are also endocytosed through Rac1-GTPase mediated macropinocytosis in normal endothelial cells (Bhattacharya et al. 2012). MWCNTs can be internalized into cells by any one of three mechanisms: (1) individually via membrane wrapping; (2) individually by direct membrane translocation; and (3) in clusters within vesicular compartments (Al-Jamal et al. 2011). At early time points following intracellular translocation, the authors observed accumulation of nanotube material within various intracellular compartments, and were able to escape vesicular (phagosome) entrapment in primary human macrophages by translocating directly into the cytoplasm.

Ability of a MWCNT functionalized with fluorescein isothiocyanate (MWCNT-FITC) was assessed as a prospective CNS-targeting drug delivery system to permeate BBB (Shityakov et al. 2015). Results show that the MWCNT-FITC conjugate can penetrate microvascular cerebral endothelial monolayers; its concentrations in the Transwell® (Corning Inc) system were fully equilibrated after 48 h. Cell viability test, together with phase-contrast and fluorescence microscopies, did not detect any signs of MWCNT-FITC toxicity on the cerebral endothelial cells. These microscopic techniques also revealed the intracellular localization of fluorescent MWCNT-FITCs apart from their massive nonfluorescent accumulation on the cellular surface due to nanotube lipophilic properties. In addition, the 1000 ps molecular dynamics simulation in vacuo discovered the phenomenon of CNT aggregation driven by van der Waals forces via MWCNT-FITC rapid dissociation as an intermediate phase.

Amino-functionalized (MWNTs-NH³⁺) can cross the BBB in an in vitro BBB model comprised of primary porcine brain endothelial cells (PBEC) and primary rat astrocytes, as well as in vivo following a systemic administration of radiolabeled fMWNTs (Kafa et al. 2015). TEM confirmed that MWNTs-NH³⁺ crossed the PBEC monolayer via energy-dependent transcytosis. A complete crossing of the in vitro BBB model was observed after 48 h, which was further confirmed by the presence of MWNTs-NH³⁺ within the astrocytes. Capillary depletion confirmed presence of fMWNT in both brain capillaries and parenchyma fractions. These results pave the way for use of CNTs as nanocarriers for delivery of drugs and biologics to the brain, after systemic administration.

Future work should focus on better understanding of the interaction of fCNTs with the BBB and neural tissues, and information about the uptake mechanisms will be useful for the design and development of fCNTs-based specific targeted drug delivery systems for the brain (Wang and Al-Jamal 2015).

Nanovesicles for Transport Across BBB

According to US patent application #20070160658, scientists at the Ben-Gurion University of the Negev, Israel are developing a targeting moiety conjugated to the nanovesicle, which comprises a therapeutic composition. These nanovesicles are useful in treatment of a wide spectrum of disorders. This technology solves the problem of transport through the BBB by using nanovesicles that can cross the BBB and which carry the desired drugs by using a targeted delivery mechanism where the drug will be released from the vesicle in the brain. The drug to be delivered is encapsulated within stable nanosized vesicles (20-100 nm) possessing surface moieties that facilitate the release of the drug at target sites, such as the brain. The method of targeting is based on head groups that are selectively cleaved at the target site by enzymatic activity, thus releasing the encapsulated material primarily at the target organ. Injection of an encapsulated analgesic peptide, encephalin, into mice showed an analgesic effect comparable to morphine, while encephalin in its free form did not to penetrate the BBB, and had no effect. Potential applications of this technology include cancer, pain, and neurodegenerative diseases such as Alzheimer's and Parkinson's. Advantages are:

- Vesicles are stable and flexible, allowing penetration through biological barriers
- Unique surface chemistry allows the incorporation of selective targeting proteins
- The targeting mechanism allow better precision in drug delivery by unloading drug from the vesicle only in predetermined location characterized by unique enzyme which causes drug release from the vesicle.
- An experimental study in xenotransplanted zebrafish model of brain cancer has shown that brain endothelial cell derived exosomes can be used as a carrier for brain delivery of anticancer drug for the treatment of brain cancer (Yang et al. 2015).

Polymeric Nanoparticles as Carriers for CNS Drug Delivery

Polymeric nanoparticles have been shown to be promising carriers for CNS drug delivery due to their potential both in encapsulating drugs, hence protecting them from excretion and metabolism, and in delivering active agents across the BBB without inflicting any damage to the barrier (Tosi et al. 2008). Polymeric NPs for delivery across BBB should have the following ideal properties: biocompatible, non-toxic, non-thrombogenic, and non-immunogenic (Martin-Banderas et al. 2011).

Mechanism of the Nanoparticle-Mediated Transport of the Drugs Across the BBB

The mechanism of the nanoparticle-mediated transport of the drugs across the BBB at present is not fully elucidated. The most likely mechanism is endocytosis by the endothelial cells lining the brain blood capillaries. Nanoparticle-mediated drug

transport to the brain depends on the overcoating of these materials with polysorbates, especially polysorbate 80, which seems to lead to the adsorption of apolipoprotein E from blood plasma onto the nanoparticle surface. The particles then seem to mimic low density lipoprotein (LDL) particles and could interact with the LDL receptor leading to their uptake by the endothelial cells. After this the drug may be released in these cells and diffuse into the brain interior or the particles may be transcytosed. Other processes such as tight junction modulation or P-glycoprotein (Pgp) inhibition also may occur. Moreover, these mechanisms may run in parallel or may be cooperative thus enabling a drug delivery to the brain.

Transcytosis of Transferrin-Containing Nanoparticles Across the BBB

Transferrin (Tf)-containing gold nanoparticles can reach the brain parenchyma from systemic administration in mice through a receptor-mediated transcytosis pathway. This transport is aided by tuning the nanoparticle avidity to Tf receptor (TfR), which is correlated with nanoparticle size and total amount of Tf decorating the nanoparticle surface (Wiley et al. 2013). Nanoparticles of both 45 nm and 80 nm diameter reach the brain parenchyma, and their accumulation there (visualized by silver enhancement light microscopy in combination with TEM imaging) is observed to be dependent on Tf content (avidity); nanoparticles with large amounts of Tf remain strongly attached to brain endothelial cells, whereas those with less Tf are capable of both interacting with TfR on the luminal side of the BBB and detaching from TfR on the brain side of the BBB. The requirement of proper avidity for nanoparticles to reach the brain parenchyma is consistent with recent behavior observed with transcytosing antibodies that bind to TfR.

Nanotechnology-Based Strategies for Drug Delivery Across BBB

Several strategies for transporting drugs across the BBB are based on nanobiotechnology. By designing well controlled and appropriate preclinical and clinical translational studies, use of nanotechnologies for safely, efficiently, and specifically delivering drugs and other molecules across the BBB may prove one of their highest impact contributions to clinical neuroscience. Two of these are in commercial development: G-technology and LipoBridge.

G-Technology®

G-Technology® (to-BBB) platform utilizes nanoliposomes coated with glutathioneconjugated PEG to mediate safe targeting and enhanced delivery of drugs to the brain. Glutathione, an endogenous tripepeptide transporter, is highly expressed on the BBB. Intravenous injections of PEGylated liposomes are already on the market (Doxil), and high dosages of glutathione in supportive therapy in cancer as well. Glutathione, a natural anti-oxidant, is found at high levels in the brain and its receptor is abundantly expressed at the BBB. Therefore, glutathione minimizes adverse effects such as adverse immunological reactions or interference with essential physiological pathways. None of the other technologies for delivery of drugs to the brain have the favorable pharmacokinetic and safety profile of the G-Technology®. This technology utilizes an endogenous receptor-mediated endocytosis mechanism in combination with nanosized drug-loaded liposomes. This approach is unique in that it does not require drug modification and at the same time gives rise to metabolic protection during transport and increased bioavailability at the target site.

LipoBridgeTM Technology

LipoBridgeTM (Genzyme Pharmaceuticals) temporarily and reversibly opens tight junctions to facilitate transport of drugs across the BBB and into the CNS. LipoBridge itself forms a clear suspension of nanoparticles in water and can solubilize or stabilize some drugs, is non-immunogenic and is excreted unmetabolized. It has been demonstrated in several laboratories that intracarotid injections of a simple mixture of LipobridgeTM and model compounds or pharmaceutical actives can deliver these actives into one or both hemispheres of the brain allowing for increased concentration in a selected hemisphere. It can be administered orally as well as intravenously. LipoBridge has been used to administer anticancer drugs for brain cancer in animals. Safety clinical studies in humans are in progress.

Nanotechnology-Based Drug Delivery to Brain Tumors

The focus of this section is glioblastoma multiforme (GBM), a primary malignant tumor of the brain. Treatment of GBM is one of the most challenging problems. Surgery remains the basic treatment in which the bulk of the tumor is removed and the peripheral infiltrating part is the target of supplementary treatments. GBM is not easily targeted but advances in nanobiotechnology have improved the prospects of delivery of therapeutics to GBM (Jain 2007).

Intravenous Gene Delivery with Nanoparticles into Brain Tumors

Brain tumors may be amenable to gene therapy with cytotoxic genes, such as the proapoptotic Apo2 ligand/tumor necrosis factor-related apoptosis-inducing ligand (Apo2L/TRAIL). Gene therapy of gliomas ideally employs intravenously given vectors, thus excluding viral vectors as they cannot cross the BBB. Cationic albumin-conjugated pegylated nanoparticles (CBSA-NP) have been synthesized and shown to accumulate in mouse brain cells upon IV administration. Plasmid

pORF-hTRAIL (pDNA) has been incorporated into CBSA-NP, and the resulting CBSA-NP-hTRAIL was evaluated as a nonviral vector for gene therapy of gliomas (Lu et al. 2006). Thirty minutes after IV administration of CBSA-NP-hTRAIL to BALB/c mice bearing intracranial C6 gliomas, CBSA-NP-hTRAIL colocalized with glycoproteins in brain and tumor microvasculature and, via absorptive-mediated transcytosis, accumulated in tumor cells. At 24 and 48 h after intravenous administration of CBSA-NP-hTRAIL, respectively, hTRAIL mRNA and protein were detected in normal brain and tumors. Furthermore, repeated IV injections of CBSA-NP-hTRAIL induced apoptosis in vivo and significantly delayed tumor growth. In conclusion, this study indicates that CBSA-NP-hTRAIL is a promising candidate for noninvasive gene therapy of malignant glioma.

Micelles for Delivery of Chemotherapy to Brain Tumors

Micelles loaded with temozolomide (TMZ) have been designed to increase the delivery of this drug to the malignant brain tumors. In an experimental study on orthotopic gliomas implanted in mice, pH-responsive micelles composed of distearoyl phosphoethanolamine-PEG-2000-amine and N-palmitoyl homocysteine and functionalized on the surface with platelet-derived growth factor (PDGF) peptide and Dylight 680 fluorophore were used for delivery of TMZ (Miller et al. 2016). PDGF-micelles containing TMZ demonstrated specific uptake and accumulation in tumors with increased killing of tumor cells compared with untargeted micelles. Targeted micelle-based drug carrier systems have a potential for delivery of a wide variety of hydrophobic drugs to the brain tumors, thereby reducing its systemic toxicity.

Multifunctional Nanoparticles for Treating Brain Tumors

An early approach combined two promising methods for diagnosing and treating cancer, creating a targeted multifunctional polymer nanoparticle that successfully images and kills brain tumors in laboratory animals (Reddy et al. 2006). The team developed of a 40 nm diameter polyacrylamide nanoparticle loaded with Photofrin, a photosensitizing agent, and iron oxide. When irradiated with laser light, Photofrin, which is used to treat several types of cancer, including esophageal, bladder, and skin cancers, triggers the production of reactive oxygen species that destroy a wide variety of molecules within a cell. The iron oxide nanoparticles function as a MRI contrast agent. As the targeting agent, the researchers used a 31-amino-acid long peptide, which targets a receptor found on the surface of new blood vessels growing around tumors and triggers cell uptake of nanoparticles attached to it. Researchers tested the nanoparticles in cell cultures and animal models. The studies showed that the nanoparticles traveled to the tumor, resulting in less Photofrin exposure throughout the body and enhanced exposure within the tumor. This allowed a larger window for activating the drug with light, which was accomplished by threading a fiber optic laser into the brain. In humans, this approach could reduce or eliminate a common side effect of photodynamic therapy, in which healthy skin becomes sensitive to light. This approach has not been used in human patients so far.

Nanoparticles for Delivery of Drugs to Brain Tumors Across BBB

Nanoparticles may be especially helpful for the treatment of malignant brain tumors. Nanoparticles made of poly(butyl cyanoacrylate) (PBCA) or PLGA coated with polysorbate 80 or poloxamer 188 enable the transport of cytostatics such as doxorubicin across the BBB. Following intravenous injection to rats bearing intracranial glioblastoma, these particles loaded with doxorubicin significantly increased the survival times and led to a complete tumor remission in 20–40% of the animals (Kreuter and Gelperina 2008). Moreover, these particles considerably reduced the dose-limiting cardiotoxicity and the testicular toxicity of this drug. The drug transport across the BBB by nanoparticles appears to be due to a receptor-mediated interaction with the brain capillary endothelial cells, which is facilitated by certain plasma apolipoproteins adsorbed by nanoparticles in the blood.

Superparamagnetic iron oxide nanoparticles (SPION) conjugates have been used to locate brain tumors earlier and more accurately than current methods and to target the tumors. To enhance the specific targeting capability of the nanoparticles, folic acid has been used as the targeting agent combined with PEG serving to improve biocompatibility of nanoparticles. Coating nanoparticles with PEG-FA significantly enhances the intracellular uptake of nanoparticles by target cells. A variety of small molecules to target receptors on tumor and chemotherapy agents, can be attached to the nanoparticles.

MRI can detect the incorporation into brain tumor vasculature of systemically administered bone marrow stem cells labeled with SPIONS as part of ongoing angiogenesis and neovascularization. This technique can be used to directly identify neovasculature in vivo and to facilitate gene therapy by noninvasively monitoring these cells as gene delivery vectors.

A polymeric nanobioconjugate based on biodegradable, nontoxic, and nonimmunogenic polymalic acid as a universal delivery nanoplatform is used for design of a nanomedicine for intravenous treatment of brain tumors (Ding et al. 2010). The polymeric drug passes through the BTB and tumor cell membrane using tandem monoclonal antibodies targeting the BTB and tumor cells. The next step for polymeric drug action is inhibition of tumor angiogenesis by specifically blocking the synthesis of a tumor neovascular trimer protein, laminin-411, by attached antisense oligonucleotides, which are released into the target cell cytoplasm via pH-activated trileucine, an endosomal escape moiety. Introduction of a trileucine endosome escape unit results in significantly increased antisense oligonucleotide delivery to tumor cells, inhibition of laminin-411 synthesis, specific accumulation in brain tumors, and suppression of intracranial glioma growth compared with pH-independent leucine ester. The availability of a systemically active polymeric drug delivery system that crosses BTB, targets tumor cells, and inhibits tumor growth is a promising strategy of glioma treatment.

NP Delivery Across the BBB for Imaging and Therapy of Brain Tumors

In vivo application of nanoparticle-based platforms in brain tumors is limited by insufficient accumulation and retention within tumors due to limited specificity for the target, and an inability to traverse the BBB. A nanoprobe has been designed that

can cross the BBB and specifically target brain tumors in a genetically engineered mouse model, by using in vivo magnetic resonance and biophotonic imaging, as well as histologic and biodistribution analyses (Veiseh et al. 2009). The nanoprobe is made of an iron oxide nanoparticle coated with biocompatible PEG-grafted chitosan copolymer, to which a tumor-targeting agent, chlorotoxin (a small peptide isolated from scorpion venom), and a near-IR fluorophore are conjugated. The particle was about 33 nm in diameter when wet, i.e. about a third the size of similar particles used in other parts of the body. The nanoprobe shows an innocuous toxicity profile and sustained retention in tumors. The nanoparticles remained in mouse tumors for up to 5 days and did not show any evidence of damaging the BBB. With the versatile affinity of the targeting ligand and the flexible conjugation chemistry for alternative diagnostic and therapeutic agents, this nanoparticle platform can be potentially used for the diagnosis and treatment of a variety of brain tumors. The fluorescent nanoparticles improved the contrast between the tumor tissue and the normal tissue in both MRI and optical imaging, which are used during surgery to see the tumor boundary more precisely. Precise imaging of brain tumor margins is important because patient survival for brain tumors is directly related to the amount of tumor that can be resected.

Nano-imaging could also help with early detection of brain tumors. Current imaging techniques have a maximum resolution of 1 millimeter. Nanoparticles could improve the resolution by a factor of 10 or more, allowing detection of smaller tumors and earlier treatment. Future research will evaluate this nanoparticle's potential for treating tumors.

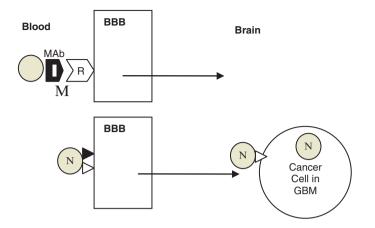
NP-Based Targeted Delivery of Chemotherapy Across the BBB

Passive targeting of brain tumors has several limitations. Some of techniques used for facilitating transport of therapeutic substances across the BBB involve damage to the BBB, which is not desirable.

Technologies based on nanoparticle-based targeted delivery of anticancer drugs across the BBB are promising. A few are in clinical trials and others are in development. Introduction of personalized medicine along with expression profiling of tumors will enable classification of patients by their genetic profile and stage of development, which may bring novel, more efficient molecular targets to design/improve targeted nanoformulations for glioma patients (Pinto et al. 2017). A concept of targeted drug delivery to GBM across the BBB is shown in Fig. 9.2.

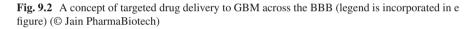
PLA Nanoparticles for Controlled Delivery of BCNU to Brain Tumors

BCNU-loaded biodegradable PLA nanoparticles have been combined with transferrin, an iron-transporting serum glycoprotein, which binds to receptors expressed on surface of glioma cells (Kang et al. 2009). In vitro drug release studies have demonstrated that BCNU-loaded PLA nanoparticles show certain sustained release characteristics. The biodistribution of transferrin -coated nanoparticles, investigated



Nanoparticle (N) combined with a monoclonal antibody (MAb) for receptor (R) crosses the blood brain barrier (BBB) into brain by Trojan horse approach

N with a ligand targeting BBB traverses the BBB by receptor-mediated transcytosis. Ligand docks on a cancer cell receptor and N delivers anticancer payload to the cancer cell in glioblastoma multiforme (GBM)



by 99Tc-labeled SPECT showed that the surface-containing transferrin PLA nanoparticles were concentrated in the brain and no radioactive foci could be found outside the brain. Inhibition of tumor growth in the C6 tumor-bearing animal model showed that BCNU-loaded PLA NPs had stronger cytotoxicity and prolonged the average survival time of rats. In contrast to the BCNU wafer approach, the stereo-tactic method of delivery used in this study may be useful in the development of a new method for delivery of chemotherapy to malignant brain tumors.

Nanoparticles as Nonviral Vectors for CNS Gene Therapy

Viral vectors for gene delivery to neuronal cells can achieve high transfection efficiency, but problems, such as host immune responses and safety concerns, currently restrict their use in humans. Nonviral nanoparticles represent a good alternative to viral vectors, but transfection efficiency need to reach levels that would be relevant for therapeutic purposes.

Silica Nanoparticles for CNS Gene Therapy

Organically modified silica (ORMOSIL) nanoparticles, because of the presence of lipophilic groups, can host active lipophilic molecules inside, as well as form electrostatic complex with therapeutic agents such as genes on their surface (Diksha 2012).

They have numerous potential applications in diagnostic imaging, as well as drug, and gene delivery. ORMOSIL nanoparticles (≈ 30 nm) can be used as as nonviral vectors for efficient in vivo gene delivery without toxic effects and with efficacy equaling or exceeding that obtained by using viral vectors. Highly monodispersed, stable aqueous suspension of nanoparticles, surface-functionalized with amino groups for binding of DNA, have been prepared and characterized. The effect on the mouse brain of intraventricular and intracerebral stereotaxic injections of nanoparticles, complexed with plasmid DNA encoding for EGFP (enhanced green fluorescent protein), can be studied. Use of an optical fiber in vivo imaging technique enables observation of the brain cells expressing genes without having to sacrifice the animal. The ORMOSIL-mediated transfections have also been used to manipulate the biology of the neural stem/progenitor cells in vivo. Transfection of a plasmid expressing the nucleus-targeting fibroblast growth factor receptor type 1 results in significant inhibition of the in vivo incorporation of bromodeoxyuridine into the DNA of the cells in the subventricular zone and the adjacent rostral migratory stream. Targeted dopamine neurons, which degenerate in Parkinson disease, take up and express a fluorescent marker gene, demonstrate the ability of nanoparticle technology to effectively deliver genes to specific types of cells in the brain. The gene-nanoparticle complexes were shown to activate adult brain stem cells in vivo, which could be effective replacements for those destroyed by neurodegenerative diseases. Thus, ORMOSIL nanoparticles have a potential for effective therapeutic manipulation of the neural stem/progenitor cells as well as in vivo targeted brain therapy. The structure and composition of ORMOSIL enables development of an extensive library of tailored nanoparticles to target gene therapies for different tissues and cell types.

Cationic Lipids for CNS Gene Therapy

Cationic lipids show very low transfection efficiency in neurons. They are useful for single cell studies, but not for lack-of-function studies. Generally, cationic lipids are toxic to neurons, although different lipidic formulations can decrease toxicity. They are not effective for gene delivery to the brain when administered intravenously, although 'Trojan horse' liposomes can be an exception.

Polyethylenimine-Based Nanoparticles for CNS Gene Therapy

Polyethylenimine (PEI) nanoparticles have higher transfection efficiency (20%) than cationic lipids in neurons, but this is still very low for therapeutic purposes. At least 70–80% transfection efficacy is required for removal of a protein. These nanoparticles are toxic for neurons and modifications of the molecule, such as PEGylation, are required to decrease neurotoxicity. Moreover, PEI-based nanoparticles are only effective for gene delivery when injected locally, which precludes their development for clinical use at present.

Dendrimers for CNS Gene Therapy

Dendrimers can deliver nucleic acids to the brain by exploiting the specific transport systems expressed on the BBB and the brain uptake of nucleic acids carried by targeted dendrimers is increased compared with nontargeted dendrimers (Somani and Dufès 2014). Dendrimers are capable of very efficient neuronal transfection in vitro (transfection efficiencies of 75% have been achieved) with low toxicity when external amino groups are masked by surface functionalization. Further developments need to be carried out to enable efficient BBB crossing to deliver genetic material to neurons and glial cells. Dendrimers are the most promising particles for genetic material delivery to the CNS either alone or in combination with carbon-based nanoparticles (nanotubes and nanohorns).

Carbon Nanotubes for CNS Gene Therapy

CNTs avoid endosomes and, once functionalized, their solubility is increased to make them biocompatible and capable of delivery of genetic material to different cells. Coupled to dendrimers, CNTs represent a new concept that can play a relevant role in gene therapy in the nervous system, if toxicological issues are solved (Posadas et al. 2010). Once the safety has been established, CNT based vectors should be able to perform an "enhanced" gene transfer in target cells. Potential applications include cerebral ischemia and Rett syndrome.

Nanoparticle-Based Drug Delivery to the Inner Ear

Drug delivery to the inner ear is important for the treatment of inner ear disorders such as those involving hearing. Another disorder, tinnitus, is a problem in management and several innovative approaches are under investigation. An obstacle to effective treatment of inner ear diseases is the atraumatic delivery of therapeutics into inner ear perilymph. It is feasible to use SPIONs as drug delivery vehicles. As a minimally-invasive approach, intratympanic delivery of multifunctional nanoparticles (MFNPs) carrying genes or drugs to the inner ear is a future therapy for treating inner ear diseases, including sensorineural hearing loss (SNHL) and Meniere's disease. Liposome nanoparticles encapsulating gadolinium-tetra-azacyclo-dodecanetetra-acetic acid (LPS + Gd-DOTA) are visible by MRI in the inner ear in vivo after either intratympanic or intracochlear administration demonstrating transport from the middle ear to the inner ear and their distribution in the inner ear (Zou et al. 2010). Passive diffusion of fluorescent NPs through the round window membrane (RWM) within the freshly frozen human temporal bone has been demonstrated and these NPs were subsequently found to be distributed in the sensory hair cells, nerve fibers and to other cells of the cochlea (Roy et al. 2012). Nontoxic NPs have a great potential for controlled drug delivery to the human inner ear across the RWM.

Nanotechnology-Based Devices and Implants for CNS

Nanoparticle-mediated drug delivery to the brain, as described in previous sections, will minimize the need for use of invasive delivery devices but there will still be need for implants and direct delivery of drugs to the brain and the cerebral ventricles. Nanomaterials, because of their action in preventing the formation of scar due to astrocyte proliferation, would improve the construction of nonreactive cerebroventricular catheters for administration of drugs into the cerebral ventricles. Nano-engineered probes can deliver drugs at the cellular level using nanofluidic channels.

Nanobiotechnology and Neuroprotection

Nanoparticles can improve drug delivery to the CNS and facilitate crossing of BBB and more precisely target a CNS injury site. These technologies were described in Chap. 6 and the topic of neuroprotection is dealt with in detail in a handbook on this topic (Jain 2011). QD technology has been used to gather information about how the CNS environment becomes inhospitable to neuronal regeneration following injury or degenerative events by studying the process of reactive gliosis. Other research is looking at how QDs might spur growth of neurites by adding bioactive molecules to the QDs, in a way to provide a medium that will encourage this growth in a directed way. At a time that there is concern for neurotoxicity of nanoparticles, it is often not realized that some nanoparticles have a neuroprotective effect as shown in Table 9.1.

Nanomaterial	Mechanism of neuroprotective effect
Cadmium Telluride (CdTe) NPs	Prevent A β formation in Alzheimer disease based on the multiple binding to A β oligomers
Carbon NP-based antioxidants	PEG-functionalized hydrophilic carbon cluster carbon nanoparticles show antioxidant activity
Ceria NPs	Protect neurons from free radical-mediated damage
Fullerene derivatives	ABS-75, attached to an NMDA receptor antagonist, combines antioxidant and anti-excitotoxic properties and can block axonal damage
Gold NPs	Immunosuppressive effect to control damage from neuroinflammation as secondary effect of TBI
PLGA nanoparticles loaded with SOD	Stability of the encapsulated enzyme and its better neuronal uptake
Redox polymer NPs	Ameliorates brain edema and oxidative damage
Yttrium oxide NPs	More effective free radical scavengers than ceria NPs

 Table 9.1
 Neuroprotective nanoparticles

Neuroprotection Due to Antioxidant Effect of Nanoparticles

Three of the most-studied nanoparticle redox reagents at the cellular level, are rare earth oxide nanoparticles (particularly cerium), fullerenes and carbon nanotubes. Ceria nanoparticles from anthanide series have several unique properties that make them highly efficient redox reagents. Several studies have reported the ability of ceria nanoparticles to mitigate oxidative stress at the biological level. Ceria nanoparticles also protect neurons from free radical-mediated damage initiated by ultraviolet (UV) light, H₂O₂ and excitotoxicity, possibly by free radical scavengingaction. When compared with single doses of other free radical scavengers, such as vitamin E, melatonin and n-acetyl cysteine, ceria nanoparticles demonstrate significantly greater neuroprotection after a 5- and 15-min UV insult. A single dose of nanoparticles delivered up to 3 h post-injury also affords neuroprotection. Ceria nanoparticles were also effective in reducing cell death associated with γ -irradiation. No toxicity is observed with ceria nanoparticle sizes of 6 and 12 nm and yttrium oxide nanoparticles are even more effective than ceria. Ceria nanoparticles larger than 30 nm or nitrates and sulfates of cerium do not have any significant effects. Several studies also suggest that ceria nanoparticles are potent antiinflammatory agents. Microglial cells, the immune cells of the brain, are 'activated' in response to neuronal damage and show an inflammatory response with release NO as well as IL-1 β . Treatment of injured organotypic cultures with ceria nanoparticles reduced their ability to activate microglia. Further, treatment of activated microglia with ceria nanoparticles reduces production of soluble factors that promoted death in uninjured neurons, including NO and IL-1β. Delivery of nanoparticles to the uninjured neurons also directly affords neuroprotection from the damaging effects of activated microglia. Thus, it appears that nanoparticles may blunt the inflammatory response in immune cells, as well as reduce inflammatory injury to non-immune cells. Study in a mouse hippocampal brain slice model of cerebral ischemia has shown that ceria nanoparticles reduce ischemic cell death by ~50%. The neuroprotective effects of nanoceria were due to a modest reduction in ROS in general, and $\sim 15\%$ reductions in the concentrations of superoxide and NO, specifically (Estevez et al. 2011). Nanoceria may be useful as a therapeutic intervention to reduce oxidative and nitrosative damage after a stroke.

PLGA nanoparticles loaded with SOD have neuroprotective effect up to 6 h after H2O2-induced oxidative stress, which appears to be due to the stability of the encapsulated enzyme and its better neuronal uptake after encapsulation (Reddy et al. 2008).

Animal studies with 1-MHz focused ultrasound coupled with microbubble produced intracerebral hemorrhage, showed that the redox polymer nanoparticle ameliorates brain edema, neurological deficit and oxidative damage (Chonpathompikunlert et al. 2012). The results sugges that redox polymer nanoparticle is a potential neuroprotective agent.

Water-soluble derivatives of buckminsterfullerene C60 derivatives are a unique class of nanoparticle compounds with potent antioxidant properties. Studies on one class of these compounds, the malonic acid C60 derivatives (carboxyfullerenes), indicated that they can eliminate both superoxide anion and H_2O_2 , and are effective

inhibitors of lipid peroxidation, as well. Carboxyfullerenes demonstrate robust neuroprotection against excitotoxic, apoptotic and metabolic insults in cortical cell cultures. They are also capable of rescuing midbrain dopaminergic neurons from both MPP(+) and 6-hydroxydopamine-induced degeneration. Although there is limited in vivo data on these compounds, systemic administration of the C3 carboxyfullerene isomer has been shown to delay motor deterioration and death in a mouse model of familial ALS. Ongoing studies in other animal models of CNS disease states suggest that these novel antioxidants are potential neuroprotective agents for other neurodegenerative disorders including PD.

PEG-functionalized hydrophilic carbon cluster carbon (PEG-HCCs) nanoparticles show antioxidant activity (Nilewski et al. 2015). PEG-HCCs can be targeted through noncovalent antibody delivery or through covalently bound peptide recognition, thereby minimizing nanoparticle dosages. PEG-HCCs have demonstrated neuroprotective in preclinical models of TBI and stroke indicating their clinical potential.

Neuroprotective Nanoparticles that Inhibit Neuroinflammation

Gold salts, known to have an immunosuppressive effect, have been considered for treatment of TBI, which results in loss of neurons caused not by the initial injury but also by the resulting neuroinflammation as a secondary effect. The systemic use of gold salts is limited by nephrotoxicity. However, implants of pure metallic gold release gold ions, which do not spread in the body, but are taken up by cells near the implant. This is a safer method of using to reduce local neuroinflammation. Release or dissolucytosis of gold ions from metallic gold surfaces requires the presence of disolycytes i.e. macrophages and the process is limited by their number and activity. In one study, the investigators injected 20-45 micron gold particles into the neocortex of mice before generating a crvo-injury (Larsen et al. 2008). Comparison of gold-treated and untreated cryolesions showed that the release of gold reduced microgliosis and neuronal apoptosis accompanied by a transient astrogliosis and an increased neural stem cell response indicating antiinflammatory and Neuroprotective effect. Intracerebral application of metallic gold as a pharmaceutical source of gold ions bypasses the BBB and enables direct drug delivery to inflamed brain tissue. The method of delivery is invasive and a gold implant could produce foreign body reaction leading to an epileptic focus. This can be refined by use of gold nanoparticles.

Neuroprotective Nanoparticles that Inhibit Aß Formation

Cadmium Telluride (CdTe) NPs can efficiently prevent $A\beta$ formation, a pathological feature of Alzheimer disease (AD), based on the multiple binding to $A\beta$ oligomers CdTe NPs (Yoo et al. 2011). By introducing tetrahedral CdTe NPs that were comparable in size with growing fibrils, the researchers discovered that the $A\beta$ plaque readily bonded to them, and CdTe NP geometry was strongly distorted resulting in

complete inhibition of further growth of $A\beta$ fibrils. CdTe NPs can inhibit the $A\beta$ fibril formation in minute quantities with much greater efficiency; 1 CdTe NP can capture more than 100 amyloid peptides. This high efficiency of CdTe NPs is like some proteins that human body uses to prevent formation of $A\beta$ fibrils and protect itself against the progression of AD. These findings provide new opportunities for the development of drugs to prevent AD.

Nanobiotechnology for Regeneration and Repair of the CNS

Nanobiotechnology applications, aimed at the regeneration and neuroprotection of the CNS, will significantly benefit from basic nanotechnology research conducted in parallel with advances in cell biology, neurophysiology, and neuropathology. The aim is to help neuroscientists better understand the physiology of and develop treatments for disorders such as traumatic brain injury (TBI), spinal cord injury (SCI), degenerative retinal disorders, and neurodegenerative disorders such as Alzheimer's disease (AD) and Parkinson's disease (PD).

Nanowire Neuroprosthetics with Functional Membrane Proteins

Living organisms use a sophisticated arsenal of membrane receptors, channels, and pumps to control signal transduction to a degree that is unmatched by manmade devices. Electronic circuits that use such biological components could achieve drastically increased functionality; however, this approach requires nearly seamless integration of biological and manmade structures. A versatile hybrid platform for such integration has been constructed that uses shielded nanowires coated with a continuous lipid bilayer (Misra et al. 2009). When shielded silicon nanowire transistors incorporate transmembrane peptide pores gramicidin A and alamethicin in the lipid bilayer they can achieve ionic to electronic signal transduction by using voltagegated or chemically gated ion transport through the membrane pores. The membrane pore could be opened and closed by changing the gate voltage of the device to enable monitor specific transport and to control the membrane protein. The work shows promise for enhancing biosensing and diagnostics tools, and neural prosthetics such as cochlear implants.

Nanotube-Neuron Electronic Interface

Thin films of CNTs deposited on transparent plastic can also serve as a surface on which cells can grow and which could potentially serve as an electrical interface between living tissues and prosthetic devices or biomedical instruments. Electrical communication at the interface has been shown by stimulating 2 different types of cells: neuroblastoma cells and neurons cultured from experimental rats (Liopo et al. 2006). Both cell types were placed on 10-layer-thick "mats" of SWCNTs deposited on transparent plastic. This enabled the use of a microscope to position a tiny electrode next to individual cells and record their responses to electrical pulses transmitted through the SWCNTs. The scientists also studied how different kinds of SWCNTs affected the growth and development of neuroblastoma cells. They compared cells placed on mats made of "functionalized" SWCNTs, CNTs with additional molecules attached to their surfaces that may be used to guide cell growth or customize nanotube electrical properties, to cells cultured on unmodified "native" CNTs and conventional tissue culture plastic. Native CNTs supported neuron attachment and growth well better than the two types of functionalized CNTs tested. Next step in the research is to find a way to functionalize the CNTs to improve neuron attachment and communication and make these surfaces more biocompatible. If CNTs turn out to be sensitive enough to record ongoing electrical activity in cells, they could form the basis of a device that can both sense and deliver stimuli to cells for prosthetic control.

A study shows that CNTs supports the growth of nerve fibers, bridging segregated neural explants and providing a functional re-connection (Usmani et al. 2016). The material is biocompatible in vivo and implanting it into the brain of small rodents does not cause large scars or a marked immune response. It is a potential nervous system prosthesis.

Role of Nanobiotechnology in Regeneration and Repair Following CNS Trauma

Repair and regeneration following CNS trauma requires a multifaceted approach (Jain 2016). Roles of nanobiotechnology in various strategies for regeneration and repair following CNS trauma are listed in Table 9.2.

Nanofibers as an Aid to CNS Regeneration by Neural Progenitor Cells

One approach to growing nerve cells in tissue cultures is to encapsulate neural progenitor cells were in vitro within a 3D network of nanofibers formed by self-assembly of peptide amphiphile molecules. The self-assembly of nanofiber scaffold

Table 9.2 Role of nanobiotechnology in regeneration and repair following CNS trauma

Neuroprotective nanoparticles to prevent further damage		
	Nanofibers to provide scaffolds for regeneration and reducing or eliminating scar formation.	
Nanofibers for providing cues to axons for regeneration		

Nanoparticles for repair of injured neurons and nerve fibers by sealing them

Nanoparticles to track stem cells implanted to replace the loss and to promote growth of neural tissues Nanoparticle-based delivery of drugs to promote growth of neural tissues

is initiated by mixing cell suspensions in media with dilute aqueous solutions of the molecules, and cells survive the growth of the nanofibers around them. These nanofibers are designed to present to cells the neurite-promoting laminin epitope. Relative to laminin or soluble peptide, the artificial nanofiber scaffold induces very rapid differentiation of neural progenitor cells into neurons, while discouraging the development of astrocytes.

These new materials, because of their chemical structure, interact with cells of the CNS in ways that may help prevent the formation of scar due to astrocyte proliferation that is often linked to paralysis resulting from traumatic spinal cord injury (SCI). Silicon neural electrodes are engineered with a nanostructured form of silicon called porous silicon, which acts as a scaffold that reduces glial scarring from electrode implantation and enhances neural growth at the brain recording sites to create a superior interface with neurons. This would be useful in the procedure of electrode implantation in neurological disorders such as PD and epilepsy.

Peptide Nanostructures for Repair of the CNS

Peptide nanostructures containing bioactive signals offer novel therapies with potential impact on regenerative medicine. These nanostructures can be designed through self-assembly strategies and supramolecular chemistry, and can combine bioactivity for multiple targets with biocompatibility. It is also possible to multiplex their functions by using them to deliver proteins, nucleic acids, drugs and cells. Self-assembling peptide nanostructures can facilitate regeneration of the CNS. Other self-assembling oligopeptide technologies and the progress made with these materials towards the development of potential therapies have been reviewed elsewhere (Webber et al. 2010).

Nanobiotechnology for Repair and Regeneration Following TBI

Challenges of using a tissue engineering approach for regeneration in TBI include a complex environment and variables that are difficult to assess. For optimal benefit, the brain should be in a condition that minimizes immune response, inflammation and rejection of the grafted material. Tissue engineering, using a bioactive scaffold counters some of the hostile factors and facilitates integration of donor cells into the brain, but transplantation of a combination biologic construct to the brain has not yet been successfully translated into clinical use (Stabenfeldt et al. 2011).

The next generation of tissue engineering scaffolds for TBI may incorporate nanoscale surface feature dimensions, which mimic natural neural tissue. Nanomaterials can enhance desirable neural cell activity while minimizing unwanted astrocyte reactivity. Composite materials with zinc oxide nanoparticles embedded into a polymer matrix can provide an electrical stimulus when mechanically deformed through ultrasound, which can act as a cue for neural tissue regeneration (Seil and Webster 2010).

Nanoparticles for Repair Following SCI

SCI can lead to serious neurological disability and the most serious form of it is paraplegia or quadriplegia. Currently, over 250,000 persons in the US and several million worldwide are living with permanent disability due to chronic SCI. There are approximately 12,000 new cases of acute SCI in the US each year. Over 90% of acute SCI victims now survive their injuries and go on to become part of the chronic SCI population, living paralyzed for an average of more than 40 years after injury.

Local spinal cord lesions are often greatly enlarged by secondary damage, which is accompanied by additional massive cell death that involves neurons, microglia and macroglia and is virtually complete at 12 h. Immediate care involves stabilization of the patient's general condition by supportive measures. Surgery is carried out in some cases for removal of compressing lesions and stabilization of spinal fractures. Several neuroprotective strategies are under investigation. Stem cell therapies are also under investigation for neuroregeneration and nanoparticles can be used to track the course of stem cells. There is no therapeutic measure available currently that enhances functional recovery significantly.

Nanomaterials injected into the severed spinal cords of mice, enable them to walk again after several weeks of therapy. The nanomaterials used in these studies were designed to self-assemble into nanofibers, which provide the framework for regeneration of nerve fibers. In a nanofiber network, progenitor cells develop into neurons and not astrocytes that form scar tissue and hinder regeneration. The research offers new insights into the near-term research potential of nanotechnology and offers hope for patients with severe neuron damage due to other causes as well.

Repair of SCI by Nanoscale Micelles

Another key approach for repairing injured spinal cord is to seal the damaged membranes at an early stage. Axonal membranes injured by compression can be effectively repaired using self-assembled monomethoxy PEG-PLA di-block copolymer micelles (Shi et al. 2010). The micelles might be used instead of conventional PEG. A critical feature of micelles is that they combine two types of polymers, one being hydrophobic and the other hydrophilic, meaning they are either unable or able to mix with water. Because of the nanoscale size and the PEG shell of the micelles, they are not quickly filtered by the kidney or captured by the liver, enabling them to remain in the bloodstream long enough to circulate to damaged tissues.

Injured spinal tissue incubated with micelles (60 nm diameter) showed rapid restoration of compound action potential and reduced calcium influx into axons for micelle concentrations much lower than the concentrations of PEG, approximately 1/100,000th, for early-stage SCI. Intravenously injected micelles effectively recovered locomotor function and reduced the volume and inflammatory response of the lesion in injured rats, without any adverse effects. These results show that copolymer micelles can interrupt the spread of primary SCI damage with minimal toxicity. The research also showed that without the micelles treatment about 18% of axons recover in a segment of damaged spinal cord tested, whereas the micelles treatment

boosted the axon recovery to about 60%. The researchers used the chamber to study how well micelles repaired damaged nerve cells by measuring the "compound action potential," or the ability of a spinal cord to transmit signals.

The experiment mimics what happens during a traumatic SCI. Findings showed that micelles might be used to repair axon membranes damaged by compression injuries, a common type of spine injury. Dyed micelles were also tracked in rats, demonstrating that the nanoparticles were successfully delivered to injury sites. Findings also showed micelles-treated animals recovered the coordinated control of all four limbs, whereas animals treated with conventional PEG did not. Further research will include work to learn about the specific mechanisms that enable the micelles to restore function to damaged nerve cells.

Nanobiotechnology-Based Devices for Restoration of Neural Function

The remarkable optical and electrical properties of nanostructured materials are now considered to be a source for a variety of biomaterials, biosensing, and cell interface applications. Some of the characteristics of nanoparticles can be exploited to custom-build new materials from the bottom up with characteristics such as compatibility with living cells and the ability to turn light into tiny electrical currents that can produce responses in nerves. A study reports construction of a hybrid bionanodevice where absorption of light by thin films of quantum confined semiconductor nanoparticles of HgTe produced by the layer-by-layer assembly stimulate adherent neural cells via a sequence of photochemical and charge-transfer reactions (Pappas et al. 2007). The development opens the door to applying the unique properties of nanoparticles to a wide variety of light-stimulated nerve-signaling devices including the possible development of a nanoparticle-based artificial retina.

Nanobiotechnology-Based Artificial Retina

Although light signals have previously been transmitted to nerve cells using silicon (whose ability to turn light into electricity is employed in solar cells and in the imaging sensors of video cameras), nanoengineered materials promise far greater efficiency and versatility. It should be possible to tune the electrical characteristics of these nanoparticle films to get properties like color sensitivity and differential stimulation, which are needed for an artificial retina. Creation of an actual implantable artificial retina is, however, a long-range project. But, a variety of less complex applications are enabled by a tiny, versatile light-activated interface with nerve cells, e.g. ways to connect with artificial limbs and new tools for imaging, diagnosis and therapy. The main advantage of this technology is that remote activation by light is possible without cumbersome wire connections. This type of technology can provide noninvasive connections between the human nervous system and prostheses that are flexible, compact and reliable. Such tools will provide nanoneurology new capabilities that were not possible with conventional methods.

Role of Nanomedicine in Treatment of Neurodegenerative Disorders

Alzheimer's disease and Parkinson's disease are the most common neurodegenerative diseases worldwide. Currently available treatments have limited effectiveness, and new molecules such as growth factors, antioxidants and metal chelators are being developed as new therapeutic approaches. However, these molecules have difficulties to cross the BBB limiting their therapeutic effects. Nanobiotechnologybased drug delivery systems may enable targeted and sustained release of old as well as new treatments offering a novel strategy to treat these neurodegenerative disorders (Hernando et al. 2016). Nanoparticle-based targeted drug delivery methods are shown in Table 9.3.

Nanoneurosurgery

Neurosurgery is an extension of neurology involving surgery, nanodiagnostics and application of new technologies for treatment of neurological disorders. Advances in nanobiotechnology have already refined many surgical approaches to diseases of the nervous system and this new field can be called nanoneurosurgery. Examples are applications in brain cancer, neuroregeneration and CNS implants.

Therapy/type of	
nanomaterial	Application
Cell therapy	Encapsulated cells secreting neurotrophic factors tagged with nanoparticles for tracking passage in the brain for delivery to target
Gene therapy	Nanoparticles as vectors for gene or DNA to target tissues of CNS
Gold nanoparticles containing transferrin (Tf)	The particles can reach the brain parenchyma from systemic administration through a receptor-mediated transcytosis pathway, which is aided by avidity of Tf decorating the nanoparticle surface to Tf receptor (Wiley et al. 2013)
Nanoliposomes	Surface is modified by targeting agents to facilitate transport across BBB (Mufamadi et al. 2013)
Nanovesicles	Drug is encapsulated within stable nanovesicles that can cross the BBB and have surface moieties that facilitate the release of the drug at target sites in the brain
Polymeric nanoparticles	Polymer nanocapsules with functionalized surfaces can be used for targeted delivery to the brain (Kreuter 2014; Musyanovych and Landfester 2014)
Solid lipid nanoparticles	Intranasal delivery of rivastigmine loaded solid lipid nanoparticles (Shah et al. 2015)

 Table 9.3 Nanoparticles for targeted drug delivery in neurodegenerative disorders

Bucky Balls for Brain Cancer

Buckyballs (fullerenes) are under investigation to improve the ability of MRIs to locate brain tumors, and deliver a payload of radiation to destroy them. Experiments on rats have shown that buckyballs packed with the MRI contrast metal gadolinium can increase the sensitivity of MRI detection by at least 40-fold. This level of precision is reaching a point at which cancer cells that have spread beyond the margins of the tumor may become visible. Stray cells, left behind after surgery, are thought to be responsible for tumor relapse. Finding and removing these cells could improve a patient's chance of survival. The scientists have created a modified version of the buckyballs with a fluorescent metal atom called terbium, which could guide surgeons to remove tumors with greater precision. Addition of yet another metal, lutetium, would deliver a lethal dose of radiation to the cancer cells, including those missed by the surgeon. The research is a few years away from testing in humans, but the potential is promising.

Electrospun Nanofiber Tubes for Regeneration of Peripheral Nerves

Several neural prostheses have been used to replace the loss of nervous tissue in peripheral nerve injuries by providing a path for regenerating nerve fibers. Most of these use rigid channel guides that may cause cell loss due to the lack of physiological local stresses exerted over the nervous tissue during the patient's movement. The electrospinning technique makes it possible to spin nanofiber flexible tubular scaffolds, with high porosity and surface/volume ratio. Electrospun tubes made of biodegradable polymers (a blend of PLGA/PCL) have been used to regenerate a 10-mm nerve gap in a rat sciatic nerve (Panseri et al. 2008). In most of the treated animals the electrospun tubes induced neural regeneration and functional reconnection of the two severed sciatic nerve tracts. Myelination occurred and no significant inflammatory responses were observed. Re-establishment of functional neuronal connections with re-innervation of the affected muscles was demonstrated by neural tracers and evoked potential recordings. These findings show that electrospun tubes, with additional biological coating or incorporated drugs are promising scaffolds for functional neural regeneration. They can be knitted in meshes and their mechanical properties can be tuned to provide biomimetic functionalization. Moreover, the conduits can be loaded with neurotrophic factors and seeded with stem cells.

Femtolaser Neurosurgery

Understanding how nerves regenerate is an important step towards developing treatments for human neurological disease, but investigation has so far been limited to complex organisms (mouse and zebrafish) in the absence of precision techniques for severing axons (axotomy). Femtosecond laser surgery has been used for axotomy in the roundworm *Caenorhabditis elegans* and these axons functionally regenerated after the operation (Yanik et al. 2004). Femtolaser acts like a pair of tiny "nanoscissors", which is able to cut nano-sized structures like nerve axons

The pulse has a very short length making the photons in the laser concentrate in one area, delivering a lot of power to a tiny, specific volume without damaging surrounding tissue. Once cut, the axons vaporize and no other tissue is harmed. The researchers cut axons they knew would impair the worms' backward motion. The worms couldn't move backwards after surgery. But within 24 h, most of the severed axons regenerated and the worms recovered backward movement, confirming that laser's cut did not damage surrounding tissue and allowed the neurons to grow a new axon to reach the muscle. Application of this precise surgical technique should enable nerve regeneration to be studied in vivo.

Graphene Technology for Neurosurgery

Uncoated graphene can be used as neuro-interface electrode without altering or damaging the neural functions such as signal loss or formation of scar tissue. Graphene-based substrates are permissive interfaces, even when uncoated by cell adhesion layers, retaining unaltered neuronal signaling properties, which makes them suitable for carbon-based neural prosthetic devices (Fabbro et al. 2016). They may be useful for restoring sensory function or paralysis in stroke or movement disorders of Parkinson disease patients. Graphene electrodes in body stay significantly more stable than currently used electrodes of tungsten or silicon because of their unique properties such as flexibility, biocompatibility, conductivity and lack of formation of reactive scar tissue. Graphene technology is expected to significantly impact several areas of neurosurgery, including neurooncology, neurointensive care, neuroregeneration research, peripheral nerve surgery, functional neurosurgery, and spine surgery (Mattei and Rehman 2014).

Nanofiber Brain Implants

Several brain probes and implants are used in neurosurgery. Examples are those for the management of epilepsy, movement disorders and pain. Many of these implants are still investigational. The ideal inert material for such implants has not yet been discovered. Silicon probes are commonly used for recording of electrical impulses and for brain stimulation. The body generally regards these materials as foreign and the probes get encapsulated with glial scar tissue, which prevents them from making good contact with the brain tissue.

An invitro study was done to determine cytocompatibility properties of formulations containing carbon nanofibers pertinent to neural implant applications (McKenzie et al. 2004). Substrates were prepared from four different types of carbon fibers, two

with nanoscale diameters (nanophase, or less than or equal to 100 nm) and two with conventional diameters (or greater than 100 nm). Within these two categories, both a high and a low surface energy fiber were investigated and tested. Astrocytes (glial scar tissue-forming cells) were seeded onto the substrates for adhesion, proliferation, and long-term function studies (such as total intracellular protein and alkaline phosphatase activity). Results provided the first evidence that astrocytes preferentially adhered and proliferated on carbon fibers that had the largest diameter and the lowest surface energy. Formulations containing carbon fibers in the nanometer regime limited astrocyte functions leading to decreased glial scar tissue formation. Positive interactions with neurons, and, at the same time, limited astrocyte functions leading to decreased gliotic scar tissue formation are essential for increased neuronal implant efficacy. Nanotubes, because of the interesting electronic properties and reduction in scar formation, hold great promise for replacing conventional silicon implants.

Nanoparticles as an Aid to Neurosurgery

A research team from Oregon Health & Science University (Portland OR) has shown that an iron oxide nanoparticle can outline not only brain tumors under MRI but also other lesions in the brain that may otherwise have gone unnoticed (Neuwelt et al. 2004). Ferumoxtran-10 (Combidex®, AMAG Pharmaceuticals Inc), a dextran-coated iron oxide nanoparticle, provides enhancement of intracranial tumors by MRI for more than 24 h and can be imaged histologically by iron staining. Each iron oxide nanoparticle is the size of a small virus and is much smaller than a bacterium but much larger than an atom or standard gadolinium contrast molecule. It's an iron oxide crystal surrounded with a carbohydrate or 'sugar' coating called dextran, which gives the particle a longer plasma half-life, allowing it to slowly slip through the BBB. Ferumoxtran-10 can also provide a "stable imaging marker" during surgery to remove brain tumors, and it remains in the brain long enough for post-operative MRI, even after surgical manipulation. These findings have the potential to assist imageguided brain surgery and improve diagnosis of lesions caused by multiple sclerosis, stroke and other neurological disorders, in addition to residual tumors. Because ferumoxtran-10 can stay in brain lesions for days - it can be administered to patients 24 h before surgery and can image other, non-cancerous lesions. It has some advantages over gadolinium, a metal used as an MRI contrast agent for 20 years and which must be administered just before surgery. However, it will complement gadolinium, but not replace it. Ferumoxtran-10 gives additional information that cannot be obtained in some patients with gadolinium. Using both the contrast agents, one can get better diagnostic information and that has the potential to improve the patient's outcome. In addition, ferumoxtran-10 can be detected with an iron stain in the tissue removed by biopsy or surgery, allowing physicians to see it in brain tissue samples under a microscope. Unlike any other MRI contrast agent, ferumoxtran-10 enables the comparison of images from an MRI scan with the tissue taken out at surgery. Moreover, it is relatively safe when diluted and administered as an infusion.

Nanoscaffold for CNS Repair

There are several barriers that must be overcome to achieve axonal regeneration after injury in the CNS: (1) scar tissue formation; (2) gaps in nervous tissue formed during phagocytosis of dying cells after injury; (3) factors that inhibit axon growth in the mature mammalian CNS; and (4) failure of many adult neurons to initiate axonal extension.

Using the mammalian visual system as a model, a self-assembling peptide nanofiber scaffold was designed, which creates a permissive environment for axons not only to regenerate through the site of an acute injury but also to knit the brain tissue together. In experiments using a severed optic tract in the hamster, it was shown that regenerated axons reconnect to target tissues with sufficient density to promote functional return of vision, as evidenced by visually elicited orienting behavior (Ellis-Behnke et al. 2006). The peptide nanofiber scaffold not only represents a previously undiscovered nanobiomedical technology for tissue repair and restoration but also raises the possibility of effective treatment of CNS and other tissue or organ trauma. This peptide nanofiber scaffold has several advantages over currently available polymer biomaterials: (1) it forms a network of nanofibers that are similar in scale to the native extracellular matrix and therefore provides an "in vivo" environment for cell growth, migration, and differentiation; (2) it can be broken down into natural L-amino acids and metabolized by the surrounding tissue; (3) it is synthetic and free of chemical and biological contaminants that may be present in animal-derived biomaterials such as collagens; and (4) it appears to be immunologically inert, thus avoiding the problem of neural tissue rejection.

Application of Nanobiotechnology to Pain Therapeutics

Nanotechnology offers the potential to address multiple, major unmet problems in the diagnosis, treatment and symptom management of a large variety of diseases and conditions, including cancer. Nanobiotechnology will contribute to improvement of cancer pain therapeutics through facilitation of drug discovery for pain. A more immediate application is in facilitating drug delivery for pain. A transbuccal transmucosal system, Buccal Patch®, has been developed for the administration of remifentanil for the management of breakthrough cancer pain (Sprintz et al. 2005). The nanochannel size of the device permits the diffusion of the drug from its reservoir to the target tissue at a consistent and controlled rate, minimizing the risk of overdosing the patient. Intravenous administration of ibuprofen in lipid nanocapsules formulation has an advantage as an analgesic over oral preparations.

US Army is supporting research to develop nanoparticles-based analgesics that can be injected with a pen-like device by injured soldiers' comrades, or even injured soldiers themselves, on the battlefield. The method will use analgesic drugs coupled to polymers but can be released to provide adequate pain relief as well as antidotes to avoid adverse effects of these drugs. For example, morphine, an analgesic commonly used to treat wounded soldiers, needs to be injected by skilled medical personnel. Patients who receive morphine need to be monitored carefully, because the painkiller can cause breathing problems. These requirements restrict the use of morphine on the battlefield. If successful, the nanotechnology approach could markedly improve the treatment of soldiers in the field. Various types of nanoparticles will be designed and tested. The aim is to create nanoparticles that can achieve the following objectives:

- Control the release of morphine over extended periods to ensure pain relief until a soldier can be evacuated to a military acute care facility.
- Continuously monitor the soldier's breathing and, if needed, release the drug naloxone, which counters morphine's effects on breathing.

References

- Al-Jamal KT, Nerl H, Müller KH, et al. Cellular uptake mechanisms of functionalised multiwalled carbon nanotubes by 3D electron tomography imaging. Nanoscale. 2011;3:2627–35.
- Baysal I, Yabanoglu-Ciftci S, Tunc-Sarisozen Y, Ulubayram K, Ucar G. Interaction of selegilineloaded PLGA-b-PEG nanoparticles with beta-amyloid fibrils. J Neural Transm. 2013;120: 903–10.
- Bhattacharya S, Roxbury D, Gong X, et al. DNA conjugated SWCNTs enter endothelial cells via Rac1 mediated macropinocytosis. Nano Lett. 2012;12:1826–30.
- Callera F, de Melo C. Magnetic resonance tracking of magnetically labeled autologous bone marrow CD34+ cells transplanted into the spinal cord via lumbar puncture technique in patients with chronic spinal cord injury: CD34+ cells' migration into the injured site. Stem Cells Dev. 2007;16:461–6.
- Chonpathompikunlert P, Fan CH, Ozaki Y, et al. Redox nanoparticle treatment protects against neurological deficit in focused ultrasound-induced intracerebral hemorrhage. Nanomedicine (Lond). 2012;7:1029–43.
- Diksha RI. Synthesis, surface modification, characterization, and biomedical in vitro applications of organically modified silica (ORMOSIL) nanoparticles. Methods Mol Biol. 2012;906:365–79.
- Ding H, Inoue S, Ljubimov AV, et al. Inhibition of brain tumor growth by intravenous poly(β-Lmalic acid) nanobioconjugate with pH-dependent drug release. Proc Natl Acad Sci U S A. 2010;107:18143–8.
- Ellis-Behnke RG, Liang YX, You SW, et al. Nano neuro knitting: peptide nanofiber scaffold for brain repair and axon regeneration with functional return of vision. Proc Natl Acad Sci U S A. 2006;103:5054–9.
- Estevez AY, Pritchard S, Harper K, et al. Neuroprotective mechanisms of cerium oxide nanoparticles in a mouse hippocampal brain slice model of ischemia. Free Radic Biol Med. 2011; 51:1155–63.
- Fabbro A, Scaini D, León V, et al. Graphene-based interfaces do not alter target nerve cells. ACS Nano. 2016;10:615–23.
- Hernando S, Gartziandia O, Herran E, et al. Advances in nanomedicine for the treatment of Alzheimer's and Parkinson's diseases. Nanomedicine (Lond). 2016;11:1267–85.
- Jain KK. Use of nanoparticles for drug delivery in glioblastoma multiforme. Expert Rev Neurother. 2007;7:363–72.
- Jain KK. Current status and future prospects of nanoneurology. J Nanoneuroscience. 2009;1: 56–64.
- Jain KK. Handbook of neuroprotection. New York: Springer; 2011.

- Jain KK. Nanobiotechnology-based strategies for crossing the blood-brain barrier. Nanomedicine (Lond). 2012;7:1225–33.
- Jain KK. Applications of biotechnology in neurology. New York: Springer; 2013.
- Jain KK. Regenerative therapy for central nervous system trauma. In: Steinhoff G, editor. Regenerative medicine. 3rd ed. London: Springer; 2016.
- Jain KK. Drug delivery in central nervous system disorders: technologies, markets and companies. Basel: Jain PharmaBiotech Publications; 2017.
- Kafa H, Wang JT, Rubio N, et al. The interaction of carbon nanotubes with an in vitro blood-brain barrier model and mouse brain in vivo. Biomaterials. 2015;53:437–52.
- Kang C, Yuan X, Zhong Y, et al. Growth inhibition against intracranial C6 glioma cells by stereotactic delivery of BCNU by controlled release from poly(D,L-lactic acid) nanoparticles. Technol Cancer Res Treat. 2009;8:61–70.
- Kim W, Ng JK, Kunitake ME, et al. Interfacing silicon nanowires with mammalian cells. J Am Chem Soc. 2007;129:7228–9.
- Kozai TD, Catt K, Du Z, et al. Chronic in vivo evaluation of PEDOT/CNT for stable neural recordings. IEEE Trans Biomed Eng. 2016;63:111–9.
- Kreuter J. Drug delivery to the central nervous system by polymeric nanoparticles: what do we know? Adv Drug Deliv Rev. 2014;71:2–14.
- Kreuter J, Gelperina S. Use of nanoparticles for cerebral cancer. Tumori. 2008;94:271-7.
- Larsen A, Kolind K, Pedersen DS, et al. Gold ions bio-released from metallic gold particles reduce inflammation and apoptosis and increase the regenerative responses in focal brain injury. Histochem Cell Biol. 2008;130:681–92.
- Lee SM, Kim JH, Park C, et al. Self-adhesive and capacitive carbon nanotube-based electrode to record electroencephalograph signals from the hairy scalp. IEEE Trans Biomed Eng. 2016; 63:138–47.
- Liopo AV, Stewart MP, Hudson J, et al. Biocompatibility of native and functionalized single-walled carbon nanotubes for neuronal interface. J Nanosci Nanotechnol. 2006;6:1365–74.
- Lu W, Sun Q, Wan J, She Z, Jiang XG. Cationic albumin-conjugated pegylated nanoparticles allow gene delivery into brain tumors via intravenous administration. Cancer Res. 2006;66:11878–87.
- Martin-Banderas L, Holgado MA, Venero JL, et al. Nanostructures for drug delivery to the brain. Curr Med Chem. 2011;18:5303–21.
- Mattei TA, Rehman AA. Technological developments and future perspectives on graphene-based metamaterials: a primer for neurosurgeons. Neurosurgery. 2014;74:499–516.
- McKenzie JL, Waid MC, Shi R, Webster TJ. Decreased functions of astrocytes on carbon nanofiber materials. Biomaterials. 2004;25:1309–17.
- Miller K, Dixit S, Bredlau AL, et al. Delivery of a drug cache to glioma cells overexpressing platelet-derived growth factor receptor using lipid nanocarriers. Nanomedicine (Lond). 2016;11:581–95.
- Misra N, Martinez JA, Huang SC, et al. Bioelectronic silicon nanowire devices using functional membrane proteins. Proc Natl Acad Sci U S A. 2009;106:13780–4.
- Mufamadi MS, Choonara YE, Kumar P, et al. Ligand-functionalized nanoliposomes for targeted delivery of galantamine. Int J Pharm. 2013;448:267–81.
- Musyanovych A, Landfester K. Polymer micro- and nanocapsules as biological carriers with multifunctional properties. Macromol Biosci. 2014;14:458–77.
- Neuwelt EA, Varallyay P, Bago AG, et al. Imaging of iron oxide nanoparticles by MR and light microscopy in patients with malignant brain tumours. Neuropathology and Applied Neurobiology. 2004;30:456–71.
- Nilewski LG, Sikkema WK, Kent TA, Tour JM. Carbon nanoparticles and oxidative stress: could an injection stop brain damage in minutes? Nanomedicine (Lond). 2015;10:1677–9.
- Panseri S, Cunha C, Lowery J, et al. Electrospun micro- and nanofiber tubes for functional nervous regeneration in sciatic nerve transections. BMC Biotechnol. 2008;8:39.
- Pappas TC, Wickramanyake WM, Jan E, et al. Nanoscale engineering of a cellular interface with semiconductor nanoparticle films for photoelectric stimulation of neurons. Nano Lett. 2007;7:513–9.

- Petry KG, Boiziau C, Dousset V, Brochet B. Magnetic resonance imaging of human brain macrophage infiltration. Neurotherapeutics. 2007;4:434–42.
- Pinto MP, Arce M, Yameen B, Vilos C. Targeted brain delivery nanoparticles for malignant gliomas. Nanomedicine (Lond). 2017;12:59–72.
- Posadas I, Guerra FJ, Ceña V. Nonviral vectors for the delivery of small interfering RNAs to the CNS. Nanomedicine. 2010;5:1219–36.
- Qing Q, Pal SK, Tian B, et al. Nanowire transistor arrays for mapping neural circuits in acute brain slices. Proc Natl Acad Sci U S A. 2010;107:1882–7.
- Reddy GR, Bhojani MS, McConville P, et al. Vascular targeted nanoparticles for imaging and treatment of brain tumors. Clin Cancer Res. 2006;12:6677–86.
- Reddy MK, Wu L, Kou W, et al. Superoxide dismutase-loaded PLGA nanoparticles protect cultured human neurons under oxidative stress. Appl Biochem Biotechnol. 2008;151:565–77.
- Robinson JT, Jorgolli M, Shalek AK, et al. Vertical nanowire electrode arrays as a scalable platform for intracellular interfacing to neuronal circuits. Nat Nanotechnol. 2012;7:180–4.
- Rocha R, Zhou Y, Kundu S, et al. In vivo observation of gold nanoparticles in the central nervous system of Blaberus discoidalis. J Nanobiotechnol. 2011;9:5.
- Roy S, Glueckert R, Johnston AH, et al. Strategies for drug delivery to the human inner ear by multifunctional nanoparticles. Nanomedicine (Lond). 2012;7:55–63.
- Seil JT, Webster TJ. Electrically active nanomaterials as improved neural tissue regeneration scaffolds. Wiley Interdiscip Rev Nanomed Nanobiotechnol. 2010;2:635–47.
- Shah B, Khunt D, Bhatt H, et al. Application of quality by design approach for intranasal delivery of rivastigmine loaded solid lipid nanoparticles: effect on formulation and characterization parameters. Eur J Pharm Sci. 2015;78:54–66.
- Shi Y, Kim S, Huff TB, et al. Effective repair of traumatically injured spinal cord by nanoscale block copolymer micelles. Nat Nanotechnol. 2010;5:80–7.
- Shityakov S, Salvador E, Pastorin G, Förster C. Blood-brain barrier transport studies, aggregation, and molecular dynamics simulation of multiwalled carbon nanotube functionalized with fluorescein isothiocyanate. Int J Nanomedicine. 2015;10:1703–13.
- Somani S, Dufès C. Applications of dendrimers for brain delivery and cancer therapy. Nanomedicine (Lond). 2014;9:2403–14.
- Sprintz M, Benedetti C, Ferrari M. Applied nanotechnology for the management of breakthrough cancer pain. Minerva Anestesiol. 2005;71:419–23.
- Stabenfeldt SE, Irons HR, Laplaca MC. Stem cells and bioactive scaffolds as a treatment for traumatic brain injury. Curr Stem Cell Res Ther. 2011;6:208–20.
- Suh WH, Suslick KS, Stucky GD, Suh YH. Nanotechnology, nanotoxicology, and neuroscience. Prog Neurobiol. 2009;87:133–70.
- Sykova E, Jendelova P. In vivo tracking of stem cells in brain and spinal cord injury. Prog Brain Res. 2007;161C:367–83.
- Tosi G, Costantino L, Ruozi B, et al. Polymeric nanoparticles for the drug delivery to the central nervous system. Expert Opin Drug Deliv. 2008;5:155–74.
- Usmani S, Aurand ER, Medelin M, et al. 3D meshes of carbon nanotubes guide functional reconnection of segregated spinal explants. Sci Adv. 2016;2(7):e1600087.
- Veiseh O, Sun C, Fang C, et al. Specific targeting of brain tumors with an optical/magnetic resonance imaging nanoprobe across the blood-brain barrier. Cancer Res. 2009;69:6200–7.
- Wang JT, Al-Jamal KT. Functionalized carbon nanotubes: revolution in brain delivery. Nanomedicine (Lond). 2015;10:2639–42.
- Webber MJ, Kessler JA, Stupp SI. Emerging peptide nanomedicine to regenerate tissues and organs. J Intern Med. 2010;267:71–88.
- Wiley DT, Webster P, Gale A, Davis ME. Transcytosis and brain uptake of transferrin-containing nanoparticles by tuning avidity to transferrin receptor. Proc Natl Acad Sci U S A. 2013;110: 8662–7.
- Xie C, Lin Z, Hanson L, et al. Intracellular recording of action potentials by nanopillar electroporation. Nat Nanotechnol. 2012;7:185–90.

- Yang T, Martin P, Fogarty B, et al. Exosome delivered anticancer drugs across the blood-brain barrier for brain cancer therapy in Danio rerio. Pharm Res. 2015;32:2003–14.
- Yanik MF, Cinar H, Cinar HN, et al. Neurosurgery: functional regeneration after laser axotomy. Nature. 2004;432:822.
- Yoo SI, Yang M, Brender JR, et al. Inhibition of amyloid peptide fibrillation by inorganic nanoparticles: functional similarities with proteins. Angew Chem Int Ed Engl. 2011;50:5110–5.
- Zou J, Sood R, Poe D, et al. Manufacturing and in vivo inner ear visualization of MRI traceable liposome nanoparticles encapsulating gadolinium. J Nanobiotechnol. 2010;8:32.

Chapter 10 Nanocardiology

Introduction

Nanocardiology is the application of nanobiotechnology to cardiovascular diseases. Recent rapid advances in nanobiotechnology offer a wealth of new opportunities for diagnosis and therapy of cardiovascular diseases (Jain 2011). As far back as 2003, the National Heart, Lung, and Blood Institute of US convened a Working Group on Nanotechnology for translational applications to heart, lung, blood disorders and cardiovascular complications of sleep apnea to solve clinical problems.

Nanotechnology-Based Cardiovascular Diagnosis

Nanobiotechnology has refined molecular diagnosis and this applies to detection of cardiovascular diseases also. Availability of genotyping and detection of single nucleotide polymorphisms (SNPs) will provide information on risks of developing genetically linked cardiovascular diseases. Application of nanodiagnostics in pharmacogenetics will be used for selection and guidance of appropriate therapy for an individual patient. This will facilitate the development of personalized medicine.

Biomarkers play an important role in diagnosis of cardiovascular disorders, particularly myocardial infarction (Jain 2010). Detection of biomarkers, particularly using proteomic technologies, has also been refined by nanobiotechnology.

Detection of Biomarkers of Myocardial Infarction in Saliva by a Nanobiochip

The feasibility and utility of saliva as an alternative diagnostic fluid for identifying biomarkers of acute myocardial infarction (AMI) has been investigated. A lab-on-a-chip method was used to assay 21 proteins in serum and unstimulated whole saliva procured from AMI patients within 48 h of chest pain onset and from apparently healthy controls (Floriano et al. 2009). Both established and novel cardiac biomarkers demonstrated significant differences in concentrations between patients with AMI and controls. The saliva-based biomarker panel of C-reactive protein (CRP), myoglobin, and myeloperoxidase showed diagnostic capability, which was better than that of ECG alone. When used in conjunction with ECG, screening capacity for AMI was enhanced and was comparable to that of a panel of brain natriuretic peptide, troponin-I, creatine kinase-MB, and myoglobin. To translating these findings into clinical practice, the whole saliva tests were adapted to a nanobiochip platform, which may provide a convenient and rapid screening method for cardiac events at point-of-care.

Nanobiosensors for Detection of Cardiovascular Disorders

Nanobiosensors can be electronically gated to respond to the binding of a single molecule. Prototype sensors have demonstrated detection of nucleic acids, proteins and ions. These sensors can operate in the liquid or gas phase, opening an enormous variety of downstream applications. The detection schemes use inexpensive low voltage measurement schemes and detect binding events directly so there is no need for costly, complicated and time-consuming labeling chemistries such as fluorescent dyes or the use of bulky and expensive optical detection systems. Therefore, these sensors are inexpensive to manufacture and portable. It may even be possible to develop implantable detections.

Use of Magnetic NPs as MRI Contrast Agents for Cardiac Imaging

Magnetic nanoparticles (MNPs) have been used as contrast agent for MRI and have refined molecular imaging. Targeted imaging of vascular inflammation or thrombosis may enable improved risk assessment of atherosclerosis by detecting plaques at high risk of acute complications (Saraste et al. 2009). Cell death in the heart can be imaged in vivo by using annexin-labeled MNPs, particularly AnxCLIO-Cy5.5 (Chen et al. 2011). Experimental studies have shown the feasibility of combination of diagnosis and therapy using MNPs. In a study on mice, MNPs conjugated with plasmid DNA expressing enhanced green fluorescent protein and coated with chitosan were injected into tail vein and directed to the heart by means of an external magnet without the need to functionalize the NPs, and their location was confirmed by fluorescent imaging (Kumar et al. 2010). This approach requires further investigations before clinical applications can be considered.

Perfluorocarbon NPs for Combining Diagnosis with Therapy in Cardiology

Perfluorocarbon (PFC) nanoparticles provide an opportunity for combining molecular imaging and local drug delivery in cardiovascular disorders. Ligands such as MAbs and peptides can be cross-linked to the outer surface of PFCs to enable active targeting to biomarkers expressed within the vasculature. PFC nanoparticles are naturally constrained by size to the circulation, which minimizes unintended binding to extravascular, nontarget tissues expressing similar epitopes. Moreover, their prolonged circulatory half-life of approximately 5 h allows saturation of receptors without addition of PEG or lipid surfactant polymerization. The utility of targeted PFC nanoparticles has been demonstrated for a variety of applications in animal models and phantoms, including the diagnosis of ruptured plaque, the quantification and antiangiogenic treatment of atherosclerotic plaque and the localization and delivery of antirestenotic therapy following angioplasty.

Cardiac Monitoring in Sleep Apnea

Because sleep apnea is a cause of irregular heartbeat, hypertension, heart attack, and stroke, it is important that patients be diagnosed and treated before these highly deleterious sequelae occur. For patients suspected of experiencing sleep apnea, in vivo sensors could constantly monitor blood concentrations of oxygen and cardiac function to detect problems during sleep. In addition, cardio-specific antibodies tagged with nanoparticles may allow physicians to visualize heart movement while a patient experiences sleep apnea to determine both short- and long-term effects of apnea on cardiac function.

Detection and Treatment of Atherosclerotic Plaques in the Arteries

A key feature of the atherosclerotic process is the angiogenic expansion of the vasa vasorum in the adventitia, which extends into the thickening intimal layer of the atheroma in concert with other neovessels originating from the primary arterial lumen.

Magnetic resonance molecular imaging of focal angiogenesis with integrin-targeted paramagnetic contrast agents has been reported with PFC nanoparticles and liposomes. Site-targeted PFC nanoparticles also offer the opportunity for local drug delivery in combination with molecular imaging.

The diagnosis and treatment of unstable plaque is an area in which nanotechnology could have an immediate impact. Fibrin-specific PFC nanoparticles may allow the detection and quantification of unstable plaque in susceptible patients, which may be an important feature of future strategies to prevent heart attacks or stroke. Research is under way using probes targeted to plaque components for noninvasive detection of patients at risk. In an extension of this approach, targeted nanoparticles, multi-functional macromolecules, or nanotechnology-based devices could deliver therapy to a specific site, localized drug release being achieved either passively (by proximity alone) or actively (through supply of energy as ultrasound, near-infrared, or magnetic field). Targeted nanoparticles or devices could also stabilize vulnerable plaque by removing material, e.g., oxidized low-density lipoproteins. Devices able to attach to unstable plaques and warn patients and emergency medical services of plaque rupture would facilitate timely medical intervention.

Monitoring for Disorders of Blood Coagulation

Patients would benefit greatly from nanotechnology devices that could monitor the body for the onset of thrombotic or hemorrhagic events. Patients with cardiovascular disease, others who are at risk for blood clotting are especially vulnerable when anticoagulant medication levels get too weak or too strong. Multifunctional devices could detect events, transmit real-time biologic data externally, and deliver anticoagulants or clotting factors to buy critical time.

A gold nanoparticle-based simple assay has been described that enables the visual detection of a protease (Guarise et al. 2006). The method takes advantage of the high molar absorptivity of the plasmon band of gold colloids and is based on the color change of their solution when treated with dithiols. Contrary to the native ones, cleaved peptides are unable to induce nanoparticles aggregation; hence, the color of the solution does not change. The assay was used to detect two proteases: thrombin (involved in blood coagulation and thrombosis) and lethal factor (an enzyme component of the toxin produced by *Bacillus anthracis*). The sensitivity of this nanoparticle-based assay is in the low nanomolar range.

A microfluidic paper-based lateral flow assay device for POC and self-monitoring screening uses the red color of RBCs as a visible marker to produce a simple and clear indicator of whether the blood coagulation is within the appropriate range for the patient's condition (Li et al. 2014). The device has been modified to use nanofiber membranes inside paper-based porous materials housed within a plastic cassette. The device utilizes whole blood, without the need for prior separation of plasma from RBCs because the porous nature of the cellulose membrane separates the aqueous plasma component from the large blood cells.

Nanotechnology-Based Therapeutic Delivery in Cardiology

Combination of Diagnostics with Therapeutics

The potential dual use of nanoparticles for both imaging and site-targeted delivery of therapeutic agents to cardiovascular disease offers great promise for individualizing therapeutics. Image-based therapeutics with site-selective agents should enable verification that the drug is reaching the intended target and a molecular effect is occurring. Experimental studies have shown that binding of paclitaxel to smooth muscle cells in culture has no effect in altering the growth characteristics of the cells. If paclitaxelloaded nanoparticles are applied to the cells, however, specific binding elicits a substantial reduction in smooth muscle cell proliferation, indicating that selective targeting may be a requirement for effective drug delivery for in this situation. Similar behavior has been demonstrated for doxorubicin containing particles. Intravenous delivery of fumagillin (an antiangiogenic agent)-loaded nanoparticles targeted to $\alpha\nu\beta3$ -integrin epitopes on vasa vasorum in growing plaques results in marked inhibition of plaque angiogenesis in cholesterol fed rabbits. The unique mechanism of drug delivery for highly lipophilic agents such as paclitaxel contained within emulsions depends on close apposition between the nanoparticle carrier and the targeted cell membrane and has been described as "contact facilitated drug delivery." In contrast to liposomal drug delivery (generally requiring endocytosis), the mechanism of drug transport in this case involves lipid exchange or lipid mixing between the emulsion vesicle and the targeted cell membrane, which depends on the extent and frequency of contact between two lipidic surfaces. The rate of lipid exchange and drug delivery can be greatly increased by the application of clinically safe levels of ultrasound energy that increase the propensity for fusion or enhanced contact between the nanoparticles and the targeted cell membrane.

The combination of targeted drug delivery and molecular imaging with MRI has the potential to enable serial characterization of the molecular epitope expression based on imaging readouts. Monitoring and confirmation of therapeutic efficacy of the therapeutic agents at the targeted site would facilitate personalized medical regimens.

Controlled Delivery of Nanoparticles to Injured Vasculature

Optimal size of nanoparticles designed for systemic delivery is ~50–150 nm, which confers a high surface area-to-volume ratio, resulting in fast diffusive drug release. Spatial control has been achieved by biopanning a phage library to discover materials that target abundant vascular antigens exposed in disease (Chan et al. 2010). Temporal control is achieved by designing 60-nm hybrid nanoparticles with a lipid shell interface surrounding a polymer core, which is loaded with slow-eluting conjugates of paclitaxel for controlled ester hydrolysis and drug release over ~12 days.

The nanoparticles inhibit human aortic smooth muscle cell proliferation in vitro and showed greater in vivo vascular retention during percutaneous angioplasty as compared to nontargeted controls. This technology may potentially be used in treatment of vascular injury.

Nanobiotechnology-Based Therapeutic Delivery in Myocardial Ischemia

Myocardial ischemia is the most critical area for management of cardiovascular disorders that requires improvement in therapeutic delivery. Reperfusion of the ischemic myocardium, overproduction of reactive oxygen species, initiation of an inflammatory response and deregulation of calcium homeostasis all contribute to injury, and difficulties in delivering an adequate quantity of drug to the affected tissue in a controlled manner are some of the limitations of current therapies that may be significantly improved by nanotechnology-based approaches (Evans et al. 2016). Most of the research on this topic is on animal models and selected studies are listed in Table 10.1.

IGF-1 Delivery by Nanofibers for Cell Therapy of Myocardial Infarction

Strategies for cardiac repair include injection of cells, but these approaches have been hampered by poor cell engraftment, survival, and differentiation. To address these shortcomings for improving cardiac function after injury, a self-assembling peptide nanofibers was designed for prolonged delivery of insulin-like growth factor 1 (IGF-1), a cardiomyocyte growth and differentiation factor, to the myocardium, using a "biotin sandwich" approach (Davis et al. 2006). Biotinylated IGF-1 was complexed with streptavidin and then bound to biotinylated self-assembling peptides. This biotin sandwich strategy enabled binding of IGF-1 but did not prevent self-assembly of the peptides into nanofibers within the myocardium. IGF-1 that was bound to peptide nanofibers activated Akt, decreased activation of caspase-3, and increased expression of cardiac troponin I in cardiomyocytes. In studies on rats, cell therapy with IGF-1 delivery by biotinylated nanofibers improved systolic function after experimental myocardial infarction. This nanobiotechnology approach has the potential to improve the results of cell therapy for myocardial infarction, which is in clinical trials currently.

Injectable Peptide Nanofibers for Myocardial Ischemia

Endothelial cells can protect cardiomyocytes from injury through platelet-derived growth factor (PDGF)-BB signaling. PDGF-BB induces cardiomyocyte Akt phosphorylation in a time- and dose-dependent manner and prevents apoptosis via

Therapeutic/category	Nanotechnology	Model/method of delivery	Comments/Reference
AID peptide + curcumin or resveratrol /antioxidants	Polymer NPs/PGMA	Ex vivo rat hearts, mouse ventricular myocytes	Combination reduces ischemia-reperfusion injury/Hardy et al. (2015)
AID peptide/L-type calcium channel antagonist	Polymer NPs/PGMA	Ex vivo guinea pig hearts; no-flow ischemia + reperfusion	Reduction in release of creatine kinase and LDH/Clemons et al. (2013)
Angiotensin II type 1 Receptor/siRNA	Dendrimer/G4 PAMAM, targeted with R9 or TAT	LAD transient occlusion/	Liu et al. (2013)
CCR2/siRNA	Liposomes	Murine transient LAD occlusion/silencing in inflammatory monocytes	Leuschner et al. (2011)
Coenzyme Q10/ Antioxidant + VEGF/growth factor	Polymer NPs/PLGA	LAD coronary artery ligation in Sprague- Dawley rats/oral	Improvement in the ejection fraction/ Simon-Yarza et al. (2013)
IGF-1/growth factor	Polymer NPs/PLGA	Murine LAD ligation/peri-infarct intramyocardial injection	Cardioprotection by induction of Akt phosphorylation/Chang et al. (2013)
Interferon regulatory factor 5/ siRNA	Lipid-based NPs	Murine LAD ligation/silencing of the transcription factor IRF5	Courties et al. (2014)
Nitric oxide/ischemic preconditioning	Dendrimer/G4 PAMAM	Ex vivo rat hearts; no-flow ischemia + reperfusion	Release of nitric oxide/Johnson et al. (2010)
PGF/growth factor	Polymer NPs/chitosanalginate	LAD ligation in rat/myocardial injection	Binsalamah et al. (2011)
Pitavastatin/statin	Polymer NPs/PLGA	Rat transient occlusion of LAD coronary artery, murine model of atherosclerosis	Cardioprotection via activation of PI3K/Akt pathway/Nagaoka et al. (2015)
VEGF/plasmid	Polymer/dendrimer	Rabbit ligation 0f first branch of left circumflex coronary artery	Ye et al. (2011)
Abbreviation: AID Alpha-inte PGMA poly(glycidyl methacry	racting domain of the L-type calc late), TAT trans-activator of transc	Abbreviation: AID Alpha-interacting domain of the L-type calcium channel, LAD Left anterior descending, NP nanoparticle, PGF placental growth factor, PGMA poly(glycidyl methacrylate), TAT trans-activator of transcription, LDH lactate dehydrogenase	VP nanoparticle, PGF placental gro

PI3K/Akt signaling. An experimental study in rats using injectable self-assembling peptide nanofibers, which bound PDGF-BB in vitro, demonstrated sustained delivery of PDGF-BB to the myocardium at the injected sites for 14 days (Hsieh et al. 2006). This blinded and randomized rat study showed that injecting nanofibers with PDGF-BB, but not nanofibers or PDGF-BB alone, decreased cardiomyocyte death and preserved systolic function after myocardial infarction. A separate blinded and randomized study showed that PDGF-BB delivered with nanofibers decreased infarct size after ischemia/reperfusion. PDGF-BB with nanofibers induced PDGFR-β and Akt phosphorylation in cardiomyocytes in vivo. These data demonstrate that PDGF-BB signaling and in vitro finding can be translated into an effective in vivo method of protecting myocardium after infarction. Furthermore, this study shows that injectable nanofibers allow precise and sustained delivery of proteins to the myocardium with potential therapeutic benefits.

Liposomal Nanodevices for Targeted Cardiovascular Drug Delivery

High affinity ligand-receptor interactions have been exploited in the design and engineering of targeting systems that use a liposomal nanodevice for site-specific cardiovascular drug delivery. An example of application is atherothrombosis, a condition in which platelet activation/adhesion/aggregation is closely associated with vascular thrombotic events. Therefore, most antithrombotic therapies have focused on drugs that impede platelet-activation pathways or block ligand-binding platelet integrins. Despite of reasonable clinical efficacy of these therapies, the magic bullet, a single drug and delivery system that selectively targets pathologically thrombotic environment without affecting hemostatic balance remains elusive. The use of antiintegrin/ anti-coagulant/antiinflammatory drugs in conjunction might be necessary to treat the multifactorial nature of pathological thrombogenesis. For this purpose, a nanoscale device that can carry such a combination selectively to a thrombotic site is being developed at the Department of Biomedical Engineering of Case Western Reserve University (Cleveland, OH). The liposomal nanodevice surface is modified by RGD (Arginine-Glycine-Aspartic Acid) motifs that specifically targets and binds activated platelets due to the high affinity interaction between the RGD-motif and the integrin GPIIb-IIIa expressed on active platelets, potentially acting as a thrombus-targeted vector. The ability of such liposomes to compete with native ligand fibrinogen in specifically binding activated platelets has been accomplished using both in vitro and in vivo approaches. The results demonstrate feasibility of using liposomes as platelet-targeted devices for delivery of cardiovascular therapeutics. By utilizing a library of synthetic peptide/peptidomimetic ligands having binding affinity towards specific receptors expressed in cardiovascular biology, it is possible to manipulate the liposome surface-modification and hence dictate targeting specificity and affinity of the liposomal nanodevices.

Low Molecular Weight Heparin-Loaded Polymeric Nanoparticles

Low molecular weight heparin (LMWH) nanoparticles are available as potential oral heparin carriers. The nanoparticles are formulated using an ultrasound probe by water-in-oil-in-water emulsification and solvent evaporation with polymers. The mean diameter of LMWH-loaded nanoparticles ranges from 240 to 490 nm and is dependent on the reduced viscosity of the polymeric organic solution. The highest encapsulation efficiencies are observed when Eudragit polymers are used in the composition of the polymeric matrix. The in vitro biological activity of released LMWH, determined by the anti-factor Xa activity with a chromogenic substrate, is preserved after the encapsulation process, making these nanoparticles good candidates for oral administration.

Magnetic Antibody-Linked Nanoparticles to Deliver Cells to the Heart

Stem cell transplantation is a promising strategy for therapeutic cardiac regeneration, but current therapies are limited by inefficient interaction of transplanted cells and the injured tissue. A targeted nanomedicine has been used to achieve in vivo cell-mediated tissue repair and imaging. Iron nanoparticles are conjugated with two types of antibodies (one against antigens on therapeutic cells and the other directed at injured cells) to produce magnetic bifunctional cell engager (MagBICE). The antibodies link the therapeutic cells to the injured cells, whereas the iron core of MagBICE enables physical enrichment and imaging (Cheng et al. 2014). Acute myocardial infarction is treated by targeting exogenous bone marrow-derived stem cells (expressing CD45) introduced into the blood stream or endogenous CD34positive cells to injured cardiomyocytes (expressing myosin light chain). Targeting can be further enhanced by magnetic attraction, leading to augmented functional benefits.

Nanoparticles for Cardiovascular Imaging and Targeted Drug Delivery

The potential dual use of nanoparticles for both imaging and site-targeted delivery of therapeutic agents to cardiovascular disease offers great promise for individualizing therapeutics. Image-based therapeutics with site-selective agents should enable verification that the drug is reaching the intended target and a molecular effect is occurring. Experimental studies have shown that binding of paclitaxel to smooth muscle cells in culture has no effect in altering the growth characteristics of the cells. If paclitaxel-loaded nanoparticles are applied to the cells, however, specific binding elicits a substantial reduction in smooth muscle cell proliferation, indicating that selective targeting may be a requirement for effective drug delivery for in this situation. Similar behavior has been demonstrated for doxorubicin containing particles. Intravenous delivery of fumagillin (an antiangiogenic agent)loaded nanoparticles targeted to $\alpha\nu\beta3$ -integrin epitopes on vasa vasorum in growing plaques results in marked inhibition of plaque angiogenesis in cholesterol fed rabbits. The unique mechanism of drug delivery for highly lipophilic agents such as paclitaxel contained within emulsions depends on close apposition between the nanoparticle carrier and the targeted cell membrane and has been described as "contact facilitated drug delivery." In contrast to liposomal drug delivery (generally requiring endocytosis), the mechanism of drug transport in this case involves lipid exchange or lipid mixing between the emulsion vesicle and the targeted cell membrane, which depends on the extent and frequency of contact between two lipidic surfaces. The rate of lipid exchange and drug delivery can be greatly increased by the application of clinically safe levels of ultrasound energy that increase the propensity for fusion or enhanced contact between the nanoparticles and the targeted cell membrane.

The combination of targeted drug delivery and molecular imaging with MRI has the potential to enable serial characterization of the molecular epitope expression based on imaging readouts. Monitoring and confirmation of therapeutic efficacy of the therapeutic agents at the targeted site would facilitate personalized medical regimens.

Nanofiber-Based Scaffolds with Drug-Release Properties

Electrospinning is a versatile technique that enables the development of nanofiberbased scaffolds, from a variety of polymers that may have drug-release properties. Using nanofibers, it is now possible to produce biomimetic scaffolds that can mimic the extracellular matrix for tissue engineering (Ashammakhi et al. 2009). Nanofibers can guide cell growth along their direction. Combining factors like fiber diameter, alignment and chemicals offers new ways to control tissue engineering. In vivo evaluation of nanomats included their degradation, tissue reactions and engineering of specific tissues. New advances made in electrospinning, especially in drug delivery, support the massive potential of these nanobiomaterials. Nevertheless, there is already at least one product based on electrospun nanofibers with drug-release properties in a phase III clinical trial, for wound dressing. Hopefully, clinical applications in tissue engineering will follow to enhance the success of regenerative therapies.

NP-Based Systemic Drug Delivery to Prevent Cardiotoxicity

Nanotechnology can have a beneficial effect on cardiovascular health by reducing cardiotoxicity of drugs used to treat noncardiac diseases. Use of halofantrine, an antimalarial drug for treatment of multi-drug-resistant malaria, is limited by prolongation of the QT interval (the time between the Q wave and the end of the T wave) as seen on ECG, which can result in bradycardia and hypotension. By encapsulating the drug in polycaprolactone nanocapsules, halofantrine was administered in in mice with blunting of the cardiotoxic effects of the drug (Leite et al. 2007). Nanoparticle encapsulation also shows promise for reduction of cardiotoxicity of other drugs. For example, administration of the anticancer drug doxorubicin is limited by cardiotoxicity. However, doxorubicin packaged into 100 nm pegylated liposomes shows comparable efficacy but reduced cardiotoxicity.

Targeted Nanoparticle-DNA Delivery to the Cardiovascular System

Targeting gene therapy to the cardiovascular system is a challenge. MNPs may represent a new method for delivering gene therapy to benefit blood vessels damaged by arterial disease. Such nanoparticles could be magnetically directed into stents inserted into a patient's partially blocked vessels to improve blood flow. Delivering anti-growth genes to stents could help prevent restenosis.

Biodegradable polymeric superparamagnetic nanoparticles have been formulated using a modified emulsification-solvent evaporation methodology with both the incorporation of oleate-coated iron oxide and a polyethylenimine oleate ion-pair surface modification for DNA binding (Chorny et al. 2007). The DNA was in the form of a plasmid, a circular molecule that carried a gene that coded for a growth-inhibiting protein adiponectin. This method of gene transfer was studied in cultured arterial smooth muscle cells and endothelial cells. Cell growth inhibition after nanoparticlemediated adiponectin plasmid transfection is an example of a therapeutic endpoint. Nanoparticle-DNA complexes protect DNA from degradation and efficiently transfected quiescent cells under both low and high serum conditions after a short exposure to a magnetic field. There was negligible transfection with nanoparticle in the absence of a magnetic field. Larger nanoparticles exhibited higher transfection rates compared with smaller nanoparticles. Internalized larger sized nanoparticles escaped lysosomal localization and released DNA in the perinuclear zone. Adiponectin plasmid DNA delivery using MNPs produced dose-dependent growth inhibition of cultured arterial smooth muscle cells. The materials composing the nanoparticles are biodegradable, so they break down into simpler, nontoxic chemicals that can be carried away in the blood. This addresses the safety concerns of the use of non-biodegradable nanoparticles in vivo.

Nanotechnology-Based Therapeutics for Cardiovascular Diseases

Nanolipoblockers for Atherosclerotic Arterial Plaques

Nanoscale particles can be synthetically designed to potentially intervene in lipoprotein matrix retention and lipoprotein uptake in cells – processes central to atherosclerosis. These micelles can be engineered to present varying levels of anionic chemistry, which is a key mechanism to induce differential retentivity of low-density lipoproteins (LDLs). Nanoengineered molecules called nanolipoblockers (NLBs) consist of nanoscale micelles self-assembled from amphiphilic scorpion-like macromolecules based on a lauryl chloride-mucic acid hydrophobic backbone and poly(ethylene glycol) shell. NLBs can be used to attack atherosclerotic plaques due to raised levels of LDLs. This approach contrasts with statin drug therapy, which aims to reduce the amount of LDL throughout the body. NLPs compete with oxidized LDLs for a macrophage's attention. The NLBs bind to receptor sites on macrophages, cutting the accumulation of oxidized LDL by as much as 75%.

Nanotechnology Approach to the Vulnerable Plaque as Cause of Cardiac Arrest

Recent studies have shown that plaque exists in two modes: non-vulnerable and vulnerable. The latter is the probable cause of death in sudden cardiac arrest. Blood passing through an artery exerts a shearing force and can cause vulnerable plaque to rupture, which often leads to occlusion and myocardial infarction. Approximately 60–80% of sudden cardiac deaths can be attributed to the physical rupture of vulnerable plaque. Biomarker-targeted nanoparticles can be used for molecular imaging as well as for pharmacologic modification of vulnerable atherosclerotic lesions that cause myocardial infarction (Mangge et al. 2014).

There is currently no satisfactory solution to the problem of vulnerable plaque but it will be tackled by following innovative solutions to combat vulnerable plaque:

- Building delivery vehicles that can be used to transport drugs and nanodevices to sites of vulnerable plaque.
- Designing a series of self-assembling polymers that can be used as molecular nano-stents to physically stabilize vulnerable plaque.
- Creating nano-machines comprised of human proteins linked to synthetic nanodevices for sensing and responding to vulnerable plaque.

Nanotechnology for Regeneration of the Cardiovascular System

Nanotechnology may facilitate repair and replacement of blood vessels, myocardium and myocardial valves. It also may be used to stimulate regenerative processes such as therapeutic angiogenesis for ischemic heart disease. Cellular function is integrally related to morphology, so the ability to control cell shape in tissue engineering is essential to ensure proper cellular function in final products. Precisely constructed nanoscaffolds and microscaffolds are needed to guide tissue repair and replacement in blood vessels and organs. Nanofiber meshes may enable vascular grafts with superior mechanical properties to avoid patency problems common in synthetic grafts, particularly small-diameter grafts. Cytokines, growth factors, and angiogenic factors can be encapsulated in biodegradable microparticles or nanoparticles and embedded in tissue scaffolds and substrates to enhance tissue regeneration. Scaffolds capable of mimicking cellular matrices should be able to stimulate the growth of new heart tissue and direct revascularization.

Nanotechnology for Cardiac Revascularization

Nanostructures promote formation of blood vessels and bolster cardiovascular function after heart attack. Scientists at the Institute of Bionanotechnology in Medicine at Northwestern University (Evanston, III) have shown that injecting nanoparticles into the hearts of mice that suffered heart attacks helped restore cardiovascular function in these animals. The finding is an important research advance that 1 day could help rapidly restore cardiovascular function in people who have heart disease. The self-assembling nanoparticles – made from naturally occurring polysaccharides and molecules known as peptide amphiphiles – boost chemical signals to nearby cells that induce formation of new blood vessels and this may be the mechanism through which they restore cardiovascular function. One month following injection, the hearts of the treated mice were capable of contracting and pumping blood almost as well as healthy mice. In contrast, the hearts of untreated mice contracted about 50% less than normal.

Cellular function is integrally related to morphology, so the ability to control cell shape in tissue engineering is essential to ensure proper cellular function in final products. Precisely constructed nanoscaffolds and microscaffolds are needed to guide tissue repair and replacement in blood vessels and organs. Nanofiber meshes may enable vascular grafts with superior mechanical properties to avoid patency problems common in synthetic grafts, particularly small-diameter grafts. Cytokines, growth factors, and angiogenic factors can be encapsulated in biode-gradable microparticles or nanoparticles and embedded in tissue scaffolds and substrates to enhance tissue regeneration. Scaffolds capable of mimicking cellular

matrices should be able to stimulate the growth of new heart tissue and direct revascularization.

Considering zinc's multitude of roles in biology and medicine, ZnO nanoflowers have been fabricated through the interaction of zinc nitrate with aqueous ammonia using microwave irradiation. The synthesized nanoflowers exhibit significant proangiogenic properties (Patra and Barui 2013). This may provide a novel alternative treatment strategy for ischemic cardiac disease in the future. Intensive characterization and quality control of these nanoflowers are the most important steps to be undertaken before this technology can be applied commercially.

Nanocomposite Hydrogels for Myocardial Tissue Engineering

New nanocomposite biomaterials are being developed to improve therapeutic delivery to the heart. Main benefits of delivery by injectable hydrogels are direct access to the damaged tissue site, accurate placement and improved retention of the therapeutics compared with other methods. An example is injectable extracellular matrix hydrogel (Ventrix Inc), which is in clinical trials for myocardial therapy (Seif-Naraghi et al. 2013). The hydrogel can provide structural support and biochemical cues to the injured site which may induce endogenous stem cell homing for natural healing. Nanohybrid hydrogels can also be very useful for cardiac tissue engineering but several challenges need to be overcome before they can be translated into clinical use including development of methods to vascularize the engineered cardiac tissues. Other concerns about the use of injectable hydrogel include long-term biosafety of the implants, ease of integration of hydrogel to host tissue and the fate of nanomaterials after implantation (Paul 2015).

Nanotechnology-Based Stents

A coronary stent is a tiny expandable mesh tube made of medical grade stainless steel. A stent is delivered on a balloon catheter and implanted in the coronary artery after balloon angioplasty to help keep the artery open. After the plaque is compressed against the arterial wall, the stent is fully expanded into position, thereby acting as miniature "scaffolding" for the artery. The balloon is then deflated and removed and the coronary stent is left behind in the patient's blood vessel. It may be necessary to place more than one stent, depending on the length of the blockage. The inside lining of the artery eventually heals around the stent. Technical advances are providing the development of improved materials for coating of DES. Nanomaterials are the most prominent among these.

Restenosis after Percutaneous Coronary Angioplasty

Restenosis after percutaneous coronary intervention continues to be a serious problem in clinical cardiology. Advances in nanoparticle technology have enabled the delivery of NK911, an antiproliferative drug, selectively to the balloon-injured artery for a longer time. NK911 is a core-shell nanoparticle of PEG-based block copolymer encapsulating doxorubicin. It accumulates in vascular lesions with increased permeability. In a balloon injury model of the rat carotid artery, intravenous administration of NK911 significantly inhibits the neointimal formation. The effect of NK911 is due to inhibition of vascular smooth muscle proliferation but not to enhancement of apoptosis or inhibition of inflammatory cell recruitment. NK911 is well tolerated without any adverse systemic effects. These results suggest that nanoparticle technology is a promising and safe approach to target vascular lesions with increased permeability for the prevention of restenosis after balloon injury. CoroxaneTM (Abraxis), a nanoparticulate microtubule stabilizer, is in phase II clinical trials in conjunction with angioplasty/stents to prevent arterial restenosis.

Vascular stents used for repair of arteries might perform better if their surfaces contained "nano-bumps" that mimic tiny features found in living tissues. The stents, which are made of titanium and other metals, enable the arteries to grow new tissue after vessel-clogging plaque deposits have been removed. A major problem, however, is that the body often perceives the metal devices as foreign invaders, hindering endothelial cells from attaching to the scaffolding and prompting the creation of scar tissue, which can build up inside blood vessels and interfere with blood flow. If a stent does not attach firmly it can become loose, and parts of it will break off and go down the bloodstream. There is need for new materials that cause the endothelial cells to attach better to these stents without creating as much dangerous scar tissue. The researchers tested discs of titanium containing surface bumps about as wide as 100 nm. The metals used to make conventional stents have features about 10 times larger bumps or none at all. The nanometer-scale bumps mimic surface features of proteins and natural tissues, prompting cells to stick better. Ideally endothelial cells should quickly attach to stents and form a coating only one cell layer thick. The researchers found that nearly three times as many cells stuck to the discs containing the nano-bumps, as compared to ordinary titanium. Further research is planned that will replace the titanium disks with tube-shaped pieces of the nano-featured metal, which will resemble the actual shape of real stents.

Currently available stents have problems with imaging within the stent structure, where potential restenosis can occur. Biophan Technologies Inc has two solutions for stent visibility: a thin-film nanomagnetic particle coating solution and an antiantenna solution. These solutions enable the non-invasive, MRI-based, imaging of these devices which today can only be accomplished through more complicated invasive procedures. These approaches will become an important part of the rapidly growing worldwide market for stents and vascular implants. By using anti-proliferative compounds that elute from the surface of a stent, the latest generation of stents has enabled a significant reduction in restenosis rates, i.e. when there is a re-narrowing of the vessel after stent implantation). Nanocarrierbased delivery presents a viable alternative to the current stent based therapies (Brito and Amiji 2007; Feng et al. 2007; Margolis et al. 2007).

Drugs Encapsulated in Biodegradable Nanoparticles

Local delivery of antiproliferative drugs encapsulated in biodegradable nanoparticles has shown promise as an experimental strategy for preventing restenosis development. A novel PDGFR β -specific tyrphostin, AGL-2043 (Calbiochem), was formulated in polylactide-based nanoparticles and was administered intraluminally to the wall of balloon-injured rat carotid and stented pig coronary arteries (Banai et al. 2005). The antiproliferative effect of nanoencapsulated tyrphostin was found to be considerably higher than that of surface-adsorbed drug. In the pig model, intramural delivery of AGL-2043 resulted in reduced in-stent neointima formation in the coronary arteries as compared to control despite similar degrees of wall injury. The results of this study suggest that locally delivered tyrphostin AGL-2043 formulated in biodegradable nanoparticles may be applicable for anti-restenotic therapy independent of stent design or type of injury.

Magnetic Nanoparticle-Coated DES

Biophan Technologies' drug delivery technology (Fig. 10.1), based on tuning magnetic nanoparticles (MNPs) to resonate at a specific frequency, led to their use for selective control of drug release. This technology can be used for reloading drugeluting coatings for surface elution on demand is active in contrast to the passive drug eluting polymer coatings. It provides a physician better control over the patient's treatment. Currently, many cardiovascular experts predict the next generation of DES will be comprised of a biocompatible, biodegradable, resorbable material with the strength to acutely open and maintain the confirmation of a vessel. The advantage is that they gradually dissolve while delivering the drug. At the end of a predetermined period, nothing is left at the site where it was introduced. Since the company is no longer in business, the current fate of this technology is not known.

Magnetic Nanoparticles Encapsulating Paclitaxel Targeted to Stents

Because current DESs lack the capacity for adjustment of the drug dose and release kinetics to the disease status of the treated vessel, attempts have been made to address these limitations by a strategy combining magnetic targeting via a uniform field-induced magnetization effect and a biocompatible magnetic nanoparticle (MNP) formulation designed for efficient entrapment and delivery of paclitaxel (PTX).

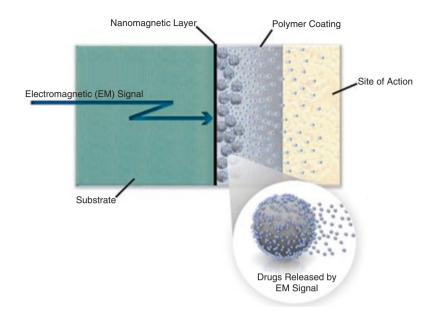


Fig. 10.1 Magnetic nanoparticle-coated stent (Source: Biophan Technologies Inc)

Magnetic treatment of cultured arterial smooth muscle cells with PTX-loaded MNPs was shown to inhibit produce cell growth significantly as compared to nonmagnetic conditions (Chorny et al. 2010). Furthermore, significantly higher localization rates of locally delivered MNPs to stented arteries were achieved with uniform-field-controlled targeting compared to nonmagnetic controls in the rat carotid stenting model. The arterial tissue levels of stent-targeted MNPs remained four to tenfold higher in magnetically treated animals vs. control over 5 days post-delivery. The enhanced retention of MNPs at target sites due to the uniform field-induced magnetization effect resulted in a significant inhibition of in-stent restenosis with a relatively low dose of MNP-encapsulated PTX. This study demonstrates the feasibility of site-specific drug delivery to implanted magnetizable stents by uniform field-controlled targeting of MNPs with efficacy for in-stent restenosis.

Nanocoated DES

MIV Therapeutics Inc. has developed unique coating technologies that utilize hydroxyapatite (HAp) for application on medical devices and drug delivery systems. The lead product in development is a HAp-coated coronary stent with a nanofilm coating. In 2006, the results of an independently conducted 4-week porcine study, performed by the Department of Cardiology, Thoraxcenter, Erasmus University Medical Center in the Netherlands, indicated that three variations of MIV's polymer-free drug-eluting coatings were at least as effective as or better than Cypher

(Johnson & Johnson). The study concluded that MIV's HAp coating, with or without drugs, demonstrated highly promising performance. A pilot clinical trial was launched in 2007 and the first HAp-coated was implanted at the Institute Dante Pazzanese of Cardiology in Sao Paulo, Brazil.

ElectroNanoSprayTM formulation technology (Nanocopoeia Inc) produces precise, ultra-pure nanoparticles. Particle sizes can be designed from 2 to 200 nm. The device can apply a coating to the particles in a single process step, producing a drugloaded core. Competitive processes to produce nanoparticles using wet milling and super critical fluid are inherently limited in their ability to produce consistently pure particles within a specified size range and distribution. ElectroNanoSprayTM technology provides a novel approach for applying challenging materials to the surfaces of medical devices. This process can generate both single- and multiple-phase coatings and apply these with tight control to small, complex surfaces. ElectroNanosprayTM process is being developed for applying nanoparticle-based drug-eluting coatings to coronary stents.

Debiotech SA in collaboration with the Laboratory of Powder Technology at Ecole Polytechnique Fédérale de Lausanne (Lausanne, Switzerland) is developing a new type of structured ceramic coatings for drug eluting stents and other implants. Ceramics offer unique properties compared to polymers. Polymers dissolve over time and residues provoke inflammation, whereas ceramic is stable and inert when in contact with living tissue. With this coating, one can combine an active release of drug during the first weeks after implantation with the long term stability of the ceramic. Nanostructured ceramics provide novel properties to biomaterials which are not attainable with other materials. The challenge in this project is to process nanosized ceramic powders to reach unique surface structures, which show a controlled porosity over a size range of 2000 times between the smallest and largest pore. Based on results of fundamental research activities in the field of ordered arrangement of nanosized particles at surfaces, the knowledge of processing particles smaller than 10 nm at large scale has been established as a key competence to achieve that goal.

Nanopores to Enhance Compatibility of DES

Scientists at the Forschungszentrum Dresden-Rossendorf in Germany have developed an innovative method to create a large number of nanopores on the surface of stainless steel. Bombarding the surface of a stent from all sides with a high dose of noble gas ions generates a scaffold of nanopores in the material below the surface. The desired porosity can be precisely engineered by tuning the ion energy, the flux and the temperature during the process. A larger amount of the highly effective drugs can be deposited on the enlarged noble metal surface, due to this nanoporous structure, which enhances the biocompatibility of the implants in the human body. Thus, this treatment results in the release of drugs over a longer period of time. This method is has been assessed as a platform technology for the next generation of DES by the Boston Scientific Corporation. The objective of this research collaboration is to further develop this technique for commercialization.

Application of Nanotechnology in Cardiac Catheterization

Cardiac catheterization involves use of flexible catheters inserted via peripheral vessels and navigated in coronary arteries or cardiac chambers and valves for diagnostic as well as therapeutic purposes. Catheters are also used for transendocardial delivery of therapeutics such as stem cells for myocardial infarction. MRI roadmaps have been overlapped on live x-ray fluoroscopy to guide targeted transendocardial delivery (Tomkowiak et al. 2011). Nanoparticles have been used to refined MRI as well as tag stem cells to track their course in vivo.

Cardiac catheterization has also been used to perform cardiac ablation for correcting heart rhythm irregularities by destroying specific heart tissue that triggers irregular heartbeats, as an alternative to open-heart surgery. Currently this catheter method requires the use of three different devices, which are inserted into the heart in succession: one to map the heart's signals and detect the problem area, a second to control positions of therapeutic actuators and their contact with the epicardium, and a third to ablate the tissue. Researchers have used stretchable electronics to create a multipurpose medical catheter that can both monitor heart functions and perform therapeutic cardiac ablation (Kim et al. 2012). Recent advances in nanomaterials research have provided versatile strategies in mechanics, designs and manufacturing techniques for high-quality electronics that can flex, twist, and stretch in ways that facilitate integration with biology. The device marks the first time stretchable electronics have been applied for cardiac ablation and is a milestone that could lead to simpler procedures for arrhythmia as well as other cardiac disorders. The authors had previously demonstrated the concept to apply stretchable electronics to heart surgery, but with this research improved the design's functionality to the point that it could be utilized in animal tests.

The catheter's exterior protects the electronics during its trip through the bloodstream; once inside the heart, the catheter is inflated like a balloon, exposing the electronics to a larger surface area inside the heart. With the catheter is in place, the individual devices within can perform their specific tasks. A pressure sensor determines the pressure on the heart; an EKG sensor monitors the heart's condition during the procedure; and a temperature sensor controls the temperature so as not to damage surrounding tissue. The temperature can also be controlled during the procedure without removing the catheter. These devices can deliver critical, high-quality information such as temperature, mechanical force, and blood flow to the surgeon in real time, and the system is designed to operate reliably without any changes in properties as the balloon inflates and deflates.

References

- Ashammakhi N, Wimpenny I, Nikkola L, Yang Y. Electrospinning: methods and development of biodegradable nanofibres for drug release. J Biomed Nanotechnol. 2009;5:1–19.
- Banai S, Chorny M, Gertz SD, et al. Locally delivered nanoencapsulated tyrphostin (AGL-2043) reduces neointima formation in balloon-injured rat carotid and stented porcine coronary arteries. Biomaterials. 2005;26:451–61.

- Binsalamah ZM, Paul A, Khan AA, et al. Intramyocardial sustained delivery of placental growth factor using nanoparticles as a vehicle for delivery in the rat infarct model. Int J Nanomedicine. 2011;6:2667–78.
- Brito L, Amiji M. Nanoparticulate carriers for the treatment of coronary restenosis. Int J Nanomedicine. 2007;2:143–61.
- Chan JM, Zhang L, Tongc R, et al. Spatiotemporal controlled delivery of nanoparticles to injured vasculature. Proc Natl Acad Sci U S A. 2010;107:2213–8.
- Chang MY, Yang YJ, Chang CH, et al. Functionalized nanoparticles provide early cardioprotection after acute myocardial infarction. J Control Release. 2013;170:287–94.
- Chen HH, Josephson L, Sosnovik DE. Imaging of apoptosis in the heart with nanoparticle technology. Wiley Interdiscip Rev Nanomed Nanobiotechnol. 2011;3:86–99.
- Cheng K, Shen D, Hensley MT, et al. Magnetic antibody-linked nanomatchmakers for therapeutic cell targeting. Nat Commun. 2014;5:4880.
- Chorny M, Fishbein I, Yellen BB, et al. Targeting stents with local delivery of paclitaxel-loaded magnetic nanoparticles using uniform fields. Proc Natl Acad Sci U S A. 2010;107:8346–51.
- Chorny M, Polyak B, Alferiev IS, et al. Magnetically driven plasmid DNA delivery with biodegradable polymeric nanoparticles. FASEB J. 2007;21:2510–9.
- Clemons TD, Viola HM, House MJ, et al. Examining efficacy of "TAT-less" delivery of a peptide against the L-type calcium channel in cardiac ischemia reperfusion injury. ACS Nano. 2013;7:2212–20.
- Courties G, Heidt T, Sebas M, et al. In vivo silencing of the transcription factor IRF5 reprograms the macrophage phenotype and improves infarct healing. J Am Coll Cardiol. 2014;63:1556–66.
- Davis ME, Hsieh PC, Takahashi T, et al. Local myocardial insulin-like growth factor 1 (IGF-1) delivery with biotinylated peptide nanofibers improves cell therapy for myocardial infarction. Proc Natl Acad Sci U S A. 2006;103:8155–60.
- Evans CW, Iyer KS, Hool LC. The potential for nanotechnology to improve delivery of therapy to the acute ischemic heart. Nanomedicine (Lond). 2016;11:817–32.
- Feng SS, Zeng W, Teng Lim Y, et al. Vitamin E TPGS-emulsified poly(lactic-co-glycolic acid) nanoparticles for cardiovascular restenosis treatment. Nanomedicine (Lond). 2007;2:333–44.
- Floriano PN, Christodoulides N, Miller CS, et al. Use of saliva-based nano-biochip tests for acute myocardial infarction at the point of care: a feasibility study. Clin Chem. 2009;55:1530–8.
- Guarise C, Pasquato L, De Filippis V, Scrimin P. Gold nanoparticles-based protease assay. Proc Natl Acad Sci U S A. 2006;103:3978–82.
- Hardy N, Viola HM, Johnstone VP, et al. Nanoparticle mediated dual delivery of an antioxidant and a peptide against the L-type Ca2+ channel enables simultaneous reduction of cardiac ischemiareperfusion injury. ACS Nano. 2015;9:279–89.
- Hsieh PCH, Davis ME, Gannon J, et al. Controlled delivery of PDGF-BB for myocardial protection using injectable self-assembling peptide nanofibers. J Clin Invest. 2006;116:237–48.
- Jain KK. Applications of biotechnology in cardiovascular therapeutics. New York: Springer; 2011.
- Jain KK. Handbook of biomarkers. New York: Springer; 2010.
- Johnson TA, Stasko NA, Matthews JL, et al. Reduced ischemia/reperfusion injury via glutathioneinitiated nitric oxide-releasing dendrimers. Nitric Oxide. 2010;22:30–6.
- Kim DH, Lu N, Ghaffari R, Rogers JA. Inorganic semiconductor nanomaterials for flexible and stretchable bio-integrated electronics. NPG Asia Materials. 2012;4:e15. doi:10.1038/ am.2012.27.
- Kumar A, Jena PK, Behera S, et al. Multifunctional magnetic nanoparticles for targeted delivery. Nanomedicine. 2010;6:64–9.
- Leite EA, Grabe-Guimarães A, Guimarães HN, et al. Cardiotoxicity reduction induced by halofantrine entrapped in nanocapsule devices. Life Sci. 2007;80:1327–34.
- Leuschner F, Dutta P, Gorbatov R, et al. Therapeutic siRNA silencing in inflammatory monocytes in mice. Nat Biotechnol. 2011;29:1005–10.
- Li H, Han D, Pauletti GM, Steckl AJ. Blood coagulation screening using a paper-based microfluidic lateral flow device. Lab Chip. 2014;14:4035–41.

- Liu J, Gu C, Cabigas EB, et al. Functionalized dendrimer based delivery of angiotensin type 1 receptor siRNA for preserving cardiac function following infarction. Biomaterials. 2013;34:3729–36.
- Mangge H, Almer G, Stelzer I, et al. Laboratory medicine for molecular imaging of atherosclerosis. Clin Chim Acta. 2014;437:19–24.
- Margolis J, McDonald J, Heuser R, et al. Systemic nanoparticle paclitaxel (nab-paclitaxel) for in-stent restenosis I (SNAPIST-I): a first-in-human safety and dose-finding study. Clin Cardiol. 2007;30:165–70.
- Nagaoka K, Matoba T, Mao Y, et al. A new therapeutic modality for acute myocardial infarction: nanoparticle mediated delivery of pitavastatin induces cardioprotection from ischemiareperfusion injury via activation of PI3K/Akt pathway and anti-inflammation in a rat model. PLoS One. 2015;10:e0132451.
- Patra CR, Barui AK. Nanoflowers: a future therapy for cardiac and ischemic disease? Nanomedicine. 2013;8:1735–8.
- Paul A. Nanocomposite hydrogels: an emerging biomimetic platform for myocardial therapy and tissue engineering. Nanomedicine. 2015;10:1371–4.
- Saraste A, Nekolla SG, Schwaiger M. Cardiovascular molecular imaging: an overview. Cardiovasc Res. 2009;83:643–52.
- Seif-Naraghi SB, Singelyn JM, Salvatore MA. Safety and efficacy of an injectable extracellular matrix hydrogel for treating myocardial infarction. Sci Transl Med. 2013;5:173ra125.
- Simon-Yarza T, Tamayo E, Benavides C, et al. Functional benefits of PLGA particulates carrying VEGF and CoQ10 in an animal of myocardial ischemia. Int J Pharm. 2013;454:784–90.
- Tomkowiak MT, Klein AJ, Vigen KK, et al. Targeted transendocardial therapeutic delivery guided by MRI-x-ray image fusion. Catheter Cardiovasc Interv. 2011;78:468–78.
- Ye L, Zhang W, Su LP, et al. Nanoparticle based delivery of hypoxia-regulated VEGF transgene system combined with myoblast engraftment for myocardial repair. Biomaterials. 2011;32: 2424–31.

Chapter 11 Nanopulmonology

Introduction

Pulmonology deals with treatment of respiratory diseases, which is a challenging task with rising incidence and limitations of currently available treatments. Application of nanobiotechnology to pulmonology, nanopulmonology, offers NP-based drug and gene delivery for treatment of lung diseases as well as a route for delivery of systemic therapy. Delivery of exogenous genes to the airway epithelium in vivo has been limited by several physiological barriers, resulting in the low success rate of these systems. NP-based drug delivery systems have revolutionized the field of pharmacotherapy by presenting the ability to alter the pharmacokinetics of the conventional drugs to extend the drug retention time, reduce the toxicity and increase the half-life of the drugs (Swai et al. 2009).

Nanoparticles for Pulmonary Drug Delivery

Pulmonary drug delivery is attractive for both local and systemic drug delivery as a non-invasive route that provides a large surface area, thin epithelial barrier, high blood flow and the avoidance of first-pass metabolism. Nanoparticles may be used for systemic drug delivery via pulmonary route or for effect on the respiratory system. Nanoparticles can be designed to have several advantages for controlled and targeted drug delivery, including controlled deposition, sustained release, reduced dosing frequency, as well as an appropriate size for avoiding alveolar macrophage clearance or promoting transepithelial transport (Rytting et al. 2008). The selection of natural or synthetic materials is important in designing particles or nanoparticle clusters with the desired characteristics, such as biocompatibility, size, charge, drug release and polymer degradation rate.

Systemic Drug Delivery Via Pulmonary Route

Biodegradable polymers can be used for nanocarrier-based strategies for the systemic delivery of drugs, peptides, proteins, genes, siRNA and vaccines by the pulmonary route. Chemical modifications to PLGA add several benefits in the selection of a suitable material for nanocarriers in the lung. The introduction of positive or negative charges can enhance the encapsulation efficiency and release profile of oppositely-charged drugs, proteins, or genetic material.

There are several advantages of pulmonary delivery over systemic administration, and siRNA drugs in clinical trials are being delivered intranasally or by inhalation. One of the limitation for of this route is that air-blood barrier has only limited permeability toward large, hydrophilic biopharmaceuticals such as nucleic acids. Nanoparticle formulations are under investigation for improving pulmonary delivery of siRNAs.

An issue that remains surrounded by considerable debate is the question whether the lung should be used as an entry port for systemic drug administration. In this context, the safety of the nanocarriers and a lack of inflammatory and immunogenic potential need to be demonstrated under chronic treatment conditions. Such studies have not been presented with drug-loaded nanocarriers, but will be necessary during future clinical trials. Such issues are not limited to pulmonary drug delivery, but are also important in oral and intravenous administration.

Nanoparticle Drug Delivery for Effects on the Respiratory System

It is generally accepted in the field of pulmonary delivery that particles must be in the range of $1-3 \mu$ to be delivered effectively to the deep lung. Larger particles have too much energy and hit the walls of the branching upper airways. Smaller particles do not have enough energy and tend to drift and adhere to the walls of the upper airways. However, as particle size is reduced further still, into the nanometer range, an increase in deep lung deposition is seen. Efficient particle deposition in the alveoli can be achieved with nanoparticles in the size range of 50–100 nm as compared to 1–5 um for the lower airways but this range of nanoparticles has not been exploited in therapeutic setting (Rogueda and Traini 2007). This is partly due to technological limitations of generating stable aerosols on nanoscale. Nebulizers are the most advanced in using the nanoscale, pressurized metered dose inhalers require further development to realize their potential, and dry powder inhalers are specifically in need of a dry solid nanoparticle generation technique to make it a reality.

Aerosolized formulation of alfa-1 antitrypsin (α 1AT) for treatment of pulmonary disorders enables 25–45% of drug particle to reach the respiratory system as compared to the intravenous infusion where only 10–15% of α 1AT reaches this site. The aerosolized α 1AT not only affects its main site of action locally, but also avoids

remaining in circulation for a long period in peripheral blood, thus avoiding immune response reactions that occur with long-term use of $\alpha 1$ AT. Aerosolozed formulation has been further refined by encapsulation of $\alpha 1$ AT in PLGA nanoparticles. A study of the size of nanoparticles in such an aerosol showed that a mean particle size of 300 nm is an appropriate size for endocytosis by the lung endothelial cells with subsequent release of $\alpha 1$ AT into the interstitial spaces where neutrophil elastase secretion affects elastin, therefore, leading to a targeted treatment for chronic obstructive pulmonary disease (Pirooznia et al. 2012).

Local delivery of siRNA to the lungs for pulmonary disorders may target resident alveolar macrophages (rAM) in the bronchoalveolar lumen, which play a critical role in lung inflammatory responses. However, appropriate formulation of siRNA in functional nanocarriers is required to avoid pulmonary toxicity. Experimental studies in mice have shown that surfactant-coated nanogels induce significant downregulation of target mRNA levels with only mild acute proinflammatory cytokine and chemokine responses (De Backer et al. 2015). Hybrid core-shell nanoparticles were shown to be safe and effective for siRNA delivery to rAM, providing a new therapeutic approach for treatment of inflammatory disorders of the lung.

Targeting of dendritic cells (DCs) that are key immune cells to enhance or suppress an immune response in the lung is a promising approach for the treatment of allergic diseases. Aerosol delivery of gold nanoparticles (AuNPs), functionalized with a DC-SIGN antibody on the particle surface, has been investigated for targeting and activating DCs in a 3D lung cellular model (Fytianos et al. 2017). DC-SIGN AuNPs showed significantly increased uptake by monocyte-derived DCs with subsequent activation compared to non-antibody-conjugated control AuNPs, independent of surface charge and show the potential of immunoengineering approaches for activation of immune cells in the lung by nanocarriers.

Fate and Toxicology of Nanoparticles Delivered to the Lungs

Soluble nanoparticles are absorbed in the blood circulation whereas insoluble nanoparticles have local action in the lung or they can be cleared by lymphatic uptake or by macrophages. Other parameters that influence toxicity of inhaled nanoparticles are chemical composition, bioavailability, surface area and morphology.

The suitability of nanoparticles, synthesized from porcine gelatin, human serum albumin, and polyalkylcyanoacrylate, as drug and gene carriers for pulmonary application was investigated in vitro on primary airway epithelium cells. Confocal laser scan microscopy and flow cytometry experiments have shown that nanoparticles were incorporated into bronchial epithelial cells provoking little or no cytotoxicity and no inflammation as measured by IL-8 release. Based on their low cytotoxicity and the lack of inflammatory reaction in combination with an efficient uptake in human bronchial epithelial cells, protein-based nanoparticles are suitable drug and gene carriers for pulmonary applications.

Nanoparticle Drug Formulations for Spray Inhalation

Drugs delivered through inhalers are usually either in a suspension (as particles dispersed in liquid), or in a solution (when the drug is dissolved in the liquid). However, there are problems with both methods – a suspension can lead to sediment in the inhaler and less of the drug reaching the target area of the lung, while solutions present problems in dissolving the drug in the inhaler propellant liquid and can make the drug itself less stable. Preparation of the drug retains its stability, providing the possibility of slowing the release of the drug in the lung for longer therapeutic effect. This could lead to the possibility of more drugs being administered effectively by inhaler, rather than by tablet or injection. Patients suffering from conditions as diverse as asthma and diabetes could benefit from this method of drug delivery.

Nanobiotechnology for Improving Insulin Delivery in Diabetes

One of the important areas of application of nanotechnology-based pulmonary drug delivery is diabetes. Some of the techniques are described in the following paragraphs.

Inhalation of Glucose-Sensitive NP for Regulated Release of Insulin

To achieve inhalable self-regulated insulin release, a microparticle agglomerate of nano-sized liposomal particles consisting of a blood sugar sensing protein named concanavalin A (Con A) has been constructed, which is loaded with insulin and cross-linkages are capable of cleavage by glucose (Karathanasis et al. 2007). Con A releases the particles to bind independently to the sugars, which then release their insulin. The particles exhibited a small aerodynamic diameter within the human respirable range, but a large geometric diameter that prevents macrophage uptake and clearance. Upon intratracheal instillation of the glucose-sensitive nanoparticle into the lungs of rats, hyperglycemic events triggered an acceleration of the release of insulin achieving normoglycemia shortly after sensing the elevated systemic glucose. This work is a demonstration of an inhalable particle with long residence times in the lungs capable of modulating insulin release based on systemic glucose levels and thus mimic the functions of the pancreas. This approach has the potential of improving management of diabetes by regulated insulin delivery.

Pulmonary Delivery of Insulin By Surface Acoustic Wave Technology

There has been growing interest in the potential for the systematic delivery of drugs and therapeutic agents (e.g. peptides and proteins) via pulmonary (inhalation) means. Surface acoustic wave technology (SAW) enables well-controlled generation of fine nanoparticles, and is ideal for this pulmonary drug delivery, particularly for several drugs that require frequent dosing. An important application of this technology will be for the development of a device producing insulin nanoparticles delivered across the pulmonary alveoli. There is already evidence for increased efficacy of inhaled insulin compared to injected insulin, due to faster uptake and clearance. An economically viable microdevice for portable pulmonary drug delivery for human use based on SAW has significant commercial potential. Another advantage of using noninvasive techniques as alternatives to frequent injections would be the profound impact on a child's willingness to comply with diabetic treatment.

Nanotechnology-Based Pharmaceuticals for Pulmonary Disorders

Nanoparticle formulations of drugs gives them an advantage over conventional dosage forms in colloidal systems for pulmonary drug delivery by inhalation (Paranjpe and Müller-Goymann 2014). Most of nanoparticle-based colloidal systems remain in the preclinical phases of drug development, and only are available in the market. Table 11.1 shows drugs incorporated into nanoparticle systems for pulmonary application.

Poorly soluble drugs can be incorporated in various colloidal systems. Lipidbased colloidal systems have an added advantage owing to their physiological components in the formulation.

Nanotechnology-Based Treatment of Pulmonary Disorders

Management of Cystic Fibrosis

Cystic fibrosis (CF) is the most common autosomal recessive disorder in Caucasians. CF affects approximately one in 2000–2500 live births with a carrier rate in white Americans of one in 25. There are about 30,000 CF patients in the US, and 2000 babies with CF are born every year. An estimated eight million are carriers. Parents of a child with CF, who are carriers but do not have the condition, are at a one-in-four risk of having a child with CF with each pregnancy. CF is a multisystem disorder of children and adults characterized by an abnormality of exocrine gland function, which manifests as chronic respiratory tract infections and malabsorption. Cystic fibrosis transmembrane conductance regulator (CFTR) gene has been isolated. Determining the sweat chloride concentration is the standard screening test (high level of chloride ion means a positive test). It is not suitable for prenatal diagnosis and cannot detect carriers. The method of choice is identification of DF508 (the most common mutation) by PCR, which detects 85–95% of CF carriers.

Disease/drug	Type of nanoparticle
Anti-asthma/anti-inflammatory	
Beclomethasone	Lipid NC
Budesonide	SLN, liposomes
Curcumin	SLN, polymeric NP
Indomethacin	Lipid NP
Fluticasone	Dried NP
Pirfenidone	Polymeric NP
Anti-cancer	
Cisplatin	Dried NP
Methotrexate	Polymeric NP
Paclitaxel	Polymeric NP
Silibinin	SLN
Anti-oxidants	
Antioxidants-multiple types	Liposomes, polymeric NP, SLM
Lung infections	
Amikacin	Liposomes, SLN
Amphotericin B (Ambisome®)	Liposomes (parenteral)
Anti-tuberculosis drugs	SLN, polymeric NP, Liposomes
Ciprofloxacin	Liposomes
Moxifloxacin-Ofloxacin	Dried NP, MP
Tobramycin-Clarithromycin-Vancomycin	Spray dried NP, MP
Voriconazole	Polymeric NP
Tacrolimus	Lipid NP
Itraconazole	Lipid NC, dried NP
Proteins, peptides and macromolecules	-
Calcitonin	Polymeric liposomes
Heparin	Polymeric NP
Insulin	SLN
Exendin-4	Polymeric NP
Pulmonary arterial hypertension/congestive hea	rt failure
Iloprost	Liposomes
Sildenafil	Polymeric NP, SLN
Carvedilol	Polymeric NP
Surfactant, gene and antibody delivery	·
siRNA/gene	Polymeric NP
Surfactant therapy	Liposomes
DNA vaccine	Polymeric liposomes
IgG1	Self-assembly NP

 Table 11.1
 Pharmaceuticals incorporated into nanoparticle systems for pulmonary application

Reproduced from: Paranjpe and Müller-Goymann (2014). By permission *Abbreviation: SLN* solid lipid nanoparticles, *SLM* solid lipid microparticles, *NP* nanoparticles, *NC* nanocarriers

CF is a potentially lethal disease although the current life expectancy has improved to >30 years with advances in the medical treatment. CF also affects the digestive system, resulting in progressive disability and early death. Thick mucous production in the airways leads to distorted mucociliary clearance and weakening of the immune system leading to frequent lung infections. Currently used methods for the treatment of pulmonary complications of CF include physiotherapy, bronchodilator therapy, mucolytic agents, corticosteroids and lung transplant. These methods are directed at the management of manifestations and none of these addresses the cause of the disease. Because of the devastating clinical sequelae and the lack of definitive therapy, CF is prime candidate for gene therapy.

The goal of gene therapy is correction of the mutant CFTR gene with wild-type (wt) DNA sequences to restore normal CFTR protein and function. Experiments with wtCFTR cDNA expression vectors have shown that Cl- ion transport pheno-type associated with CF can be corrected to resemble that in normal cells. Several methods of gene transfer are use including those involving nanobiotechnology.

Nanobiotechnology-Based Gene Transfer in CF

Nonviral DNA Nanoparticle-Mediated CFTR Gene Transfer

CF is not readily amenable to gene therapy because of its systemic nature and difficulties including in vivo gene delivery and transient gene expression. Nanoparticles have been used for CFTR gene delivery in the nose of CF patients in clinical trials and led to partial correction of the chloride transport defect in nasal epithelium. Several experimental studies have explored refinements in nanoparticle-mediated CFTR gene transfer.

Nanoparticles consisting of single molecules of DNA condensed with PEGsubstituted lysine 30-mers have been shown to efficiently transfect lung epithelium following intrapulmonary administration (Fink et al. 2006). Nanoparticles formulated with lysine polymers having different counterions at the time of DNA mixing have distinct geometric shapes: trifluoroacetate or acetate counterions produce ellipsoids or rods, respectively. Based on intracytoplasmic microinjection studies, nanoparticle ellipsoids having a minimum diameter less than the 25-nm nuclear membrane pore efficiently transfect non-dividing cells. This 25-nm size restriction corresponds to a 5.8 kbp plasmid when compacted into spheroids, whereas the 8-11 nm diameter of rod-like particles is smaller than the nuclear pore diameter. In mice, up to 50% of lung cells are transfected after dosing with a rod-like compacted expression plasmid, and correction of the CFTR chloride channel was observed in humans following intranasal administration. To further investigate the potential size and shape limitations of DNA nanoparticles for in vivo lung delivery, reporter gene activity of ellipsoidal and rod-like compacted luciferase plasmids ranging in size between 5.3 and 20.2 kbp was investigated. Equivalent molar reporter gene activities

were observed for each formulation, indicating that microinjection size limitations do not apply to the in vivo gene transfer setting.

Chitosan-DNA-FAP-B nanoparticles are good candidates for targeted gene delivery to fibronectin molecules (FAP-B receptors) of lung epithelial cell membrane. In a study aerosol delivery of chitosan-DNA-FAP-B nanoparticles resulted in 16-fold increase of gene expression in the mice lungs compared with chitosan-DNA nanoparticles suggested that Chitosan-FAP-B nanoparticle can be a promising carrier for targeted gene delivery to the lung (Mohammadi et al. 2011).

A hCFTR expression plasmid was optimized as a payload for compacted DNA nanoparticles formulated with PEG-substituted 30-mer lysine peptides. Compared to hCFTR cDNA, the codon-optimized version (CO-CFTR) produced a 9-fold increased level of hCFTR protein in CF mice, when compacted as DNA nanoparticles (Padegimas et al. 2012).

Triplex-forming PNA molecules and donor DNA in biodegradable polymer nanoparticles have been used to correct F508del mutation and this modification was confirmed with sequencing as well as a functional chloride efflux assay, which shows that in vitro correction occurs in up to 25% of human cells. Intranasal application of nanoparticles in CF mice produces changes in nasal epithelium consistent with corrected CFTR, with gene correction also detected in lung tissue (McNeer et al. 2015). Thus, genome engineering in vivo with oligonucleotides using a nanoparticle system can achieve clinically relevant levels of gene editing without off-target effects. This vector can be used for direct in vivo gene editing with other nucleic-acid based approaches, such as short fragment homologous recombination and CRISPR/Cas9 plasmid systems.

Liposome-Mediated CFTR Gene Transfer

Lipofection of cells in vitro with CFTR cDNA constructs can, like virally transduced cells, elicit the electrophysiological responses characteristic of the CFTR ion channel. The advantages of liposome-mediated gene transfer are the potential for standardized production of large amount of vector, freedom from risk of viruses, and the possibility of re-administration with minimal host reaction. The disadvantages are the lack of sustained expression using current strategies. The safety and efficacy of this technique was demonstrated in rodents and clinical trials have been conducted in CF patients.

Magnetofection for Enhancing Nonviral Gene Transfer to the Airways

In experimental studies, superparamagnetic nanoparticles with either the therapeutic CF gene or a reported gene attached to them were inhaled and targeted to the airway epithelium via positioning of a strong magnet over the target site, which functions to pull the particles into contact with the cells. To improve the in vivo transfection efficiency of DNA delivery of this system, an oscillating magnet array system (TransMAG) was developed to introduce energy and a lateral component to advance the movement and interaction of the particles coupled with Lipofectamine 2000 to form a plasmid DNA (pDNA) liposome complexes for enhancing interaction with the epithelial cells (Xenariou et al. 2006). Although exposure to a magnetic field improved in vitro transfection efficiency, translation to the in vivo setting has remained difficult.

NP-Based Delivery of Antibiotics for Treatment of Pulmonary Infections in CF

Pulmonary infections are common in CF and are currently treated with antibiotics for the infectious agent. However, many of these bacteria are resistant to multiple antibiotics and require prolonged treatment with intravenous antibiotics such as tobramycin, ciprofloxacin and piperacillin. Inhaled therapy with other antibiotics is also followed in some cases to improve lung function by impeding the growth of colonized bacteria. These antibiotics may produce side effects such as hearing loss and kidney failure. To address these shortfalls, a liposomal formulation of ciprofloxacin powder manufactured using a sprayfreeze drying process with the required mass mean aerodynamic diameter and fine particle fraction has been used. This is administered by inhalation and thus increases the bioavailability of the drug.

Respiratory tract infections are the primary cause of death in persons with CF, and there are no effective therapies for patients infected with bacterial species that are resistant to all known antibiotics. A surfactant-stabilized oil-in-water nanoemulsion, NB-402 (NanoBio Corporation), was found to be bactericidal against all but two of 150 bacterial strains, regardless of their levels of resistance (LiPuma et al. 2009). NB-402 has been shown to be highly efficacious in vitro against *Pseudomonas aeru-ginosa, Burkholderia, Acinetobacter, Stenotrophomonas,* and other multidrug-resistant bacterial strains from CF patients. In addition, the nanoemulsion retains activity when organisms are growing in biofilms and mucus. Resistance to the nanoemulsion is not anticipated based on its unique mechanism of action of interacting with the bacterial membrane and causing lysis. These results support NB-402's potential role as a novel antimicrobial agent for the treatment of infection due to CF-related opportunistic pathogens. NB-402 is being investigated for antibiotic-resistant skin infections in burns but no further development for CF has been reported.

Nanotechnology-Based Treatment of Chronic Obstructive Pulmonary Disease

Chronic airway inflammation and mucous hypersecretion are features of chronic obstructive pulmonary disease (COPD), asthma and CF. One of the major challenges in drug delivery and therapeutic efficacy are airway defense, severe inflammation and mucous hypersecretion, which are further aggravated by infection. Treatments such as corticosteroids and antibiotics aim to controlling chronic inflammation.

Few of the numerous available nano-based drug delivery systems have been tested for COPD. Targeted nanoparticle-mediated sustained drug delivery is required to control inflammatory cell chemotaxis, fibrosis, protease-mediated chronic emphysema and/or chronic lung obstruction in COPD. Design and development of nano-based targeted vehicles with integrated therapeutic, imaging and airway-defense penetrating capability are currently being evaluated to treat the underlying cause of CF and COPD lung disease (Vij 2011).

Nanotechnology-Based Treatment of Pulmonary Inflammation

Inflammation can be inhibited by Mycobacterium tuberculosis mannose-capped lipoarabinomannan, which inhibits the release of proinflammatory cytokines by LPS-stimulated human dendritic cells (DCs) via targeting the C-type lectin receptor DC-specific intercellular adhesion molecule 3-grabbing nonintegrin (DC-SIGN). A set of poly(phosphorhydrazone) dendrimers grafted with mannose units that differed by size and the number and length of their ($\alpha 1 \rightarrow 2$)-oligon manoside caps, called mannodendrimers, have been designed and synthesized with the aim of mimicking the bioactive supramolecular structure of mannose-capped lipoarabinomannan (Blattes et al. 2013). A third-generation dendrimer bearing 48 trimannoside caps (3 T) and a fourth-generation dendrimer bearing 96 dimannosides (4D) displayed the highest binding avidity for DC-SIGN. Moreover, these dendrimers inhibited proinflammatory cytokines, including TNF- α , production by LPS-stimulated DCs in a DC-SIGN-dependent fashion. Finally, in a model of acute lung inflammation in which mice were exposed to aerosolized LPS, oral administration of 3 T mannodendrimer was found to significantly reduce neutrophil influx via targeting the DC-SIGN murine homolog SIGN-related 1. The 3 T mannodendrimer therefore represents an innovative fully synthetic compound for the treatment of lung inflammatory diseases.

References

- Blattes E, Vercellone A, Eutamène H, et al. Mannodendrimers prevent acute lung inflammation by inhibiting neutrophil recruitment. Proc Natl Acad Sci U S A. 2013;110:8795–800.
- De Backer L, Naessens T, De Koker S, et al. Hybrid pulmonary surfactant-coated nanogels mediate efficient in vivo delivery of siRNA to murine alveolar macrophages. J Control Release. 2015;217:53–63.
- Fink TL, Klepcyk PJ, Oette SM, et al. Plasmid size up to 20 kbp does not limit effective in vivo lung gene transfer using compacted DNA nanoparticles. Gene Ther. 2006;13:1048–51.
- Fytianos K, Chortarea S, Rodriguez-Lorenzo L, et al. Aerosol delivery of functionalized gold nanoparticles target and activate dendritic cells in a 3D lung cellular model. ACS Nano. 2017;11:375–83.
- Karathanasis E, Bhavane E, Annapragada AV. Glucose-sensing pulmonary delivery of human insulin to the systemic circulation of rats. Int J Nanomedicine. 2007;2:501–13.

- LiPuma JJ, Rathinavelu S, Foster BK, et al. In vitro activities of a novel nanoemulsion against Burkholderia and other multidrug-resistant cystic fibrosis-associated bacterial species. Antimicrob Agents Chemother. 2009;53:249–55.
- McNeer NA, Anandalingam K, Fields RJ, et al. Nanoparticles that deliver triplex-forming peptide nucleic acid molecules correct F508del CFTR in airway epithelium. Nat Commun. 2015;6:6952.
- Mohammadi Z, Dorkoosh FA, Hosseinkhani S, et al. In vivo transfection study of chitosan-DNA-FAP-B nanoparticles as a new non viral vector for gene delivery to the lung. Int J Pharm. 2011;421:183–8.
- Padegimas L, Kowalczyk TH, Adams S, et al. Optimization of hCFTR lung expression in mice using DNA nanoparticles. Mol Ther. 2012;20:63–72.
- Paranjpe M, Müller-Goymann CC. Nanoparticle-mediated pulmonary drug delivery: a review. Int J Mol Sci. 2014;15:5852–73.
- Pirooznia N, Hasannia S, Lotfi AS, Ghanei M. Encapsulation of alpha-1 antitrypsin in PLGA nanoparticles: in vitro characterization as an effective aerosol formulation in pulmonary diseases. J Nanobiotechnol. 2012;10:20.
- Rogueda P, Traini D. The nanoscale in pulmonary delivery: parts I and II. Expert Opin Drug Deliv. 2007;4:595–620.
- Rytting E, Nguyen J, Wang X, Kissel T. Biodegradable polymeric nanocarriers for pulmonary drug delivery. Expert Opin Drug Deliv. 2008;5:629–39.
- Swai H, Semete B, Kalombo L, et al. Nanomedicine for respiratory diseases. Wiley Interdiscip Rev Nanomed Nanobiotechnol. 2009;1:255–63.
- Vij N. Nano-based theranostics for chronic obstructive lung diseases: challenges and therapeutic potential. Expert Opin Drug Deliv. 2011;8:1105–9.
- Xenariou S, Griesenbach U, Ferrari S. Using magnetic forces to enhance non-viral gene transfer to airway epithelium in vivo. Gene Ther. 2006;13:1445–52.

Chapter 12 Nanoorthopedics

Introduction

Nanoorthopedics means the application of nanobiotechnology in orthopedics, the medical specialty dealing with disorders of bones and joints. Two important areas of application are bone implants and joint injuries involving cartilage.

Application of Nanotechnology for Bone Research

There is a significant need and demand for the development of a bone substitute that is bioactive and exhibits material properties (mechanical and surface) comparable with those of natural, healthy bone. Nano-sized ceramics, polymers, metals and composites are receiving considerable attention for bone tissue engineering.

Nanomechanical heterogeneity is expected to influence elasticity, damage, fracture and remodeling of bone. The spatial distribution of nanomechanical properties of bone has been quantified at the length scale of individual collagen fibrils (Tai et al. 2007). This study sheds new light on how bone absorbs energy by probing its fundamental building block, collagen embedded with tiny nanoparticles of mineral, at nanoscale. The mechanical properties of bone were shown to vary greatly within a single region only two micrometers wide. Because a variety of bone disorders lead to changes in bone structure, the discovery of the non-uniformity of bone's mechanical properties at nanoscale could lead to improved diagnoses of diseases. For example, if specific nanoscale patterns of stiffness within bone structure are tied to disease or aging, these could potentially be identified earlier or provide more conclusive evidence of a disorder. The results of this study could lead to new ways of producing improved structural composites that mimic nature's clever design that enables bones to resist sudden fractures.

Reducing Reaction to Orthopedic Implants

Currently used materials for joint replacement are not acceptable for many reasons including the non-biocompatibility of metallic materials, which produce debris due to wear and, and results in a short lifetime requiring several revisions. In orthopedic implants, titanium and/or titanium alloys often become encapsulated with undesirable soft fibrous but not hard bony tissue. There is no ideal material but use of nanomaterials for this purpose has been explored.

Although possessing intriguing electrical and mechanical properties for neural and orthopedic applications, carbon nanofibers/nanotubes have not been widely considered for these applications previously. A carbon nanofiber (CN) reinforced polycarbonate urethane composite has been developed to determine the possibility of using it inorthopedic prosthetic devices. Mechanical characterization studies determined that such composites have properties suitable for orthopedic applications. These materials enhanced osteoblast (bone-forming cell) functions whereas functions of cells that contribute to fibrous-tissue encapsulation events for bone implants (fibroblasts) decreased on PU composites containing increasing amounts of CNs. In this manner, this study provided the first evidence of the future that CN formulations may have towards interacting with bone cells, which is important for the design of successful orthopedic implants.

Control of the nanostructure can provide ceramic materials with better fatigue resistance in static and dynamic conditions whereas control of the macrostructure can provide flow tolerant materials. Combination of both materials may provide a new generation of longer lasting implants for joint replacement (Torrecillas et al. 2009).

Enhancing the Activity of Bone Cells on the Surface of Orthopedic Implants

It is of the very important to increase the activity of bone cells on the surface of materials used in the design of orthopedic implants so that such cells can promote either integration of these materials into surrounding bone or complete replacement with naturally produced bone if biodegradable materials are used. Osteoblasts are boneproducing cells and, for that reason, are the cells of interest in initial studies of new orthopedic implants. If these cells are functioning normally, they lay down bone matrix onto both existing bone and prosthetic materials implanted into the body. It is generally accepted that a successful material should enhance osteoblast function, leading to more bone deposition and, consequently, increased strength of the interface between the material and juxtaposed bone. There is evidence that carbon and alumina formulations induce significant osteoblast formation that mimics the nanodimensional crystal geometry of hydroxyapatite found in bone.

Synthetic Nanomaterials as Bone Implants

Nanoscale molecular scaffolds have been designed that resembles the basic structure of bone. Design of peptide-amphiphile structures allows nanofibers to be reversibly cross-linked to enhance or decrease their structural integrity. After cross-linking, the fibers can direct mineralization of hydroxyapatite to form a composite material. Nanofibers, approximately 8 nm in size, come in the form of a gel that can be injected into a broken bone to help the crystallization process for repair of fracture. This approach recreates the structure of bone at the nanoscale level and has implications beyond bone repair. It could lead to development of a hardening gel that speeds the healing of fractures. It could also help patients avoid conventional surgery or be used to repair bone fractures of soldiers in battlefield.

NanoBone Implants

Another method of repairing bones using nanotechnology is based on bone scaffold material (nano- hydroxyapatite (HA)/collagen/PLA composite) produced by biomimetic synthesis. It shows some features of natural bone both in main composition and hierarchical microstructure, which is nano-hydroxyapatite and collagen assembled into mineralized fibrils. The 3D porous scaffold materials mimic the microstructure of cancellous bone. When implanted into bone defects in animal models, it is partially substituted by new bone after a few months.

The scaffolds or "NanoBones" have successfully implanted in patients in China for repair of bone defects after fractures or tumor removal and for spinal fusion. The NanoBone material is inserted where the bone needs to heal. The critical material is calcium phosphorus, which is reduced to 30 nm in thickness and 60 nm in width. At this size, the properties of calcium phosphorus change. On a large scale the calcium phosphorus does not degrade, but it does so on a nanoscale. The nanoscale material degrades after a minimum of 6 m, and the space is filled by natural bone. This technology is better than current methods that use ceramics or metals because those materials remain in the patient's body and can cause infection, pain and make the repaired bone more vulnerable to fracture. The technology has been found to be effective in repairing small bones ranging from 1 to 2 cm in length, making the technology useful after removal of bone tumors. Research is currently being performed on larger bones up to 4 cm in length. The NanoBone technology, which was approved by China's regulatory agency, is available for commercial use in Chinese hospitals. The cost of the NanoBone implant, which is initially high, is expected to be reduced over time to be economically competitive with other technologies available.

Although nano hydroxyapatite (HA) has wide range of medical applications, particle mobilization and slow resorption limits its use in certain applications, particularly, periodontal and alveolar ridge augmentation. However, the rate of resorption of a composite of hydroxyapatite and chitosan is higher than hydroxyapatite

and may have a great impact on human health care systems as bioresorbable bone substitute. A transparent and slight yellow chitosan (CS)/HA nanocomposite with high performed, potential application as internal fixation of bone fracture was prepared in China by a novel and simple in situ hybridization. The bending strength and modulus of CS/HA with ratio of 100/5 (wt/wt) was slightly higher than that of pure CS rod.

NanoBone Versus BioOss

A study has compared the biocompatibility of a synthetic bone substitute, NanoBone®, to the widely used natural bovine bone replacement material BioOss® (Liu et al. 2011). The in vitro response of human osteoblasts to both materials was investigated. Cell performance was assessed using SEM, cell vitality staining and biocompatibility tests. Both materials showed low cytotoxicity and good biocompatibility as they caused only little damage to human osteoblasts, which can justify their clinical application. However, NanoBone® could support and promote proliferation of human osteoblasts slightly better than BioOss®. The results may guide physicians in the choice between a natural or a synthetic biomaterial. Further experiments are necessary to determine the comparison of biocompatibility in vivo.

Nanoparticles for Repairing Bone Cracks

Bone microcracks, which can lead to broken bones in patients with osteoporosis and other related conditions, generate ion gradients that can be utilized for active targeting and treatment. Fluorescent quantum dots made from a synthetic material have been safely delivered to microcracks model system using bone from a human tibia and femur (Yadav et al. 2014). The aim is to attach the biological material, in this case a drug used to treat osteoporosis, to a FDA-approved synthetic material such as a nanotruck, to a crack in human bone. Using the ion gradient as a power source, the researchers hope to develop a self-powered nanotruck that could effectively carry and deliver the osteoporosis drug, and be safe to use within the human body. In a final series of experiments, the nanodrug was tested on live human bone cells, which increased in number as compared with those that were not treated with the osteoporosis drug. This confirms other studies that have demonstrated that this drug is effective in repairing human bones.

Nanotechnology-Based Bone Regeneration

Traumatic wounds and congenital defects that require large-scale bone tissue repair have few successful clinical therapies. Although bioactive materials are available for bone repair, there is need for an optimized materials system for reproducible, safe, and targeted repair. Controlled, rapid bone formation in large bone defects could be induced by simultaneously delivering multiple biological growth factors to the site of the wound.

Delivery of Growth Factors for Bone Repair and Regeneration

A nanotechnology-based approach has been described for bone repair using a polyelectrolye multilayer coating carrying as little as 200 ng of bone morphogenetic protein-2 and PDGF-BB that were eluted over readily adapted time scales to induce rapid bone repair (Shah et al. 2014). Based on electrostatic interactions between the polymer multilayers and growth factors alone, mitogenic and osteogenic signals were sustained with these growth factors in an easily tunable and controlled manner to direct endogenous cell function. To prove the role of this adaptive release system, polyelectrolyte coating was applied on a well-studied biodegradable PLGA support membrane. The released growth factors directed cellular processes to induce bone repair in a critical-size rat calvaria model. The released growth factors promoted local bone formation that bridged a critical-size defect in the calvaria as early as 2 week after implantation, and was mechanically competent. Such an approach could be clinically useful and has significant benefits as a synthetic, off-the-shelf, cell-free option for bone tissue repair and restoration.

Role of Nanoparticles in Regenerative Therapy for Osteoporosis

Osteoporosis is characterized by progressive loss of bone due to aging and menopause in women leading to bone fragility with increased susceptibility to fractures. Therapy is based on either promoting strength (via osteoblast action) or preventing disease (via osteoclast action). Current pharmacotherapy with antiresorptive and anabolic drugs as well as hormones are limited by poor pharmacokinetic and pharmacodynamic profiles. Diagnosis and therapy of osteoporosis is challenging. Nanoparticles (NPs) provide an imaging tool as well as an effective therapeutic carrier in bone diseases. Nanotechnology-based therapeutics include the use of inorganic nanoparticles containing gold, platinum, silica and ceria have an additional advantage of inducing osteoblastic proliferation of bone. Incorporation of NPs into the scaffolds improves mechanical strength as well as regeneration during bone grafting (Gera et al. 2017). Targeted, modified and coated magnetic nanoparticles along with gold and quantum dots provide opportunities for biomedical imaging by replacing the traditional invasive radionuclide techniques.

Aligning Nanotubes to Improve Artificial Joints

Artificial joints might be improved by making the implants out of tiny carbon nanotubes (CNTs) with diameter ~ 60 nm and filaments that are all aligned in the same direction, mimicking the alignment of collagen fibers and natural ceramic crystals in real bones. The smaller features stimulate the growth of more new bone tissue, which is critical for the proper attachment of artificial joints once they are implanted. CNTs and nanofibers are aligned in the same direction and this orientation is like the way collagen and natural ceramic crystals, called hydroxyapatite, are aligned in bone. One-third more bone-forming cells (osteoblasts) attach to CNTs that possess surface bumps about as wide as 100 nm than to conventional titanium, which has surface features on the scale of microns. The nanometer-scale bumps mimic surface features of proteins and natural tissues, prompting cells to stick better and promoting the growth of new cells. Using such nanometer-scale materials might cause less of a rejection response from the body. Rejection eventually weakens the attachment of implants and causes them to become loose and painful, requiring replacement surgery. Aligning the nanotubes to further mimic natural bone also might provide more strength.

Carbon Nanotubes as Scaffolds for Bone Growth

Artificial bone scaffolds have been made from a wide variety of materials, such as polymers or peptide fibers. Their drawbacks include low strength and the potential for rejection in the body. Chemically functionalized SWCNTs have been used as scaffolds for the growth of artificial bone material. The strength, flexibility and light weight of SWCNTs enable them to act as scaffolds to hold up regenerating bone. Bone tissue is a natural composite of collagen fibers and crystalline hydroxyapatite, which is a mineral based on calcium phosphate. SWCNTs can mimic the role of collagen as a scaffold for inducing the growth of hydroxyapatite crystals. By chemically treating the nanotubes, it is possible to attract calcium ions and to promote the crystallization process while improving the biocompatibility of the nanotubes by increasing their water solubility. SWCNTs may lead to improved flexibility and strength of artificial bone, new types of bone grafts and to inroads in the treatment of osteoporosis and fractures.

A nanowire coating on the surface of biocompatible titanium can be used to create more effective surfaces for hip replacement, dental reconstruction and vascular stenting. Further, the material can easily be sterilized using ultraviolet light and water or using ethanol, making it useful in hospital settings. The length, the height, the pore openings and the pore volumes within the nanowire scaffolds can be controlled by varying the time, temperature and alkali concentration in the reaction. In contrast to the titanium implant, which may fail after some years because of nonadherence to it of muscle tissue and require reoperation, the nanowire-coated joint adheres to the muscle tissue as shown in experimental animals.

Bone cells can grow and proliferate on a scaffold of CNTs because they are not biodegradable, but behave like an inert matrix on which cells can proliferate and deposit new living material, which becomes functional, normal bone. CNTs carrying neutral electric charge sustained the highest cell growth and production of plateshaped crystals. There was a dramatic change in cell morphology in osteoblasts cultured on multiwalled CNTs, which correlated with changes in plasma membrane functions. CNTs hold promise in the treatment of bone defects in humans associated with the removal of tumors, trauma, and abnormal bone development and in dental implants. More research is needed to determine how the body will interact with carbon nanotubes, specifically in its immune response.

By using stem cells attached to titanium oxide nanotube implants, precise change in nanotube diameter can be controlled to induce selective differentiation of hMSCs into osteoblasts (Oh et al. 2009). Small (\approx 30-nm diameter) nanotubes promoted adhesion without noticeable differentiation, whereas larger (\approx 70- to 100-nm diameter) nanotubes elicited a dramatic stem cell elongation (\approx 10-fold increased), which induced cytoskeletal stress and selective differentiation into osteoblast-like cells, offering a promising nanotechnology-based route for unique orthopedics-related hMSC treatments. Use of nanostructures is preferable to chemicals for stem cell implants to control cell differentiation as chemicals can sometimes have undesirable side effects on the human body. Clinical implication of this research is that if the surgeon uses titanium oxide nanotubes with stem cells, the bone healing could be accelerated following fracture of leg bones and a patient may be able to walk in 1 month instead of being on crunches for 3 months.

Nanoparticle-Based Hydrogels for Cartilage Regeneration

Chondrocytes, the cartilage-producing cells within a joint, are mostly inactive. However, when the same joint is moving the cells activate receptors that respond to growth factors produced within the body. Simultaneously, the chondrocytes become sensitive to treatments that will help them regenerate. A hydrogel capable of promoting cartilage regeneration has been developed, which will deliver drugs only once it has reached a threshold temperature by generation of heat from friction in the movement of the joint (Moghadam et al. 2014). The matrix contains liposomal nanoparticles and TGF- β growth factor. Under the effect of heat, the nanoparticle diameter decreases by a third, leaving gaps in the matrix where the growth factor will flow out into the target area. The matrix could be arthroscopically implanted at the site of the damaged cartilage, before targeted physical therapy.

Nanotechnology for Engineering of Cartilage Replacement

Use of nanotechnology is being explored to produce viable structural and functional scaffolds capable of promoting the growth of mesenchymal stem cells (MSCs), and differentiate these cells into meniscal tissue. A thorough understanding is needed of how MSCs interact with scaffolds and how to optimize conditions promoting the cell growth around these scaffolds, which should not only encourage cell growth, but must also degrade at the correct rate so that all that remains is meniscal tissue.

In an experimental study, the nanofiber scaffolds enhanced cartilaginous tissue formation by mimicking physical and biological cues of native extracellular matrix, suggesting their potential utility for articular cartilage repair (Coburn et al. 2012).

Apart from the knee, regeneration of intervertebral disc (IVD) may be a useful procedure as an alternative for spinal fusion because there is inherent limitation of hardware-based IVD replacement prostheses, which indicates the importance of biological approaches to disc repair. In one study, multipotent, adult human MSCs were seeded into a novel biomaterial amalgam to develop a biphasic construct that consisted of electrospun, biodegradable nanofibrous scaffold (NFS) enveloping a hyaluronic acid (HA) hydrogel center (Nesti et al. 2008). The cartilaginous HA/NFS construct architecturally resembled a native IVD, with an outer annulus fibrosus-like region and inner nucleus pulposus-like region. Histological and biochemical analyses, immunohistochemistry, and gene expression profiling revealed the time-dependent development of chondrocytic phenotype of the seeded cells. The cells also maintain the microarchitecture of a native IVD. These findings suggest the potential of MSC-seeded HA/NFS constructs for the tissue engineering of biological replacements of degenerated IVD.

Cartilage Disorders of Knee Joint

The meniscus is the knee's shock absorber. It is a cartilage spacer for preventing friction and absorbing approximately one third of the impact load that the joint cartilage surface experiences. Cartilage injuries of the knees are one of the common injuries in sports, particularly football and hockey. Unlike other body tissues, the meniscus does not repair itself because only a very small part receives blood. The conventional treatment of a torn cartilage is surgical removal of the loose pieces and repair of the tear where possible to save as much as possible of the cartilage. The procedure has become refined with arthroscopy. Although the results are generally good in terms of relief of pain and recovery of function of the joint, there are long-term effects if the cartilage is lost and degenerative changes in the joints may occur.

Several methods have been developed to encourage the regeneration of cartilage defects. Procedures such as debridement, lavage, microfracturing, subchondral bone drilling and abrasion arthroplasty may perhaps alleviate symptoms, but cannot restore the hyaline articular cartilage. The regenerated tissue formed in response to these procedures consists of fibrocartilage and does not possess the biomechanical or biochemical properties of hyaline articular cartilage. Nanotechnology and cell therapy are being used as refinements of procedures to replace the torn knee cartilage.

Nanotechnology as an Aid to Arthroscopy

Arthroscopy of joints, particularly the knee joint is an established procedure for diagnosis and treatment. Nanotechnology has been used to refine this procedure. The first step was the study of cartilage by AFM as a basis for the construction of a scanning force arthroscope (SFA).

Cartilage stiffness was measured ex vivo at the micrometer and nanometer scales to explore structure-mechanical property relationships at smaller scales than has been done previously. It is possible to measure the dynamic elastic modulus in compression by indentation-type AFM. Spherical indenter tips (radius ~ 2.5 μ m) and sharp pyramidal tips (radius ~ 20 nm) were employed to probe micrometer-scale and nanometer-scale response, respectively on subsurface cartilage from porcine femoral condyles. From results of AFM imaging of cartilage, the micrometer-scale spherical tips resolved no fine structure except some chondrocytes, whereas the nanometer-scale pyramidal tips resolved individual collagen fibers and their 67-nm axial repeat distance. The cartilage compressive stiffness was different at the nanometer scale compared to the overall structural stiffness measured at the micrometer and larger scales because of the fine nanometer-scale structure, and enzyme-induced structural changes can affect this scale-dependent stiffness differently. The collagen fibers were seen to coalesce together as evidence of disease state.

Early detection and the ability to monitor the progression of osteoarthritis are important for developing effective therapies. Indentation-type AFM can monitor agerelated morphological and biomechanical changes in the hips of normal and osteoarthritic mice (Stolz et al. 2009). Early damage in the cartilage of osteoarthritic patients undergoing hip or knee replacements could similarly be detected using this method. Changes due to aging and osteoarthritis are clearly depicted at the nanometer scale well before morphological changes can be observed using current diagnostic methods. Indentation-type AFM may potentially be developed into a minimally invasive arthroscopic tool, the SFA, to diagnose the early onset of osteoarthritis in situ.

The SFA will help management of osteoarthritis by monitoring the efficiency of new drugs. It may be possible to use a hollow cantilever and tip to inject such a drug right into the affected area. A further step in the treatment of irreparably damaged cartilage is to replace it with engineered tissue, and arrays of AFM probes could be used to inspect the surface at nanometer scale.

A prototype SFA constructed at Muller Institute for Structural Biology (Basel, Switzerland) combines both diagnostics and therapeutics in a single tube in contrast to the conventional arthroscopes which have two tubes - one for visualization and the other for manipulation with instruments. There are inflatable balloons to provide an irrigation system. This prototype fulfills the requirements of an ideal arthroscope:

- It is user friendly
- · It provides information not obtainable by conventional methods
- It is expected to have an affordable price tag.

The device has been tested only in models of knee joint. It is expected to be in the market in the future.

Nanotechnology-Based Therapy for Osteoarthritis

Osteoarthritis (OA) is a major cause of disability and morbidity in the aging population. Joint injury leads to cartilage damage, a known determinant for subsequent development of posttraumatic OA, which accounts for 12% of all OA. Understanding the early molecular and cellular responses postinjury may provide targets for therapeutic interventions that limit articular degeneration. Using a murine model of controlled knee joint impact injury that allows the examination of cartilage responses to injury at specific time points, a study has shown that intraarticular delivery of a peptidic nanoparticle complexed to NF-KB siRNA significantly reduces early chondrocyte apoptosis and reactive synovitis (Yan et al. 2016). The data suggest that NF-kB siRNA nanotherapy maintains cartilage homeostasis by enhancing AMPK signaling while suppressing mTORC1 and Wnt/ β -catenin activity. These findings delineate an extensive crosstalk between NF-KB and signaling pathways that govern cartilage responses postinjury and suggest that delivery of NF-kB siRNA nanotherapy to attenuate early inflammation may limit the chronic consequences of joint injury. Therapeutic benefits of siRNA nanotherapy may also apply to primary OA in which NF-kB activation mediates chondrocyte catabolic responses. Additionally, a critical barrier to the successful development of OA treatment includes ineffective delivery of therapeutic agents to the resident chondrocytes in the avascular cartilage. Here, we show that the peptide-siRNA nanocomplexes are nonimmunogenic, are freely and deeply penetrant to human OA cartilage, and persist in chondrocyte lacunae for at least 2 week. The peptide-siRNA platform thus provides a clinically relevant and promising approach to overcoming the obstacles of drug delivery to the highly inaccessible chondrocytes.

References

- Coburn JM, Gibson M, Monagle S, et al. Bioinspired nanofibers support chondrogenesis for articular cartilage repair. Proc Natl Acad Sci U S A. 2012;109:10012–7.
- Gera S, Sampathi S, Dodoala S. Role of nanoparticles in drug delivery and regenerative therapy for bone diseases. Curr Drug Deliv. 2017 (in press); Epub ahead of print.
- Liu Q, Douglas T, Zamponi C, et al. Comparison of in vitro biocompatibility of NanoBone® and BioOss® for human osteoblasts. Clin Oral Implants Res. 2011;22:1259–64.
- Moghadam MN, Kolesov V, Vogel A, et al. Controlled release from a mechanically-stimulated thermosensitive self-heating composite hydrogel. Biomaterials. 2014;35:450–5.
- Nesti LJ, Li WJ, Shanti RM, et al. Intervertebral disc tissue engineering using a novel hyaluronic acid-nanofibrous scaffold (HANFS) amalgam. Tissue Eng Part A. 2008;14:1527–37.
- Oh S, Brammer KS, Lib YS, et al. Stem cell fate dictated solely by altered nanotube dimension. Proc Natl Acad Sci U S A. 2009;106:2130–5.
- Shah NJ, Hyder MN, Quadir MA, et al. Adaptive growth factor delivery from a polyelectrolyte coating promotes synergistic bone tissue repair and reconstruction. Proc Natl Acad Sci U S A. 2014;111:12847–52.
- Stolz M, Gottardi R, Raiteri R, et al. Early detection of aging cartilage and osteoarthritis in mice and patient samples using atomic force microscopy. Nat Nanotechnol. 2009;4:186–92.
- Tai K, Dao M, Suresh S, et al. Nanoscale heterogeneity promotes energy dissipation in bone. Nat Mater. 2007;6:454–62.
- Torrecillas R, Moya JS, Diaz LA. Nanotechnology in joint replacement. WIREs Nanomed Nanobiotechnol. 2009;1:540–52.
- Yadav V, Freedman JD, Grinstaff M, Sen A. Bone-crack detection, targeting, and repair using ion gradients. Angew Chem Int Ed. 2014;15:5852–73.
- Yan H, Duan X, Pan H, et al. Suppression of NF-κB activity via nanoparticle-based siRNA delivery alters early cartilage responses to injury. Proc Natl Acad Sci U S A. 2016;113:E6199–208.

Chapter 13 Nanoophthalmology

Introduction

Nanotechnology has many applications in disorders of eye, which could be included under the heading of nanoophthalmology. These include drug delivery, study of pathomechanism of eye diseases, regeneration of the optic nerve and counteracting neovascularization involved in some degenerative disorders. Nanoparticles enable delivery of ocular drugs to specific target sites and results to date strongly suggest that ophthalmology will benefit enormously from the use of this nanometric scale technology.

Nanocarriers for Ocular Drug Delivery

Approximately 90% of all ophthalmic drug formulations are applied as eye drops. While eye drops are convenient, ~95% of the drug contained in the drops is lost through tear drainage, a mechanism for protecting the eye against exposure to noxious substances. Moreover, several barriers impede direct and systemic drug access to the specific site of action. The tissue barriers such as cornea, conjunctiva, blood aqueous barrier, and blood-retinal barrier limit the access of drugs to their targets. Drug delivery systems should be able to overcome ocular barriers and increase ocular bioavailability while reducing side effects (Sánchez-López et al. 2017a). The tight epithelium of the cornea compromises the permeation of drug molecules. An ideal topical drug delivery system should possess certain desirable properties, such as good corneal and conjunctival penetration, prolonged precorneal residence time, easy instillation, non-irritative and comfortable to minimize lachrymation and reflex blinking, and appropriate rheological properties.

Advantages of using nanoparticles include improved topical passage of large, poorly water-soluble molecules such as glucocorticoid drugs or cyclosporine for

Nanoparticles	Drug delivered	Advantages
Acrylate polymer nanosuspensions	Flurbiprofen	Higher drug levels in the aqueous humor and inhibition of paracentesis-induced miosis
Albumin nanoparticles	Gancyclovir	Enhanced antiviral activity against cytomegalovirus infection
Chitosan-sodium alginate nanoparticles	Antibiotic, gatifloxacin	Enhanced delivery to external ocular tissues without systemic drug exposure and/or affecting the intraocular structures (Motwani et al. 2008)
Dendrimers	Pilocarpine nitrate, tropicamide	Prolonged miotic activity
Discomes	Timolol maleate	Entraps greater amount of drug than niosomes
Lipid nanoparticles	Acetazolamide	Improve corneal absorption of drugs and well tolerated
Nanoparticles	Amikacin	Improved delivery of drug to cornea and aqueous humor
Niosomes	Cyclopentolate	Enhanced ocular absorption of the drug
Poly(butyl)-cyano acrylate nanoparticles	Pilocarpine	Enhanced miotic response by 22% and decreased IOP

Table 13.1 Nanoparticles used for drug delivery in ophthalmology

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immune-related diseases that threaten vision. Other large and unstable molecules, such as nucleic acids, delivered using nanoparticles, offer promising results for gene transfer therapy in severe retinal diseases. Nanoparticles enable targeted delivery to specific types of cancer such as melanoma, while sparing normal cells (Diebold and Calonge 2010).

Nanocarriers, such as nanoparticles, liposomes and dendrimers, are used to enhance ocular drug delivery (Vandervoort and Ludwig 2007). Easily administered as eye drops, these systems provide a prolonged residence time at the ocular surface after instillation, thus avoiding the clearance mechanisms of the eye. In combination with a controlled drug delivery, it should be possible to develop ocular formulations that provide therapeutic concentrations for a long period at the site of action, thereby reducing the dose administered as well as the instillation frequency. In intraocular drug delivery, the same systems can be used to protect and release the drug in a controlled way, reducing the number of injections required. Another potential advantage is the targeting of the drug to the site of action, leading to a decrease in the dose required and a decrease in side effects. Nanoparticles used for drug delivery in ophthalmology are shown in Table 13.1.

Dendrimers for Drug Delivery in Ophthalmology

One of the main motives of using dendrimers in ophthalmology is to overcome the limitation of agents targeted to a single molecule or receptor. Dendrimers enable polyvalent medicines, larger molecules where several ligands can bind to several

receptors to get the desired biological response. The use of dendrimers in drug delivery to the eye is also being explored to target multiple pathologies. Dendrimers can be used to prevent scar formation following eye surgery. Another use would be to disrupt inflammation and angiogenesis in the posterior chamber of the eye. Synthetically engineered dendrimers can be tailored to have defined immunomodulatory and antiangiogenic properties; they can be used synergistically to prevent scar tissue formation.

DNA Nanoparticles for Nonviral Gene Transfer to the Eye

The eye is an excellent candidate for gene therapy as it is immune privileged and much of the disease-causing genetics are well understood. Compacted DNA nanoparticles have been investigated as a system for nonviral gene transfer to ocular tissues. The compacted DNA nanoparticles have already been shown to be safe and effective in a human clinical trial, have no theoretical limitation on plasmid size, do not provoke immune responses, and can be highly concentrated. An experimental study has shown that DNA nanoparticles can be targeted to different tissues within the eye by varying the site of injection (Farjo et al. 2006). Almost all cell types of the eye can be transfected by nanoparticles and produce robust levels of gene expression that are dose-dependent. Subretinal delivery of these nanoparticles transfects nearly all the photoreceptor population and produces expression levels almost equal to that of rodopsin, the highest expressed gene in the retina. As no deleterious effects on retinal function have been observed, this treatment strategy appears to be clinically viable and provides a highly efficient nonviral technology to safely deliver and express nucleic acids in the retina and other ocular tissues. These findings have implications for the development of DNA-based therapeutics for various eye disorders, including retinitis pigmentosa, diabetic retinopathy, and macular degeneration.

Nanoparticle-Based Topical Drug Application to the Eye

Nanoparticle technology has been use for ophthalmic formulations for a decade but research is still in progress to improve the delivery and safety of drugs used for treating disorders of the eye. Topical application of nonsteroidal antiinflammatory drugs on the eye is a common treatment used to treat the inflammatory reaction manifested by narrowing of the pupil (miosis) induced by surgical injury such as cataract extraction. With the aim of improving the availability of sodium ibuprofen (IBU) at the intraocular level, IBU-loaded polymeric nanoparticle suspensions have been made from Eudragit RS100, an inert polymer resin. Particles in nanosuspension have a mean size of ~100 nm and a positive charge making them suitable for ophthalmic applications. In vitro dissolution tests indicated a controlled release profile of IBU from nanoparticles. Drug levels in the aqueous humor are also higher after application of the nanosuspensions; moreover, IBU-loaded nanosuspensions do not show toxicity on ocular tissues.

Use of chitosan (CS) nanoparticles for ocular drug delivery has been investigated by studying their interaction with the ocular mucosa in vivo and their toxicity in conjunctival cell cultures (de Salamanca et al. 2006). The in vivo interaction of fluorescent CS (CS-fl) nanoparticles with the rabbit cornea and conjunctiva was analyzed by spectrofluorimetry and confocal microscopy. CS-fl nanoparticles were found to be stable upon incubation with lysozyme and did not affect the viscosity of mucin dispersion. In vivo studies showed that the amounts of CS-fl in cornea and conjunctiva were significantly higher for CS-fl nanoparticles than for a control CS-fl solution, these amounts being constant for up to 24 h. Confocal studies suggest that nanoparticles penetrate the corneal and conjunctival epithelia. Cell survival at 24 h after incubation with CS nanoparticles was high and the viability of the recovered cells was near 100%. These findings indicate that CS nanoparticles are promising vehicles for ocular drug delivery.

Chitosan has been modified by covalent coupling to cholesterol (Yuan et al. 2006). These molecules self-aggregate into nanoparticles with a size of approximately 200 nm. Cyclosporin was incorporated with a drug loading of 6.2%. In vitro tests demonstrated that the drug was gradually released over a period of 48 h. Use of SPECT and scintillation counter demonstrated that 71% of the drug was still present at the ocular surface after 112 min.

These and other studies indicate that chitosan-based nanostructures are versatile systems that can be tailor-made according to required compositions, surface characteristics and particle size. Such parameters, which are known to influence their in vivo performance, can be modulated by adjusting the formulation conditions of the nanotechnologies responsible for their formation, by incorporating additional materials in the preparation steps, and/or by using synthetically modified chitosan.

Polylactide (PLA) nanoparticles incorporating flurbiprofen are prepared by the solvent displacement technique using poloxamer 188 as a stabilizer to improve the availability of the drug for the prevention of the inflammation caused by ocular surgery. Formulations, with particle size of 230 nm, do not show toxicity on ocular tissues. In vivo studies in rabbits have demonstrated that the formulations do not induce toxicity or irritation. Nanoparticle formulations have been compared with commercial eye drops (OcuflurTM) after induction of inflammation by instillation of sodium arachidonate. The commercial eye drop showed a suppression of inflammation, with minimal inflammation reached after 90 min. A comparable nanoparticle formulation demonstrates a higher suppression, which increased throughout the 150-min observation period.

Lipid Nanoparticles for Ocular Drug Delivery

Lipid nanoparticles are composed either of solid lipids (SLN) or of solid and liquid lipids (NLC) stabilized with surfactants. These systems have the advantages of other colloidal particles such as polymeric nanoparticles, fat emulsions and liposomes but avoid their disadvantages. Lipid nanoparticles are useful for drug or gene delivery to the eye as they can improve the corneal absorption of drugs and enhance their bioavailability. The GRAS (Generally Recognized As Safe) status of formulation excipients, the scaling-up facilities and the possibility of sterilization, make them suitable for industrial production (Sánchez-López et al. 2017b).

Nanoparticles for Intraocular Drug Delivery

Nanoparticles have also been investigated for intraocular drug delivery to provide controlled drug release, protect the drug against enzymatic degradation and to direct the drug to the site of action. The kinetics of PLA nanoparticle localization within the intraocular tissues and their potential to release encapsulated material has been studied in experimental animals. Intravitreous injection of PLA nanoparticles appears to result in transretinal movement, with a preferential localization in the retinal pigmented epithelial (RPE) cells. Encapsulated rhodamine dye diffuses from the nanoparticles and stains the neuroretina and the RPE cells. The findings support the idea that specific targeting of these tissues is feasible. Furthermore, the presence of the nanoparticles within the RPE cells 4 months after a single injection shows that a steady and continuous delivery of drugs can be achieved.

Subconjunctivally administered 200-nm and larger PLA nanoparticles can be almost completely retained at the site of injection in male Sprague-Dawley rats for at least 2 months (Amrite and Kompella 2005). The 20-nm particles disappeared more rapidly, with 8% of the administered dose remaining after 7 days. The neuroprotective effects of PLGA nanospheres to encapsulate pigment epithelium-derived factor (PEDF) has been evaluated in induced retinal ischemic injury (Li et al. 2006). Intravitreal injection of the naked peptides demonstrated a 44% reduction of cell death of the retinal ganglion cells (RGCs) after 48 h. Injection of the encapsulated peptide showed a very similar protective effect that lasted for at least 7 days. The authors attributed the extended effect to the slow release of PEDF from the PLGA particles and to the protection of the peptide against degradation and rapid clearance.

Besides size, grafting polymers with PEG is another method of controlling particle distribution. A hydrophobic polymer, cyanoacrylate-co-hexadecyl cyanoacrylate, can be coupled to hydrophilic PEG chains to produce tamoxifen-loaded nanoparticles. Intraocular injection in rats resulted in a significant inhibition of experimentally induced autoimmune uveoretinitis, whereas injection of the free drug did not alter the disease.

Nanoparticles Impregnated Ocular Inserts for Drug Delivery to the Eye

Eudragit is the brand name for a diverse range of polymethacrylate-based copolymers. Eudragit nanoparticles (NPs) have been prepared by the solvent diffusion nanoprecipitation technique and evaluated for various parameters such as particle size, zeta potential, % entrapment efficiency, % drug loading, and stability (Rathod et al. 2017). Ocular inserts of NPs, prepared by solvent casting method, were evaluated for thickness, content uniformity, folding endurance, disintegration time, morphology and stability study. Finally, the authors of this study evaluated NPs and ocular inserts for in vitro drug diffusion study, ex vivo trans-corneal permeability, in vivo ocular tolerability and intra ocular pressure reduction. The optimized formulations had size range of ~367 nm, zeta potential around +7 mV and entrapment efficiency of ~51% with ~19% drug loading. The ex vivo transcorneal study showed higher cumulative corneal permeation, flux across corneal tissue and apparent corneal permeability from drug loaded Eudragit NPs and ocular inserts as compared to drug solution Eudragit NPs were well tolerated in rabbit eyes with no inflammation indicating that a trial in humans would be safe.

Ophthalmic Drug Delivery Through Nanoparticles in Contact Lenses

Polymeric lens materials that can be loaded with nanoparticulate eye medication for ophthalmic drug delivery applications. The solution to constitute the lens contains a mixture of molecules, which create nanochannels when they set. The channels act as conduits for the drug to be released when the lens meets eye fluid. The channels also render the lens nanoporous, i.e. tears and gases can cross into and out of lens, making it more compatible with the human eye. The rate of delivery can be controlled by adjusting the channel size. The use of contact lenses loaded with nanoparticles is better than topical application of ophthalmic drugs in the form of eye drops. The drug molecules will have a much longer residence time of several days in the post lens tear film, compared with about 2–5 min in the case of topical application of drugs in the form of eye drops. This method of drug delivery would reduce drug waste and adverse effects of systemic absorption resulting and increase patient compliance. The duration of drug delivery from contact lenses can be significantly increased if the drug is first entrapped in niosomes, which are non-ionic surfactant vesicles, before they are dispersed throughout the contact lens material. This also prevents the interaction of drug with the polymerization mixture and provides additional resistance to drug release, as the drug must first diffuse through the nanoparticle and penetrate the particle surface to reach the hydrogel matrix.

Nanotechnology-Based Therapeutics for Eye Disorders

Various eye disorders where nanobiotechnology-based therapeutic delivery is useful are listed in Table 13.2.

Ophthalmic disorder/procedure	Nanotechnology-based therapeutic
Corneal disorders	
Miscellaneous corneal disorders	Indomethacin-chitosan (CS) nanoemulsion
	CS-cyclosporine (CsA) SLN
	CS/thiolated CS-sodium alginate NPs
Viral keratitis	SLNs and nanostructured lipid carriers (NLCs)
Corneal epithelial wounds	All-trans retinoic acid (atRA) NPs
Corneal neovascularization	NPs to deliver plasmids expressing Flt23k (anti-VEGF)
Keratoplasty	FK506 (immunosuppressant) PLGA
Corneal tissue engineering	Nanofibrous tissue engineering scaffolds
Corneal gene therapy	Plasmid delivery of CS-DNA NPs
Retinal diseases	
Age-related macular degeneration	PEGylated liposome-protamine-hyaluronic acid NPs (PEG-LPH-NP) loaded with siRNA
Choroidal neovascularization	Basic fibroblast growth factor (bFGF) NPs
Retinal diseases general	Aerosolized NPs
X linked juvenile retinoschisis	Gene therapy: dextran-protamine-DNA-SLN complex
	for expression of EGFP
Glaucoma	PAMAM dendrimer hydrogel/ PLGA NP for delivery of antiglaucoma drugs brimonidine and timolol maleate
Uveitis	PEG-block-PLA

Table 13.2 Nanobiotechnology-based therapy of eye disorders

Abbreviation: *EGFP* enhanced green fluorescent protein, *PLGA* poly (lactic-co-glycolic acid) copolymer, *SLN* solid lipid nanoparticles

Nanotechnology for Prevention of Neovascularization

Some of the strategies for treatment of eye disorders involve prevention of neovascularization. Examples of how nanotechnology can refine these procedures are as follows.

Photodynamic therapy (PDT) has been used for exudative age-related macular degeneration (AMD). This therapy can be refined by using a supramolecular nanomedical device, i.e. a novel dendritic photosensitizer (DP) encapsulated by a polymeric micelle formulation. The characteristic dendritic structure of the DP prevents aggregation of its core sensitizer, thereby inducing a highly effective photochemical reaction. With its highly selective accumulation on choroidal neovascularization (CNV) lesions, this treatment results in a remarkably efficacious CNV occlusion with minimal unfavorable phototoxicity.

A long-term study was performed into the use of a lipophilic amino-acid dendrimer to deliver an antivascular endothelial growth factor (VEGF) oligonucleotide (ODN-1) into the eyes of rats and inhibit laser-induced CNV (Marano et al. 2005). In addition, the uptake, distribution and retinal tolerance of the dendrimer plus oligonucleotide conjugates were examined. Analysis of fluorescein angiograms of laser photocoagulated eyes revealed that dendrimer plus ODN-1 significantly inhibited the development of CNV for 4–6 months by up to 95% in the initial stages. Eyes similarly injected with ODN-1 alone showed no significant difference. Intravitreally injected ODN-1 was absorbed by a wide area of the retina and penetrated all retinal cell layers to the retinal pigment epithelium. Ophthalmological examinations indicated that the dendrimers plus ODN-1 conjugates were well tolerated in vivo, which was later confirmed using immunohistochemistry, which showed no observable increase in antigens associated with inflammation. The use of such dendrimers may provide a viable mechanism for the delivery of therapeutic oligonucleotides for the treatment of angiogenic eye diseases.

Nanoparticles as Nonviral Vectors for Gene Therapy of Retinal Disorders

DNA nanoparticles have been shown to correct visual defects in a mouse model of retinitis pigmentosa by delivery of normal copies of genes into photoreceptor cells. DNA nanoparticles may also offer the potential to provide effective treatments for more complex eye disorders such as diabetic retinopathy, macular degeneration, and various diseases that injure ganglion cells and the optic nerve. There is a plan to move these studies to a potential human clinical trial.

Nonviral vectors based on solid lipid nanoparticles (SLN) have been investigated for the treatment of X linked juvenile retinoschisis (XLRS) by gene therapy (Delgado et al. 2012). After ocular administration of the dextran-protamine-DNA-SLN complex to the rat eyes, expression of EGFP was detected in various types of cells depending on the administration route. The vectors were also able to transfect corneal cells after topical application. Results of the study demonstrated the potential usefulness of nonviral vectors loading XLRS1 plasmid and provided evidence for their potential application for the treatment of degenerative retina disorders as well as diseases of ocular surface.

Nanobiotechnology for Treatment of Glaucoma

Glaucoma involves abnormally high pressure of the fluid inside the eye, which, if left untreated, can result in damage to the optic nerve and vision loss. Human carbonic anhydrase (hCAII), a metalloenzyme that catalyzes the reversible hydration of carbon dioxide to bicarbonate, is associated with glaucoma. High pressure occurs, in part, because of a buildup of carbon dioxide inside the eye. Drug therapy is aimed at blocking hCAII. Carbonic anhydrase inhibitors such as acetazolamide, methazolamide, ethoxzolamide and dichlorophenamide were and still are widely used systemic antiglaucoma drugs. Their mechanism of action consists in inhibition of CA isozymes present in ciliary processes of the eye with the consequent reduction of bicarbonate and aqueous humor secretion, and of elevated intraocular pressure. Nanoparticleimpregnated ocular inserts can effectively deliver significant concentrations of drugs to the posterior segment of eye after topical administration for treatment of glaucoma. Drug loaded nanoparticles in ocular insert reduce side effects of orally administered acetazolamide. Eudragit NPs and ocular insert produce significant lowering in intraocular pressure compared with the solution of free drug after topical ocular administration.

However, barely 1–3% of existing glaucoma medicines penetrate the eye. Earlier experiments with nanoparticles have shown not only high penetration rates but also little patient discomfort. The miniscule size of the nanoparticles makes them less abrasive than some of the complex polymers now used in most eye drops. A specialized cerium oxide nanoparticle has been bound with a compound that has been shown to block the activity of an hCAII (Patel et al. 2007). Carboxybenzenesulfonamide, an inhibitor of the hCAII enzyme, was attached to nanoceria particles using epichlorohydrin as an intermediate linkage. Along with the CA inhibitor, a fluorophore (carboxyfluorescein) was also attached on the nanoparticles to enable the tracking of the nanoparticles in vitro as well as in vivo. X-ray photoelectron spectroscopic studies carried out at each reaction step confirmed the successful derivatization of the nanoceria particles. The attachment of carboxyfluorescein was also confirmed by confocal fluorescence microscopy. Preliminary studies suggest that carboxybenzenesulfonamide-functionalized nanoceria retains its inhibitory potency for hCAII.

Dendrimers and other nanotechnology devices are being used for research on ophthalmic genetics and genomics as applied to glaucoma. Apart from study of the disease, there is a search for improved methods of drug delivery. The investigators are interested in devices that will enable: (1) genotyping in real-time in clinical or point-of-care situations; (2) assaying levels of gene expression in situ to enable evaluation of effects during attempted interventions; and (3) methods to deliver gene therapy to specific cell types without using viral vectors.

One of the problems in treating glaucoma is to get the drug into the cells rather than in the surrounding space or on cell surface. Trabecular meshwork (TM) cells have phagocytic properties and could be induced to take up a variety of carrier particles. A latrotoxin analog can be used to direct the dendrimer to the latrotoxin receptor on the surface of the TM cells. The presence of a relatively specific protease, PCSK1, in TM cells offers the possibility of genetically engineering the protein to be attached to the particle. This can be done via a cleavable peptide attachment that will result in release from the dendrimer once it enters the cell in which the protease is located.

Nanotechnology for Treatment for Age-Related Macular Degeneration

Although the retina is an accessible portion of the CNS, there are virtually no treatments for early age-related macular degeneration (AMD), a degenerative retinal disease that causes progressive loss of central vision and is the leading cause of irreversible vision loss in persons over the age of 50. Drugs that inhibit vascular endothelial growth factor (VEGF) have proven effective in treating late-stage AMD, but drug delivery is a problem. Nanoparticles show considerable promise for drug delivery to the retina, for gene therapy, and for construction of prosthetic artificial retinas (Birch and Liang 2007).

References

- Amrite AC, Kompella UB. Size-dependent disposition of nanoparticles and microparticles following subconjunctival administration. J Pharm Pharmacol. 2005;57:1555–63.
- Birch DG, Liang FQ. Age-related macular degeneration: a target for nanotechnology derived medicines. Int J Nanomedicine. 2007;2:65–77.
- de Salamanca AE, Diebold Y, Calonge M, et al. Chitosan nanoparticles as a potential drug delivery system for the ocular surface: toxicity, uptake mechanism and in vivo tolerance. Invest Ophthalmol Vis Sci. 2006;47:1416–25.
- Delgado D, Del Pozo-Rodríguez A, Solinís MA, et al. Dextran and protamine-based solid lipid nanoparticles as potential vectors for the treatment of X linked juvenile retinoschisis. Hum Gene Ther. 2012;23:345–55.
- Diebold Y, Calonge M. Applications of nanoparticles in ophthalmology. Prog Retin Eye Res. 2010;29:596–609.
- Farjo R, Skaggs J, Quiambao AB, et al. Efficient non-viral ocular gene transfer with compacted DNA nanoparticles. PLoS One. 2006;1:e38.
- Li H, Tran V, Hu Y, et al. A PEDF N-terminal peptide protects the retina from ischemic injury when delivered in PLGA nanospheres. Exp Eye Res. 2006;83:824–33.
- Marano RJ, Toth I, Wimmer N, et al. Dendrimer delivery of an anti-VEGF oligonucleotide into the eye: a long-term study into inhibition of laser-induced CNV, distribution, uptake and toxicity. Gene Ther. 2005;12:1544–50.
- Motwani SK, Chopra S, Talegaonkar S, et al. Chitosan-sodium alginate nanoparticles as submicroscopic reservoirs for ocular delivery: formulation, optimisation and in vitro characterisation. Eur J Pharm Biopharm. 2008;68:513–25.
- Patil S, Reshetnikov S, Haldar MK, et al. Surface-derivatized nanoceria with human carbonic anhydrase II inhibitors and fluorophores: a potential drug delivery device. J Phys Chem C. 2007;111(24):8437–42.
- Rathod LV, Kapadia R, Sawant KK. A novel nanoparticles impregnated ocular insert for enhanced bioavailability to posterior segment of eye: in vitro, in vivo and stability studies. Mater Sci Eng C Mater Biol Appl. 2017;71:529–40.
- Sánchez-López E, Espina M, Doktorovova S, et al. Lipid nanoparticles (SLN, NLC): overcoming the anatomical and physiological barriers of the eye – part I – barriers and determining factors in ocular delivery. Eur J Pharm Biopharm. 2017a;110:70–5.
- Sánchez-López E, Espina M, Doktorovova S, et al. Lipid nanoparticles (SLN, NLC): overcoming the anatomical and physiological barriers of the eye – part II – ocular drug-loaded lipid nanoparticles. Eur J Pharm Biopharm. 2017b;110:58–69.
- Vandervoort J, Ludwig A. Ocular drug delivery: nanomedicine applications. Nanomedicine. 2007;2:11–21.
- Yuan X, Li H, Yuan Y. Preparation of cholesterol-modified chitosan self-aggregated nanoparticles for delivery of drugs to ocular surface. Carbohydr Polym. 2006;65:337–45.

Chapter 14 Nanomicrobiology

Introduction

Microbiology plays an important role in practice of medicine. Nanodiagnostics have refined the detection of infectious diseases and many new nanotechnology-based therapies, particularly of viral diseases, are in development.

Nanodiagnosis of Infections

Nanobiotechnology based molecular diagnostic techniques were described in Chap. 4. Examples of specific applications for detection of infectious agents will be given in this chapter.

Detection of Viruses

Several nanotechnology-based methods have already been described in Chap. 4 including ferrofluid magnetic nanoparticles, ceramic nanospheres and nanowire sensors for viruses. Role of cantilevers, SWCNTs, QDs and surface enhanced Raman scattering (SERS) will be described in this section.

Cantilever Beams for Detection of Single Virus Particles

Microfabrication and application of arrays of silicon cantilever beams as microresonator sensors with nanoscale thickness have been applied to detect the mass of individual virus particles. The dimensions of the fabricated cantilever beams are in the range

of 4–5 μ m in length, 1–2 μ m in width and 20–30 nm in thickness. The frequency spectra of the cantilever beams, due to thermal and ambient noise, are measured using a laser Doppler vibrometer under ambient conditions. The change in resonant frequency as a function of the virus particle mass binding on the cantilever beam surface forms the basis of the detection scheme. This device can detect a single vaccinia virus particle with an average mass of 9.5 fg. Such devices can be very useful as components of biosensors for the detection of airborne virus particles. This technology has been refined as described under nanocantilever biosensors.

Carbon Nanotubes-Based Detection of Viruses

Single-walled CNTs (SWCNTs) have been functionalized under ambient conditions with either the Knob protein domain from adenovirus serotype 12 (Ad 12 Knob) or its human cellular receptor, the CAR protein, via diimide-activated amidation (Zhang et al. 2007). The biological activity of Knob protein immobilized on the nanotube surfaces was confirmed by using its labeled conjugate antibody. The activity and specificity of bound CAR on SWCNTs was evaluated first, in the presence of fluorescently labeled Knob, which interacts specifically with CAR, and second, with a negative control protein, YieF, which is not recognized by biologically active CAR proteins. In addition, current-gate voltage measurements on a dozen nanotube devices explored the effect of protein binding on the intrinsic electronic properties of the SWCNTs, and demonstrated the devices' high sensitivity in detecting protein activity. All data show that both Knob and CAR immobilized on SWCNT surfaces fully retain their biological activities, suggesting that SWCNT-CAR complexes can serve as biosensors for detecting environmental adenoviruses.

Most viruses range between 20 and 300 nm in size. Although established methods, such as PCR, virus isolation, and next-generation sequencing (NGS) have been used to detect viruses, field samples with low virus count pose major challenges in virus surveillance and discovery. A unique CNT size-tunable enrichment microdevice (CNT-STEM) can efficiently enrich and concentrate viruses collected from field samples (Yeh et al. 2016). The channel sidewall in the microdevice was made by growing arrays of vertically aligned nitrogen-doped multiwalled CNTs (N-MWCNT), where the intertubular distance between CNTs could be engineered in the range of 17–325 nm to accurately match the size of different viruses. By adjusting the iron catalyst thickness, the intertubular distance between N-MWCNTs can be adjusted to snag and trap viruses. The CNT-STEM significantly improves detection limits and virus isolation rates by at least 100 times. Using this device, the authors successfully identified an emerging avian influenza virus strain as shown in Fig. 14.1. The device is useful for low handling viral titer samples filled with contaminants. Once virus samples are purified, the researchers can transport the sealed device to a lab for analysis by NGS, PCR, ELISA, or other tests.

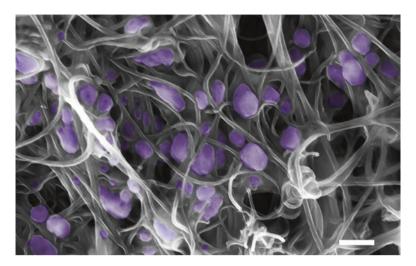


Fig. 14.1 CNTs for improvement of detection and isolation of viruses (Image from a scanning electron microscope (scale bar at 200 nm) of the H5N2 avian influenza virus seen in purple is trapped inside the aligned carbon nanotube. Source: Yeh et al. (2016), by permission)

Electric Fields for Accelerating Detection of Viruses

The rapid detection of viruses in biological samples is of increasing interest, particularly with the recent emergence of new viruses. A device that can quickly and easily detect them is difficult to construct because viral particles are present at such low concentrations in biological samples, such as blood. Typical procedures involve using passive diffusion to get the viral particles to bind to an antibody, a slow process that is not feasible for many applications, such as on the battlefield, where quick results are critical. However, liquid crystals are known to amplify signals from low concentrations of viral particles, quickly indicating if a virus is present on a surface. A study to speed up the collection of viral particles, particularly vesicular stomatitis virus, used directed assembly, in which external electrical and fluid flow fields are designed to drive nanoparticles to specific locations and in specific concentrations on a substrate (Docoslis et al. 2007). Electrical fields are advantageous because by designing the electrodes in a certain way, engineers can control directionality and intensity of electrical forces acting on nanoparticles. By using electrodes separated by just a few micrometers together with electrothermally induced fluid flow, one can accelerate the transport of viral particles from aqueous suspensions with physiological ionic strength to specific points on a surface, allowing them to reach local concentrations high enough to enable subsequent rapid detection. These observations provide a potentially useful approach for addressing a bottleneck in the development of devices that allow for rapid sampling and 'on-the-spot' detection of infectious biological agents such as viruses.

QD Fluorescent Probes for Detection of Respiratory Viral Infections

Respiratory syncytial virus (RSV) causes about one million deaths annually worldwide. RSV mediates serious lower respiratory tract illness in infants and young children and is a significant pathogen of the elderly and immune compromised. Although it is only life-threatening in one case out of every 100, it infects virtually all children by the time they are 5 years old. Approximately 120,000 children are hospitalized with RSV in the US each year. Few children in the US die from RSV but it causes 17,000–18,000 deaths annually among the elderly.

Rapid and sensitive RSV diagnosis is important for infection control and efforts to develop antiviral drugs. Current RSV detection methods are limited by sensitivity and/or time required for detection, which can take 2–6 days. This can delay effective treatment. Antibody-conjugated nanoparticles rapidly and sensitively detect RSV and estimate relative levels of surface protein expression. A major development is use of dual-color QDs or fluorescence energy transfer nanobeads that can be simultaneously excited with a single light source.

A QD system can detect the presence of particles of the RSV in a matter of hours. It is also more sensitive, allowing it to detect the virus earlier during an infection. When an RSV virus infects lung cells, it leaves part of its coat containing F and G proteins on the cell's surface. QDs have been linked to antibodies keyed to structures unique to RSV's coat. Therefore, when QDs come in contact with either viral particles or infected cells they stick to their surface. In addition, co-localization of these viral proteins was shown using confocal microscopy. The potential benefits for such an early detection system are that it can:

- 1. Increase the proper use of antiviral medicines. Although such medicines have been developed for some respiratory viruses, they are not used often as therapy because they are only effective if given early in the course of infection. By the time current tests identify the virus, it is generally too late for them to work.
- 2. Reduce the inappropriate use of antibiotics. Currently, physicians often prescribe antibiotics for respiratory illnesses. However, antibiotics combat respiratory illness caused by bacteria and are ineffective on viral infections. An early virus detection method would reduce the frequency with which doctors prescribe antibiotics for viral infections inappropriately, thereby reducing unnecessary antibiotic side-effects and cutting down on the development of antibiotic-resistance in bacteria.
- 3. Allow hospital personnel to isolate RSV patients. RSV is extremely infectious so early detection would allow hospital personnel to keep the RSV patients separate from other patients who are especially susceptible to infection, such as those undergoing bone-marrow transplants.

Currently, there are three diagnostic tests available for identifying respiratory viruses like RSV. The "gold standard" involves incubating an infected sample in a tissue culture for a few days and then using a fluorescent dye to test for the presence of the virus. The main problem with this technique is that the virus is multiplying in the patient at the same time as it is growing in the culture. This has caused many

hospitals to switch to real time PCR, which is extremely sensitive but still takes several hours because of the need for a technician well trained in molecular biologist to conduct the test in a reference laboratory. The third method, the antigen test, takes ~30 min but it is not sensitive enough to detect the presence of the virus at the early stages of an infection. By comparison, the QD method takes 1–2 h and is even more sensitive than real time PCR. It can detect the presence of RSV within an hour after the virus is added to a culture. QDs have an advantage over many traditional fluorophores because their fluorescence properties can be finely tuned and they are resistant to photobleaching (Halfpenny and Wright 2010).

Verigene Respiratory Virus Plus Assay

Verigene (Nanosphere Inc) platform is based on a direct genomic detection technology uses DNA probes coated with gold nanoparticles to identify a unique oligonucleotide sequence and combines it with biobarcode protein detection technology. Verigene Respiratory Virus Plus Assay, which runs on an automated sample-to-result molecular diagnostic instrument, is more sensitive than currently available rapid tests. It combines optimized ease of use and turnaround time not found in either traditional culture methods or the currently available molecular tests for viruses and is cleared by the FDA for detection of influenza and RSV.

Surface Enhanced Raman Scattering for Detection of Viruses

Although surface enhanced Raman scattering (SERS) is well known, previous attempts to use spectroscopy to diagnose viruses failed because the signal produced is inherently weak. A spectroscopic assay based on SERS using silver nanorods, which significantly amplify the signal, has been developed for rapid detection of trace levels of viruses with a high degree of sensitivity and specificity (Shanmukh et al. 2006). The technique measures the change in frequency of a near-infrared laser as it scatters viral DNA or RNA. That change in frequency is as distinct as a fingerprint. This novel SERS assay can detect spectral differences between viruses, viral strains, and viruses with gene deletions in biological media. The method provides rapid diagnostics (<1 min) for detection and characterization of viruses generating reproducible spectra without viral manipulation. It is also quite cheap and is very reproducible.

A dual-mode molecular beacon, based on a combined SERS and fluorescent molecular beacon assay that is assembled on nanobarcode particles, has been developed and used to measure unlabeled human viral RNA (Sha et al. 2007). The molecular beacon probe is a single-stranded oligonucleotide that has been designed with a hairpin structure that holds the dye at 3'-end close to the particle surface when the probe is attached through a 5'-thiol group. In this configuration, the SERS spectrum of the label is obtained and its fluorescence quenched because the dye is in very close to a noble metal surface with nanoscale features. The SERS signal decreases

and the fluorescence signal increases when target viral RNA is captured by this molecular beacon probe. In addition, a HCV RT-PCR product is detected using this dual-mode beacon. The development of a multiplexed, label-free assay system with the reassurance offered by detection of two distinctly separate signals offers significant benefits for rapid molecular diagnostics.

Detection of Bacteria

The rapid and sensitive detection of pathogenic bacteria is extremely important in diagnosis of infections at POC. Limitations of most of the conventional diagnostic methods are lack of ultrasensitivity or delay in getting results. Nanobiotechnology has made a significant contribution to improvements in detection of bacterial infections.

Nanoparticle-Based Methods for Bacterial Detection

Bioconjugated nanoparticle-based assays for in situ pathogen quantification can detect a single bacterium within minutes. Such nanoparticles provide high fluorescent signals for bioanalysis and can be easily incorporated in a biorecognition molecule such as an antibody. The antibody-conjugated nanoparticles can readily and specifically identify a variety of bacteria such as *Escherichia coli O157:H7* through antibody-antigen interaction and recognition. This method can be applied to multiple bacterial samples with high throughput and has a potential for application in ultrasensitive detection of disease biomarkers and infectious agents.

Verigene Gram-Positive Blood Culture (BC-GP) Test (Nanosphere Inc) is a multiplexed, nanoparticle-based automated nucleic acid test for the identification of genus, species, and genetic resistance determinants for a broad panel of the most common gram-positive blood culture isolates. Whereas conventional microbiological methods may require 2–4 days to produce bacterial identification and resistance results, the Verigene BC-GP test provides results within 2.5 h of blood culture positivity. The Verigene System's unique instrumentation with <5 min of user hands-on time per test, enables true random access test processing directly from positive blood culture bottles.

Multifunctional magnetic-plasmonic Fe_3O_4 -Au core-shell nanoparticles (Au-MNPs) have been prepared for simultaneous fast concentration of bacterial cells by applying an external point magnetic field, and sensitive detection and identification of bacteria using SERS (Zhang et al. 2012). Surrounded by dense uniformly packed Au-MNPs, bacteria can be sensitively and reproducibly detected directly using SERS. This method can be used in molecular diagnosis of bacterial infections.

AuNPs functionalized with single stranded oligonucleotides as visual detection probes (AuNP-oligo probe) have been used for rapid and specific detection of E. coli (Padmavathy et al. 2012). The AuNP- oligo probe on hybridization with target DNA samples containing complementary sequences remain red whereas test samples without complementary DNA sequences to the probe turns purple due to acid induced aggregation of AuNP-oligo probes. The color change of the solution is observed visually by naked eve demonstrating direct and rapid detection of the pathogenic E. coli from its genomic DNA without the need for PCR amplification. The limit of detection is ~54 ng for unamplified genomic DNA and the method requires <30 m to complete after genomic DNA extraction. However, by using unamplified enzymatic digested genomic DNA, the detection limit of 11.4 ng can be attained. Results of UV-Vis spectroscopic measurement and AFM imaging further support the feasibility of aggregation-based visual discrimination. This assay has been validated on clinical specimens of pathogenic E. coli obtained from local hospitals and found to be 100% sensitive as well as highly specific without any cross reaction with non-Escherichia coli strains. The salient features of this approach include POC application, low-cost, robust reagents and simple colorimetric detection of pathogen.

QDs for Detection of Bacterial Infections

Detection of single-molecule hybridization has been achieved by a hybridization detection method using multicolor oligonucleotide-functionalized QDs as nanoprobes. In the presence of various target sequences, combinatorial self-assembly of nanoprobes via independent hybridization reactions leads to the generation of discernible sequence-specific spectral codings. This method can be used for genetic analysis of anthrax pathogenicity by simultaneous detection of multiple relevant sequences.

Fluorescent QDs coated with zinc(ii)-dipicolylamine coordination complexes can selectively stain a rough *E. coli* mutant that lacks an O-antigen element and permit optical detection in a living mouse leg infection model (Leevy et al. 2008). QDs have potential use as labeling agents for bacteriophages associated with bacterial infections. A rapid and simple method has been reported that combines in vivo biotinylation of engineered host-specific bacteriophage and conjugation of the phage to streptavidin-coated QDs (Edgar et al. 2006). The method provides specific detection of as few as 10 bacterial cells per ml in experimental samples, with an approximately 100-fold amplification of the signal over background in 1 h. The method can be applied to any bacteria susceptible to specific phages and would be particularly useful for detection of bacterial strains that are slow growing such as Mycobacterium, or are highly infectious such as *B. anthracis*. To monitor the infection of *E. coli* cells by light microscopy, procedures have been developed for the tagging of mature bacteriophages with QDs (Edgar et al. 2008). Fluorescent QDs have been used for detection and sorting of pathogenic bacteria by flow-cytometry (Zahavy et al. 2012).

Role of Nanobiotechnology in Diagnosis of Fungal Infections

Conventional methods for diagnosis of invasive fungal infections in the clinical microbiology laboratory are time-consuming process or result in misidentification of the fungus due to low sensitivity or low specificity. There is need for improvement of methods of detection of fungi and nanobiotechnology-based techniques have been used.

Magnetic Nanoparticle-Based Technique for Detection of Fungi

Magnetic Resonance Detection (T2 Biosystems) uses magnetic nanoparticles coupled with reagents to quickly detect, within minutes, the presence of specific substances in solution using a miniaturized, portable MRI instrument. Detection of a high intensity MRI signal from the solution enables the detection of low concentrations of target agents or substances. Unlike most existing diagnostic detection techniques which are based on optical detection methods that require pure samples and multiple processing steps, T2's technology is not optical and therefore does not require purification of biological samples. The significant advantage allows the T2 system to perform single-step processing and rapid turnaround times without the need for trained technicians. Furthermore, the technology can accurately identify almost any specimen, including proteins, nucleic acids, or enzymes; microbes; or small molecule drug compounds within almost any sample, including whole blood, plasma, serum and urine. This method has been used to analyze whole blood specimens from patients with five different types of Candida spp. infections and is currently in clinical trials with an aim for regulatory approval for diagnosis of Candida infection.

Nano-amplification Technique for the Detection of Fungal Pathogens

In one method, fungal ribosomal DNA was amplified using PCR and the products were hybridized with the species-specific probes immobilized on the surface of a microarray where hybridizing signals were enhanced with gold nanoparticles and silver deposition (Lu et al. 2010). The probes were designed to detect several different clinical pathogenic fungi using a flatbed scanner or visually. The technique showed higher efficiency, specificity and sensitivity compared with other methods.

Role of Nanobacteria in Human Diseases

Nanobacteria are mineral-forming, sterile-filterable, slow-growing Gram-negative infectious agents. They are detected in bovine/human blood and urine. Nanobacterialike particles have been detected in synovial fluids of arthritis patients and were shown to gradually increase in number and in size in culture (Tsurumoto et al. 2006). Nanobacteria have been implicated in a variety of human diseases associated with pathological calcification. Their most remarkable characteristic is the formation of carbonate apatite crystals of neutral pH and at physiologic phosphate and calcium concentrations. The extracellular mineralization forms a hardprotective shelter for these hardy microorganisms, and enables them to survive conditions of physical stress that would be lethal to most other bacterial species. The Olavi Kajander group (Finland) suggests that the apatite produced by nanobacteria may play a key role in the formation of all kidney stones, by providing a central calcium phosphate deposit around which other crystalline components can collect. Nanobacteria seem to be causative agents of diseases related to biomineralization processes. Nanobacteria are also associated with calcified geological specimens, human kidney stones and psammona bodies in ovarian cancer. Much research has focused attention on the potential role these particles may play in the development of urologic pathology, including polycystic kidney disease, renal calculi, and chronic prostatitis. Nanobacteria may be an important etiological factor for type III prostatitis, which was reproduced in rat prostate infection models by infusing nanobacteria suspension transurethrally (Shen et al. 2010). Recent clinical research on agents targeting nanobacteria has proven effective in treating some patients with refractory category III prostatitis.

Nature of Nanobacteria

According to their 16S rDNA structure, nanobacteria belong to the alpha-2 Proteobacteria, subgroup, which includes the Brucella and Bartonella species. Nanobacterium sanguineum (nanobacteria) is the smallest self-replicating organism ever detected – at 50–500 billionths of a meter, 1/1000th the size of the smallest previously known bacteria. Primordial proteins in nanobacteria, only recently identified in the atmosphere, could play a significant role in clouds, accelerating the formation of cloud droplets and interconnecting nanobacteria (and possibly nanobacteria and other microorganisms), thus enhancing their chances to eventually reach the Earth.

Several research studies indicate that nanobacteria are alive, but it is still unclear whether they represent novel life forms, overlooked nanometer-size bacteria, or some other primitive self-replicating microorganisms. A study has shown that CaCO₃ precipitates prepared *in vitro* are remarkably like the purported nanobacteria in terms of their uniformly sized, membrane-delineated vesicular shapes, with cellular division-like formations and aggregations in the form of colonies (Martel and Young 2008). The gradual appearance of nanobacteria-like particles in incubated human serum as well as the changes seen with their size and shape can be influenced and explained by introducing varying levels of CO₂ and NaHCO₃ as well as other conditions known to influence the precipitation of CaCO₃. Western blotting reveals that the monoclonal antibodies, claimed to be specific for nanobacteria, react in fact with serum albumin. Furthermore, nanobacteria-like particles obtained from human blood can withstand high doses of -irradiation up to 30 kGy, and no bacterial DNA is found by performing broad-range PCR amplifications. These findings provide a more plausible abiotic explanation for the unusual properties of purported nanobacteria.

Nanobacteria and Kidney Stone Formation

Approximately 12% of men and 5% of women develop kidney stones by the time they reach the age of 70 years but exactly how kidney stones form is not known. Kidney stones can be debilitating and recur in 50% of patients within 5 years. Kidney stone formation is a multifactorial disease in which the defense mechanisms and risk factors are imbalanced in favor of stone formation. One theory is that if nanoparticles accumulate in the kidney, they can form the focus of subsequent growth into larger stones over months to years. Other factors, such as physical chemistry and protein inhibitors of crystal growth, also play a role.

Mineral forming nanobacteria are active nidi that attach to, invade and damage the urinary epithelium of collecting ducts and papilla forming the calcium phosphate center(s) found in most kidney stones. Scientists at NASA have used multiple techniques to determine that nanobacteria infection multiplies faster in space flight simulated conditions than on earth. Nanobacteria are considered to initiate kidney stone formation as they grow faster in a microgravity environment and may explain why astronauts get kidney stones on space missions. This discovery may prove to be critical for future exploratory missions to the moon and Mars. For further proof to this hypothesis, screening of the nanobacterial antigen and antibody level in flight crew before and after flight would be necessary. This concept also opens the door for new diagnostic and therapeutic techniques addressing nanobacterial infection in kidney stones.

Nanoparticles have been isolated and cultured from most of renal stones obtained at the time of surgical resection (Kumar et al. 2006). Isolates were susceptible to selected metabolic inhibitors and antibiotics and contained conserved bacterial proteins and DNA. These results suggest that renal stone formation is unlikely to be driven solely by physical chemistry; rather, it is critically influenced by specific proteins and cellular responses, and understanding these events will provide clues toward novel therapeutic targets. Using high-spatial and energy resolution nearedge x-ray absorption fine structure at the 25 nm spatial scale, it is possible to define a biochemical signature for cultured calcified bacteria, including proteins, polysaccharides, nucleic acids, and hydroxyapatite (Benzerara et al. 2006). These preliminary studies suggest that nanoparticles isolated from human samples share spectroscopic characteristics with calcified proteins.

Nanobacteria in Cardiovascular Disease

Nanometer-scale objects, spherical in shape and ranging in size from 30–100 nm with a spectral pattern of calcium and phosphorus (high-energy dispersive spectroscopy), have been identified with positive immunostaining in surgical specimens from patients with cardiovascular pathology. Nano-sized particles cultured from calcified but not from non-calcified aneurysms were recognized by a DNA-specific dye, incorporated radiolabeled uridine, and after decalcification, appeared via electron microscopy to contain cell walls. Nanometer-scale particles like those described as nanobacteria isolated from geological specimens and human kidney stones can be visualized in and cultured from human calcified cardiovascular tissue. In further studies, nanoparticles were found near plaque-filled arteries in animal models. These observations suggest that nanoparticles potentially represent a previously unrecognized factor in the development of arteriosclerosis and calcific arterial disease.

Nanotechnology-Based Microbicidal Agents

Carbon Nanotubes as Antimicrobial Agents

CNTs have the potential to address the challenges of combating infectious agents by both minimizing toxicity by dose reduction of standard therapeutics and allowing a multiple payload capacity to achieve both targeted activity and combating infectious strains, particularly those resistant to antibiotics (Rosen and Elman 2009). One of their unique characteristics is the network of carbon atoms in the nanometer scale, allowing the creation of nanochannels via cellular membranes.

Attempts have been made to destroy anthrax spores by antimicrobial agents targeted to bind to carbohydrates on the spore surface but with limited success. SWCNTs have been successfully used as a truly unique scaffold for displaying multivalent monosaccharide ligands that bind effectively to anthrax spores with divalent cation mediation to cause significant spore aggregation (Wang et al. 2006). The work should have far-reaching implications in development of technologies to counteract bioterrorism such as by use of anthrax. For SWCNTs to be effective against anthrax, they must be made into a fine powder that can easily enter the lungs when inhaled. That nanotechnology-based agent clings to the anthrax spores to make their inhalation into the lungs difficult. Similar approach using sugar-coated carbon nanotubes to stop the spread of *E. coli* bacteria was tested successfully.

Gold and Silver Nanoparticles as Antibacterial Agents

Colloidal silver has been used as an antibacterial agent since ancient Greece. Unlike antibiotic drugs, bacteria cannot easily develop resistance because silver targets multiple components in the bacterial cell. Effects of gold and silver NPs have been investigated on BCG and *E. coli* (Zhou et al. 2012). Experimentally, particle size and shape were characterized using TEM. Different concentrations of NPs were applied in bacterial culture. The growth of *E. coli* was monitored through colony forming units (CFU). The mechanism of interaction between NPs and bacterial was analyzed through bacterial thin sections followed by TEM and SEM. Antibacterial

effects on BCG were observed by recording fluorescent protein expression levels. The results suggest NPs have potential applications as anti-TB compounds. The antibacterial effects and mechanism of action for NPs were dependent upon composition and surface modifications. Synthetic-peptides containing arginine, tryptophan and cysteine can target negatively-charged bacteria and penetrate bacterial cell membrane. Peptide immobilized gold nanoparticles (AuNPs) were shown to have targeting capacity and antibacterial activity against Staphylococci, Enterococci and antibiotic-resistant bacterial strain (Kuo et al. 2016).

Gold Nanoparticles for Targeting Drug-Resistant Bacteria

To address the problem of antibiotic drug resistance, a study has used S. aureus as a proof-of-principle pathogen to demonstrate that an appropriate antibiotic (daptomycin) can be incorporated into polydopamine-coated gold nanocages (AuNC@PDA), which can be conjugated to antibodies targeting a species-specific surface protein (staphylococcal protein A: Spa) as a means of achieving selective delivery of the nanoconstructs directly to the bacterial cell surface (Meeker et al. 2016b). Targeting specificity was confirmed by demonstrating a lack of binding to mammalian cells, reduced photothermal and antibiotic killing of the Spa-negative species Staphylococcus epidermidis, and reduced killing of S. aureus in the presence of unconjugated anti-Spa antibodies. The authors demonstrated that laser irradiation at levels within the current safety standard for use in humans can be used to achieve both a lethal photothermal effect and controlled release of the antibiotic, thus resulting in a degree of therapeutic synergy capable of eradicating viable S. aureus cells. The system was validated using planktonic bacterial cultures of both methicillinsensitive and methicillin-resistant S. aureus strains. This approach has the potential to be expanded to deal with other bacterial pathogens that could be targeted by substituting an effective antibiotic and an appropriate targeting agent (antibody, peptide, etc.). Thus, the concept of using photoactivatable nanodrugs has tremendous potential to overcome the growing problem of acquired antibiotic resistance in bacteria as well as the intrinsic resistance of biofilm-associated infections (Meeker et al. 2016a).

Nanocarriers for Antibacterial Peptides

Antimicrobial peptides are natural weapons against bacteria in the body and occur in many organisms. They offer a possible alternative to conventional antibiotics because of increasing resistance to conventional antibiotics, but have not yet been successfully used clinically, because they are broken down in the human body too quickly to exert their effect. Efforts are being made to develop liquid-crystalline nanocarriers to protect the peptides and thus ensure they are safely delivered to the target site. Small-angle X-ray scattering, dynamic light scattering, and cryogenic transmission electron microscopy studies have shown that amphiphilic peptide LL-37 integrates into the bicontinuous cubic structure, and induces colloidal transformations of micelles in a concentration-dependent manner (Gontsarik et al. 2016). These investigations, along with in vitro evaluation studies using a clinically relevant bacterial strain, have determined the composition-nanostructure-activity relationship that can guide the design of new nanocarriers for antimicrobial peptides and may provide essential knowledge about the mechanisms underlying bacterial membrane disruption with peptide-loaded nanostructures. The protective coverings formed by the lipids not only ensure the safe delivery of the peptides to the area where they are needed, but also intensify their action at the target site. The structure of nanocarriers may be modified in a way that enables their controlled release at a specific time. This is a topic for further research.

Nanoemulsions as Microbicidal Agents

The antimicrobial nanoemulsions (NanoBio) are emulsions that contain water and soya bean oil with uniformly sized droplets in the 200–400 nm range. These droplets are stabilized by surfactant and are responsible for the microbicidal activity. In concentrated form, the nanoemulsions appear as a white milky substance with a taste and consistency of cream. They can be formulated in a variety of carriers allowing for gels, creams, liquid products, etc. In most applications, the nanoemulsions become largely water-based, and in some cases such as a beverage preservative comprise 0.01% or less of the resultant mixture. Laboratory results indicate a shelf life of at least 2 years and virtually no toxicity. NanoBio Corporation's nanoemulsions destroy microbes effectively without toxicity or harmful residual effects. The nanoparticles fuse with the membrane of the microbe and the surfactant disrupts the membrane, killing the microbe. The classes of microbes eradicated are virus (e.g. HIV, herpes), bacteria (e.g. E. coli, Salmonella), spores (e.g. anthrax), and fungi (e.g. Candida albicans, Byssochlamys fulva). NB-402 (NanoBio), a nanoemulsion antimicrobial agent for the treatment of infection due to CF-related opportunistic pathogens is in development (see Chapter on Nanopulmonology). Clinical trials have shown efficacy in healing cold sores due to herpes simplex virus 1 and toenail fungus. The nanoemulsions also can be formulated to kill only one or two classes of microbes. Due in large part to the low toxicity profile, the nanoemulsions are a platform technology for any number of topical, oral, vaginal, cutaneous, preservative, decontamination, veterinary, and agricultural antimicrobial applications.

Since it is non-toxic and non-corrosive, nanoemulsion can be used to decontaminate personnel, equipment, terrain, structures, and water. Further, tests by DTRA (Defense Threat Reduction Agency), an agency of the US Department of Defense, have demonstrated that the nanoemulsion is a chemical decontaminating agent. The US Army tested the nanoemulsion and nine other biodecontamination technologies at against an anthrax surrogate. The nanoemulsion was one of four technologies that proved effective.

Nanoparticles for Overcoming Antibiotic Resistance

Antibiotic resistance in bacteria can be caused by localized acidity, a phenomenon that can occur due to the combined actions of bacterial metabolism and the host immune response. NPs have shown promise in treating bacterial infections, but a significant challenge has been to develop a formulation that may be suitable for systemic administration. Drug-encapsulated, pH-responsive, surface charge-switching poly(d,l-lactic-co-glycolic acid)-b-poly(l-histidine)-b-poly(ethylene glycol) (PLGA-PLH-PEG) nanoparticles have now been developed for treating bacterial infections (Radovic-Moreno et al. 2012). Antibiotic-carrying NPs were designed to switch their charge depending on their environment. While they circulate in the bloodstream, the particles have a slight negative charge. However, when they encounter an infection site, the particles gain a positive charge, allowing them to tightly bind to bacteria and release their drug payload. This switch is provoked by the slightly acidic environment surrounding bacteria, which is due to lack of oxygen triggering a change in bacterial metabolism, leading them to produce organic acids. The body's immune cells, neutrophils, also produce acids as they try to consume the bacteria. These NP drug carriers are designed to shield nontarget interactions at pH 7.4 but bind avidly to bacteria in acidity, delivering drugs and mitigating in part the loss of drug activity with declining pH. NP binding studies demonstrate pH-sensitive NP binding to bacteria with a ~3.5-fold increase in binding to bacteria at pH 6.0 compared to 7.4. Further, PLGA-PLH-PEG-encapsulated vancomycin demonstrates reduced loss of efficacy at low pH, with an increase in minimum inhibitory concentration of 1.3-fold as compared to 2-fold and 2.3-fold for free and PLGA-PEG-encapsulated vancomycin, respectively. The PLGA-PLH-PEG NPs are a first step toward developing systemically administered drug carriers that can target and potentially treat Gram-positive, Gram-negative, or polymicrobial infections associated with acidity. This approach would enable targeted delivery of high doses of antibiotics over an extended period to overcome antibiotic resistance, but protect the beneficial bacteria that normally live inside human bodies. A potential challenge to this approach is that negatively charged tissue cells and proteins at infection sites can compete with bacteria in binding to nanoparticles and potentially block them from binding to bacteria. The investigators are studying how much this might limit the effectiveness of the NP delivery. They are also conducting studies in animals to determine whether the particles will remain pH-sensitive in the body and survive in the circulation long enough to reach their targets.

Nanoformulations of Antifungal Agents

An example of this is Nanosomal Amphotericin B (Jina Pharmaceuticals Inc) formulated in lipids without using any detergent or toxic organic solvents during the preparation (Sheikh et al. 2010). Electron microscopy and particle size determination of this preparation showed a homogeneous population of nanosized particles <100 nm. Hemolysis assay indicated that Nanosomal Amphotericin B causes significantly less lysis of red blood cells than Amphotericin B deoxycholate and was comparable to Ambisome, the approved liposome preparation. A maximum daily dose of Nanosomal Amphotericin B at 5 mg/kg in rabbits and 10 mg/kg in mice for 28 days showed no symptoms of toxicity, mortality or significant body weight reduction. Nanosomal Amphotericin B and Ambisome were injected intravenously at 2 mg/kg consecutively for 5 days into mice infected with *Aspergillus fumigatus*. The treatment resulted in 90% survival with Nanosomal Amphotericin B and only 30% survival with Ambisome after 10 days of fungal infection. However, all the 10 control mice not treated with Amphotericin B, died within 5 days of fungal infection. Nanosomal Amphotericin B is safe, cost-effective and provides an alternative option for treatment of fungal disease.

Nanoscale Bactericidal Powders

Certain formulations of nanoscale powders possess antimicrobial properties. These formulations are made of simple, nontoxic metal oxides such as magnesium oxide (MgO) and calcium oxide (CaO, lime) in nanocrystalline form, carrying active forms of halogens, e.g., MgO.Cl₂ and MgO.Br₂. When these ultrafine powders contact vegetative cells of *Escherichia coli, Bacillus cereus*, or *Bacillus globigii*, over 90% are killed within a few minutes. Likewise, spore forms of the Bacillus species are decontaminated within several hours. Dry contact with aflatoxins and contact with MS2 bacteriophage (surrogate of human enterovirus) in water also causes decontamination in minutes.

A nanopowder of MgO can scour contaminated rooms of anthrax spores. Unlike antibacterial gases and foams, which are messy, corrosive and ruin electrical equipment, the powder can be sprayed into rooms and swept or vacuumed up. The chemical specks attract oppositely charged spores. The particles then chemically break down the spores' tough outer shell. Based on this technology, NanoScale Corporation markets a dry powder dubbed FAST-ACT® (First Applied Sorbent Treatment Against Chemical Threats) that decomposes toxic chemicals. The powder contains reactive nanoparticles that attract and then break down at least 24 commonly transported toxic chemicals, including some acids. Unlike foams, the powder need not be wet to be effective and works on liquids and vapors.

Nanotubes for Detection and Destruction of Bacteria

A simple molecule, synthesized from a hydrocarbon and an ammonium compound, produces a unique nanotube structure with antimicrobial capability. The quaternary ammonium compound is known for its ability to disrupt cell membranes and causes cell death whereas the hydrocarbon diacetylene can change colors when appropriately formulated; the resulting molecule would have the desired properties of both a biosensor and a biocide. Self-assembled nanotubes are perfectly uniform and organize themselves into an expanse of upright clusters that when magnified a million times resemble the fibers of a shag rug leading to the name "nanocarpet". The self-assembling nanotubes have all the same diameter (89 nm) and wall thickness (27 nm). The nanocarpet measures about 1 µm in height, approximately the same height as the free-form nanotubes. This alignment of nanotubes in the absence of a template is unprecedented and represents an important step toward rational design of bioactive nanostructures. In addition, because they form within hours under room-temperature conditions, the significant costs of synthesizing carbon nanotubes can be reduced. Normally a neutral color, when exposed to ultraviolet light the nanotubes changed to a permanent deep blue. The process also chemically altered the nanotubes so that they became polymerized, giving them a firmer structure. Polymerized, these nanotubes could change from blue to other colors, depending on its exposure to different materials. For instance, in tests with acids and detergents, they turned red or yellow.

Because they display sensitivity to different agents by changing color, these nanotubes can be trained to kill bacteria. In the presence of *E. coli*, some strains of which are food-borne pathogens, the nanotubes turned shades of red and pink. Moreover, with the aid of an electron microscope, the researchers observed the tubes piercing the membranes of the bacteria like a needle being inserted into the cell. Both the polymerized (those that can change color) and the unpolymerized nanotube structures were effective antimicrobials, completely killing all the *E. coli* within an hour's time. The findings have implications for developing products that can simultaneously detect and kill biological weapons. The research, funded by the Department of Defense's Army Research Office, has as its goal the development of a paint that in the event of biological or chemical agents being deployed would change color and simultaneously destroy the deadly substances.

Nanoscale Surface Structure for Antibacterial Defense

The first natural surface found to kill bacteria simply by its physical structure is an array of hexagonal "nanopillars" on the wings of a clanger cicada (Psaltoda claripennis) that can put enough strain on bacterial cells to rupture them (Pogodin et al. 2013). Nanopillars do not puncture the bacteria, which stick to the tips of the nanopillars, then stretch into the hexagonal spaces between them, putting extreme strain on the cell. The nanoscale defense only appears to work on bacteria with relatively soft membranes, but those with greater membrane rigidity could survive the stretch of the pillars. However, decreasing the rigidity of surface-resistant strains through microwave irradiation of the cells renders them susceptible to the wing effects. This finding provides a new strategy for antibacterial prophylaxis. Common sources of transmission of bacterial infections such as public railings can be designed to mimic nanopillars to provide an antibacterial surface.

Silver Nanoparticle Coating as Prophylaxis Against Infection

Silver is used in medical equipment coatings and dental resin components. The mechanism underlying its antibacterial activity is that it weakens DNA replication and inactivates proteins. The Institute for New Materials (Saarbrucken, Germany), a research institute specializing in applied nanotechnology applications, has developed a silver nanoparticles surface coating that is deadly to fungi and bacteria. The researchers added the germicidal ability by sprinkling copious amounts of silver nanoparticles through the coating material (every square centimeter contains more than one billion of the invisible particles) and aligning them so that they release a tiny number of silver ions. These ions are the death knell for fungus and bacteria that might have succeeded in gathering on the surface despite its already dirtrepellent qualities. Applications include any surface where germs can gather and possibly endanger people's health. That includes surfaces in hospitals, public buildings, factories or in the home. The coating could be applied to almost any surface that people touch often such as metal, glass or plastic and would remove the need for constant cleaning with liquid disinfectants, especially in areas where hygienic conditions are crucial. People who normally cannot use hearing aids that lie inside the ear because of the risk of infection of the auditory canal can safely wear nanocoated appliances.

Bio-Gate (Nürnberg, Germany) produces NanoSilver BG, a nanoporous silver powder with particle size ranging from 50 nm to 100 nm. It has a homogeneous distribution of nanoparticles in the material and antiinfective properties.

Silver nanoparticles have been incorporated in preparations for wound care to prevent infection. Acticoat bandages (Smith & Nephew) contain nanocrystal silver, which is highly toxic to pathogens in wounds.

AcryMed's silver nanoparticle technology, SilvaGard, involves coating with silver nanoparticles with size range of 2–20 nm in a stable solution and antimicrobial treatment levels last for more than a year. With other technologies, nano-based silver coatings must be applied through vapor deposition, which coats only on one side, whereas AcryMed technology is a solution that provides a complete surface treatment rather than a coating.

Nanobiotechnology and Virology

Study of Interaction of Nanoparticles with Viruses

Scanning surface confocal microscopy, simultaneous recording of high-resolution topography and cell surface fluorescence in a single scan enables imaging of individual fluorescent particles in the nanometer range on fixed or live cells. This technique has been used to record the interaction of single virus-like particles with the cell surface and demonstrated that single particles sink into the membrane in invaginations reminiscent of pinocytic vesicles. This method enables elucidation

of the interaction of individual viruses and other nanoparticles, such as gene therapy vectors, with target cells.

Silver nanoparticles undergo a size-dependent interaction with HIV-1 and particles in the range of 1–10 nm attached to the virus. The regular spatial arrangement of the attached nanoparticles, the center-to-center distance between nanoparticles, and the fact that the exposed sulfur-bearing residues of the glycoprotein knobs would be attractive sites for nanoparticle interaction suggest that silver nanoparticles interact with the HIV-1 virus via preferential binding to the gp120 glycoprotein knobs. Due to this interaction, silver nanoparticles inhibit the virus from binding to host cells, as demonstrated in vitro.

Study of Pathomechanism of Viral Diseases

Research in nanobiotechnology helps in understanding the pathomechanism of viral diseases and devising strategies for treatment. An example is the neurotropic herpes simplex virus (HSV), which infects mucosal epithelia and enters nerve terminals, from where it travels in axons to dorsal root ganglia neurons and delivers its genome into the nucleus of the cell body. In the nucleus, the genome may give rise to infectious progeny or become latent with little gene expression. The silenced genome can be reactivated upon stress and establish a productive infection in the peripheral nervous system and, later, also in the mucosal periphery. To achieve this, a virus must elude host restrictions at multiple levels, including entry, cytoplasmic transport, replication, innate and adaptive immune recognition, and egress from the infected cell.

Research on virus nanoparticles has provided cues to the regulation of cytoplasmic transport. Viruses that replicate their genomes in the nucleus make use of the microtubule and the actin cytoskeleton as molecular motors for trafficking toward the nuclear membrane during entry and the periphery during egress after replication. Analyzing the underlying principles of viral cytosolic transport will be helpful in the design of viral vectors to be used in research as well as human gene therapy, and in the identification of new antiviral target molecules.

Transdermal Nanoparticles for Immune Enhancement in HIV

DermaVir Patch (Genetic Immunity) in a transdermally delivered nanomedicine to enhance de novo HIV-specific memory T-cell responses of HIV-infected individuals and improve the ability of their own immune system to control the disease by killing only HIV-infected cells. Mice receiving DermaVir formulated with HIV-1 Gag plasmid in the presence of IL-7- or IL-15-encoding plasmid have significantly enhanced Gag-specific central memory T-cells, as measured by a peptide-based cultured IFN- γ ELISPOT (Calarota et al. 2008). In a DermaVir prime/vaccinia vector boost regimen, the inclusion of IL-15 together with DermaVir significantly improved Gag-specific effector memory T-cell responses. This study demonstrates IL-15 is a promising DermaVir adjuvant to enhance antigen-specific central memory type T-cells in a prime-boost setting. It is in phase II clinical trials.

Nanofiltration to Remove Viruses from Plasma Transfusion Products

One of the complications of blood transfusion is transmission of viral infections. Nanofiltration, use of nanotechnology in viral removal filtration systems, is an important safety step in the manufacture of plasma-derived coagulation factor concentrates and other biopharmaceutical products from human blood. Nanofiltration of plasma products has already been carried out since the early 1990s to improve margin of viral safety, as a complement to the viral reduction treatments, such as solventdetergent and heat treatments, which are applied for the inactivation of HIV as well as hepatitis B and C viruses. The main reason for the introduction of nanofiltration was the need to improve product safety against non-enveloped viruses and to provide a possible safeguard against new infectious agents potentially entering the human plasma pool. Nanofiltration has gained quick acceptance as it is a relatively simple manufacturing step that consists in filtering protein solution through membranes with nanopores (pore size typically 15-40 nm) under conditions that retain viruses by a mechanism largely based on size exclusion. Recent large-scale experience throughout the world has now established that nanofiltration is a robust and reliable viral reduction technique that can be applied to essentially all plasma products. Many of the licensed plasma products are currently nanofiltered. The technology has major advantages as it is flexible and it may combine efficient and largely predictable removal of a wide range of viruses. Compared with other viral reduction means, nanofiltration may be the only method to date permitting efficient removal of enveloped and non-enveloped viruses under conditions where 90–95% of protein activity is recovered. New data indicate that nanofiltration may also remove prions, opening new perspectives in the development of this technique.

Shortcomings of some membranes are that they often form pin-holes and cracks during the fabrication process, resulting in wasted membranes Specially designed ceramic membranes have been used as nano-mesh for nanofiltration as they are less likely to be damaged during manufacture and have the potential to remove viruses from water, air and blood. Mesh structure, which is the most efficient form of filtration, has been successfully constructed on a nanoscale with ceramic fibers. This modification has increased the rates of flow that pass through the membranes 10-fold compared with current ceramic membranes, while maintaining the efficiency of capturing over 96% of the unwanted particles. This technology could be used to filter airborne viruses such as the severe acute respiratory syndrome (SARS) and the avian flu virus. It may be possible to filter HIV from human blood to treat patients with AIDS.

Nanotechnology-Based Antiviral Agents

Dendrimer-Based Intracellular Delivery of Antibodies

Antibodies typically neutralize viruses by binding to virion particles in solution prior to attachment to susceptible cells. Once viruses enter cells, conventional antibodies cannot inhibit virus infection or replication. A method has been described for the delivery of small recombinant antibody fragments into virus-infected cells using a dendrimer-based molecular transporter (Sapparapu et al. 2014). The construct penetrated virus-infected cells efficiently and inhibited virus replication. This method provides a novel approach for the immediate delivery of inhibitory antibodies directed to virus proteins that are exposed only in the intracellular environment. This approach circumvents the current and rather complicated expression of inhibitory antibodies in cells following gene transfer. Internalization via the molecular transporter-antibody conjugate to reach conserved internal viral proteins in infected cells could expand the use of antibodies beyond prophylactic indications to therapeutic applications. These novel antibodies could also be coupled with RNAi strategies for combination antiviral therapy that is more powerful than monotherapy due to synergistic effects.

Dendrimers as Nonviral Vectors in Dendritic Cell-Based Immunotherapies

DC-based immunotherapies have various limitations, but one of the most critical point is the antigen loading into DCs. Nanotechnology offers new tools to overcome these constraints. Dendrimers have been proposed as carriers for targeted delivery of HIV antigens in DCs. These nanosystems can release the antigens in a controlled manner leading to a more potent specific immune response. Improvements in rational synthesis and engineering of dendrimer as well as new strategies in HIV epitopes selection and antigen design (overlapping peptides, bioinformatic-designed mosaic antigens or immunogenic broadly neutralizing antibody-derived peptides) will permit the design of novel safe and immunogenic nanovaccines that effectively target antigen delivery in vivo, replacing the expensive and unbeatable ex vivo culturing techniques and facilitating large-scale application of DC-based vaccination (Vacas-Córdoba et al. 2014).

Fullerenes as Antiviral Agents

A series of bis-fulleropyrrolidines bearing two ammonium groups have been synthesized and their activities against HIV-1 and HIV-2 have been evaluated (Marchesan et al. 2005). Two trans isomers were found to have interesting antiviral

properties, confirming the importance of the relative positions of the substituent on the C60 cage. None of the compounds showed any inhibitory activity against a variety of DNA and RNA viruses other than HIV.

Cationic, anionic and amino acid-type fullerene derivatives have inhibitory effect against HIV-reverse transcriptase and HCV. Out of all derivatives of fullerenes, anionic fullerenes, were found to be the most active. All the tried fullerene derivatives were more active than the non-nucleoside analog of HIV-RT inhibitor. The effect of long alkyl chains on fullerenes was not significant; rather it depressed the inhibition strength. The two important targets for anti-HIV characteristics are the HIV-protease and HIV-reverse transcriptase. The molecular modeling experimental designs exhibit that C60-core could penetrate hydrophobic binding site of HIV protease. However, the mechanism of this anti-HIV activity is through HIV-protease inhibition, which has not been experimentally demonstrated.

Gold Nanorod-Based Delivery of RNA Antiviral Therapeutics

The emergence of the pandemic 2009 H1N1 influenza virus has become a worldwide health concern. As drug resistance appears, a new generation of therapeutic strategies will be required. Use of RNA immune activator molecule is limited by their instability when delivered into cells but this can be overcome by using a nanobiotechnology-based delivery system. Gold nanorods protect the RNA from degrading once inside cells, while allowing for more selected targeting of cells Usefulness of delivery of a biocompatible gold nanorod, GNR-5'PPP-ssRNA nanoplex, has been demonstrated for innate immune activation against type A influenza virus (Chakravarthy et al. 2010). In human respiratory bronchial epithelial cells, this nanoplex containing the single strand RNA molecule activated the retinoic acidinducible gene I pathogen recognition pathway, resulting in increased expression of IFN (interferon)-β and other IFN-stimulated genes (e.g. PKR, MDA5, IRF1, IRF7, and MX1), which resulted in a decrease in the replication of H1N1 influenza viruses. The novelty of this approach is that most of RNA viruses share a common hostresponse immune pathway, and enhancement of the host immune response reduces the ongoing viral resistance generated through mutations. Diseases that could be effectively targeted with this new approach include any viruses that are susceptible to the innate immune response triggered by IFN. Animal studies have started based on these in vitro results, and further evaluation of biocompatible nanoplexes as unique antivirals for treatment of seasonal and pandemic influenza viruses is warranted.

Nanocoating for Antiviral Effect

Laboratory testing of the permanent nanocoating SERQETTM (LaamScience Inc) showed the coating kills 99.9% of influenza viruses and 99.99% of vaccinia viruses that cause rash, fever, head and body aches. This technology may enable one to

protect oneself from virtually all viruses and bacteria by simply exposing a surface to light.

In 2006, Mass Transit Railway (MTR), the corporation that runs Hong Kong subway, announced that Nano Silver-Titanium Dioxide Coating (NSTDC, a non-toxic disinfectant) will be applied to surfaces that passengers commonly touch to enhance hygiene levels in MTR stations and trains. The coating is manufactured using nanotechnology, which maximizes coverage and effectiveness of NSTDC. Developed in Japan, NSTDC is certified to be effective in killing a wide range of bacteria, viruses and mold including the H1N1 Influenza Virus A. It is used in hospitals, offices and homes in Japan. NSTDC's main component, titanium dioxide (TiO2), has been approved for use in foods by the FDA and under the Public Health and Municipal Services Ordinance in Hong Kong.

Nanoviricides

Nanoviricides (NanoViricides Inc) are polymeric micelles, which act as nanomedicines to destroy viruses. As defined by NanoViricides Inc, "a nanoviricide is a polymeric single chemical chain with covalently attached ligands that specify the virus target. The antiviral spectrum of the drug is determined by the specificity of the set of ligands attached to the chain, in addition to other functionally important aspects inherent in the chemistries". Nanoviricide is designed to seek a specific virus type, attach to the virus particle, engulf or coat the virus particle, thereby neutralizing the virus's infectivity, destabilize and possibly dismantle the virus particle, and optionally it may also be made capable of attacking the viral genome thereby destroying the virus completely. Active pharmaceutical ingredients are optional and can be hidden in the core of the nanoviricide missile.

In contrast to other approaches, a NanoViricide[™] micelle can recognize and bind to more than one type of binding site on the virus. The NanoViricide[™] system enables design of a drug that binds to more than one type of site – currently as many as three different sites, on the virus - for a highly effective attack. NanoViricides Inc terms this as "multi-specific targeting". A NanoViricide[™] drug goes much further than just blocking all of the binding sites of the virus. The base material of a NanoViricideTM is a specially designed polymeric micelle material. It can disassemble an HIV particle by itself. Thus, after coating the virus particle, the NanoViricideTM loosens the virus particle, and weakens it. Some virus particles will even fall apart (uncoat). This provides a further therapeutic benefit. NanoViricides plans to enhance the viral disassembly capabilities of the nanoviricides[™] by attaching specially designed "molecular chisels" to the NanoViricideTM. Once the NanoViricideTM micelles coat the virus particle, the attached "molecular chisels" will go to work. They literally insert themselves into the virus coat at specific vulnerable points and pry apart the coat proteins so that the virus particle falls apart readily. The mechanism of action of NanoViricide is depicted schematically in Fig. 14.2.

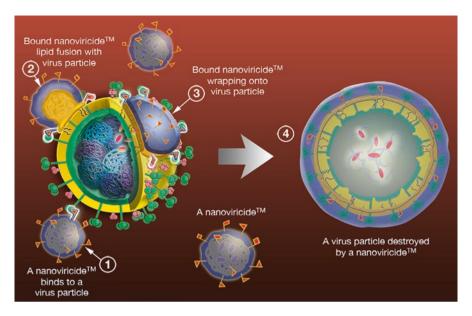


Fig. 14.2 Schematic representation of NanoViricide attacking a virus particle (Reproduced by permission of NanoViricide Inc.)

NanoViricides have been compared to current approaches to viral diseases, which are seldom curative and some of the advantages include the following:

- Specific targeting of the virus with no metabolic adverse effects on the host.
- The biological efficacy of NanoViricides drugs may be several orders of magnitude better than that of usual chemical drugs. This may limit the potential for mutant generation.
- There are also other key aspects of the design of NanoViricides that are expected to lead to minimizing mutant generation.
- Nanoviricides are safe because of their unique design and the fact that they are designed to be biodegradable within the body.
- The new technology enables rapid drug development against an emerging virus, which would be important for global biosecurity against natural as well as manmade (bioterrorism) situations. It is possible to develop a research drug against a novel life-threatening viral disease within 3–6 weeks after the infection is found, i.e. as soon as an antibody from any animal source is available.
- It is possible to make a single NanoViricide drug that responds to several viral threats by using targeting ligands against the desired set of viruses in the construction of the drug. It is possible to "tune" the specificity and range (spectrum) of a NanoViricide drug within a virus type, subtype, or strain, by appropriate choices of the targeting ligand(s).
- The safety of NanoViricide drugs is proven now as they specifically attack the virus and not the host.

- A variety of formulations, release profiles and routes of administration are possible.
- Low cost of drug development, manufacture, distribution.

Targets for this approach include influenzas, HIV, HCV, rabies and other viruses. NanoViricide drug candidates are currently in preclinical studies. Clinical trials are planned. Initially injectable products are the most effective but alternative routes of administrations such as nasal sprays and bronchial aerosols can also be developed.

NanoViricides Inc developed and evaluated NanoViricides against influenza and avian flu H5N1 for efficacy and safety. FluCideTM nanoviricide is designed as a polymeric surfactant micelle which has covalently attached to it ligands that bind to the influenza A virus on conserved sites. The current drug candidate was effective against both H1 and H5, and different strains of H5. This is a direct result of using a conserved binding strategy, very like that used by zanamivir. However, FluCide is directed to bind to HA rather than to inhibit neuraminidase. Binding to HA followed by putative engulfment of the virus particle should lead to viral load reduction and therapeutic benefit. Preclinical studies have shown that FluCide does more than an antibody does, in that it completes the task of encapsulating and possibly dismantling the virus, rather than merely tagging it for the immune system as a foreign particle. In mouse model of common murine-adapted influenza A/H1N1, it would require about eight times greater dosage of oseltamivir as compared to FluCide to achieve the same survival advantage results. In cell cultures (MDCK and PMKC) against influenza A/H5N1 bird flu strains (Clade 1 and Clade 2), these drug candidates have shown as high as 70% CPE inhibition. An intravenous preparation for systemic administration is in development with a ready-to-use preloaded syringe. Other routes of administration are being explored. A pre-IND briefing document about FluCide has been submitted to the FDA.

Nanocarrier-Mediated siRNA Delivery for Treatment of HIV/AIDS

Nanocarrier-mediated delivery of siRNA enhances the efficacy of siRNA-based therapies for HIV/AIDS (Mishra et al. 2014). In vivo use of siRNA is limited by various factors including degradation by RNase, rapid elimination, endosomal trapping, and low cell permeability because of the aqueous solubility and high negative charge of siRNAs. However, several promising nanoparticles, including liposomes and dendrimers are in development for siRNA-mediated gene silencing as treatment for HIV-1. Such nanocarriers have improved specificity, minimal toxicity, and ability to shepherd siRNA delivery toward the specified target site by crossing the plasma membrane.

Silver Nanoparticles as Antiviral Agents

Silver nanoparticles possess many unique properties that make them attractive for use in biological applications. Silver nanoparticles are used as surface coatings for prophylaxis of infections. It has been shown that 10 nm silver nanoparticles are bactericidal, and possible use of silver nanoparticles as an antiviral agent is being explored.

Silver nanoparticles undergo a size-dependent interaction with HIV-1 and particles in the range of 1–10 nm attached to the virus. The regular spatial arrangement of the attached nanoparticles, the center-to-center distance between nanoparticles, and the fact that the exposed sulfur-bearing residues of the glycoprotein knobs would be attractive sites for nanoparticle interaction suggest that silver nanoparticles interact with the HIV-1 virus via preferential binding to the gp120 glycoprotein knobs. Due to this interaction, silver nanoparticles inhibit the virus from binding to host cells, as demonstrated in vitro.

Silver nanoparticles can inhibit a prototype arenavirus, Tacaribe virus, at non-toxic concentrations and effectively inhibit arenavirus replication when administered prior to viral infection or early after initial virus exposure (Speshock et al. 2010). This suggests that the mode of action of viral neutralization by silver nanoparticles occurs during the early phases of viral replication.

siRNA Lipid Nanoparticle for the Treatment of Ebola Virus Infection

TKM-130803 (Arbutus Biopharma), a siRNA lipid nanoparticle, is a novel antiviral drug for the treatment of Ebola virus (EV) infection. Arbutus has conducted a series of studies in collaboration with the US Army Medical Research Institute of Infectious Diseases demonstrating the ability of TKM-130803 to protect nonhuman primates from EV (Geisbert et al. 2010). When used to treat infected nonhuman primates, TKM-130803 resulted in complete protection from an otherwise lethal dose of Zaire EV, which has been associated with periodic outbreaks of hemorrhagic fever in human populations with mortality rates reaching 90%. These data show the potential of RNAi as an effective postexposure treatment strategy for people infected with EV, and suggest that this strategy might also be useful for treatment of other emerging viral infections. In 2010, Arbutus was awarded up to a \$140 million contract from the US Government's Transformational Medical Technologies Program to advance TKM-130803 and IND application was approved by the FDA in 2011 and phase I safety trials with this drug started. The FDA placed a hold on this trial owing to "cytokine release", but then partially relaxed it to allow its use in EV-infected patients. In 2014, the FDA granted a Fast Track designation for the further development of TKM-130803. In a single-arm phase II trial, on adults with

laboratory-confirmed EVD, administration of TKM-130803 at a dose of 0.3 mg/kg/day by intravenous infusion to adult patients with severe EVD was not shown to improve survival when compared to historic controls (Dunning et al. 2016).

References

- Benzerara K, Miller VM, Barell G, et al. Search for microbial signatures within human and microbial calcifications using soft X-ray spectromicroscopy. J Invest Med. 2006;54:367–79.
- Calarota SA, Dai A, Trocio JN, et al. IL-15 as memory T-cell adjuvant for topical HIV-1 DermaVir vaccine. Vaccine. 2008;26:5188–95.
- Chakravarthy KV, Bonoiud AC, Davis WG, et al. Gold nanorod delivery of an ssRNA immune activator inhibits pandemic H1N1 influenza viral replication. Proc Natl Acad Sci U S A. 2010;107:10172–7.
- Docoslis A, Espinoza LA, Zhang B, et al. Using nonuniform electric fields to accelerate the transport of viruses to surfaces from media of physiological ionic strength. Langmuir. 2007;23:3840–8.
- Dunning J, Sahr F, Rojek A, et al. Experimental treatment of Ebola virus disease with TKM-130803: a single-arm phase 2 clinical trial. PLoS Med. 2016;13(4):e1001997.
- Edgar R, McKinstry M, Hwang J, et al. High-sensitivity bacterial detection using biotin-tagged phage and quantum-dot nanocomplexes. Proc Natl Acad Sci U S A. 2006;103:4841–5.
- Edgar R, Rokney A, Feeney M, et al. Bacteriophage infection is targeted to cellular poles. Mol Microbiol. 2008;68:1107–16.
- Geisbert TW, Lee AC, Robbins M, et al. Postexposure protection of non-human primates against a lethal Ebola virus challenge with RNA interference: a proof-of-concept study. Lancet. 2010;375:1896–905.
- Gontsarik M, Buhmann MT, Yaghmur A, et al. Antimicrobial peptide-driven colloidal transformations in liquid-crystalline nanocarriers. J Phys Chem Lett. 2016;7:3482–6.
- Halfpenny KC, Wright DW. Nanoparticle detection of respiratory infection. Wiley Interdiscip Rev Nanomed Nanobiotechnol. 2010;2:277–90.
- Kumar V, Farell G, Yu S, Harrington S, et al. Cell biology of pathologic renal calcification: contribution of crystal transcytosis, cell-mediated calcification, and nanoparticles. J Invest Med. 2006;54:412–24.
- Kuo YL, Wang SG, Wu CY, et al. Functional gold nanoparticle-based antibacterial agents for nosocomial and antibiotic-resistant bacteria. Nanomedicine (Lond). 2016;11:2497–510.
- Leevy WM, Lambert TN, Johnson JR, et al. Quantum dot probes for bacteria distinguish Escherichia coli mutants and permit in vivo imaging. Chem Commun (Camb). 2008;20:2331–3.
- Lu W, Gu D, Chen X, et al. Application of an oligonucleotide microarray-based nano-amplification technique for the detection of fungal pathogens. Clin Chem Lab Med. 2010;48:1507–14.
- Marchesan S, Da Ros T, Spalluto G, et al. Anti-HIV properties of cationic fullerene derivatives. Bioorg Med Chem Lett. 2005;15:3615–8.
- Martel J, Young JD. Purported nanobacteria in human blood as calcium carbonate nanoparticles. Proc Natl Acad Sci U S A. 2008;105:5549–54.
- Meeker DG, Chen J, Smeltzer MS. Could targeted, antibiotic-loaded gold nanoconstructs be a new magic bullet to fight infection? Nanomedicine (Lond). 2016a;11:2379–82.
- Meeker DG, Jenkins SV, Miller EK, et al. Synergistic photothermal and antibiotic killing of biofilmassociated Staphylococcus aureus using targeted antibiotic-loaded gold nanoconstructs. ACS Infect Dis. 2016b;2:241–50.
- Mishra V, Kesharwani P, Jain NK. siRNA nanotherapeutics: a Trojan horse approach against HIV. Drug Discov Today. 2014;19:1913–20.

- Padmavathy B, Vinoth Kumar R, Jaffar Ali BM. A direct detection of Escherichia coli genomic DNA using gold nanoprobes. J Nanobiotechnol. 2012;10(1):8.
- Pogodin S, Hasan J, Baulin VA, et al. Biophysical model of bacterial cell interactions with nanopatterned cicada wing surfaces. Biophys J. 2013;104:835–40.
- Radovic-Moreno AF, Lu TK, Puscasu VA, et al. Surface charge-switching polymeric nanoparticles for bacterial cell wall-targeted delivery of antibiotics. ACS Nano. 2012;6:4279–87.
- Rosen Y, Elman NM. Carbon nanotubes in drug delivery: focus on infectious diseases. Expert Opin Drug Deliv. 2009;6:517–30.
- Sapparapu G, Sims AL, Aiyegbo MS, et al. Intracellular neutralization of a virus using a cellpenetrating molecular transporter. Nanomedicine (Lond). 2014;9:1613–24.
- Sha MY, Penn S, Freeman G, Doering WE. Detection of human viral RNA via a combined fluorescence and SERS molecular beacon assay. NanoBiotechnology. 2007;3:23–30.
- Shanmukh S, Jones L, Driskell J, et al. Rapid and sensitive detection of respiratory virus molecular signatures using a silver nanorod array SERS substrate. Nano Lett. 2006;6:2630–6.
- Sheikh S, Ali SM, Ahmad MU, et al. Nanosomal Amphotericin B is an efficacious alternative to Ambisome for fungal therapy. Int J Pharm. 2010;397:103–8.
- Shen X, Ming A, Li X, Zhou Z, Song B. Nanobacteria: a possible etiology for type III prostatitis. J Urol. 2010;184:364–9.
- Speshock JL, Murdock RC, Braydich-Stolle ILK, et al. Interaction of silver nanoparticles with Tacaribe virus. J Nanobiotechnol. 2010;8:19.
- Tsurumoto T, Matsumoto T, Yonekura A, Shindo H. Nanobacteria-like particles in human arthritic synovial fluids. J Proteome Res. 2006;5:1276–8.
- Vacas-Córdoba E, Climent N, De La Mata FJ, et al. Dendrimers as nonviral vectors in dendritic cell-based immunotherapies against human immunodeficiency virus: steps toward their clinical evaluation. Nanomedicine (Lond). 2014;9:2683–702.
- Wang H, Gu L, Lin Y, et al. Unique aggregation of anthrax (Bacillus anthracis) spores by sugarcoated single-walled carbon nanotubes. J Am Chem Soc. 2006;128:13364–5.
- Yeh YT, Tang Y, Sebastian A, et al. Tunable and label-free virus enrichment for ultrasensitive virus detection using carbon nanotube arrays. Sci Adv. 2016;2:e1601026.
- Zahavy E, Ber R, Gur D, et al. Application of nanoparticles for the detection and sorting of pathogenic bacteria by flow-cytometry. Adv Exp Med Biol. 2012;733:23–36.
- Zhang YB, Kanungo M, Ho AJ, et al. Functionalized carbon nanotubes for detecting viral proteins. Nano Lett. 2007;7:3086–91.
- Zhang L, Xu J, Mi L, et al. Multifunctional magnetic-plasmonic nanoparticles for fast concentration and sensitive detection of bacteria using SERS. Biosens Bioelectron. 2012;31:130–6.
- Zhou Y, Kong Y, Kundu S, et al. Antibacterial activities of gold and silver nanoparticles against Escherichia coli and bacillus Calmette-Guerin. J Nanobiotechnol. 2012;10:19.

Chapter 15 Miscellaneous Healthcare Applications of Nanobiotechnology

Introduction

Nanobiotechnology impacts nearly all aspects of healthcare. Separate chapters were devoted to major therapeutic areas. Role of nanotechnology in delivery of vaccines for infectious diseases, nanovaccines, was discussed in Chap. 6. Other areas which are not well defined or specialties where the use of nanobiotechnology is still limited are all included in this chapter.

Nanoimmunology

Allergic and immune disorders are leading cause illness. Although various treatments have been developed to control allergy, no cure has yet been found. Nanobiotechnology is now being applied to tackle allergic and immune disorders to advance the emerging field of medicine known as nanoimmunology. The immune system can protect as well as cause harm, so there is need to help manage the harmful effects. Role of nanobiotechnology for improving immunotherapy is described in Chap. 8 (Nanooncology).

Fullerenes for Interruption of Allergic/Immune Response

Mast cells are responsible for causing allergic response and are stuffed with granules containing histamine. They are present in nearly all tissues except blood. When mast cells are triggered, inflammatory substances such as histamine, heparin, and several cytokines are quickly released into the tissues and blood, promoting an allergic response. Fullerenes (buckyballs) can interrupt the allergy/immune response by suppressing

a fundamental process in the mast cells that leads to the release of histamine. Human mast cells and peripheral blood basophils exhibit a significant inhibition of IgE dependent mediator release when preincubated with C60 fullerenes (Ryan et al. 2007). Protein microarray demonstrated that inhibition of mediator release involves profound reductions in the activation of signaling molecules involved in mediator release and oxidative stress. Follow-up studies demonstrated that the tyrosine phosphorylation of Syk was dramatically inhibited in Ag-challenged cells first incubated with fullerenes. In addition, fullerene preincubation significantly inhibited IgE-induced elevation in cytoplasmic reactive oxygen species levels. Furthermore, fullerenes prevented the in vivo release of histamine and drop in core body temperature in vivo using a mast cell-dependent model of anaphylaxis. These findings identify a new biological function for fullerenes and may represent a novel way to control mast cell-dependent diseases including asthma, inflammatory arthritis, heart disease, and multiple sclerosis.

Carbon Nanoparticle-Based Immunomodulation

Autoimmune diseases mediated by T lymphocytes are currently treated by use of broad-spectrum immunosuppressants that can lead to adverse side effects. Antioxidants represent an alternative approach for therapy of autoimmune disorders, but dietary antioxidants are inadequate for this purpose. Antioxidant carbon nanoparticles scavenge reactive oxygen species (ROS) with higher efficacy than dietary and endogenous antioxidants. Furthermore, the affinity of carbon nanoparticles for specific cell types represents an emerging tactic for cell-targeted therapy. A study has shown that nontoxic poly(ethylene glycol)-functionalized hydrophilic carbon clusters (PEG-HCCs), known scavengers of the ROS superoxide (O2⁻) and hydroxyl radical, are preferentially internalized by T lymphocytes over other splenic immune cells (Huq et al. 2016). The authors used this selectivity to inhibit T cell activation without affecting major functions of macrophages, antigen-presenting cells that are crucial for T cell activation. They also showed in vivo effectiveness of PEG-HCCs in reducing T lymphocyte-mediated inflammation in delayed-type hypersensitivity and in experimental autoimmune encephalomyelitis, an animal model of multiple sclerosis. These results indicate preferential targeting of PEG-HCCs to T lymphocytes without affecting other immune cells as a novel approach for T lymphocyte immunomodulation in autoimmune diseases.

Systemic Lupus Erythematosus

In systemic lupus erythematosus (SLE), multiorgan injury results from the dysregulated activation of adaptive and innate immune cell subsets, which leads to autoantibody deposition in tissues and subsequent inflammatory damage. Current treatment strategies aim to attenuate these cellular responses and thus prevent the spontaneous recurrence of lupus flares and worsening of disease, such as renal failure, but there are several limitations. Small-molecule drugs usually require lifelong, daily dosing and compliance rates are low. Some drugs such as cyclophosphamide and glucocorticoids are particularly toxic. Biological therapies such as monoclonal antibodies that have been tested in recent clinical trials provided marginal or no benefit despite being tailored for cell-specific suppression.

Nanoparticulate drug delivery systems can improve SLE therapy because they can be designed to effectively target small-molecule drugs or other agents to immune cells that contribute to disease. Nanogels show enhanced biodistribution to organs associated with immune cells. A nanogel drug delivery vehicle for the immunosuppressant mycophenolic acid has been shown to increase the median survival time of lupus-prone NZB/W F1 mice by 3 months with prophylactic use and by 2 months when administered after the development of severe renal damage (Look et al. 2013). CD4-targeted nanogels yielded similar therapeutic results compared with nontargeted formulations, with protection from glomerulonephritis and decreases in IFN- γ positive CD4T cells. DCs that internalize nanogels help mediate immunosuppression, as they reduce production of inflammatory cytokines such as IFN- γ and IL-12. These results demonstrate efficacy of nanogel-based lupus therapy and implicate a mechanism by which immunosuppression is enhanced, in part, by the targeting of antigen-presenting cells.

Inflammatory Diseases

Inflammation is a feature of several diseases such as rheumatoid arthritis. Inflamed tissues show monocyte recruitment from circulation and development of endothelial gaps that facilitate plasma leakage into the injured site. Inflammatory mediators can be overexpressed and persistent in chronic inflammatory conditions, leading to 'leaky' vasculature like that seen in cancer. In addition to increased permeability, inflamed tissues also have more activated macrophages or other monocytes that can be utilized as targets for site-specific drug delivery. Moreover, it has been shown that certain cell adhesion molecules (CAMs) are overexpressed on endothelial cells in inflammatory bowel disease and that vasoactive intestinal peptide (VIP) receptors are overexpressed in activated synoviocytes in patients with rheumatoid arthritis (Koo et al. 2011). Ligands specific to those overexpressed molecules can be conjugated to a nanomedicine to actively target the drug to inflammatory tissues.

Rheumatoid Arthritis

Adalimumab (Humira), etanercept (Enbrel) and infliximab (Remicade) are biologics that are currently among the top 10 best-selling drugs in the USA. They are used for the treatment of rheumatoid arthritis (RA) and other inflammatory diseases. Use of nanocarriers enables increased site-specific drug delivery to

Formulation/route of delivery	Targeting mechanism
Lipid nanoparticles/IV	Active (av _{β3}
	receptor)
Tranilast nanogel ointment/TD	Passive
Polymeric nanocomplexes/SC	Passive
PEGylated lipid micelles/SC	Active (VIP)
PEGylated liposomes/SC	Active (av _{β3}
	receptor)
Polymeric nanoparticles/IV	Passive
Dendrimers/IV	Active (folate
	receptor)
Liposomes/IV	Passive
Polymeric nanoparticles/IA	Passive
PEGylated lipid micelles/SC	Passive and active/VIP
Polymeric nanoparticles/IV	Passive
	Lipid nanoparticles/IV Tranilast nanogel ointment/TD Polymeric nanocomplexes/SC PEGylated lipid micelles/SC PEGylated liposomes/SC Polymeric nanoparticles/IV Dendrimers/IV Liposomes/IV Polymeric nanoparticles/IA PEGylated lipid micelles/SC

Table 15.1 Preclinical studies of nanomedicines for rheumatoid arthritis

Abbreviations: *DAPT* N,(N-[3,5-difluorophenacetyl]-l-alanyl)-S-phenylglycine t-butyl ester, *NSAID* nonsteroidal anti-inflammatory drug, *IA* intra-articular, *IV* intravenous, *SC* subcutaneous, *TD* transdermal, *TNF* tumor necrosis factor, *VIP* Vasoactive intestinal peptide

inflamed tissues, by utilizing the disease state including, but not limited to, enhanced permeability or changes in pH of inflamed tissues and by exploiting monocytes as active targets for drug delivery. For RA, IV, intra-articular, and subcutaneous routes of administration enable systemic delivery into circulation with access to 'leaky' vasculature, or local administration directly to diseased tissues; thereby, allowing optimal drug action.

Selected preclinical studies of nanomedicines for RA, as reported in the literature during the preceding decade, are summarized in Table 15.1. These studies evaluated the use of passive or active targeting for drug delivery, as well as the ability to increase the efficacy of existing therapies by utilizing nanoformulations (Prasad et al. 2015).

The ability of as nanoparticles, to permeate into and/or retain within the inflamed joint after intravenous and/or intra-articular administration of nanomedicines has proven to improve rheumatoid arthritis therapy, while reducing systemic exposure of patients to potentially toxic anti-arthritic drugs (O'Mary et al. 2016). Folic acid-targeted nanoparticles to target synovial macrophages are effective against rheumatoid arthritis because activated macrophages are critical in the pathogenesis of RA and specifically express a folate receptor β for the vitamin folic acid (Nogueira et al. 2016). Methotrexate-loaded lipid-core nanocapsules (MTX-LNCs) reduce proinflammatory and T cell-derived cytokines such as interferon- γ and IL-17A in activated mononuclear cells derived from RA patients (Boechat et al. 2015). This result, combined with the reduction in the dose required for therapy of experimental inflammatory arthritis, shows that MTX-LNCs are a promising system for the treatment of RA.

However, there are few nanomedicines that are in clinical trials for treatment of RA. A phase II trial to study the safety of a single, intravenous administration of long-circulating liposomal prednisolone disodium phosphate in patients with active rheumatoid arthritis has been completed (ClinicalTrials.gov identifier: NCT00241982) but the results are not published yet. A review of this topic has concluded that targeted nanodelivery of therapeutics for RA has achieved some success; however, not many biodegradable and safe polymeric nanoparticles have been investigated. The potential of and oligonucleotides aptamers also remains vastly unexplored. Despite considerable research several promising strategies, such as locked nucleic acids and aptamers have not been explored to find a suitable and appropriate agent against RA (Roy et al. 2015).

Nanohematology

Artificial Red Cells

The artificial mechanical red blood cell, called respirocyte measures about 1 µm in diameter and just flows along the bloodstream (Freitas 1998). It is a spherical nanorobot made of 18 billion atoms. The respirocyte is equipped with a variety of chemical, thermal, and pressure sensors and an onboard nanocomputer. This device is intended to function as an artificial erythrocyte, duplicating the oxygen and carbon dioxide transport functions of red cells, mimicking the action of natural hemoglobin-filled red blood cells. It is expected to deliver 236 times more oxygen per unit volume than a natural red cell. Specially installed equipment enables this device to display many complex responses and behaviors. Additionally, it has been designed to draw power from abundant natural serum glucose supplies, and thus is capable of operating intelligently and virtually indefinitely, whilst red blood cells have a natural lifespan of 4 months.

Feraheme

Feraheme (ferumoxytol) is a superparamagnetic iron oxide nanoparticle (SPION) coated with a low molecular weight semi-synthetic carbohydrate. It helps to isolate the bioactive iron from plasma components until the iron-carbohydrate complex enters the reticuloendothelial system macrophages of the liver, spleen and bone marrow. The iron is released from the iron-carbohydrate complex within vesicles in the macrophages. Iron then either enters the intracellular storage iron pool (e.g. ferritin) or is transferred to plasma transferrin for transport to erythroid precursor cells for incorporation into hemoglobin. Feraheme is approved by the FDA and specifically indicated for the treatment of iron deficiency anemia in adult patients with chronic kidney disease.

Nanoparticle-Based Drug Delivery for Gastrointestinal Disorders

For inflammatory bowel disease (IBS), including ulcerative colitis and Crohn disease, the colon represents the targeted organ. In contrast to systemic therapy, targeted therapy for IBS more efficient, safer and less costly. Numerous drugs are can be loaded into nanoparticles. Small molecules, such as tripeptides and siRNA, or larger molecules, such as proteins (hormones, antibodies, etc), can be encapsulated alone or in a complex form inside the nanoparticles. Nanoparticles can be synthesized, loaded with antiinflammatory compounds, and delivered to the colon. An efficient technique has been developed for nanoparticle targeting to the colon using a hydrogel based on electrostatic interactions between positive ions and negative polysaccharides (Laroui et al. 2012). An in situ double cross-linking process, mediated by Ca2+ and SO_4^{2-} , of chitosan and alginate administered to the mouse gastrointestinal tract by double gavage, is used for gel formation. The drug given as nanoparticulate formulation is targeted to the colon, and its degradation by aggressive environmental conditions in the gastrointestinal tract is significantly reduced. Using a hydrogel as nanoparticulate carrier, lower doses of drug can be loaded efficiently and delivered to the colon to reduce colonic inflammation.

Ginger Nanoparticles for IBS

Ginger has been used medicinally in ancient medical systems as digestive aids. Part of the therapeutic effect is due to high levels of lipids in the particles, a result of the natural lipids in the ginger plant. The nanoparticles also retained key active constituents found naturally in ginger, such as 6-gingerol and 6-shogaol, which in previous studies have shown to be active against oxidation, inflammation, and cancer. Now it has been shown that delivery of the ginger-derived compounds in a nanoparticle may be a more efficient way to target colon tissue than just providing the herb as a food or supplement. The advantage of ginger is that it is nontoxic and is a very cost-effective source of medicine.

Ginger root is converted into ginger-derived nanoparticles (GDNPs) by use of a blender, high-speed centrifugation, and ultrasonic dispersion of the ginger juice to break it up into single pellets. GDNPs could provide a supplemental therapy for patients suffering from Crohn's disease and ulcerative colitis, the two main forms of IBD (Zhang et al. 2016). Additionally, GDNPs reduce acute colitis and prevent chronic colitis and colitis-associated cancer. Moreover, the particles enhance intestinal repair by boosting the survival and proliferation of the cells that make up the lining of the colon, while concomitantly lowering the production of proteins that promote inflammation.

Each ginger-based nanoparticle is ~230 nm in diameter. Using mouse models of IBD, the research team showed that the nanoparticles targeted the colon efficiently and were absorbed mainly by cells in the lining of the intestines, where inflammation

from IBD occurs. GDNPs contain high levels of lipids, a few proteins, ~125 miRNAs and large amounts of ginger bioactive constituents. GDNPs are mainly taken up by intestinal epithelial cells (IECs) and macrophages, and are nontoxic. Oral administration of GDNPs increase the survival and proliferation of IECs and reduce the proinflammatory cytokines (TNF- α , IL-6, and IL-1 β), and increased the antiinflammatory cytokines (IL-10 and IL-22) in colitis models, suggesting that GDNPs have the potential to attenuate damaging factors while promoting the healing effect.

Nanoparticles for Targeted Therapeutic Delivery to the Liver

The liver is an essential organ because it metabolizes various waste products. It is affected by hepatitis viruses and cancer. Liver dysfunction can cause hepatitis, cirrhosis, hyperlipemia, hyperuricemia, type II diabetes and infarction. Liver is protected by a major immune defense system, the reticuloendothelial system, which captures micro- and nano-scaled materials from the bloodstream in the liver and provides obstacles to the development of liver-specific nanoparticle-based medicines. Several nanoparticles-based therapeutic materials have been developed for delivery of proteins, genes and siRNAs to the human liver to treat various diseases. Liposomes (including lipoplex), polymer micelles, polymers (including polyplex) are modified to enhance liver specificity and delivery efficiency. Drug and gene delivery systems specific to the human liver have used bionanocapsules comprising hepatitis B virus (HBV) envelope L protein, which has a pivotal role in vaccination against HBV infection (Kasuya and Kuroda 2009).

Nanonephrology

Nephrology is the branch of medicine that deals with diseases of the kidney. Nanonephrology is application of nanobiotechnology for the study of renal structure and function as well as for treatment of renal disorders. Nanobiotechnology applications for renal cancer management follows the same patterns as cancer management of other organs. For example, imaging of renal cancer and chemotherapy may be nanobiotechnology-based. One serious problem is renal failure, which is usually managed with renal dialysis.

Nanobiotechnology-Based Renal Dialysis

Renal dialysis is used to provide an artificial replacement for lost kidney function due to renal failure. It is a life support treatment and not treatment of the kidney disease, which is cause of renal failure. Dialysis provides filtration of toxins in the blood that would have normally been the function of the kidneys. Approximately one million patients worldwide suffer from end-stage renal disease and require treatment through dialysis or transplantation. There are approximately 480,000 patients in the US alone who suffer from kidney failure. The number is expected to more than double by 2010, placing considerable stress on healthcare systems throughout the world. Despite the availability of various forms of renal replacement therapy for nearly four decades, mortality and morbidity is high and patients often have a poor quality of life. The average survival rate of a dialysis patient is only 5 years. Renal transplantation is not available for all the patients as there are not enough kidney donors. Classical dialysis techniques remained in practice for more than 40 years. Within the last decade, there have been some innovations in techniques for renal dialysis. Those involving nanotechnology will be mentioned here.

Nanotechnology-Based Human Nephron Filter for Renal Failure

A human nephron filter (HNF) development could eventually enable a continuously functioning, portable or implantable artificial kidney. The HNF is the first application in developing a renal replacement therapy to potentially eliminate the need for dialysis or kidney transplantation in end-stage renal disease patients. The HNF utilizes a unique membrane system created through applied nanotechnology. The ideal renal replacement device should mimic the function of natural kidneys, continuously operating, and should be adjustable to individual patient needs. No dialysis solution would be used in this device. Operating 12 h a day, 7 days a week, the filtration rate of the HNF is double that of conventional hemodialysis administered three times a week. The HNF system, by eliminating dialysate and utilizing a novel membrane system, represents a breakthrough in renal replacement therapy based on the functioning of native kidneys. The enhanced solute removal and wearable design should substantially improve patient outcomes and quality of life. Animal studies using this technology are scheduled.

Blood-Compatible Membranes for Renal Dialysis

A novel heparin- and cellulose-based biocomposite membrane has been fabricated with nanopores by exploiting the enhanced dissolution of polysaccharides in room temperature ionic liquids (Murugesan et al. 2006). Using this approach, it is possible to fabricate the biomaterials in any form, such as films or membranes, nanofibers, nanospheres, or any shape using templates. Surface morphological studies on this biocomposite film showed the uniformly distributed presence of heparin throughout the cellulose matrix. Activated partial thromboplastin time and thromboelastography demonstrate that this composite is superior to other existing heparinized biomaterials in preventing clot formation in human blood plasma and in human

whole blood. Membranes made of these composites allow the passage of urea while retaining albumin, representing a promising blood-compatible biomaterial for renal dialysis, with a possibility of eliminating the systemic administration of heparin to the patients undergoing renal dialysis.

Ceramic Filter for Renal Dialysis

A new ceramic filter has the potential to make kidney dialysis much more efficient and to reduce by 30 min to 1 h the time required for a dialysis treatment. Specifically, the new filter promises to double the quantity of toxins removed during dialysis and to double the glomerular filtration rate (GFR), or rate of toxin removal. GFR is 100% in a normal person but only 15% at best for a dialysis patient, a rate that has changed little in the past 30 years. The ceramic filter's secret lies in its nanopores, which are organized in orderly rows and columns and correspond more closely to the nanosized toxins in the blood than do the larger pores of the standard dialysis filter.

Nanotechnology for Wound Healing

Several nanotechnology-based products have been used for wound care. Polyurethane membrane, produced via electrospinning (a process by which nanofibers can be produced by an electrostatically driven jet of polymer solution), is particularly useful as a wound dressing because of the following properties: it soaks fluid from the wound so that it does not build up under the covering, and does not cause wound desiccation. Water loss by evaporation is controlled, there is excellent oxygen permeability, and exogenous microorganism invasion inhibited because of the ultra-fine pores size. Histological examination of the wound shows that the rate of epithelialization is increased and the dermis becomes well organized if wounds are covered with electrospun nanofibrous membrane. This membrane has potential applications for wound dressing.

Chronic wounds are associated with poor epidermal and dermal remodeling. Efficacy of keratinocyte growth factor (KGF) in reepithelialization and elastin in dermal wound healing is well known. A fusion protein comprising of elastin-like peptides and KGF has been fabricated that retains the performance characteristics of KGF and elastin as evidenced by its enhancement of keratinocyte and fibroblast proliferation (Koria et al. 2011). It was also shown to self-assemble into nanoparticles at physiological temperatures. When applied to full thickness, wounds in diabetic mice these particles enhanced reepithelialization and granulation, by two and threefold respectively as compared to the controls. These findings suggest that self-assembled nanoparticles may be beneficial in the treatment of chronic wounds resulting from diabetes or other underlying circulatory conditions.

Nanotechnology-Based Products for Skin Disorders

Cubosomes for Treating Skin Disorders of Premature Infants

Cubosomes are potential drug delivery vehicles. After cutaneous administration, the lipid matrix of cubic phases and cubosomes coalesces with the lipids of the stratum comeum and leads to the formation of a lipid depot from which the drug associated to the nanosystem can be released in the deeper skin strata in a controlled manner (Esposito et al. 2016). Among many other applications, cubosomes have been investigated to create new treatments for skin disorders of premature infants. The cubosomes permit a 'breathing layer' for skin at the nano-level, which is due to their bicontinuous structure of oil and water interweaved together but never crossing each other. Unlike vaseline, which forms a protective barrier layer over the skin, cubosomes can both protect skin from outside elements and at the same time let the skin 'breathe' and exchange moisture with its environment.

Newborn babies arrive covered with a waxy substance known as vernix, which serves several functions including cleansing moisturizing, protecting and insulating the skin. Although vernix appears to have potential therapeutic uses, applications have been limited because it is difficult to collect sufficient quantities of the natural substance. Skin Science Institute of the University Children's Hospital (Cincinnati, OH), once worked on "artificial vernix" – cubosome-based outer protective layer to will help premature babies born without a fully developed outer skin layer. US patent #7,959,935 titled "Simulated vernix compositions for skin cleansing and other applications" was awarded in 2012. Efforts are being made to find a way to make large scale manufacture of cubosomes more efficient. The only way known to manufacture cubosomes initially was to use very high energy processes like ultrasound to fragment bulk cubic phase into cubosomes for use in cosmetic products for the skin. There is no commercial product available in the market that is based on cubosomes.

Nanoparticles for Improving Targeted Topical Therapy of Skin

Long term topical glucocorticoid treatment can induce skin atrophy by the inhibition of fibroblasts. Therefore, investigators have looked for the newly developed drug carriers that may contribute to a reduction of this risk by an epidermal targeting. Prednicarbate (PC, 0.25%) was incorporated into solid lipid nanoparticles of various compositions and studies were conducted where conventional PC cream of 0.25% and ointment served as reference. Local tolerability as well as drug penetration and metabolism were studied in excised human skin and reconstructed epidermis. With the latter drug recovery from the acceptor medium was about 2% of the applied amount following PC cream and ointment but 6.65% following nanoparticle dispersion. Moreover, PC incorporation into nanoparticles appeared to induce a localizing effect in the epidermal layer which was pronounced at 6 h and declined later. Dilution of the PC-loaded nanoparticle preparation with cream did not reduce the targeting effect while adding drug-free nanoparticles to PC cream did not induce PC targeting. Therefore, the targeting effect is closely related to the PC-nanoparticles and not a result of either the specific lipid or PC adsorbance to the surface of the formerly drug free nanoparticles. Lipid nanoparticle-induced epidermal targeting may increase the benefit/risk ratio of topical therapy.

Since nanoparticles can penetrate the skin barrier along the transfollicular route, chitosan nanoparticles loaded with minoxidil sulfate have been studied for their ability to sustain the release of the drug, in a targeted delivery system for the topical treatment of alopecia (Gelfuso et al. 2011). Results of these studies revealed that the chitosan nanoparticles can sustain about three times the release rate of minoxidil indicating the potential to target and improve topical therapy of alopecia with minoxidil.

Nanoparticle-Based Sun Screens

Zinc oxide offers the best broad-spectrum protection from the sun. Unlike titanium dioxide, another commonly used inorganic sunscreen, zinc oxide offers protection from both UV B and the more harmful UV A rays. Despite of the advantage of zinc oxide as a natural UV filter, its marketability was lacking because of its whiteness. This has been overcome with the use of nanoparticle technology to create an invisible screen. ZinScreen is such a product that has been marketed successfully in Australia since 2003.

NanoArc® zinc oxide (Nanophase Technologies Corporation), which is produced under cGMP conditions and is FDA approved for use as an active ingredient in personal care products, can also provide effective UV attenuation. The application of solid lipid nanoparticles as physical sunscreens and as active carriers for molecular sunscreens has been investigated. The amount of molecular sunscreen could be decreased by 50% while maintaining the protection level compared to a conventional emulsion.

Solaveil XT-40 W (Croda) based on Oxonica Ltd's OPTISOL[™] technology is a photostable UV absorber with enhanced that has applications in skin-care products and other materials. The OPTISOL technology works by absorbing UVA radiation without the concurrent formation of free radicals. Furthermore, while providing balanced UVA and UVB protection, OPTISOL also provides additional benefits in absorbing free radicals that may be generated by other components of the sunscreen formulation and enhances formulation stability. OPTISOL is based on ultra-fine titanium dioxide with the inclusion in the crystal of a small amount (<1%) of manganese. This causes a reconfiguration of the crystal's internal electronic structure that allows absorbed UV energy to be dissipated, virtually eliminating the generation of free radicals. Secondly, manganese near the crystal surface can catalyze free radicals that have been generated by other sunscreen components into harmless chemical species. A reduction in free radical load has benefits for both the skin, and for the sunscreen formulation. Free radicals are implicated in photoaging of the skin, photocarcinogenesis, and organic component degradation.

Nanoengineered Bionic Skin

NanoApplications Center at Oak Ridge National Laboratory (ORNL), in collaboration with NASA, is developing Flexible Integrated Lightweight Multifunctional skin (FILMskin), a revolutionary concept for the skin used in human prosthetic devices. Nanotechnology is used to create a water-resistant skin composite, which is shaped by lasers to be life like. The nano-enabled FILMskin will contain pressure- and temperature-sensing capabilities, like human skin, yet will be tough and flexible. ORNL scientists and engineers are using the novel properties of carbon nanotubes and aligned nanotube arrays to enhance electroactive polymers to provide multifunctional capabilities to next-generation prosthetic devices. Scientists at ORNL are also providing robotic and cognitive capabilities for the prosthetics. It may be used for skin replacement in burns patients.

Topical Nanocreams for Inflammatory Disorders of the Skin

Inflammatory skin diseases, including atopic dermatitis and psoriasis, are common. The current treatment is unsatisfactory although several topical and systemic therapies, including steroids and immunomodulators are available. The efficacy is not durable and they are associated with adverse effects. Efforts continue to develop safer alternative treatment for these disorders.

Nanocrystalline silver has been demonstrated to have exceptional antimicrobial properties, and has been successfully used in wound healing. Studies conducted by Nucryst Pharmaceuticals have revealed that topical application of Nanocrystalline silver cream (0.5%, and 1%) ointment produced significant suppressive effects on allergic contact dermatitis in a guinea pig model. There was a clear concentration-response relationship to the decrease of inflammation as lower concentrations were not effective. The effects were equivalent to the immunosuppressant tacrolimus ointment. This study suggests that nanocrystalline silver cream has therapeutic potential for treating inflammatory skin diseases.

Nanobiotechnology for Disorders of Aging

The human life expectancy has nearly doubled during the last century. Aging is not a disease but certain diseases are associated with aging. The incidence of these diseases, many of which are incurable at the present state of knowledge, has spurred research activity. In the academic sectors there is an increase in the research activity to unravel the biology of ageing and several companies are developing products for managing disorders associated with aging. Several factors play a role in aging process. These include mitochondria and telomeres. Telomeres are proteins that function like caps on the ends of chromosomes and ensure successful DNA replication when a cell divides. However, every time a cell divides, the telomeres shorten and eventually become exhausted. In general, aging cells become progressively less able to form and maintain tissue. This dysfunction plays a key role in a variety of presently incurable age-associated diseases such as macular degeneration, arteriosclerosis, atherosclerosis, osteoporosis, skin atrophy, progeria, and others.

Stanford University has developed and patented DNA nanocircles that can be used to simply and efficiently synthesize long telomere repeats on human chromosomes without the need for telomerase. Because telomere length acts as a cellular clock to define the lifespan of a cell population, this technology could potentially extend the life of cells used for ex vivo cell therapy without cancerous transformation. The applications include enhancing the growth and delaying or preventing senescence in cultured primary tissues such as islet cells, bone marrow, skin, hepatic tissues, and stem cells. Currently it is not clear if this technology has any potential applications in disorders associated with aging.

Personal Care Products Based on Nanotechnology

Several personal care products are referred to as cosmetics, which are defined by the FDA as "articles intended to be applied to the human body or any part thereof for cleansing, beautifying, promoting attractiveness, or altering the appearance". The term "cosmeceutical" is used for a product that is between a drug and cosmetics; it has biological action in the skin like a drug, but is regulated as a cosmetic since it claims to affect appearance.

Effects on skin hydration and viscoelasticity are important criteria during the development of novel cosmetic formulations. Solid lipid nanoparticles represent a promising compound for hydrating new cosmetic formulations. Addition of solid lipid nanoparticles to conventional creams lead to an increase of skin hydration after repeated applications for a few weeks. Cosmeceuticals are the fastest growing segment of the personal care industry, and several topical cosmeceuticals are being used for skin conditions such as photoaging, hyperpigmentation, wrinkles, and hair damage.

Nanocosmeceuticals

Nanotechnology has opened new perspectives for the future of cosmeceutical industry and nanotechnology-based cosmeceuticals are referred to nanocosmeceuticals as an anology to nanopharmaceuticals. Nanoparticles used in cosmeceuticals include liposomes, solid lipid nanoparticles, dendrimers, nanocapsules, nanocrystals, gold nanoparticles, silver nanoparticles, cubosomes, niosomes, and fullerenes (Lohani et al. 2014). Nanotechnology has increased bioavailability of active ingredients and increase the aesthetic appeal of cosmeceutical products with prolonged effects. However, there is a concern about the possible penetration of nanoparticles through the skin and potential hazards to the human health (see Chap. 17).

Nanotechnology is used in several personal care products such as sun creams and deodorants. Nanomaterials can act as sun blockers to protect human skin in formulations that eliminate unnecessary exposure to the harmful UV rays of the sun. Nanomaterials can impart antibacterial and anti-odor functionality on human skin in powder, gel, stick or spray underarm products that can be applied smoothly without plugging the spray nozzle, caking or staining while maintaining clarity. The market trends for deodorants and antiperspirants are toward clear and highly effective formulations that are mild and non-irritating.

Nanomaterials can be introduced into a variety of oral care products to impart antimicrobial and anti-irritant properties without sacrificing flow, texture or color. Dental pastes, creams and cleaners need to thoroughly clean teeth and gums, and leave a clean and crisp feeling in the mouth afterwards.

Nanotechnology for Hair Care

Human hair is a nanocomposite biological fiber with well-characterized microstructures. Nanomechanical characterization of human hair can help to evaluate the effect of cosmetic products on hair surface, can provide a better understanding of the physicochemical properties of a wide variety of composite biological systems, and can provide the dermatologists with some useful markers for the diagnosis of hair disorders. A systematic study of nanomechanical properties of human hair including hardness, elastic modulus and creep, was carried out using the nanoindentation technique (Wei et al. 2005). The samples include Caucasian, Asian and African hair at virgin, chemo-mechanically damaged and treated conditions. Hair morphology was studied using scanning electron microscopy (SEM). Indentation experiments were performed on both the surface and cross-section of the hair, and the indents were studied using SEM. The techniques were used to test a new high-tech hair conditioner. Ultimately, the same techniques could be used to improve lipstick, nail polish and other beauty products. Application of nanotribology - the measurement of very small things such as the friction between moving parts in microelectronics is important for study of hair as friction is a major issue. Everyday activities like washing, drying, combing and brushing all cause hairs to rub against objects and against each other. Over time, the friction causes wear and tear. If damaged hair is exposed to humidity; the hairs plump up, and the cuticles stick out even further, leading to more friction - a fact confirmed by the AFM when a tiny needle across the surface. This research is being utilized by manufacturers of hair care products for developing a new formula with additives to make the conditioner coat the hair evenly. In the future, the AFM techniques could be used to develop wear-resistant nail polishes and lipsticks.

Nanodentistry

Nanodentistry will make possible the maintenance of comprehensive oral health by involving the use of nanomaterials, biotechnology (including tissue engineering) and, ultimately, dental nanorobotics. The first dental nanorobots could be constructed by the year 2015 and will enable precisely controlled oral analgesia, dental replacement therapy using autologous cells teeth and rapid nanometer-scale precision restorative dentistry.

Bonding Materials

NANO-BOND Universal Bonding System (Pentron Clinical Technologies) is based on Hybrid Plastics' POSS® technology (Polyhedral Oligomeric Sil sesquioxanes). It results in strengthened resin while it infiltrates the etched surface and provides strong interface between the tooth and the restorative material. The system consists of a uniquely formulated self-etch primer and adhesive system that are said to work together for great bonding to dentin and cut enamel. The kit also contains a dual cure activator that promotes reliable bonding to self and dual-cured materials. The Nano-Bond System greatly alleviates the problem of post-bonding sensitivity by keeping tubules occluded during the self-etching step.

AdperTM Single Bond Plus Adhesive (3M ESPE) is a high bond strength dental adhesives. The improved adhesive incorporates a nanofiller technology that contributes to higher dentin bond strength performance. Adper is ideal for bonding all classes of direct composite restorations, as well as root surface desensitization and porcelain veneers. The nanofiller particles in Adper are added in a manner that does not allow them to cluster together. The particles are stable and will not settle out of dispersion. Therefore, no shaking is needed prior to use.

Dental Caries

The conventional treatment of dental caries involves mechanical removal of the affected part and filling of the hole with a resin or metal alloy. However, this method is not suitable for small early cavities because a disproportionate amount of healthy tooth must be removed to make the alloy or resin hold in place. A dental paste has been produced from synthetic enamel that rapidly and seamlessly repairs early caries lesions by nanocrystalline growth, with minimal wastage of the natural enamel (Yamagishi et al. 2005).

The application of surfactants as reverse micelles or microemulsions for the synthesis and self-assembly of nanoscale structures is one of the most widely adopted methods in nanotechnology. The resulting synthetic nanostructure assemblies sometimes have an ordered arrangement. These developments in nanotechnology

have been used to mimic the natural biomineralization process to create dental enamel – the hardest tissue in the human body. This is the outermost layer of the teeth and consists of enamel prisms, highly organized micro-architectural units of nanorod-like calcium hydroxyapatite (HA) crystals arranged roughly parallel to each other. The hydroxyapatite nanorods surface was synthesized and modified with monolayers of surfactants to create specific surface characteristics, which enable the nanorods to self-assemble into an enamel prism-like structure at a water/air interface (Chen et al. 2005). The size of the synthetic hydroxyapatite nanorods can be controlled and nanorods similar in size to human enamel were synthesized. The prepared nanorod assemblies were examined using TEM and AFM and were shown to be comprised of enamel prism-like nanorod assemblies with a Ca/P ratio between 1.6 and 1.7. It is possible that an enamel-like composite would be available within a year and crowns suitable for repairing decayed teeth within about 4 years. Application of synthetic enamel will not be limited to filling cavities. It has potential for use in bone repair and bone augmentation.

New treatment opportunities based on nanobiotechnology may include detection of dental decay spots prior to formation of cavities and repair of these, improved nanomaterials for covering dental enamel and continuous oral health maintenance by use of mechanical dentifrobots.

Nanospheres for Dental Hypersensitivity

Dental hypersensitivity, a painful condition due to exposure of the dentine of the tooth affects millions of people worldwide. The dentine contains tiny fluid-filled channels which radiate outwards from the nerve terminals at the center of the tooth. Heat or cold and some chemicals, can cause the fluid in these channels to move in or out irritating the nerve endings and causing sharp pain. Nanospheres of hydroxyapatite, a ceramic material, could be a longterm solution or cure for sensitive teeth. Commercially available silica nanospheres are ~40 nm in diameter. Nanospheres could help dentists fill the tiny holes in the teeth that make them incredibly sensitive. If these channels are fully or partially blocked, the flow can be reduced and the pain stopped or significantly reduced. The next stage of the research will be to synthesize nanospheres combining hydroxyapatite and fluorine, which would fill the holes and encourage re-mineralization at the same time and provide a powerful repair tool for dentists.

Nanomaterials for Dental Filling

The standard composite resin filling, a natural-looking restoration, is the method of choice when appearance is an issue. A dentist creates the filling by mixing the pure liquid resin with a powder that contains coloring, reinforcement and other materials, packing the resulting paste into the cavity, and illuminating the tooth with a light

that causes the paste to polymerize and harden. For decay-fighting composite fillings, the problem arises from an additive that is included in the powder to provide a steady release of calcium and phosphate ions. These ions are essential to the long-term success of the filling because they not only strengthen the crystal structure of the tooth itself, but buffer it against the decay-causing acid produced by bacteria in the mouth. Yet the available ion-releasing compounds are structurally quite weak, to the point where they weaken the whole filling.

Nanotechnology has the potential to produce tooth restorations that are both stronger and more effective at preventing secondary decay than any decay-fighting fillings available currently. The new spray-drying technique yields particles of several compounds, one of which being dicalcium phosphate anhydrous (DCPA), which are about 50 nm across, 20 times smaller than the 1 μ m particles in a conventional DCPA powder. Because these nanoscale particles have a much higher surface to volume ratio, they are much more effective at releasing ions, which means that much less of the material is required to produce the same effect. That, in turn, leaves more room in the resin for reinforcing fibers that strengthen the final filling. To exploit that opportunity, the Paffenbarger researchers also have developed nanoscale silica-fused fibers that produce a composite resin nearly twice as strong as the currently available commercial variety.

Nanomaterials for Dental Implants

Dental manufacturers are incorporating nanotechnology into their dental implant surface designs because the technology is purported to cut healing time in half and improve osseointegration. These include 3i and Bicon, both of which have branded their nanotechnology-based dental implant surfaces as "NanoTite", Astra Tech with its OsseoSpeed, and Straumann with its SLActive.

Nanodiamonds for Root Canal Repair

Root canal therapy (RCT) is a standard of treatment that addresses infected pulp tissue in teeth and protects against future infection. It involves removing dental pulp comprising blood vessels and nerve tissue, decontaminating residual infected tissue, and use of a filler material to replace the space in the root canal that was previously composed of dental pulp. Gutta percha (GP) is commonly used as the filler material, as it is malleable, inert, and biocompatible. However, GP has drawbacks including leakage, root canal reinfection, and poor mechanical properties. Use of root filling materials other than GP has been explored to address these challenges. Nanodiamonds (NDs) may offer unique advantages due to their favorable properties that include versatile faceted surface chemistry, biocompatibility, and their role in improving mechanical properties. A ND-embedded GP (NDGP) was developed and

functionalized with amoxicillin, a broad-spectrum antibiotic commonly used for endodontic infection (Lee et al. 2015). Comprehensive materials characterization confirmed improved mechanical properties of NDGP over unmodified GP. In addition, digital radiography and microCT imaging demonstrated that filling of root canals with NDGP could be achieved using clinically relevant techniques. Furthermore, bacterial growth inhibition assays confirmed efficacy of NDGP functionalized with amoxicillin. NDGP can improve treatment outcomes in RCT.

Nanomedical Aspects of Oxidative Stress

Free radical reactions involving reactive oxygen species (ROS) and reactive nitrogen species (RNS) contribute to the pathogenesis and progression of several human diseases. Antioxidants, such as vitamins C and E, 21-aminosteroids and other free radical scavengers, have met with only limited success in clinical applications. This is partly due to our inability to design efficient antioxidants with site-directed, controlled activity. Nanotechnology has provided dramatic improvement in controlling or eliminating oxidation reactions in materials applications, which may provide a new basis for pharmacological treatment of diseases related to oxidative stress.

Nanoparticle Antioxidants

Nanotechnology has made significant advances in the reduction of free radical damage in the field of materials science. Cross-disciplinary interactions and the application of this technology to biological systems have led to the elucidation of novel nanoparticle antioxidants. Three of the most-studied nanoparticle redox reagents at the cellular level, are rare earth oxide nanoparticles (particularly cerium), fullerenes and carbon nanotubes.

Fullerene-Based Antioxidants

Water-soluble derivatives of buckminsterfullerene C60 derivatives are a unique class of nanoparticle compounds with potent antioxidant properties. Studies on one class of these compounds, the malonic acid C60 derivatives (carboxyfullerenes), indicated that they can eliminate both superoxide anion and H_2O_2 , and were effective inhibitors of lipid peroxidation, as well. Carboxyfullerenes demonstrated robust neuroprotection against excitotoxic, apoptotic and metabolic insults in cortical cell cultures. They were also capable of rescuing mesencephalic dopaminergic neurons from both MPP(+) and 6-hydroxydopamine-induced degeneration. Although there is limited in vivo data on these compounds, systemic administration of the C3 carboxyfullerene isomer has been shown to delay motor deterioration and death in a mouse model familial amyotrophic lateral sclerosis. Ongoing studies in other animal models of CNS disease states suggest that these novel antioxidants are potential neuroprotective agents for other neurodegenerative disorders including Parkinson's disease.

Ceria Nanoparticles as Neuroprotective Antioxidants

Ceria nanoparticles from anthanide series have several unique properties that make them highly efficient redox reagents. Several studies have reported the ability of ceria nanoparticles to mitigate oxidative stress at the biological level. Ceria nanoparticles also protect neurons from free radical-mediated damage initiated by ultraviolet (UV) light, H2O2 and excitotoxicity, leading to the hypothesis that the mechanism of action is one of free radical scavenging (Rzigalinski et al. 2006). When compared with single doses of other free radical scavengers, such as vitamin E, melatonin and n-acetyl cysteine, ceria nanoparticles demonstrated significantly greater neuroprotection after a 5- and 15-min UV insult. A single dose of nanoparticles delivered up to 3 h post-injury also afforded neuroprotection. Ceria nanoparticles were also effective in reducing cell death associated with γ -irradiation. In another study, nanoparticles were shown to directly decrease free radical production (Schubert et al. 2006). No toxicity was observed with ceria nanoparticle sizes of 6 and 12 nm and yttrium oxide nanoparticles were even more effective than ceria. Ceria nanoparticles larger than 30 nm or nitrates and sulfates of cerium did not have any significant effects. A unique feature of cerium nanocrystals is that they can be applied multiple times over weeks, and slowly return to their starting cerium while remaining colloidally stable allowing multiple applications as antioxidants. A self-renewing antioxidant that can stay in place to protect organs would have clear benefits over toxic radioprotectants that usually must be eliminated from the body before causing serious harm to healthy tissue.

Several studies also suggest that ceria nanoparticles are potent antiinflammatory agents. Microglia, the immune cells of the brain, are 'activated' in response to neuronal damage and show an inflammatory response with release NO as well as IL-1β. Treatment of injured organotypic cultures with ceria nanoparticles reduced their ability to activate microglia. Further, treatment of activated microglia with ceria nanoparticles reduces production of soluble factors that promoted death in uninjured neurons, including NO and IL-1β. Delivery of nanoparticles to the uninjured neurons also directly affords neuroprotection from the damaging effects of activated microglia. Thus, it appears that nanoparticles may blunt the inflammatory response in immune cells, as well as reduce inflammatory injury to nonimmune cells. When tested with H2O2, a strong oxidizing agent, ceria nanoparticles were found to perform 9-times better than a common antioxidant, Trolox, and are still significantly oxidizing through 20 redox cycles. Cerium nanoparticles can reduce oxidative stress in human dermal fibroblasts exposed to H2O2 with efficiency comparable to their solution phase reactivity (Lee et al. 2013). These data suggest that organic coatings on cerium oxide nanocrystals do not limit the antioxidant behavior of the nanocrystals, and that their redox cycling behavior can be preserved even when stabilized.

Antioxidant Nanoparticles for Treating Diseases Due to Oxidative Stress

The prospects for the use of nanoparticles for free radical scavenging in diseases due to oxidative stress are promising. However, further studies in animals and clinical trials will be needed to ascertain this beneficial effect. Other nanoparticles such as fullerenes also show biological antioxidant activity and potent neuroprotective effects, which need to be investigated. Some studies indicate that there may be an optimal level of free radical scavenging above which antioxidant nanoparticles may interfere with the beneficial roles of free radicals within the cell and have harmful effects. This is important for establishing the safety and proper doses of antioxidant nanomedicines.

Nanotechnology and Homeopathic Medicines

Homeopathy was founded in Germany in 1789. The basic principle is that "like cures like." The materia medica of this system is based on the description of symptoms induced by several substances including metals and plant derivatives. Extreme dilutions of the same substance are effective for the treatment of the symptoms. Currently, there is a resurgence of interest in homeopathy both in Europe and the US. Clinical trials have produced mixed results.

Homeopathy is controversial because medicines in high potencies designated as as 30c and 200c involve huge dilution factors (10⁶⁰ and 10⁴⁰⁰ respectively) which are many orders of magnitude greater than Avogadro's number, so that theoretically there should be no measurable remnants of the starting materials. No hypothesis which predicts the retention of properties of starting materials has been proposed nor has any physical entity been shown to exist in these high potency medicines. A study has used TEM, electron diffraction and chemical analysis by Inductively Coupled Plasma-Atomic Emission Spectroscopy (ICP-AES) to examine market samples of metal-derived medicines from reputable homeopathic manufacturers, and demonstrated for the first time the presence of physical entities in these extreme dilutions, in the form of nanoparticles of the starting metals and their aggregates (Chikramane et al. 2010). Further investigations are in progress to determine if presence of nanoparticles is related to therapeutic effect.

Nanoparticles as Antidotes for Poisons

Currently antidotes are not available to treat many harmful, even life-threatening reactions. Drug removal differs from drug delivery in that some drugs are given in encapsulated form to prolong action whereas drug removal musto be accomplished rapidly. Removal agents must reduce the available drug concentration to below the toxicity threshold and they must be biocompatible.

In experimental studies on animal hearts, emulsion-based NPs extract bupivacaine from the aqueous phase in a physiological salt solution and attenuate the drug's cardiotoxicity than a macroemulsion. Nanoparticles can sequester bupiyacaine from the aqueous phase of human blood and merit further investigation in animal models of intoxication. Synthetic polymer NPs that bind poisonous molecules and neutralize their effect in vivo have been investigated as plastic antidotes. Although techniques are now available for synthesizing polymer NPs with affinity for target peptides, their performance in vivo is a far greater challenge. Particle size, surface charge, and hydrophobicity affect not only the binding affinity and capacity to the target toxin but also the toxicity of NPs and the creation of a layer of proteins around a NP that can alter and or suppress the intended performance. Design rationale of a plastic antidote for in vivo applications has been reported, which optimizes the choice and ratio of functional monomers incorporated in the NP, and maximizes the binding affinity to a target peptide (Hoshino et al. 2012). Biocompatibility tests of the NPs in vitro and in vivo revealed the importance of tuning surface charge and hydrophobicity to minimize NP toxicity and prevent aggregation induced by nonspecific interactions with plasma proteins. The toxin neutralization capacity of NPs in vivo showed a strong correlation with binding affinity and capacity in vitro. Furthermore, in vivo imaging experiments established the NPs accelerate clearance of the toxic peptide and eventually accumulate in macrophages in the liver. These results provide a platform to design plastic antidotes and reveal the potential and possible limitations of using synthetic polymer nanoparticles as plastic antidotes.

Magnetic nanoparticles conjugated with β -cyclodextrin adsorb diazepam, which can then be removed from blood by an external magnetic field; this has potential applications in treatment of diazepam overdose and other poisonings (Cai et al. 2011).

Because existing detoxification platforms such as antisera, MAbs, smallmolecule inhibitors and molecularly imprinted polymers act by targeting the molecular structures of toxins, customized treatments are required for different diseases. A biomimetic toxin nanosponge, which consists of a polymeric nanoparticle core surrounded by red blood cell membranes, functions as a toxin decoy in vivo absorbs membrane-damaging toxins and diverts them away from their cellular targets (Hu et al. 2013). In a mouse model, the nanosponges markedly reduced the toxicity of staphylococcal α -toxin and thus improve the survival rate of toxin-challenged mice. The toxin-laden nanosponge primarily wound up in the mouse livers, which appeared normal. This toxin nanosponge can potentially treat a variety of injuries and diseases caused by pore-forming toxins.

Nanoparticles for Chemo-Radioprotection

Chemotherapy and radiotherapy are the standard treatments for cancer but they have severe adverse effects on the body. Radiation can damage epithelial cells and lead to permanent hair loss, among other effects, and certain types of systemic chemotherapy can produce hearing loss and damage to several organs, including the heart and kidneys. Only one drug, amifostine, has been approved to date by the FDA to help protect normal tissue from the side effects of chemotherapy and radiation, and there is a need for new and improved agents.

Animal experimental studies have shown that the nanoparticle, fullerene CD60_DF1 (C Sixty), can help fend off damage to normal tissue from radiation. It acts like an "oxygen sink," binding to dangerous oxygen radicals produced by radiation. Fullerenes can be considered as a potentially new class of radioprotective agents. CD60_DF1 given before and even immediately after exposure to X-rays reduces organ damage by one-half to two-thirds, which is equal to the level of protection given by amifostine. Moreover, the fullerene provides organ-specific protection, e.g. the kidney as well as certain parts of the nervous system.

Radioprotecting ability of the silver nanoparticle (SN)-glyzyrrhizic acid (GLY) complex has been evaluated in an in vivo model using Swiss albino mice (Chandrasekharan and Nair 2012). SNs with particle size of <50 nm were dispersed in an aqueous solution of Pluronic F127 and complexed with the phytoceutical GLY. The potential of the complex as an adjuvant during radiotherapy was also analyzed in tumor-bearing mice. The administration of SN-GLY, SN, and GLY protected the hematopoietic and gastrointestinal systems against radiation-induced damages as revealed by the total white blood cell count, bone marrow cellularity, endogenous spleen colony formation, levels of cellular antioxidants, and histopathologcal examination of gastrointestinal tract. Oral administration of SN-GLY, SN, and GLY 1 h before a sublethal dose of radiation exposure reduced the depletion of cellular antioxidants and lipid peroxidation in various tissues of mice. Survival of animals following exposure to a lethal dose of gamma radiation was also improved. Another finding was that the oral administration of the SN-GLY complex to tumor-bearing mice before 4 Gy gamma irradiation resulted in a faster tumor regression.

Role of Nanobiotechnology in Biodefense

Nanobiotechnology provides several devices for the diagnosis of agents used in biological warfare and bioterrorism. Because of its ability to create structures of nanoscale dimension with large aggregate particle surface area-to-volume ratios, nanotechnology offers new opportunities to treat drug poisonings. Some examples from experimental studies support this potential.

Nanoparticles to Combat Microbial Warfare Agents

Nanomaterials could play a role as an anthrax antibiotic. Antibodies that latch on to dormant anthrax spores and drugs that destroy anthrax could be linked to the spherical carbon molecule fullerene to make an antibiotic. The drug would kick in when an inhaled spore germinates, killing the anthrax before it releases deadly amounts of toxin.

This could be effective if one has just been exposed or the exposure is expected within 24 h following administration of the drug.

Preventing the interaction of toxins with their cellular receptors CMG2 and ATR/TEM8 is an important goal for anthrax therapy. Nanotechnology approaches have been used for the multivalent display of engineered receptor decoys, and their efficacy against anthrax lethal toxin in vitro and in vivo.

Several concepts of targeting of nanosuspension dosage forms for treatment of bioweapon-mediated diseases have been developed at the Baxter Healthcare Corporation. Alterations of pharmacokinetic profiles of existing antibiotics can lead to enhanced efficacy with reduced side effects. This has been shown for a nanosuspension formulation of the antifungal agent itraconazole. Secondly, viral sanctuaries breed resistance and often include the brain and lymphatics. These may be targeted by loading nanoparticulate drug into macrophages which target these organs, increasing antiviral drug concentration in these typically inaccessible regions. Finally, a strategy for dendritic cell vaccines has been developed for use against bioweapons.

Removal of Toxins from Blood

An important part of treatment of poisoning is removal of toxins circulating in the blood. An even more critical need is for removal of biological and radiological toxic material from the blood after exposure to bioterrorist attacks or biochemical warfare. The Argonne National Laboratory and the University of Chicago are collaborating to develop a magnetic nanoparticle-based technology that removes biological, radiological and in some cases chemical toxins from blood. Their goal is to devise a portable system that is fast and thorough using magnetic nanoparticles coated with antibodies or chemicals that complement toxins. Once injected into the patient, the particles latch onto toxins and are later removed when the blood is pumped through tubing into a magnetic separator. Cleansed blood is then returned into the body. The approach is particularly safe because the closed loop system never exposes blood to the outside environment. Regardless of the type of exposure, if the toxins are removed before they accumulate in tissues, then organs will not fail and the patients will survive. This method may not be effective in case of rapidly acting agents such as nerve gas where the time between exposure and death is a matter of minutes. However, some chemical and many biological and radiological agents need hours or even days to cause fatal damage, allowing a wide enough window for the particle treatment to be effective. Some requirements for the development of this technology are:

- The particles, which start with magnetic cores in the 8–12 nm range, must be the right size to navigate within the body. If they are too small, they may pass out the kidneys; and if they are too large they may get trapped.
- The particles also need to be biocompatible so the body accepts them
- They should be biodegradable in case some remain after treatment.

Several companies are already developing magnetic nanoparticles for medical applications. Their use of FDA-approved antibodies, reagents and off-the-shelf medical components could remove some regulatory hurdles. That could pave the way for not only military and civilian defense applications but clinical treatments such as overdoses. However, it will take a couple of years for this development.

Nanobiotechnology for Public Health

Emphasis on preventive medicine and public health is increasing. High technology medicines will benefit a limited number of population and mostly in the developed countries. Measures to improve public health will have a much larger impact on the future healthcare for most of the people on this earth. One of the major problems in developing countries is sanitary water supply.

Nanotechnology for Water Purification

Nanotechnology has the potential to provide novel nanomaterials for treatment of surface water, groundwater, and waste water contaminated by toxic metal ions, organic and inorganic solutes, and microorganisms. These consist of nanomaterials for water filtration, nanotechnologies for water remediation, and NPs for disinfection of water.

Nanofiltration to Remove Viruses from Water

Nanofiltration is a relatively simple and reliable procedure that consists in filtering water through membranes with nanopores (size 15–40 nm) that retain viruses by size exclusion.

Shortcomings of some membranes are that they often form pin-holes and cracks during the fabrication process, resulting in wasted membranes. Scientists at the Queensland University of Technology (QUT) in Australia have developed specially designed ceramic membranes used as nano-mesh for nanofiltration, which are less likely to be damaged during manufacture and have the potential to remove viruses from water. This modification has increased the rates of flow that pass through the membranes tenfold compared with current ceramic membranes, while maintaining the efficiency of capturing over 96% of the unwanted particles.

Nanostructured Membranes for Water Purification

Current methods for the purification of contaminated water sources are chemicalintensive, energy-intensive, and/or require post-treatment due to unwanted byproduct formation. Integration of nanostructured materials and Fe-catalyzed free radical reactions enables detoxification of water. Harmful organic contaminants can be degraded through the addition of a substrate, glucose, which is enzymatically converted to H2O2 without adding harmful chemicals (Lewis et al. 2011). Application of these technologies can be extended to disinfection and/or virus inactivation.

Plasma-modified ultralong CNTs have been reported to exhibit ultrahigh specific adsorption capacity for salt (exceeding 400% by weight) that is two orders of magnitude higher than that found in the current state-of-the-art activated carbon-based water treatment systems. This adsorption capacity was exploited in ultralong CNT-based membranes that can remove salt, as well as organic and metal contaminants (Yang et al. 2013). These may lead to next-generation rechargeable, point-of-use potable water purification appliances with superior desalination, disinfection and filtration properties.

Nanotechnologies for Water Remediation

Advantages of use of nanomaterials for water remediation are their enhanced reactivity, surface area and sequestration characteristics. Several nanomaterials are in development for this purpose including the following:

- Biopolymers
- Carbon nanotubes
- Iron nanoparticles
- Zeolites

Cyanobacterial metabolites – microcystin, cylindrospermopsin (CYN), 2-methylisoborneol (MIB) and geosmin (GSM) – are a major problem for the water industry. Low molecular weight cut-off (MWCO), or 'tight' NF, membranes afford average removals above 90% for CYN, while removal by higher MWCO, or 'loose' NF membranes is lower. MIB and GSM are removed effectively (>75%) by tight NF but less effectively by loose NF. Microcystin variants are removed to above 90% by tight NF membranes; however, removal using loose NF membranes depends on the hydrophobicity and charge of the variant. Natural organic matter concentration in the waters treated with this method had no effect on the removal of cyanobacterial metabolites (Dixon et al. 2011).

Several NPs have been shown to have antibacterial effects and are used as disinfectants, e.g. silver NP coated on surfaces. A study has shown that lanthanum calcium manganate (LCMO) NPs have greater antibacterial efficacy against P. aeruginosa-ATCC 27853, a soil and water born pathogenic bacteria as compared to Eu3+ doped lanthanum calcium manganate (LECMO) NPs (De et al. 2010). Size of synthesized NPs was 50–200 nm and X-ray diffraction pattern showed the formation of a single phase LCMO or LECMO of an orthorhombic crystal structure after annealing the precursor at 10000 C for 2 h in air. LCMO NPs can offer future applications as antimicrobial drugs and for water purification. Iron oxide $(\alpha$ -Fe₂O₃) nanoparticles, 5 nm in size, have been used to remove arsenic ions from natural water samples (Tang et al. 2011). Iron nanoparticles maintained their arsenic adsorption capacity even at very high competing anion concentrations. This method was used to purify contaminated natural lake water sample to meet the US Environmental Protection Agency's drinking water standard for arsenic.

Nanotechnology-Based Photochemical Water Purification

Nanotechnology-based photochemical water purification is also feasible. Bioactive nanoparticles can be used for disinfection of water, e.g. metal-oxide NPs, particularly silver, and titanium dioxide for photocatalytic disinfection can provide alternative to chlorination of water. Multiple wavelengths of a light emitting device or natural light illuminate a high-surface-area nanotechnology coating to cause photochemical reactions. In development by Puralytic Inc., this process effectively removes the broadest range of contaminants including:

- Organic compounds: pharmaceuticals, petrochemicals.
- Heavy metals: lead, mercury, arsenic, and selenium
- Microorganisms: viruses, bacteria, protozoa, cysts

The process is environment friendly and cost-effective with no chemicals or additives, waste water, or pressure loss.

Magnetic Nanoscavengers for Water Purification

The development of sustainable, robust and energy efficient water purification technology is still challenging. Although use of nanoparticles is promising, methods are needed for their efficient recovery post treatment. This issue has been addressed by fabrication of magnetically ultraresponsive 'nanoscavengers', nanoparticles containing synthetic antiferromagnetic core layers and functional capping layers (Zhang et al. 2013). When dispersed in water, the nanoscavengers efficiently interact with contaminants to remove them from the water. They are then quickly collected (<5 min) with a permanent magnet, owing to their magnetically ultraresponsive core layers. Specifically, we demonstrate fabrication and deployment of Silver-capped nanoscavengers have been used for disinfection of water followed by application of an external magnetic field for separation. A collision-based model for pathogen inactivation was also developed and the authors of this study have proposed a cyclical water purification scheme in which nanoscavengers are recovered and recycled for contaminant removal.

Nanobiotechnology and Nutrition

Nanotechnologies will have an impact on nutrition research in many ways. Nanodevices can be used for real-time optical intracellular sensing. These technologies may be particularly useful in obtaining accurate spatial information and low-level detection of essential and nonessential bioactive food components (nutrients) and their metabolites, and in enhancing the understanding of the impact of nutrient/ metabolite and biomolecular interactions. Nanobiotechnology will have an impact on food production as well as improved nutrition. Nanotechnologies can provide many benefits as shown in Table 15.2.

Nanobiotechnology and Food Industry

A major challenge in food production lies in the translation of established technologies into food production for delivering the optimal health and sensory benefits such as taste and smell. The major company involved in this area is Nestle SA. The Company believes that nutrition, consumers and use of new technologies in food science will be key drivers for future product innovation.

Table 15.2	Applications c	f nanotechnologies in food and nutrition sciences

Table 15.2 Applications of nanotechnologies in food and nutrition sciences		
Food manufacture		
Nanoparticles and nanocrystals of essential nutrients to improve bioavailability		
Use of self-assembly in nature and materials on a nanoscale with bottom up approach		
Use of nanoparticles to increase material strength barriers		
Product research and innovation		
Development of new products based on nanoscience research of natural foods		
Control of bioavailability		
Products based on simulation of customer preferences based on taste and smell nanosensing		
Study of molecular physiology and genomics of taste cells		
Testing of food effects via biomarkers		
Product marketing		
Unique nanobarcodes on proprietary products		
Shelf life indicators		
Quality control and testing		
Nanodiagnostics for food contaminants and microorganisms		
Nanosensors for quality control of food		
Nutrition		
Development of personalized nutrition based on metabolic needs of individual		
Development of foods based on personalized sensory needs of the individual		
Development of nutriceuticals		
Development of nutricosmetics		
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One example is that of lycopene, the carotenoid that gives tomatoes and other fruits and vegetables their red color. Health benefits of lycopene are well recognized. Lycopene has been of interest recently for its role in prostate cancer. Lycopene from fresh and unprocessed tomatoes is poorly absorbed by humans. Absorption of lycopene is higher from processed foods such as tomato paste and tomato juice heated in oil. Nestle has developed a food-grade lycopene formulation that is bioavailable in humans. Called "lactolycopene", it is made by trapping lycopene with whey proteins. However, bioavailability of lycopene in lactolycopene is no higher than that of tomato paste. Lycopene crystallizes in aqueous solution and forms nanocrystals. Micelles provide a convenient, inexpensive, and nontoxic vehicle for dissolving and stabilizing as lycopene in tissue culture media and then delivering it to cells growing in culture. Nestle is researching this area for improving bioavailability of lycopene.

BioDelivery Sciences International has applied nanotechnology to food processing to encochleate sensitive and easily-degraded nutrients (beta carotene, anti-oxidants, and other) for addition to processed food and beverages. Nanoencochleation's all-natural process encochleates and preserves essential nutrients like anti-oxidants into a protected "shell" for in high-temperature/pressure canning and bottling applications.

Another consideration is absorption of minerals and other essential nutrient supplements. Reducing the size of low-solubility iron (Fe)-containing compounds to nanoscale has the potential to improve their bioavailability. Because Fe and zinc (Zn) deficiencies often coexist in populations, combined Fe/Zn-containing nanostructured compounds may be useful for nutritional applications (Hilty et al. 2009). Phosphates and oxides of Fe and atomically mixed Fe/Zn-containing (primarily ZnFe2O4) nanostructured powders were produced by flame spray pyrolysis. Solubility of the nanostructured compounds is dependent on their particle size. Nanostructured powders produce minimal color changes when added to dairy products containing chocolate or fruit compared to the changes produced when ferrous sulfate or ferrous fumarate are added to these foods. Flame-made Fe- and Fe/ Zn-containing nanostructured powders have solubilities comparable to ferrous and Zn sulfate but may produce fewer color changes when added to difficult-to-fortify foods. Therefore, these powders are promising for fortification of food and other nutritional applications.

Role of Nanobiotechnology in Personalized Nutrition

Nutrition plays a crucial role in health as well as disease. With advances in molecular biology, there is a shift in focus from epidemiology and biochemistry to an understanding of how nutrients act at molecular level. Advances in genomics have led to recognition of the importance of genes in human nutrition. Genetic predisposition is an important factor in mortality linked to diet such as cardiovascular disease. Technologies such as high-density microarrays enable the simultaneous study of the whole transcriptome relevant to nutrition. Advances in proteomic and metabolomic technologies will also enable the analysis of the whole system at proteomic and metabolomic levels as well. Introduction of nanotechnologies will further improve and enable practical personalization of nutrition.

References

- Boechat AL, de Oliveira CP, Tarragô AM, et al. Methotrexate-loaded lipid-core nanocapsules are highly effective in the control of inflammation in synovial cells and a chronic arthritis model. Int J Nanomedicine. 2015;10:6603–14.
- Cai K, Li J, Luo Z, et al. β-cyclodextrin conjugated magnetic nanoparticles for diazepam removal from blood. Chem Commun (Camb). 2011;47:7719–21.
- Chandrasekharan DK, Nair CK. Studies on silver nanoparticle–Glycyrrhizic acid complex as a radioprotector and an adjuvant in radiotherapy under in vivo conditions. Cancer Biother Radiopharm. 2012;27:642–51.
- Chen H, Clarkson BH, Sun K, Mansfield JF. Self-assembly of synthetic hydroxyapatite nanorods into an enamel prism-like structure. J Colloid Interface Sci. 2005;288:97–103.
- Chikramane PS, Suresh AK, Bellare JR, Kane SG. Extreme homeopathic dilutions retain starting materials: a nanoparticulate perspective. Homeopathy. 2010;99:231–42.
- De D, Mandal SM, Gauri SS, et al. Antibacterial effect of lanthanum calcium manganate (La0.67Ca0.33MnO3) nanoparticles against Pseudomonas Aeruginosa ATCC 27853. J Biomed Nanotechnol. 2010;6:138–44.
- Dixon MB, Falconet C, Ho L, et al. Removal of cyanobacterial metabolites by nanofiltration from two treated waters. J Hazard Mater. 2011;188:288–95.
- Esposito E, Drechsler M, Nastruzzi C, Cortesi R. Cubic phases, cubosomes and Ethosomes for cutaneous application. Curr Pharm Des. 2016;22:5382–99.
- Freitas Jr RA. Exploratory design in medical nanotechnology: a mechanical artificial red cell. Artif Cells Blood Substit Immobil Biotechnol. 1998;26:411–30.
- Gelfuso GM, Gratieri T, Simão PS, et al. Chitosan microparticles for sustaining the topical delivery of minoxidil sulphate. J Microencapsul. 2011;28:650–8.
- Hilty FM, Teleki A, Krumeich F, et al. Development and optimization of iron- and zinc-containing nanostructured powders for nutritional applications. Nanotechnology. 2009;20:475101.
- Hoshino Y, Koide H, Furuya K, et al. The rational design of a synthetic polymer nanoparticle that neutralizes a toxic peptide in vivo. Proc Natl Acad Sci U S A. 2012;109:33–8.
- Hu CM, Fang RH, Copp J, et al. A biomimetic nanosponge that absorbs pore-forming toxins. Nat Nanotechnol. 2013;8:336–40.
- Huq R, Samuel EL, Sikkema WK, et al. Preferential uptake of antioxidant carbon nanoparticles by T lymphocytes for immunomodulation. Sci Rep. 2016;6:33808.
- Kasuya T, Kuroda S. Nanoparticles for human liver-specific drug and gene delivery systems: in vitro and in vivo advances. Expert Opin Drug Deliv. 2009;6:39–52.
- Koo O, Rubinstein I, Önyüksel H. Actively targeted low-dose camptothecin as a safe, long-acting, disease-modifying nanomedicine for rheumatoid arthritis. Pharm Res. 2011;28:776–87.
- Koria P, Yagi H, Kitagawa Y, et al. Self-assembling elastin-like peptides growth factor chimeric nanoparticles for the treatment of chronic wounds. Proc Natl Acad Sci U S A. 2011;108:1034–9.
- Laroui H, Sitaraman SV, Merlin D. Gastrointestinal delivery of anti-inflammatory nanoparticles. Methods Enzymol. 2012;509:101–25.
- Lee DK, Kim SV, Limansubroto AN, et al. Nanodiamond-Gutta percha composite biomaterials for root canal therapy. ACS Nano. 2015;9:11490–501.

- Lee SS, Song W, Cho M, et al. Antioxidant properties of cerium oxide nanocrystals as a function of nanocrystal diameter and surface coating. ACS Nano. 2013;7:9693–703.
- Lewis SR, Datta S, Gui M, et al. Reactive nanostructured membranes for water purification. Proc Natl Acad Sci U S A. 2011;108:8577–82.
- Lohani A, Verma A, Joshi H, et al. Nanotechnology-based cosmeceuticals. ISRN Dermatol. 2014;2014:843687.
- Look M, Stern E, Wang QA, et al. Nanogel-based delivery of mycophenolic acid ameliorates systemic lupus erythematosus in mice. J Clin Invest. 2013;123:1741–9.
- Murugesan S, Mousa S, Vijayaraghavan A, et al. Ionic liquid-derived blood-compatible composite membranes for kidney dialysis. J Biomed Mater Res B Appl Biomater. 2006;79:298–304.
- Nogueira E, Gomes AC, Preto A, Cavaco-Paulo A. Folate-targeted nanoparticles for rheumatoid arthritis therapy. Nanomedicine. 2016;12:1113–26.
- O'Mary H, Del Rincón I, Cui Z. Nanomedicine for intra-articular drug delivery in rheumatoid arthritis. Curr Med Chem. 2016;23:2490–506.
- Prasad LK, O'Mary H, Cui Z. Nanomedicine delivers promising treatments for rheumatoid arthritis. Nanomedicine (Lond). 2015;10:2063–74.
- Roy K, Kanwar RK, Kanwar JR. Molecular targets in arthritis and recent trends in nanotherapy. Int J Nanomedicine. 2015;10:5407–20.
- Ryan JJ, Bateman HR, Stover A, et al. Fullerene nanomaterials inhibit the allergic response. J Immunol. 2007;179:665–72.
- Rzigalinski BA, Meehan K, Davis RM, et al. Radical nanomedicine. Nanomedicine. 2006;1: 399–412.
- Schubert D, Dargusch R, Raitano J, Chan S. Cerium and yttrium oxide nanoparticles are neuroprotective. Biochem Biophys Res Commun. 2006;342:86–91.
- Tang W, Li Q, Gao S, Shang JK. Arsenic (III,V) removal from aqueous solution by ultrafine α -Fe2O3 nanoparticles synthesized from solvent thermal method. J Hazard Mater. 2011;192:131–8.
- Wei G, Bhushan B, Torgerson PM, et al. Nanomechanical characterization of human hair using nanoindentation and SEM. Ultramicroscopy. 2005;105:248–66.
- Yamagishi K, Onuma K, Suzuki T, Okada F, Tagami J, Otsuki M, Senawangse P. Materials chemistry: a synthetic enamel for rapid tooth repair. Nature. 2005;433:819.
- Yang HY, Han ZJ, Yu SF, et al. Carbon nanotube membranes with ultrahigh specific adsorption capacity for water desalination and purification. Nat Commun. 2013;4:2220.
- Zhang M, Viennois E, Prasad M, et al. Edible ginger-derived nanoparticles: a novel therapeutic approach for the prevention and treatment of inflammatory bowel disease and colitis-associated cancer. Biomaterials. 2016;101:321–40.
- Zhang M, Xie X, Tang M, et al. Magnetically ultraresponsive nanoscavengers for next-generation water purification systems. Nat Commun. 2013;4:1866.

Chapter 16 Nanobiotechnology and Personalized Medicine

Introduction

Personalized medicine simply means the prescription of specific therapeutics best suited for an individual. It is usually based on pharmacogenetic, pharmacogenomic, transcriptomic, pharmacoproteomic and pharmacometabolomic information. Other individual variations in patients and environmental factors are also taken into consideration (Jain 2015). Personalized medicine means improving healthcare by incorporating early detection of disease, preventive medicine, rational drug discovery and development, and monitoring of therapy. Concept of personalized medicine as systems medicine is the best way of integrating new technologies and translating them into clinical application for improving healthcare. Application of nanobiotechnology is described for personalized management of cancer and cardiovascular disorders. Advances in nanobiotechnology will facilitate the development of personalized medicine by:

- Nanodiagnostics will improve the sensitivity and extend the present limits of molecular diagnostics/molecular imaging of CNS disorders.
- Nanotechnology can be integrated in detection of biomarkers, POC devices, biochips and biosensors.
- Biomarkers discovered by use of nanodiagnostics will facilitate the development of new personalized drugs for various disorders.
- Nanobiotechnology will facilitate integration of diagnosis and therapy, which is an important part personalized medicine.

Figure 16.1 shows the broad scope and interrelationships of personalized medicine.

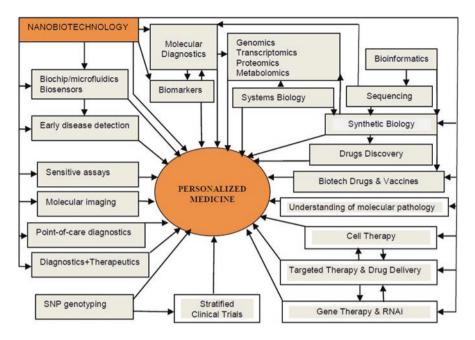


Fig. 16.1 Relationship of nanobiotechnology to personalized medicine (© Jain PharmaBiotech)

Role of Nanobiotechnology in Personalized Management of Cancer

In case of cancer the variation in behavior of cancer of the same histological type from one patient to another is also taken into consideration in addition to variations among patients. Personalization of cancer therapies is based on a better understanding of the disease at the molecular level and nanotechnology will play an important role in this area. Various components of personalized therapy of cancer that are relevant to nanobiotechnology are shown in Fig. 16.2.

Nanobiotechnology, by enabling early detection of cancer, refinement of cancer diagnosis and monitoring of cancer therapy will contribute to the development of personalized therapy of cancer (Jain 2012). Nanobiotechnology will facilitate combination of diagnostics with therapeutics, which will be useful for personalized oncology.

QDs, which play an important role in cancer diagnosis, drug delivery, and monitoring of therapy in combination with cancer biomarkers, will provide useful tools for personalizing cancer therapy. Flexible surface chemistry, unique optical properties, high sensitivity, and multiplexing capabilities of QDs certainly make them a most promising tool for personalized medicine (Tripathi et al. 2015). Patient-specific customized therapeutic strategies can be engineered using exosomes derived from the patient's own healthy cells, and has the potential to become an important part of personalized cancer therapy (Srivastava et al. 2016).

How nanoparticle size, shape, and surface chemistry can affect their accumulation, retention, and penetration in tumors is being actively investigated, because such findings

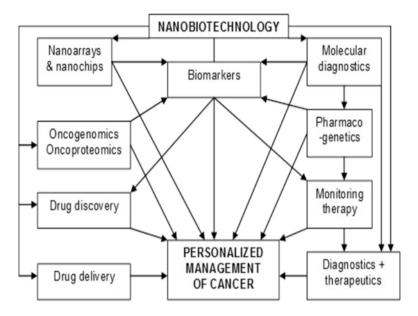


Fig. 16.2 Role of nanobiotechnology in personalized management of cancer (© Jain PharmaBiotech)

provide guiding principles for engineering optimal nanosystems for tumor targeting. The experimental focus has been on particle design and not on the biological system. A study has varied tumor volume to determine whether cancer pathophysiology can influence tumor accumulation and penetration of different sized nanoparticles (Sykes et al. 2016). Monte Carlo simulations were used to model the process of nanoparticle accumulation. The authors discovered that changes in pathophysiology associated with tumor volume can selectively change tumor uptake of nanoparticles of varying size. They further determined that nanoparticle retention within tumors depends on the frequency of interaction of particles with the perivascular extracellular matrix for smaller nanoparticles, whereas transport of larger nanomaterials is dominated by Brownian motion. This finding presents a paradigm shift in nanomedicine away from identifying and using a universal nanoparticle design for cancer detection and treatment. Rather, these results suggest that in the future it will be possible to tailor the design of nanoparticles to the patient's tumor characteristics. This concept of "personalized nanomedicine" was tested for detection of prostate tumors and was successfully demonstrated to improve nanoparticle targeting by over 50%.

Nanotechnology-Based Personalized Medicine for Cardiology

The future of cardiovascular diagnosis already is being impacted by nanosystems that can both diagnose pathology and treat it with targeted delivery systems. The potential dual use of nanoparticles for both imaging and site-targeted delivery of therapeutic agents to cardiovascular disease offers great promise for individualizing therapeutics. Image-based therapeutics with site-selective agents should enable verification that the drug is reaching the intended target and a molecular effect is occurring. Experimental studies have shown that binding of paclitaxel to smooth muscle cells in culture has no effect in altering the growth characteristics of the cells. If paclitaxel-loaded nanoparticles are applied to the cells, however, specific binding elicits a substantial reduction in smooth muscle cell proliferation, indicating that selective targeting may be a requirement for effective drug delivery for in this situation. Similar behavior has been demonstrated for doxorubicin containing particles. Intravenous delivery of fumagillin (an antiangiogenic agent)-loaded nanoparticles targeted to ανβ3-integrin epitopes on vasa vasorum in growing plaques results in marked inhibition of plaque angiogenesis in cholesterol fed rabbits. The unique mechanism of drug delivery for highly lipophilic agents such as paclitaxel contained within emulsions depends on close apposition between the nanoparticle carrier and the targeted cell membrane and has been described as "contact facilitated drug delivery." In contrast to liposomal drug delivery (generally requiring endocytosis), the mechanism of drug transport in this case involves lipid exchange or lipid mixing between the emulsion vesicle and the targeted cell membrane, which depends on the extent and frequency of contact between two lipidic surfaces. The rate of lipid exchange and drug delivery can be greatly increased by the application of clinically safe levels of ultrasound energy that increase the propensity for fusion or enhanced contact between the nanoparticles and the targeted cell membrane.

The combination of targeted drug delivery and molecular imaging with MRI has the potential to enable serial characterization of the molecular epitope expression based on imaging readouts. Monitoring and confirmation of therapeutic efficacy of the therapeutic agents at the targeted site would permit personalized medical regimens.

Nanobiotechnology for Therapeutics Design and Monitoring

Current therapeutic design involves combinatorial chemistry and system biologybased molecular synthesis and bulk pharmacological assays. Therapeutics delivery is usually non-specific to disease targets and requires excessive dosage. Efficient therapeutic discovery and delivery would require molecular level understanding of the therapeutics-effectors (e.g. channels and receptors) interactions and their cell and tissue responses. A multidimensional nanobiotechnology-based approach to personalized medicine starts with scanning probe techniques, especially AFM to identify potential targets for drug discovery (Lal and Arnsdorf 2010). AFM can be integrated with nanocarriers and implantable vehicles for controlled delivery. Characterization of nanocarrier-based drug delivery can enable high efficiency of in vivo or topical administration of a small dosage of therapeutics. High-throughput parallel nanosensors, comprising integrated cantilevered microarrays, total internal reflection fluorescence (TIRF) microscopy, microfluidics and nanoelectronics, can be used for rapid diagnosis of diseases, detection of biomarkers as well as for therapeutics design. Therapeutic efficacy can be assessed by monitoring biomechanics.

Smart Nanosystems for Personalized Medicine

Nantechnologies intended for human clinical applications need to be designed to interact with a living host environment. Smart nanosystems have been described and classified in two categories (Kwon et al. 2015): (1) those that sense the host environment and respond; and (2) those that first prime the host environment to interact with engineered nanoparticles. Smart nanosystems have the potential for designing personalized diagnostic and therapeutic approaches by using the local environment to drive material behavior and ultimately improve human health.

Nanosystems That Respond to Disease Environments

There are several alterations of biochemical properties (redox potential, pH, enzymatic activity, homeostatic pathways) in disease, and response to these could be the basis of nanosystems for managing these as shown in Table 16.1.

Local/disease environment	Nanosystem behavior/ properties	Nanosystem effect/reference	
Redox responsive		· · ·	
Reduced cytosol	Disulfide cleavage	siRNA release (Singh et al. 2010)	
Redox state of organs	Paramagnetic nitroxide reduction	MRI-NIR switching in oxidative-reductive environment (Sowers et al. 2014)	
pH responsive			
Decreased pH in tumor environment	Conformational change	Release of cargo in tumor environment	
Decreased pH of endolysosome	Conformational change	Membrane disruption and release of payload into cytosol (Berguig et al. 2015)	
Enzyme responsive			
Atherosclerosis	Protein cleavage of disease-specific substrates	NIR signal at site of disease (Jaffer et al. 2009).	
Fibrosis, tumors	Protein cleavage of disease-specific substrates	Release of synthetic biomarkers (Warren et al. 2014)	
Homeostatic			
Diabetes	Glucose competition	Insulin release in presence of glucose (Veiseh et al. 2015).	
Clotting	Cross linking of fibrin clots	Engineered hemostatic polymer (PolySTAT) circulates innocuously in the blood, identifies sites of vascular injury, and promotes clot formation to stop bleeding (Chan et al. 2015)	

 Table 16.1 Examples of nanosystems that respond to disease environments

References

- Berguig GY, Convertine AJ, Frayo S. Intracellular delivery system for antibody-peptide drug conjugates. Mol Ther. 2015;23:907–17.
- Chan LW, Wang X, Wei H. A synthetic fibrin cross-linking polymer for modulating clot properties and inducing hemostasis. Sci Transl Med. 2015;7:277ra29.
- Jaffer FA, Libby P, Weissleder R. Optical and multimodality molecular imaging: insights into atherosclerosis. Arterioscler Thromb Vasc Biol. 2009;29:1017–24.
- Jain KK. Role of nanodiagnostics in personalized cancer therapy. Clin Lab Med. 2012;32:15-31.
- Jain KK. Textbook of personalized medicine. 2nd ed. New York: Springer; 2015.
- Kwon EJ, Lo JH, Bhatia SN. Smart nanosystems: bio-inspired technologies that interact with the host environment. Proc Natl Acad Sci U S A. 2015;112:14460–6.
- Lal R, Arnsdorf MF. Multidimensional atomic force microscopy for drug discovery: a versatile tool for defining targets, designing therapeutics and monitoring their efficacy. Life Sci. 2010;86:545–62.
- Singh N, Agrawal A, Leung AK, et al. Effect of nanoparticle conjugation on gene silencing by RNA interference. J Am Chem Soc. 2010;132:8241–3.
- Sowers MA, McCombs J, Wang Y, et al. Redox-responsive branched-bottlebrush polymers for in vivo MRI and fluorescence imaging. Nat Commun. 2014;5:5460.
- Srivastava A, Babu A, Filant J, et al. Exploitation of exosomes as nanocarriers for gene-, chemo-, and immune-therapy of cancer. J Biomed Nanotechnol. 2016;12:1159–73.
- Sykes EA, Dai Q, Sarsons CD, et al. Tailoring nanoparticle designs to target cancer based on tumor pathophysiology. Proc Natl Acad Sci U S A. 2016;113:E1142–51.
- Tripathi SK, Kaur G, Khurana RK, et al. Quantum dots and their potential role in cancer theranostics. Crit Rev Ther Drug Carrier Syst. 2015;32:461–502.
- Veiseh O, Tang BC, Whitehead KA, et al. Managing diabetes with nanomedicine: challenges and opportunities. Nat Rev Drug Discov. 2015;14:45–57.
- Warren AD, Gaylord ST, Ngan KC, et al. Disease detection by ultrasensitive quantification of microdosed synthetic urinary biomarkers. J Am Chem Soc. 2014;136:13709–14.

Chapter 17 Nanotoxicology

Introduction

Toxicology is the branch of medicine that deals with the study of the adverse effects of chemicals and biological agents on the human body. It is the study of symptoms, mechanisms, treatments and detection of poisoning. The broad scope of toxicology covers not only the adverse effects of therapeutics but also environmental agents and poisons. Nanotoxicology covers safety issues relevant to nanomaterials.

The success of nanomaterials is due to their small size, which enables us to deliver them into parts of the body where usual inorganic materials cannot enter because of their large particle size. There is an enormous advantage in drug delivery systems or cancer therapeutics. Current research is trying to find simple ways to control the degree of a particle's toxicity. This control means that the particle will be toxic only under certain desirable circumstances, such as for curing cancer. This also raises questions about unintentional effects of such powerful agents on the human body. This, however, would not be an issue for the use of nanoparticles for in vitro diagnostics.

Effects of particles on human health have been studied by toxicologists previously. Effects of larger particles generated by wearing down of implants in the body and aerosolized particles of all sizes on have been studied. However, there is little information on health impacts of very small, nano-engineered particles under 20 nm. The main concern will be about particles less than 50 nm, which can enter the cells. There are still many unanswered questions about their fate in the living body. Of the >150,000 publications dealing with nanotechnology, <1% deal with their toxicity. Because of the huge diversity of materials used and the wide range in size of nanoparticles, these effects will vary a lot. It is conceivable that certain sizes of some materials may turn out to have toxic effects. At this stage, no categorical statement can be made about the safety of nanoparticles, i.e. one cannot say that nanoparticles are entirely safe or that they are dangerous. Further investigations will be needed.

Fate of Nanoparticles in the Human Body

The biological impacts of nanoparticles are dependent on size, chemical composition, surface structure, solubility, shape, and aggregation. These parameters can modify cellular uptake, protein binding, translocation from portal of entry to the target site, and the possibility of causing tissue injury. Effects of nanoparticles depend on the routes of exposure that include gastrointestinal tract, skin, lung, and systemic administration for diagnostic and therapeutic purposes. Nanoparticles interactions with cells, body fluids, and proteins play a role in their biological effects and ability to distribute throughout the body. Nanoparticle binding to proteins may generate complexes that are more mobile and can enter tissue sites that are normally inaccessible. Accelerated protein denaturation or degradation on the nanoparticle surface may lead to functional and structural changes, including interference in enzyme function. Nanoparticles also encounter several defenses that can eliminate, sequester, or dissolve them.

Safety data is available from in vitro tests of various nanoparticles, which can be extrapolated to predict in vivo effects. However, engineered nanomaterials with novel physicochemical properties require in vivo studies of their interactions at the nano/bio interface for detection of any harmful effects. An understanding of these interactions including the physicochemical properties that control bioavailability is required to understand how material properties influence uptake, transport and fate as well as the biological consequences of these is at cellular level. The mechanisms of toxicity of different engineered nanomaterials differ according to size and surface, which directly correlate with their physicochemical activities in vivo (Zhu et al. 2013). This knowledge can be used for safer nanomaterial design.

In Vitro Testing for Toxicity of Nanoparticles

Screening nanomaterials by means of in vitro studies has been suggested as a fast and economical approach to distinguish between low and high toxicity nanomaterials. However, to maximize the use of in vitro assays for this purpose, their values and limitations need to be revealed. Even in risk assessment frameworks for regular chemicals, in vitro studies play a minor role. A comparative analysis of published in vitro data with nanomaterials demonstrates that there are several issues that need resolving before in vitro studies can play a role in the risk assessment of nanomaterials (Park et al. 2009). A major limitation of in vitro assays is that the exposure and dispersion methods most often used do not adequately reflect the exposure as it occurs in vivo. As more in vivo studies with nanomaterials become available, the values and limitations of in vitro studies as predictive tools in risk assessment of nanomaterials will come to light. Over the next 10 years, a balance will be sought between decreasing the use of in vivo studies by replacing them with in vitro studies and reliably predicting the risks of nanomaterials.

Stem Cell Lines for Testing Toxicity of Nanoparticles

A mouse spermatogonial stem cell line has been used as a model to assess nanotoxicity in the male germ line in vitro (Braydich-Stolle et al. 2005). The effects of different types of nanoparticles on these cells were evaluated using light microscopy, cell proliferation and standard cytotoxicity assays. The results demonstrated a concentration-dependent toxicity for all types of particles tested, while the corresponding soluble salts had no significant effect. Silver nanoparticles were the most toxic while MoO3 nanoparticles were the least toxic. These results suggest that this cell line provides a valuable model to assess the cytotoxicity of nanoparticles in the germ line in vitro.

Experiments have been conducted to test silica, silica/iron oxide, and gold nanoparticles for their effects on the growth and activity of *E. coli* (Williams et al. 2006). TEM and dynamic light scattering were used to characterize the morphology and quantify size distribution of the nanoparticles, respectively. TEM was also used to verify the interactions between composite iron oxide nanoparticles and *E. coli*. The results from DLS indicated that the inorganic nanoparticles formed small aggregates in the growth media. Growth studies measured the influence of the nanoparticles on cell proliferation at various concentrations, showing that the growth of *E. coli* in media containing the nanoparticles indicated no overt signs of toxicity. Although the in vitro study has its limitations, it does indicate the relative safety of the nanoparticles tested under certain conditions.

Variations in Safety Issues of Different Nanoparticles

Carbon Nanotube Safety

In contrast to the use of nanoparticles, the use of carbon nanotubes (CNTs) in life sciences is more recent. Toxicity of MWCNTs, carbon nanofibers, and carbon nanoparticles was tested in vitro on lung tumor cells and clearly showed that these materials are toxic while the hazardous effect was size-dependent (Magrez et al. 2006). Moreover, cytotoxicity is enhanced when the surface of the particles is functionalized after an acid treatment.

Similarity between asbestos and CNTs in terms of physicochemical properties and their responses in in vitro genotoxicity tests, has led to concern about potential CNT-elicited genotoxicity. Generation of reactive oxygen species (ROS) is a crucial driving mechanism of toxic effects attributed to particles and fibers including asbestos. Although there are clear similarities between asbestos fibers and CNTs regarding their dimensions, biopersistence and aspect ratio, there appears to be a marked difference in their ROS-generating potential. Several CNTs have ROS-quenching action and are novel antioxidants. The toxic potential of CNTs has been linked to the presence of structural defects, which may also possibly drive their scavenging activity. In view of inconsistent findings reported in various studies, no definite statement can be made at present regarding the actual hazard of CNTs. The challenge for future research will be to address genotoxic effects of CNT in controlled experimental settings and selection of an appropriate dose range based on available human exposure data (van Berlo et al. 2012). Testing should also consider an extensive characterization of the CNTs under the applied assay conditions, and aim to identificy underlying mechanism of action.

Water-soluble, single-walled CNTs (SWCNTs) have been functionalized with the chelating molecule diethylentriaminepentaacetic (DTPA) and labeled with indium (¹¹¹In) for imaging purposes (Singh et al. 2006). Intravenous administration of these functionalized SWCNTs (f-SWCNTs) followed by radioactivity tracing using gamma scintigraphy indicated that f-SWCNTs are not retained in any of the reticuloendothelial system organs (liver or spleen) and are rapidly cleared from systemic blood circulation through the renal excretion route. The observed rapid blood clearance and half-life (3 h) of f-SWCNTs has major implications for all potential clinical uses. Moreover, urine excretion studies using both f-SWCNT and functionalized multiwalled CNT followed by electron microscopy analysis of urine samples revealed that both types of nanotubes were excreted as intact nanotubes. The next step for this research is to prolong the blood circulation of CNTs to give them enough time before excretion to get to a target tissue. The researchers are also considering pharmaceutical development of functionalized CNTs for drug delivery.

In one study, carbon nanoparticles including CNTs, except C60 fullerenes, stimulated platelet aggregation and accelerated the rate of vascular thrombosis in rat carotid arteries (Radomski et al. 2005). All particles resulted in upregulation of GPIIb/IIIa in platelets. In contrast, particles differentially affected the release of platelet granules, as well as the activity of thromboxane-, ADP, matrix metalloproteinase- and protein kinase C-dependent pathways of aggregation. Furthermore, particle-induced aggregation was inhibited by prostacyclin and S-nitroso-glutathione, but not by aspirin. Thus, some carbon nanoparticles can activate platelets and enhance vascular thrombosis. These observations are of importance for the pharmacological use of CNTs and support the safety of C60 fullerenes.

Manufactured SWCNT usually contain significant amounts of iron as impurities that may act as a catalyst of oxidative stress. Because macrophages are the primary responders to different particles that initiate and propagate inflammatory reactions and oxidative stress, interaction of SWCNT (0.23 wt % of iron) with macrophages has been studied (Kagan et al. 2006). Non-purified SWCNT more effectively converted superoxide radicals generated by xanthine oxidase/xanthine into hydroxyl radicals as compared to purified SWCNT. Iron-rich SWCNT caused significant loss of intracellular low molecular weight thiols (GSH) and accumulation of lipid hydroperoxides in macrophages. Catalase could partially protect macrophages against SWCNT-induced elevation of biomarkers of oxidative stress (enhancement of lipid peroxidation and GSH depletion). Thus, the presence of iron in SWCNT may be important in determining redox-dependent responses of macrophages.

Raman spectroscopic signatures of SWCNTs were measured following intravenous injection in mice (Liu et al. 2008). SWCNTs were detected in various organs and tissues over a period of 3 months. Functionalization of SWCNTs by branched PEG chains prolonged their blood circulation up to 1 day, reduced uptake in the reticuloendothelial system, and near-complete clearance from the main organs in ~2 months. Raman spectroscopy detected SWCNT in the intestine, feces, kidney, and the bladder, suggesting excretion and clearance via the biliary and renal pathways. No toxic side effect of SWCNTs to mice was observed at necropsy, histology, and blood chemistry. These findings clear the way to future biomedical applications of SWCNTs.

Fullerene Toxicity

Recent toxicology studies suggest that nanosized aggregates of fullerene molecules can enter cells and alter their functions, and cross the BBB. Computer simulations have been used to explore the translocation of fullerene clusters through a model lipid membrane and the effect of high fullerene concentrations on membrane properties (Wong-Ekkabut et al. 2008). The fullerene molecules rapidly aggregate in water but disaggregate after entering the membrane interior. The permeation of a solid-like fullerene aggregate into the lipid bilayer is thermodynamically favored and occurs on the microsecond timescale. High concentrations of fullerene induce changes in the structural and elastic properties of the lipid bilayer, but these are not large enough to mechanically damage the membrane. These results suggest that mechanical damage is an unlikely mechanism for membrane disruption and fullerene toxicity.

Gold Nanoparticle Toxicity

Toxicity has been observed at high concentrations using gold nanoparticles (AuNPs). Cationic AuNPs are moderately toxic, whereas anionic AuNPs are nontoxic. Concentration-dependent lysis mediated by initial electrostatic binding has been observed in dye release studies using lipid vesicles, providing the probable mechanism for observed toxicity with the cationic AuNPs.

Relation of duration of exposure to toxic effect of AuNPs on human cells has been studied. A study has report the in vitro long-term (20 week) changes in cells exposed to well-characterized AuNPs with varying shapes and surface coatings under both chronic exposure (>20 week) and acute exposure (Falagan-Lotsch et al. 2016). Both chronic and acute AuNPs exposures at low dose induce modifications at the gene level after long periods. In attempt to overcome from the injuries caused by nanoparticle exposure, genes related to oxidative stress, cell cycle regulation, and inflammation are among those presenting differential expression levels. Acute exposure induced more gene expression changes than its chronic counterpart and the stress effects caused by this type of exposure were sustained even after 20 week without any additional AuNP exposure. AuNP surface chemistry played an important role in the alteration of gene regulation. Overall, it was found that an acute burst of exposure is more harmful to cells, and that cells can adapt to long-term nanoparticle exposure.

Graphene Toxicity

The toxicity of graphene has been extensively debated in the literature. The most comprehensive review on graphene toxicity published by exclusively summarizes the in vitro, in vivo, antimicrobial and environmental effects and highlights the various mechanisms of graphene toxicity (Lalwani et al. 2016). Results show that the toxicity of graphene is dependent on several factors such as shape, size, purity, post-production processing steps, oxidative state, functional groups, dispersion state, synthesis methods, route and dose of administration, and exposure times. Graphene nanoribbons, graphene nanoplatelets and graphene nano–onions are non-toxic at concentrations up to 50 μ g/ml. These nanoparticles do not alter the differentiation of human bone marrow stem cells towards osteoblasts or adipocytes suggesting that at low doses graphene nanoparticles are safe for biomedical applications (Talukdar et al. 2014).

Quantum Dot Safety Issues

To increase the stability, QDs are made from cadmium selenide (CdSe) and zinc sulfide for use as fluorescent labels. These QDs may release potentially toxic cadmium and zinc ions into cells. While cytotoxicity of bulk CdSe is well documented, CdSe QDs are generally cytocompatible, at least with some immortalized cell lines. Using primary hepatocytes as a liver model, CdSe-core QDs were found to be acutely toxic under certain conditions (Derfus et al. 2004). Although previous in vitro studies had not shown significant toxicity as the cell line used in these studies were not sensitive to heavy metals or the exposed to short-time QD labeling. The authors found that the cytotoxicity of QDs was modulated by processing parameters during synthesis, exposure to ultraviolet light, and surface coatings. These data further suggest that cytotoxicity correlates with the liberation of free Cd2+ ions due to deterioration of the CdSe lattice. When appropriately coated, CdSe-core QDs can be rendered nontoxic and used to track cell migration and reorganization in vitro. These results provide information for design criteria for the use of QDs in vitro and especially in vivo, where deterioration over time may occur. Capping QDs with ZnO effectively prevented Cd²⁺ formation upon exposure to air but not to ultraviolet radiation and attempts have continued to find better coating materials.

To solve this problem, Scientists at the US Department of Energy's Lawrence Berkeley National Laboratory, have coated QDs with a protective layer of PEG, which is a very nonreactive and stable compound that is used extensively by the pharmaceutical industry in drug formulation. This layer is designed to prevent the dots from leaking heavy metal ions into cells once they are inside. The tool used test the safety of QDs is a gene chip packed with 18,400 probes of known human genes and it is a comprehensive method to measure the toxicity of nanoscale particles. This chip is designed to enable the researchers to expose the human genome QDs, and determine the extent to which the compound forces the genes to express themselves abnormally.

A high-throughput gene expression test determined that specially coated QD fluorescent nanoprobes affect only 0.2% of the human genome, dispelling the concern that the mere presence of these potentially toxic sentinels disrupts a cell's function (Zhang et al. 2006). The number of genes affected is very small given the large dose of QDs used in the study, which is up to 1000 times greater than the dose that would typically be used in human applications. Moreover, the affected genes are not related to heavy metal exposure, which would be the case if the cells had been exposed to cadmium or zinc ions. Because of their protective coating, QDs have minimal impact on cells; the only gene changes are in transporter proteins, which are expected because the dots must be transported into and within the cell.

Skin penetration is one of the major routes of exposure for nanoparticles to gain access to a biological system. Biological interactions of QD nanoparticles with skin have been studied. QD621 are nail-shaped nanoparticles that contain a cadmium/ selenide core with a cadmium sulfide shell coated with PEG and are soluble in water. QD were topically applied to porcine skin flow-through diffusion cells to assess penetration, which was found to be minimal and limited primarily to the outer stratum corneum layers (Zhang et al. 2008). QD655 and QD565, coated with carboxylic acid, were studied for 8 and 24 h in flow-through diffusion cells with flexed, tape-stripped and abraded rat skin to determine if these mechanical actions could perturb the barrier and affect penetration (Zhang and Monteiro-Riviere 2008). Barrier perturbation by tape stripping did not cause penetration, but abrasion allowed QD to penetrate deeper into the dermal layers. While the study shows that QDs of different sizes, shapes and surface coatings do not penetrate rat skin unless there is an abrasion, it shows that even minor cuts or scratches could potentially allow these nanoparticles to penetrate deep into the viable dermal layer - or living part of the skin - and potentially reach the bloodstream. These findings indicate safety concerns for workers handling QDs.

Effects of Nanoparticles on Various Body Systems

A kinetic study was performed to determine the influence of particle size on the in vivo tissue distribution of spherical-shaped gold nanoparticles in the rat (De Jong et al. 2008). For all sizes of gold nanoparticles most the gold was demonstrated to be present in liver and spleen. A clear difference was observed between the distribution of the 10 nm particles and the larger particles. The 10 nm particles were present in various organ systems including blood, liver, spleen, kidney, testis, thymus, heart,

lung and brain, whereas the larger particles were only detected in blood, liver and spleen. The results demonstrate that tissue distribution of gold nanoparticles is size-dependent with the smallest 10 nm nanoparticles showing the most widespread organ distribution.

Smaller particles apparently circulate for much longer and can cross the BBB to lodge in the brain. They can leak out of capillaries and get into the fluids between cells. They can go to places in the body that an average inorganic mineral cannot. Such effects may not be a concern in case of targeted delivery of nanoparticle-based therapy in cancer. The eventual decision to use nanoparticle-based therapy may depend on a risk-versus-benefit assessment.

Pulmonary Effects of Nanoparticles

Modern humans breathe in considerable numbers of nanoparticles daily in traffic fumes and even from cooking. Nanoparticles are used increasingly in industrial processes and have been hypothesized to be an important contributing factor in the toxicity and adverse health effects of particulate air pollution.

Following inhalation, ultrafine and fine particles can penetrate through the different tissue compartments of the lungs and eventually reach the capillaries and circulating cells or constituents, e.g. erythrocytes. These particles are then translocated by the circulation to other organs including the liver, the spleen, the kidneys, the heart and the brain, where they may be deposited. In one study, a series of NIR fluorescent nanoparticles were systematically varied in chemical composition, shape, size and surface charge, and their biodistribution and elimination were quantified in rat models after lung instillation (Choi et al. 2010). Nanoparticles with hydrodynamic diameter <34 nm and a noncationic surface charge translocate rapidly from the lung to mediastinal lymph nodes. Nanoparticles of <6 nm can traffic rapidly from the lungs to lymph nodes and the bloodstream, and are subsequently cleared by the kidneys.

Since the lung is the main portal of entry into the human body for nanomaterials released within the environment, it is important to understand how nanomaterials interact with the respiratory tract. Small size, a large surface area, and an ability to generate reactive oxygen species play a role in the ability of nanoparticles to induce lung injury. In some individuals, they can trigger asthma by setting off an inflammatory response from the body's immune system. In one study, rats were instilled with fine and ultra-fine carbon black and titanium dioxide (Renwick et al. 2004). Ultra-fine particles induced more polymorphonuclear recruitment, epithelial damage, and cytotoxicity than their fine counterparts, exposed at equal mass. Both ultra-fine and fine particles significantly impaired the phagocytic ability of alveolar macrophages. Only ultra-fine particle treatment significantly enhanced the sensitivity of alveolar macrophages to chemotact towards C5a. It was concluded that ultrafine particles of two very different materials induced inflammation and epithelial damage more than their fine counterparts. In general, the effect of ultra-fine carbon black was greater

than ultra-fine titanium dioxide, suggesting that there are differences in the likely harmfulness of different types of ultra-fine particles. Epithelial injury and toxicity were associated with the development of inflammation after exposure to ultra fines. Increased sensitivity to a C5a chemotactic gradient could make the ultra-fine exposed macrophages more likely to be retained in the lungs, so allowing dose to accumulate.

The experience of researchers at DuPont, who tested CNTs, was different (Warheit et al. 2004). When the researchers injected CNTs into the lungs of rats, the animals unexpectedly began gasping for breath and 15% of them quickly died. Yet surprisingly, all the surviving rats seemed completely normal within 24 h. What initially looked like disaster pointed to a possible safety feature: the CNTs' tendency to clump rapidly led to suffocation for some rats exposed to huge doses, but it also kept most tubes from reaching deep regions of the lung where they could not be expelled by coughing and could cause long-term damage. Now researchers see the clumping of CNTs and other nanomaterials as a new field for inquiry. Other findings of Dupont scientists were:

- Exposures to quartz particles produced significant increases versus controls in pulmonary inflammation, cytotoxicity, and lung cell parenchymal cell proliferation indices.
- Exposures to carbon nanotubes produced transient inflammatory and cell injury effects. They produced a non-dose-dependent series of multifocal granulomas, which were evidence of a foreign tissue body reaction and were nonuniform in distribution and not progressive beyond 1 month following exposure.

In further studies, DuPont scientists observed that exposures to the various alphaquartz particles produced differential degrees of pulmonary inflammation and cytotoxicity, which were not always consistent with particle size. The results of their studies demonstrate that the pulmonary toxicities of alpha-quartz particles appear to correlate better with surface activity than particle size and surface area (Warheit et al. 2007).

Polyamidoamine (PAMAM) dendrimer can induce acute lung injury in vivo as it triggers autophagic cell death by deregulating the Akt-TSC2-mTOR signaling pathway. The autophagy inhibitor 3-methyladenine was shown to rescue PAMAM-induced cell death and ameliorate acute lung injury caused by PAMAM in mice (Li et al. 2009).

It has been suggested that the nanoparticulate component of 10 μ M (PM10) is capable of translocating into the circulation with the potential for direct effects on the vasculature and is a potential risk factor for cardiovascular disease. A study was conducted in healthy volunteers to determine the extent to which inhaled technetium-99 m (99mTc) labeled CNTs (Technegas), were able to access the systemic circulation (Mills et al. 2006). Technegas particles were 4–20 nm in diameter and aggregated to a median particle diameter of ~100 nm. Radioactivity was immediately detected in blood, with levels increasing over 60 min. Thin layer chromatography of whole blood identified a species that moved with the solvent front, corresponding to unbound 99mTc-pertechnetate, which was excreted in urine. There was no evidence of particle-bound 99mTc at the origin. Gamma camera images demonstrated high levels of Technegas retention in the lungs, with no accumulation of radioactivity detected over the liver or spleen. Thus, most of 99mTc-labelled carbon nanoparticles remain within the lung up to 6 h after inhalation. In contrast to previous published studies, thin layer chromatography did not support the hypothesis that inhaled Technegas carbon nanoparticles pass directly from the lungs into the systemic circulation. An excellent review has concluded that further research is required to understand the potential adverse effects of nanomaterials on the respiratory tract and, via systemic distribution, on the human body in general (Jud et al. 2013). Meanwhile researchers and workers should take all possible precautions to minimize their exposure to nanomaterials until their specific hazard potential has been clarified.

The physiological relevance of various findings should ultimately be determined by conducting an inhalation toxicity study. No one has created a realistic test for the effects of inhaled nanoparticles so far; such a test could easily cost more than \$1 million to design and carry out. Some studies have been planned to study any possible adverse effects of nanoparticles on the lungs. One of those studies is a multiyear project led by the US National Institute of Environmental Health Sciences that will examine the potential toxic and carcinogenic effects of inhalation exposure to nanomaterials.

Neuronanotoxicology

Neuronanotoxicology is the study of potential toxic effects of nanoparticles on the nervous system. The concern has arisen because nanoparticles can cross the BBB to enter the brain following introduction into the systemic circulation and are not cleared out. The effect depends on the type of nanoparticle introduced as some are neuroprotective whereas others are neurotoxic.

Nanoparticle Deposits in the Brain

Passage of nanoparticles across the BBB to enter the brain has already been documented. There is a possible risk in inhaling nanoparticles that are so small that they can slip through membranes inside the lungs, enter systemic circulation and lodge in the brain. Research on rats has shown nanoparticles deposited in the nose can migrate to the brain and move from the lungs into the bloodstream. They can also change shape as they move from liquid solutions to the air, making it harder to draw general conclusions about their potential impact on living things. More experiments are needed to establish the impact of nanoparticles on the brain if they remain there.

Fullerenes (buckyballs) are lipophilic and localize into lipid-rich regions such as cell membranes in vitro, and they are redox active. Other nanosize particles and soluble metals have been shown to selectively translocate into the brain via the olfactory bulb in mammals and fish. A preliminary study found rates of brain damage

17 times higher in largemouth bass exposed to a form of water-soluble buckyballs than unexposed fish (Oberdorster 2004). Significant lipid peroxidation was found in brains of largemouth bass after 48 h of exposure to 0.5 ppm uncoated nano-C60. Buckyballs are also toxic in vitro, causing 50% of the cultured human cells to die at a concentration of 20 parts per billion (Sayes et al. 2004). With the addition of an antioxidant, l-ascorbic acid, the oxidative damage and resultant toxicity of nano-C60 was completely prevented (Sayes et al. 2005).

Nanoparticles and Neurodegeneration

There is the potential for neurodegenerative consequence of nanoparticle entry to the brain. Histological evidence of neurodegeneration has been reported in both canine and human brains exposed to high ambient particulate matter levels, which may be caused by the oxidative stress pathway. Thus, oxidative stress due to nutrition, age, genetics among others may increase the susceptibility for neurodegenerative diseases (Peters et al. 2006).

A multicenter project of European Commission FP7 program called NeuroNano has investigated if engineered nanoparticles could constitute a significant risk to humans for neurodegenerative diseases. Details are available at the following web site: http://www.neuronano.eu. NeuroNano partners include universities of Ulster, Dublin, Cork, Edinburgh and Munich in Europe; universities of California, Rochester and Rice in the US; and the National Institute of Materials Science in Japan. Key findings of the NeuroNano project were:

- The existing body of research into the impacts of nanomaterials was not sufficient for the project partners' purposes. Therefore, they had to produce their own evidence base from scratch, using both cellular systems and carefully selected animal studies.
- Despite the brain being a 'sacrosanct' organ which most particles cannot enter, very small quantities of NPs can pass through the BBB. However, there is no evidence that the amounts of engineered nanomaterials that pass the barrier are sufficient to affect human health.
- Several new modes of interactions of nanoparticles with the BBB were observed, using the most advanced microscopy every applied to such systems. For example, a propensity for NPs to accumulate in the lysosomes of the BBB endothelial monolayer was observed. Additional work is required to understand if similar effects are also observed in animals, as current approaches to quantify uptake in vivo do not distinguish between the nanoparticle load in the brain versus in the endothelium separating the brain from the blood, i.e. within the BBB.

The University of Ulster experts, funded by a 2009 grant from the European Commission, specifically looked at nanoparticles present in chemicals found in sunscreens and an additive in some diesel fuels – titanium dioxide and cerium oxide – and their connection to Alzheimer's as well as Parkinson's diseases. Nanoparticles can have highly significant impact on the rate of misfolding of key proteins associated with neurodegenerative diseases.

Effect of Nanoparticles on the Heart

Some nanoparticles may influence the heart function, whereas others do not. The effect of nanoparticles is being studied on the Langendorff Heart or 'isolated perfused heart', which is an in vitro technique used in pharmacological and physiological research (Stampfl et al. 2011). The modified Langendorff heart is a particularly good test object as it has its own impulse generator, the sinus node, enabling it to function outside the body for several hours. This model enables observation and analysis of electrophysiological parameters over a minimal period of 4 h without influence by systemic effects complications of an intact animal while enabling the determination of stimulated release of substances under influence of NPs. A significant dose and material dependent increase in heart rate up to 15% was found accompanied by arrhythmia evoked by NPs made of flame soot (Printex 90), spark discharge generated soot, anatas (TiO2), and silicon dioxide (SiO2). However, flame derived SiO2 (Aerosil) and monodisperse polystyrene lattices exhibited no effects. The increase in heart rate is attributed to catecholamine release from adrenergic nerve endings within the heart. This new heart model may prove to be particularly useful in medical research and could serve as a test organ to help select nanoparticles that do not affect the heart adversely. The manufacturing process as well as the shape of a NP may play an important role. Therefore, further studies will examine the surfaces of different types of NPs and their interactions with the cells of the cardiac wall.

Blood Compatibility of Nanoparticles

Given that most of nanoparticles are intended to travel to tumors through the bloodstream, the effects of nanoparticles on blood cells are of particular concern to those developing nanoparticle-based therapeutic and imaging agents. The blood compatibility of nanoparticles depends on the material used.

Carbon Nanoparticle-Induced Platelet Aggregation

To determine the potential for blood platelet-nanoparticle interactions, the effects of engineered and combustion-derived carbon nanoparticles were studied on human platelet aggregation in vitro and rat vascular thrombosis in vivo (Radomski et al. 2005). Multiple-wall and single-wall nanotubes, C60 fullerenes and mixed carbon nanoparticles were compared with standard urban particulate matter (average size 1.4 μ m). Carbon particles, except C60 fullerenes, stimulated platelet aggregation and accelerated the rate of vascular thrombosis in rat carotid arteries. All particles resulted in upregulation of GPIIb/IIIa in platelets. The particle-induced aggregation was inhibited by prostacyclin and S-nitroso-glutathione, but

not by aspirin. It is concluded that some carbon nanoparticles and microparticles can activate platelets and enhance vascular thrombosis. These observations are of importance for the pharmacological use of carbon nanoparticles and pathology of urban particulate matter.

Compatibility of Lipid-Based Nanoparticles with Blood and Blood Cells

Pegylated and nonpegylated cetyl alcohol/polysorbate nanoparticles (E78 NPs) are being tested as drug carriers for specific tumor and brain targeting. Because these nanoparticle formulations are designed for systemic administration, the compatibility of these lipid-based NPs with blood and blood cells was tested with a special focus on hemolytic activity, platelet function, and blood coagulation (Koziara et al. 2005). E78 NPs did not cause in vitro red blood cell lysis at concentrations up to 1 mg/mL. In addition, under conditions tested, E78 and polyethylene glycol (PEG)-coated E78 NPs (PEG-E78 NPs) did not activate platelets. In fact, both NP formulations very rapidly inhibited agonist-induced platelet activation and aggregation in a dose-dependent manner. It was concluded that PEG-coated and nonpegylated E78 NPs have potential blood compatibility at clinically relevant doses. Based on the calculated nanoparticle-to-platelet ratio, the concentration at which E78 NPs could potentially affect platelet function in vivo was approximately 1 mg/mL.

Transfer of Nanoparticles from Mother to Fetus

A study has shown that QDs may be transferred from female mice to their fetuses across the placental barrier (Chu et al. 2010). Smaller QDs are more easily transferred than larger QDs and the number of QDs transferred increases with increasing dosage. Capping with an inorganic silica shell or organic PEG reduces QD transfer but does not eliminate it. These results suggest that the clinical utility of QDs could be limited in pregnant women. One study has shown that silica and titanium dioxide nanoparticles with diameters of 70 and 35 nm, respectively, can cause pregnancy complications when injected intravenously into pregnant mice (Yamashita et al. 2011). These nanoparticles were found in the placenta, fetal liver and fetal brain and mice treated with these nanoparticles had smaller uteri as well as smaller fetuses than untreated controls. Fullerene molecules and larger (300 and 1000 nm) silica particles did not induce these complications. These detrimental effects are linked to structural and functional abnormalities in the placenta on the maternal side, and are abolished when the surfaces of the silica nanoparticles are modified with carboxyl and amine groups.

Porous silicon nanoparticles (Psi NPs) are biocompatible, biodegradable and nontoxic in vivo. An experimental study in mice has shown that fluorescently labeled PSi NPs, injected into the mouse embryonic brains intraventricularly and to the mother intravenously, penetrate deep in the brain tissues (80% of cortical depth) of embryos and are higly motile (Yuryev et al. 2016). No developmental and macromorphological changes or increased cell apoptosis were observed although the NPs entered the cells. This study shows the possible behavior of nanomedicines in the embryonic brain that can open up new avenues for therapy of developmental-related diseases.

Cytotoxicity of Nanoparticles

Cytotoxicity refers to toxic effects on individual cells. In cytotoxicological studies, identical cell cultures are exposed to various forms and concentrations of toxins. To compare the toxicity of different compounds, scientists determine the concentration, measured in parts per million or parts per billion, of materials that lead to the death of 50% of the cells in a culture within 48 h.

A particle's surface chemistry may determine how it interacts with the tissues of the body. AFM shows that aqueous solutions of poly(amidoamine) dendrimers cause the formation of holes 15–40 nm in diameter in previously intact lipid bilayers. In contrast, carboxyl-terminated core-shell tectodendrimer clusters do not create holes in the lipid membrane but instead show a strong affinity to adsorb to the edges of existing bilayer defects. MWCNTs, not derivatized nor optimized for biological applications, are capable of both localizing within and initiating an irritation response in human epidermal keratinocytes, which may occur in the skin of workers as occupational exposure during manufacture of nanotubes (Monteiro-Riviere et al. 2005).

Indirect DNA Damage Caused by Nanoparticles Across Cellular Barriers

Cobalt-chromium nanoparticles (29.5 + - 6.3 nm in diameter) have been shown to damage human fibroblast cells across an intact cellular barrier without having to cross the barrier (Bhabra et al. 2009). The damage is mediated by a novel mechanism involving transmission of purine nucleotides (such as ATP) and intercellular signaling within the barrier through connexin gap junctions or hemichannels and pannexin channels. The outcome, which includes DNA damage without significant cell death, is different from that observed in cells subjected to direct exposure to nanoparticles. These results suggest the importance of indirect effects when evaluating the safety of nanoparticles. The potential damage to tissues located behind cellular barriers needs to be considered when using nanoparticles for targeting diseased states

Measures to Reduce Toxicity of Nanoparticles

Scientists at the Rice University's Center for Biological and Environmental Nanotechnology can significantly lower the toxicity level of buckyballs when exposed to liver and skin cells in a petri dish. They have accomplished this by attaching other molecules to the surface of buckyballs. This simple chemical modification could lower potential exposure risks during disposal of a product like a fuel cell or within a manufacturing plant. Removing attached molecules and enhancing toxicity could also be useful in chemotherapy treatments, for instance.

There is a huge potential for a new generation of gold nanoparticle (AuNP)based nanomedicinal products, nontoxic AuNP constructs and formulations that can be readily administered site-specifically through the intravenous mode, for diagnostic imaging by CT scan or for therapy via various modalities. The use of gum arabic (GA) was explored as it has been used for a long time to stabilize foods such as yogurt and hamburgers. It has unique structural features, including a highly branched polysaccharide structure consisting of a complex mixture of potassium, calcium and magnesium salts derived from arabic acid. GA can be used to absorb and assimilate metals and create a "coating" that makes gold nanoparticles stable and nontoxic. A study has described the synthesis and stabilization of AuNPs within the nontoxic phytochemical gum arabic matrix (GA-AuNPs) and has presented detailed in vitro analysis and in vivo pharmacokinetics studies of GA-AuNPs in pigs to gain insight into the organ-specific localization of this new generation of AuNP vector (Kattumuri et al. 2007). X-ray CT contrast measurements of GA-AuNP vectors were carried out for potential application in molecular imaging. The results demonstrate that naturally occurring GA can be used as a nontoxic phytochemical excipient in the production of readily administrable biocompatible AuNPs for diagnostic and therapeutic applications in nanomedicine.

Reducing Toxicity of Carbon Nanotubes

Water-soluble SWCNTs are significantly less toxic to begin with and can be rendered nontoxic with minor chemical modifications. SWCNTs can be rendered soluble via the attachment of the chemical subgroups hydrogen sulfite, sodium sulfite and carboxylic acid. The research is a continuation of pioneering efforts to both identify and mitigate potential nanotechnology risks. The cytotoxicity of undecorated SWCNTs is 200 parts per billion, which compares to the level of 20 parts per billion for undecorated buckyballs (Sayes et al. 2006). Competitive bindings of blood proteins on the SWCNT surface can greatly alter their cellular interaction pathways and result in much reduced cytotoxicity for these protein-coated SWCNTs (Ge et al. 2011). For medical applications, it is encouraging to see that the cytotoxicity of nanotubes is low and can be further reduced with simple chemical changes.

SWCNTs can be catalytically biodegraded over several weeks by the plant-derived enzyme, horseradish peroxidase. A study has shown that hypochlorite and reactive radical intermediates of the human neutrophil enzyme myeloperoxidase catalyse the biodegradation of SWCNTs in vitro, in neutrophils and to a lesser degree in macrophages (Kagan et al. 2010). Molecular modeling suggests that interactions of basic amino acids of the enzyme with the carboxyls on the CNTs position the nano-tubes near the catalytic site. Importantly, the biodegraded CNTs do not generate an inflammatory response when aspirated into the lungs of mice. These findings suggest that the extent to which CNTs are biodegraded may be a major determinant of the scale and severity of the associated inflammatory responses in exposed individuals. These findings will open the door to using SWCNTs as a safe drug delivery tool and lead to the development of a natural treatment for people exposed to nanotubes.

A Screening Strategy for the Hazard Identification of Nanomaterials

The International Life Sciences Institute Research Foundation/Risk Science Institute convened an expert working group to develop a screening strategy for the hazard identification of engineered nanomaterials. The working group report presented the elements of a screening strategy rather than a detailed testing protocol (Oberdorster et al. 2005). Based on an evaluation of the limited information available in 2005, the report presented a broad data gathering strategy applicable to this early stage in the development of a risk assessment process for nanomaterials. Oral, dermal, inhalation, and injection routes of exposure are included recognizing that, depending on use patterns, exposure to nanomaterials may occur by any of these routes. The three key elements of the toxicity screening strategy are: (1) physicochemical characteristics: (2) in vitro assays (cellular and non-cellular); and (3) in vivo assays. There is a strong likelihood that biological activity of nanoparticles will depend on physicochemical parameters not routinely considered in toxicity screening studies. Physicochemical properties that may be important in understanding the toxic effects of test materials include particle size and size distribution, agglomeration state, shape, crystal structure, chemical composition, surface area, surface chemistry, surface charge, and porosity. In vitro techniques allow specific biological and mechanistic pathways to be isolated and tested under controlled conditions, in ways that are not feasible in in vivo tests. Tests are suggested for portal-of-entry toxicity for lungs, skin, and the mucosal membranes, and target organ toxicity for endothelium, blood, spleen, liver, nervous system, heart, and kidney. Non-cellular assessment of nanoparticle durability, protein interactions, complement activation, and pro-oxidant activity is also considered. The report focuses on the likely toxic impact of nanoparticles in the body but does not comment on the actual risk of exposure because currently there are few situations where people are directly exposed to the nanoparticles.

Concluding Remarks on Safety Issues of Nanoparticles

There is no consensus on the real risks of nanomaterials. Risk evaluation presents challenges due to a lack of data, the complexity of nanomaterials, measurement difficulties, and undeveloped hazard assessment frameworks. There is a paucity of published material on this topic, which could provide scientific guidance; less than 800 journal articles on health risks of engineered nanomaterials have been published. Until the risk assessment is evaluated further, some precautionary measures should be considered to reduce risks, such as exposure control. It is recommended that manufacturers of nanomaterials should inventory all products and applications to potential exposures across the product life cycle. The risk of each application should be characterized based on exposure and available knowledge about hazard. The risk of exposure should be mitigated through additional testing and product redesign.

Research into Effects of Nanoparticles in the Environment

Nanoparticles may be released in the atmosphere from natural sources or from pollutants released from the industrial or other sources related to human lifestyle activities. Research strategies for safety evaluation of nanomaterials have been planned in the US, Europe and Japan. An important component of these programs is the development of reliable risk and safety evaluations for these materials to ensure their safety for human health and the environment. The scope of each of these programs includes efforts to assess the hazards posed by nanomaterials in realistic exposure conditions. University of Wisconsin-Madison's Nanotechnology in Society Project has published some of the key data gaps, uncertainties, and unknowns that need to be addressed to develop adequate risk assessments for nanomaterials and to take timely and appropriate public health precautions.

Effect of Magnetite Pollution Nanoparticles on the Human Brain

Biologically formed nanoparticles of the strongly magnetic mineral, magnetite, were first detected in the human brain over 20 years ago. Magnetite can have potentially large impacts on the brain due to its unique combination of redox activity, surface charge, and strongly magnetic behavior. A study has used magnetic analyses and electron microscopy to identify the abundant presence in the brain of magnetite nanoparticles that are consistent with high-temperature formation, suggesting, therefore, an external, not internal, source (Maher et al. 2016). Comprising a separate nanoparticle population from the euhedral particles ascribed to endogenous sources, these brain magnetites are often found with other transition metal nanoparticles, and they display rounded crystal morphologies and fused surface textures, reflecting crystallization upon cooling from an initially heated, iron-bearing source material. Such high-temperature magnetite nanospheres are ubiquitous and abundant in airborne particulate matter pollution. They arise as combustion-derived, iron-rich particles, often associated with other transition metal particles, which condense and/ or oxidize upon airborne release. Those magnetite pollutant particles which are <200 nm in diameter can enter the brain directly via the olfactory bulb. Their presence proves that externally sourced iron-bearing nanoparticles, rather than their soluble compounds, can be transported directly into the brain. This discovery is important because nanoscale magnetite can respond to external magnetic fields, and is toxic to the brain, being implicated in production of damaging reactive oxygen species (ROS) Because enhanced ROS production is causally linked to neurodegenerative diseases such as Alzheimer's disease, exposure to such airborne particulate matterderived magnetite nanoparticles might need to be examined as a possible hazard to human health.

Environmental Safety of Aerosols Released from Nanoparticle Manufacture

Det Norske Veritas (Oslo, Norway), a classification society, conducted the EU project NANOTRANSPORT (2006–2008), which addressed the behavior of aerosols released to ambient air from nanoparticle manufacturing. The project brought together leading expert organizations in risk management, aerosol monitoring, filtration, nanoparticle technology and online particle characterization fields. Key conclusions of the study are:

- There is considerable evolution of nanoaerosols over time: their average size increases, while their concentration decreases.
- Natural background aerosols are scavengers for nanoparticles
- The time scale for size evolution depends on concentration and primary size of the nanoparticles and that of the background aerosol it may range from a matter of a few minutes up to half an hour.
- Nanoparticles will be physically/chemically present in size classes other than those in which they were originally emitted.
- Filtration efficiency of primary nanoparticles <80 nm is usually sufficiently high, but their agglomerates may be in the Most Penetrating Particle Size range of 80–200 nm.

Role of US Government Agencies in Research on Safety of Nanoparticles

Nanotechnology advocates say they support faster and broader environmental research, but paying for it has not been a priority for businesses or the government. The Environmental Protection Agency, which had previously focused on supporting research into how nanotechnology could help clean or protect the environment, is seeking grant proposals from researchers looking at potential risks. But the amounts awarded are only a fraction of those allocated for nanotechnology research and development. The difficulty and cost of researching risk are influencing business decisions. L'Oréal, the cosmetics company, for instance, dropped its research on the characteristics of nanoparticles after outside researchers raised questions about toxicity. Some smaller nanotechnology start-ups say they simply do not have the resources to push into promising areas that pose health questions.

Work at NanoSafety Laboratories Inc UCLA

UCLA (University of California, Los Angeles, CA) developed a method that would help manufacturers monitor and test the safety and health risks of engineered nanomaterials (Nel et al. 2006). The testing model developed at UCLA is based on toxicity testing for occupational and air pollution particles, which include nanoparticles. The strong scientific foundation of air pollution particle testing is used to help understand the health impact of engineered nanoparticles and ensure safe manufacturing of nanoproducts. The impact of nanoparticle interactions with the body is dependent on their size, chemical composition, surface structure, solubility, shape, how the individual nanoparticles amass together and the potential routes of exposure such as the gastrointestinal tract, skin or lungs. Nanoparticles may modify the way cells behave. The three key elements of the toxicity screening strategy include: (1) the physical and chemical characterization of nanomaterials; (2) tissue cellular assays; and (3) animal studies.

A mature toxicological science has emerged from the study of these particles, providing a framework for a predictive testing strategy applicable to engineered nanomaterials. A predictive strategy is one in which a series of simple but high-quality tests can be employed to predict which materials could be hazardous, and therefore speed up the process of classifying materials into those that are safe and those that could pose toxicity problems. This type of approach is like that used by the National Toxicology Program for evaluation of chemical agents. The UCLA model predicts toxicity according to the ability of some nanoparticles to generate toxic oxygen radicals that can cause tissue injury, including inflammation and other toxic effects. For air pollution particles, this injury can translate into asthma and atherosclerotic heart disease. Using this model, the UCLA laboratory has developed

a series of tests to assess nanoparticle toxicity in non-biological environments as well as in tissue cultures and animal models. Funding for the research on air pollution particles that contributed to this paper came from the National Institute of Environmental Health Sciences and the US Environmental Protection Agency.

Center for Biological and Environmental Nanotechnology

Rice University's Center for Biological and Environmental Nanotechnology (CBEN) has played an active role in informing the public, lawmakers and industry about potential unintended environmental consequences of nanotechnology. CBEN's research aims to understand how nanomaterials function in water-based environments such as living organisms and ecosystems. In its first 5 years since its founding in 2000, CBEN helped produce groundbreaking research in nanomedicine, nanobiotechnology, nanotoxicology and nanoscale methods for environmental remediation. Further details of CBEN can be viewed at its web site (http://cben.rice.edu/). Environmental Nanotechnology is no longer an active department at Rice University, but this web page is still running to provide resources to those who still need access to them.

European NEST Project for Risk Assessment of Exposure to Nanoparticles

A study, led by the Institute of Occupational Medicine (UK), is investigating the safety of new and emerging science and technologies (NEST) that have the potential to generate particulates, which can enter the body via inhalation, ingestion or dermal absorption. Information is needed regarding the possible risks from exposure to these particles including: the routes of exposure and subsequent disposition; their potential toxicity; appropriate toxicological testing procedures; and susceptible subpopulations. The institute will acquire a bank of five particles potentially generated by NEST (NESTP) and will assess the health risk from exposure to these materials through air or the food supply with a work program, integrating in vitro experiments, animal models of healthy/susceptible individuals and exposure/risk assessment.

Nanoparticles and Food Safety

Nanomaterials are starting to enter the food chain through well-known food products and their packaging, but majority of food companies have not been responsive in providing information about their specific uses, plans, and policies on this topic and no US laws require disclosure. In addition, there are few, if any, studies adequately demonstrating the safety of nanoparticles in food additives or packaging. Scientists are still investigating how the broad range of nanoparticles, with their myriad potential uses, will react in the body and what the appropriate testing methodologies are to determine this. A report has been published about the emerging use of engineered nanomaterials in food and highlights the potential risks of nanotechnology for consumers as well as companies that are knowingly or unknowingly using it in their products and for public health (Behar et al. 2013). The authors surveyed 25,000 food manufacturers and tested a range of products; the results of both inquiries proved that nanomaterials are currently being used in food products. The report presents:

- A summary of the emerging usage of nanomaterials within the food industry and international policies and regulations.
- Analysis of findings on the use of nanomaterials in food products, packaging, and supplements.
- Results and methods of laboratory tests on currently available foods containing nanomaterials.
- Recommendations for companies, investors, and consumers interested in this issue.

Only 26 out of 2500 companies, including PepsiCo, Whole Foods and the corporate parent of Pizza Hut and Taco Bell, responded to the above survey about their use of nanomaterials. Only 14 said they do not use nanomaterials, and of those only two had any policies on the use of nanomaterials. Various food companies are interested in nanotechnology, which can help make products creamier without additional fat, intensify and improve flavors and brighten colors. Nine out of ten donut products tested positive for the presence of titanium dioxide (TiO2) materials of <10 nm. TiO2 is used to brighten white substances and the nano variety is under investigation by the EPA. TiO2 nanoparticles can penetrate cells and interfere with several subcellular mechanisms including structure and function of genomic DNA (Trouiller et al. 2009).

Titanium Dioxide Nanoparticles in Food

The concentration of nano titanium dioxide, a common whitener, is >10% in certain powdered doughnuts. Titanium dioxide is chemically inert and has entered humans for decades, often during surgery and frequently as part of a joint replacement. However, nanoparticulate titanium dioxide acts quite differently than it does under normal circumstances. Nano-size titanium dioxide, particularly, can sneak into parts of the body that most particles cannot, such as bone marrow, ovaries, lymph nodes, and nerves. It can also cross the blood-brain barrier or enter cells and destroy genetic material. The particles have been found to accumulate in the small intestine, particularly in areas used by our immune system. In experimental studies on mice,

lacing drinking water with nano titanium dioxide wreaks havoc on the animals' chromosomes and DNA, which can lead to increased rates of cancer, as well as heart and neurological diseases. The International Agency for Research on Cancer (part of the WHO) has linked nano titanium dioxide in powder form to cancers, especially when inhaled. The substance is commonly added to products we use everyday. The Environmental Working Group, a research organization based in Washington, DC, estimates that nano titanium dioxide is found in about 10,000 over-the-counter products, even food. Because the particle reflects light well it was a common whitener in foods, showing up in powdered doughnuts.

Regulatory Viewpoint on Nanoparticles in Food

In 2011, the European Union passed regulations on the labeling of nanomaterials in food. The new law combined two directives into one piece of legislation: 2000/13/ EC on labeling, presentation, and advertising of foodstuffs, and 90/496/EEC on nutrition labeling for foodstuffs. The new law contains a definition of the term "nanomaterials" and mandates the labeling of all ingredients falling under this definition. In 2011, the FDA draft guidance on nanotechnology defined nanomaterials if they are <1000 nm, whereas the National Nanotechnology Initiative of US Government had earlier defined it at 100 nm (http://www.fda.gov/RegulatoryInformation/Guidances/ucm257698.htm). In 2010, the US National Organic Standards Board called for nanomaterials <300 nm to be excluded from organic foods as they can be taken up by individual cells (http://www.ams.usda.gov/AMSv1.0/getfile?dDocName =STELPRDC5087795&acct=nosb). In 2012, the FDA issued an unusual statement on nanomaterials, saying it did not have enough data to determine the safety of nanomaterials in food.

Use of Water Nanostructures for Inactivation of Foodborne Microorganisms

Foodborne diseases caused by the consumption of food contaminated with pathogenic microorganisms or their toxins have very serious economic and public health consequences. A method for inactivation of microorganisms on fresh foods and food production surfaces uses Engineered Water Nanostructures (EWNS) produced by electrospraying of water vapor (Pyrgiotakis et al. 2015). EWNS possess unique properties; they are 25 nm in diameter, remain airborne in indoor conditions for hours, contain Reactive Oxygen Species (ROS) and have very strong surface charge (on average 10e/structure). Here, their efficacy in inactivating representative foodborne bacteria such as *Escherichia coli*, Salmonella enterica, and Listeria innocua, on stainless steel surfaces and on organic tomatoes, was assessed. This chemical-free, non-toxic, and and environmentally friendly method has potential for development and application in the food industry, as a "green" alternative to existing disinfection methods.

Public Perceptions of the Safety of Nanotechnology

Past and current experience in biotechnology has shown how environmentally concerned public reacts to new technologies. One can predict that there will be antinanotechnology groups in the future like the anti-biotechnology groups. Apart from the unknown long-term effects of nanomaterials in the human body, a much greater concern is expressed about the environmental effects of release of nanoparticles from the industry. A question that is being already asked is about the possibility of accumulation of nanomaterials in water or the earth, and the risk if this takes place. Some of these issues are already under investigation. The public's outlook on nanotechnology remains positive despite a lack of knowledge, but press coverage and agitation from various groups indicates that nanotechnology industry will not be able to dodge these questions much longer. Instead of remaining silent on this issue, companies need a communication strategy to share their safety studies, collaborate with trusted partners, and explain the benefits nanotechnology can bring. The public relations departments of research institutes and companies involved in nanotechnology will have a major task of educating the public about the safety of nanotechnology. Although there has been a very public debate in Europe about the risk of genetically modified organisms(GMOs) in food, the question of nanomaterials has largely stayed out of the mainstream.

As an example, it was anticipated that exploration of the human genome could result in public concerns – ethical, legal, and cultural. Therefore, 3-5% of federal research money was set aside to fund the study of these issues and to communicate with the public and encourage lots of openness and transparency. This is now the model for a proactive approach to new technology development.

The largest and most comprehensive survey of public perceptions of nanotechnology products finds that US consumers are willing to use specific nano-containing products – even if there are health and safety risks – when the potential benefits are high (Currall et al. 2006). The study, which was conducted by researchers at Rice University's Center for Biological and Environmental Nanotechnology (Houston, TX), University College London and the London Business School, also finds that US consumers rate nanotechnology as less risky than everyday technologies like herbicides, chemical disinfectants, handguns and food preservatives. The research was based on more than 5500 survey responses. One survey polled consumers about how likely they would be to use four specific, nano-containing products: a drug, skin lotion, automobile tires and refrigerator gas coolant. This is the first large-scale study to experimentally gauge the public's reaction to specific, nano-containing products, and the use of scenarios about plausible, specific products yielded results that challenge the assumption that the public focuses narrowly on risk. The greater the potential benefits, the more risks people are willing to tolerate.

Evaluation of Consumer Exposure to Nanoscale Materials

Although there are numerous likely consumer advantages from products containing nanoscale materials, there is very little information available regarding consumer exposure to the nanoscale materials in these products or any associated risks from these exposures. The products include cosmetics, sunscreen, textiles, and sporting goods. An important component in addressing potential health risks is the potential exposure to the consumer. The presence of a toxic substance in a consumer product does not constitute a health hazard if the product design or use prevents the consumer from being exposed to the substance. For consumer product applications, if the nanomaterial is attached to the product in a manner that minimizes its release, the exposure potential will be minimal. If the nanomaterials are released in significant quantities during reasonably foreseeable product use or foreseeable misuse, exposure may result via dermal contact, ingestion, or inhalation.

Toxic Substances Control Act gives the US Environmental Protection Agency (EPA) authority to regulate the manufacture, use, distribution in commerce, and disposal of chemical substances. This act authorizes the agency to regulate both new and existing compounds and is currently undergoing scrutiny by the agency to determine to what extent it can incorporate engineered nanomaterials. FDA regulates very few materials but many types of products. Cosmetics do not require premarket approval from the FDA, but if the FDA considers that there is a safety concern resulting from the use of any cosmetic ingredient, including nanoparticles, it has several options to prohibit the marketing and sale of these products. Sunscreens are cosmetics in Europe but regulated similar to drugs in the US. Currently, the FDA is involved in studies of marketed sunscreens in collaboration with the National Toxicology Program and the National Institute for Standards and Technology. These studies will help identify those sunscreens that contain nanoscale particles of titanium dioxide and zinc oxide, and characterize the size ranges for these nanoscale particles.

US Consumer Product Safety Commission (CPSC) is charged with protecting the public from unreasonable risks of serious injury or death from over 15,000 types of consumer products under the agency's jurisdiction. Nanotechnology-derived products entering commerce, containing materials with novel chemical, physical, biological, optical, and electronic properties, will require assessment to determine if there may be exposure to a potential health risk that might negatively impact consumer safety. The potential health risk of nanomaterials can be assessed with existing CPSC statutes, their administering regulations, and interpretative guidelines.

Safety of Nanoparticle-Based Cosmetics

Regulations in the European Union

Under cosmetics regulations in the European Union (EU), ingredients (including those in the form of nanoparticles) can be used for most purposes without prior approval, provided they are not on the list of banned or restricted use chemicals and

that manufacturers declare the final product to be safe. Given the concerns about toxicity of any nanoparticles penetrating the skin, the Royal Society of UK recommends that their use in products be dependent on a favorable opinion by the relevant European Commission scientific safety advisory committee. A favorable opinion has been given for the nanoparticulate form of titanium dioxide (because chemicals used as UV filters must undergo an assessment by the advisory committee before they can be used) but insufficient information has been provided to allow an assessment of zinc oxide. It is recommended that manufacturers publish details of the methods they have used in assessing the safety of their products containing nanoparticles that demonstrate how they have recognized that properties of nanoparticles may be different from larger forms. Because nanoparticles of zinc oxide are not used extensively in cosmetics in Europe, this is not a major problem. If chemicals produced in the form of nanoparticles are to be treated as new chemicals, the product label would identify that nanoparticles have been used in manufacture.

The Cosmetic Products Regulation 1223/2009 in the EU attempts to address concerns about nanomaterials. According to this regulation, since 2013, all nanomaterial formulations must be indicated on the package, with the suffix "nano", e.g. TiO2-nano. Moreover, all marketed cosmetics and sunscreens using nanoparticles should be individually tested for safety. Cosmetic products containing nanomaterials must be notified by electronic means to the European Commission, providing data on identification, specification, quantity, toxicological profile, safety data, and foreseeable exposure conditions. Such notification must occur 6 months before a cosmetic product containing nanomaterials is placed on the market.

Nanotechnology-Based Sunscreens

In 2006, a petition was filed by consumer, health and environmental groups in the US that asked the FDA to recall sunscreens that contain nanoparticles unless they are proven safe. The petition also called for premarket safety testing of nano sunscreens, and for nano-specific toxicity testing and mandatory labeling of nano products.

According to the sunscreen industry, sun creams are safe and academic experts do not have enough evidence for harmful effects to justify a recall of sunscreens, although some recommend labeling of the products and more public access to information about safety studies done by industry. The FDA is participating in studies of skin absorption of nano-sized titanium dioxide and zinc oxide preparations used in sunscreens.

Friends of the Earth, one of the petitioners, published a list of 116 personal care products, cosmetics and sunscreens that contain nanomaterials. The sunscreen ingredients the petitioners warned about are nanoparticles of titanium dioxide and zinc oxide smaller than 100 nm, the upper size limit of what is usually called nanoparticles. It's unclear whether such particles can enter intact skin. The FDA has previously classified 16 sunscreen ingredients as safe and effective, and particle size did not affect the classification of these ingredients. But the petitioners argue that size does matter, in that nanoparticles are likely more harmful than larger particles

of the same material, and products that contain them should therefore be recalled and tested for safety.

The Cosmetic, Toiletry and Fragrance Association (now called Personal Care Products Council), an industry group, issued a statement that sunscreens use small microparticles, which are larger than 100 nm (not nanoparticles by strict definition), have been deemed safe by the FDA. Some manufacturers call their products 'nano' only for promotional reasons. However, some face creams and moisturizers contain fullerenes that have a potential for toxic effects due to elevation of free radicals in the brain as a reaction to the particles.

Cosmetic Industry's White Paper on Nanoparticles in Personal Care

The Personal Care Products Council (http://www.personalcarecouncil.org/) has released a white paper on the application of nanotechnology in personal care products, including cosmetics and certain over-the-counter drug products, specifically sunscreens. The report discusses the advantages of the use of nanomaterials, the regulatory evaluation of personal care products using nanotechnology, properties of nanoparticles, the potential for dermal absorption of nanoparticles used in topical lotions or creams, and what it characterizes as the general scientific consensus and toxicology conclusions about the use of nanotech in personal care products. The report specifically addresses the issue of titanium dioxide and zinc oxide used in nanoparticle form in sunscreens. The industry-supported report argues that nanoparticles applied topically to the skin in lotions or creams are safe.

Skin Penetration of Nanoparticles Used in Sunscreens

Nanoparticles are commonly used in sunscreens and other cosmetics. Eight in 10 of the leading beauty brands have been found to contain nanoparticles that act as "penetration enhancers." Since consumer use of sunscreen is often applied to sun damaged skin, the effect of ultraviolet radiation (UVR) on nanoparticle skin penetration is a concern due to potential toxicity. A study has investigated nanoparticle skin penetration by employing an in vivo semiconductor QD nanoparticle model system, which improves imaging capabilities (Mortensen et al. 2008). In these experiments, carboxylate QD were applied to the skin of SKH-1 mice in a glycerol vehicle with and without UVR exposure. The skin collection and penetration patterns were evaluated 8 and 24 h after QD application using tissue histology, confocal microscopy, and transmission electron microscopy. Low levels of penetration were seen in both the non-UVR exposed mice and the UVR exposed mice. The particles accumulate around the hair follicles and in tiny skin folds. These results provide important insight

into the ability of QD to penetrate intact and UVR compromised skin barrier. Part of the explanation likely lies with the complex reaction of skin when it is assaulted by the UVR. The cells proliferate, and molecules in the skin known as tight-junction proteins loosen so that new cells can migrate to where they are needed. Those proteins normally act as gatekeepers that determine which molecules to allow through the skin and into the body, and which molecules to block. When the proteins loosen up, they become less selective than usual, possibly giving nanoparticles an opportunity to pass through the barrier. In the future, the investigators plan to study titanium dioxide and zinc oxide, two materials that are widely used in sunscreens and other cosmetic products to help block the damaging effects of UVR.

Titanium Dioxide in Cosmetics

Mixed in a liquid, such as sunscreen or a lotion, titanium dioxide has little chance of moving through skin and into the bloodstream, where it might cause problems. A face powder with titanium dioxide, however, presents plenty of opportunity for inhalation. From the lungs it can enter blood circulation.

In the past, tests from manufacturers and labs that work with the FDA and EPA, had proved that part of what made nano titanium dioxide safe in viscous mixes like sunscreens was the fact that the particles clustered and clumped, creating structures bigger than the individual nanoparticles and therefore less likely to slip through skin. However, more recent studies showed that after exposure to UV radiation as in sunlight, nanoparticles in lotions, cosmetics, and sunscreens were no longer as clumped as before. Individual particles had broken off and many of these had become even smaller.

References

- Behar A, Fugere D, Passoff M. Slipping through the cracks an issue brief on nanomaterials in food. Published by "As You Sow", Oakland, California, 2013. Available at the web site: http:// www.asyousow.org/ays_report/slipping-through-the-cracks/.
- Bhabra G, Sood A, Fisher B, et al. Nanoparticles can cause DNA damage across a cellular barrier. Nat Nanotech. 2009;4:876–83.
- Braydich-Stolle L, Hussain S, Schlager J, Hofmann MC. In vitro cytotoxicity of nanoparticles in mammalian germ-line stem cells. Toxicol Sci. 2005;88:412–9.
- Choi HS, Ashitate Y, Lee JH, et al. Rapid translocation of nanoparticles from the lung airspaces to the body. Nat Biotechnol. 2010;28:1300–3.
- Chu M, Wu Q, Yang H, et al. Transfer of quantum dots from pregnant mice to pups across the placental barrier. Small. 2010;6:670–8.
- Currall SC, King EB, Lane N, et al. What drives public acceptance of nanotechnology? Nat Nanotechnol. 2006;1:153–5.
- De Jong WH, Hagens WI, Krystek P, et al. Particle size-dependent organ distribution of gold nanoparticles after intravenous administration. Biomaterials. 2008;29:1912–9.

- Derfus AM, Chan CW, Bhatia SN, et al. Probing the cytotoxicity of semiconductor quantum dots. Nano Lett. 2004;4:11–8.
- Falagan-Lotsch P, Grzincic EM, Murphy CJ. One low-dose exposure of gold nanoparticles induces long-term changes in human cells. Proc Natl Acad Sci U S A. 2016;113:13318–23.
- Ge C, Du J, Zhao L, et al. Binding of blood proteins to carbon nanotubes reduces cytotoxicity. Proc Natl Acad Sci U S A. 2011;108:16968–73.
- Jud C, Clift MJ, Petri-Fink A, Rothen-Rutishauser B. Nanomaterials and the human lung: what is known and what must be deciphered to realise their potential advantages? Swiss Med Wkly. 2013;143:w13758.
- Kagan VE, Konduru NV, Feng W, et al. Carbon nanotubes degraded by neutrophil myeloperoxidase induce less pulmonary inflammation. Nat Nanotechnol. 2010;5:354–9.
- Kagan VE, Tyurina YY, Tyurin VA, et al. Direct and indirect effects of single walled carbon nanotubes on RAW 264.7 macrophages: role of iron. Toxicol Lett. 2006;165:88–100.
- Kattumuri V, Katti K, Bhaskaran S, et al. Gum arabic as a phytochemical construct for the stabilization of gold nanoparticles: in vivo pharmacokinetics and X-ray-contrast-imaging studies. Small. 2007;3:333–41.
- Koziara JM, Oh JJ, Akers WS, Ferraris SP, Mumper RJ. Blood compatibility of cetyl alcohol/ polysorbate-based nanoparticles. Pharm Res. 2005;22:1821–8.
- Lalwani G, D'Agati M, Khan AM, Sitharaman B. Toxicology of graphene-based nanomaterials. Adv Drug Deliv Rev. 2016;105(Pt B):109–44.
- Li C, Liu H, Sun Y, et al. PAMAM nanoparticles promote acute lung injury by inducing autophagic cell death through the Akt-TSC2-mTOR signaling pathway. J Mol Cell Biol. 2009;1:37–45.
- Liu Z, Davis C, Cai W, et al. Circulation and long-term fate of functionalized, biocompatible single-walled carbon nanotubes in mice probed by Raman spectroscopy. Proc Natl Acad Sci U S A. 2008;105:1410–5.
- Magrez A, Kasas S, Salicio V, et al. Cellular toxicity of carbon-based nanomaterials. Nano Lett. 2006;6:1121–5.
- Maher BA, Ahmed IA, Karloukovski V, et al. Magnetite pollution nanoparticles in the human brain. Proc Natl Acad Sci U S A. 2016;113:10797–801.
- Mills NL, Amin N, Robinson SD, et al. Do inhaled carbon nanoparticles translocate directly into the circulation in man? Am J Respir Crit Care Med. 2006;173:426–31.
- Monteiro-Riviere NA, Nemanich RJ, Inman AO, et al. Multi-walled carbon nanotube interactions with human epidermal keratinocytes. Toxicol Lett. 2005;155:377–84.
- Mortensen LJ, Oberdörster G, Pentland AP, Delouise LA. In vivo skin penetration of quantum dot nanoparticles in the murine model: the effect of UVR. Nano Lett. 2008;8:2779–87.
- Nel A, Xia T, Madler L, Li N. Toxic potential of materials at the nanolevel. Science. 2006;311:622-7.
- Oberdorster E. Manufactured nanomaterials (fullerenes, C60) induce oxidative stress in the brain of juvenile largemouth bass. Environ Health Perspect. 2004;112:1058–62.
- Oberdorster G, Maynard A, Castranova V, et al. Principles for characterizing the potential human health effects from exposure to nanomaterials: elements of a screening strategy. Part Fibre Toxicol. 2005;2:8.
- Park MV, Lankveld DP, van Loveren H, de Jong WH. The status of in vitro toxicity studies in the risk assessment of nanomaterials. Nanomedicine. 2009;4:669–85.
- Peters A, Veronesi B, Calderon-Garciduenas L, et al. Translocation and potential neurological effects of fine and ultrafine particles: a critical update. Part Fibre Toxicol. 2006;3:13.
- Pyrgiotakis G, Vasanthakumar A, Gao Y, et al. Inactivation of foodborne microorganisms using engineered water nanostructures (EWNS). Environ Sci Technol. 2015;49:3737–45.
- Radomski A, Jurasz P, Alonso-Escolano D, et al. Nanoparticle-induced platelet aggregation and vascular thrombosis. Br J Pharmacol. 2005;146:882–93.
- Renwick LC, Brown D, Clouter A, Donaldson K. Increased inflammation and altered macrophage chemotactic responses caused by two ultrafine particle types. Occup Environ Med. 2004;61: 442–7.
- Sayes C, et al. The differential cytotoxicity of water-soluble fullerenes. Nano Lett. 2004;4:881-7.

- Sayes CM, Gobin AM, Ausman KD, et al. Nano-C(60) cytotoxicity is due to lipid peroxidation. Biomaterials. 2005;26:7587–95.
- Sayes CM, Liang F, Hudson JL, et al. Functionalization density dependence of single-walled carbon nanotubes cytotoxicity in vitro. Toxicol Lett. 2006;161:135–42.
- Singh R, Pantarotto D, Lacerda L, et al. Tissue biodistribution and blood clearance rates of intravenously administered carbon nanotube radiotracers. Proc Natl Acad Sci U S A. 2006; 103:3357–62.
- Stampfl A, Maier M, Radykewicz R, et al. Langendorff heart: a model system to study cardiovascular effects of engineered nanoparticles. ACS Nano. 2011;5:5345–53.
- Talukdar Y, Rashkow JT, Lalwani G, et al. The effects of graphene nanostructures on mesenchymal stem cells. Biomaterials. 2014;35:4863–77.
- Trouiller B, Reliene R, Westbrook A, et al. Titanium dioxide nanoparticles induce DNA damage and genetic instability in vivo in mice. Cancer Res. 2009;69:8784–9.
- van Berlo D, Clift MJD, Albrecht C, Schins RPF. Carbon nanotubes: an insight into the mechanisms of their potential genotoxicity. Swiss Med Wkly. 2012;142:w13698.
- Warheit DB, Laurence BR, Reed KL, et al. Comparative pulmonary toxicity assessment of singlewall carbon nanotubes in rats. Toxicol Sci. 2004;77:117–25.
- Warheit DB, Webb TR, Colvin VL, et al. Pulmonary bioassay studies with nanoscale and finequartz particles in rats: toxicity is not dependent upon particle size but on surface characteristics. Toxicol Sci. 2007;95:270–80.
- Williams DN, Ehrman SH, Holoman TR. Evaluation of the microbial growth response to inorganic nanoparticles. J Nanobiotechnol. 2006;4:3.
- Wong-Ekkabut J, Baoukina S, Triampo W, et al. Computer simulation study of fullerene translocation through lipid membranes. Nat Nanotechnol. 2008;3:363–8.
- Yamashita K, Yoshioka Y, Higashisaka K, et al. Silica and titanium dioxide nanoparticles cause pregnancy complications in mice. Nat Nanotechnol. 2011;6:321–8.
- Yuryev M, Ferreira MP, Balasubramanian V, et al. Active diffusion of nanoparticles of maternal origin within the embryonic brain. Nanomedicine (Lond). 2016;11:2471–81.
- Zhang LW, Monteiro-Riviere NA. Assessment of quantum dot penetration into intact, tape-stripped, abraded and flexed rat skin. Skin Pharmacol Physiol. 2008;21:166–80.
- Zhang LW, Yu WW, Colvin VL, Monteiro-Riviere NA. Biological interactions of quantum dot nanoparticles in skin and in human epidermal keratinocytes. Toxicol Appl Pharmacol. 2008;228:200–11.
- Zhang T, Stilwell JL, Gerion D, et al. Cellular effect of high doses of silica-coated quantum dot profiled with high throughput gene expression analysis and high content cellomics measurements. Nano Lett. 2006;6:800–8.
- Zhu M, Nie G, Meng H, et al. Physicochemical properties determine nanomaterial cellular uptake, transport, and fate. Acc Chem Res. 2013;46:622–31.

Chapter 18 Ethical and Regulatory Aspects of Nanomedicine

Introduction

Ethical and regulatory aspects are important in practice of medicine and the same applies to nanomedicine. As has happened with introduction of all new technologies, in healthcare, these issues need to be considered. The FDA is formulating specific regulations relevant to nanobiotechnology products. The development of pharmaceuticals containing nanoparticles and methods of drug delivery, however, will be regulated by the FDA like any other biopharmaceutical product.

Ethical and Social Implications of Nanobiotechnology

Nanotechnology's impact has been mostly in engineering, communications, electronics and consumer products. Now that nanobiotechnology is being applied to pharmaceuticals, food sciences and human medicine, there is awareness of the consequences, good or bad, that are still not well understood. Most technologies have potential for good or evil. New technologies may have disruptive influence on the society as evidenced by the introduction of biotechnology in agriculture. Genetically modified foods continue to disturb trade between the US and Europe and the products find a mixed reception in supermarkets. In 2005, the Swiss public voted to place a moratorium on application of biotechnology in agriculture for a period of 5 years. There is a concern that the same thing could happen to nanotechnology.

Communication with the public is important at this stage. This will involve education of the public and consideration of their opinion. Greenpeace argues that current research priorities need to shift in favor of environmental and health protection to engender public support and/or an ongoing need to remain sensitive to emerging societal preferences (Parr 2005). US Federal grants have been awarded to universities for research on ethical, legal and social issues arising from introduction of nanotechnology.

Nanoethics

Ethical aspects are important for all new technologies and nanobiotechnology is no exception. Although nanotechnology has not raised any new ethical issues, it is worthwhile to keep these considerations in mind while developing and applying nanobiotechnologies to medicine. Ethical, social and legal issues arising from the application of nanotechnology to medicine have been reviewed recently (Resnik and Tinkle 2007).

In the ethical debate on nanotechnology (nanoethics) there has been a strong tendency to strongly focus on extremes either the upside or the downside with the result that ethical assessments tend to diverge radically. Many of the extreme views are based on simplified and outdated visions of a nanotechnology dominated by self-replicating assemblers and nanomachines. There is a need for development of more balanced and better-informed assessments (Gordijn 2005). Various pitfalls of nanoethics are; (1) the restriction of ethics to prudence understood as rational risk management; (2) the reduction of ethics to cost/benefit analysis; and (3) the confusion of technique with technology and of human nature with the human condition (Dupuy 2007). Once these points have been clarified, it is possible to take up some philosophical and metaphysical questions about nanobiotechnologies.

In 2006, the Nanoethics Group (http://www.nanoethics.org/), located in Cal Poly State University (San Luis Obispo, California), were awarded grants the National Science Foundation to study ethical issues related to human enhancement and nanotechnology. The role of nanotechnology in enhancement procedures is not clear. Enhancement may mean use of hormones or cosmetic surgeries or other procedures to enhance human performance (mental or physical) or appearance. The group is concerned that the accelerating pace of new technology may lead to some fantastic scenarios such as advanced cybernetic body parts and computers imbedded in the brains, which will raise ethical issues. In 2007, the Nanoethics Group released a collection of papers to address both urgent and distant issues related to nanotechnology's impact on society (Allhoff et al. 2007). It tackles a full range of issues facing nanotechnology, such as those related to: benefits, risk, environment, health, human enhancement, privacy, military, democracy, education, humanitarianism, molecular manufacturing, space exploration, artificial intelligence, life extension, and more (Allhoff et al. 2010).

In 2007, EGE, the European Group on Ethics in Science and New Technologies (http://ec.europa.eu/european_group_ethics/activities/index_en.htm) issued a draft report that recognizes the potential of nanomedicine in terms of developing new diagnostics and therapies. The group proposes that measures be established to verify the safety of nanomedical products and devices, and calls on the relevant authorities to carry out a proper assessment of the risks and safety of nanomedicine. It also recommended that there should be an EU website on ethics and nanomedicine, where citizens can find information and pose questions to researchers. Academic and public debates should be held on the issues raised by forthcoming developments

in nanomedicine. The report also placed a strong emphasis on the importance of carrying out more research into the ethical, legal and social implications (ELSI) of nanomedicine. They recommend that up to 3% of the nanotech research budget be set aside for ELSI research. They also call on the EC to set up a dedicated European Network on Nanotechnology Ethics. This network would bring together experts from a range of fields, promote deeper understanding of the ethical issues arising from nanotechnology and nanomedicine, promote education in these fields and work to ensure that ethics become embedded in research practices in nanomedicine and nanotechnology. The group also suggests that the EC fund a study on the social effects on nanomedicine in developing countries. On the legal front, EGE does not believe that structures set up specifically to deal with nanomedicine are needed right now. However, they suggest monitoring existing regulatory systems to ensure they do address all nanomedical products.

Nanotechnology Patents

Because of the tremendous potential of application of nanobiotechnology in healthcare, i.e. nanomedicine, and opportunities for commercialization, securing valid and defensible patent protection will be important in the future. Medical device companies seeking to implement nanotechnology in their products need to be aware of the emerging intellectual property (IP) trends in nanotechnology. US holds approximately 70% of the world patents in nanotechnology. The number of issued patents in nanotechnology has grown from less than 200 in 2000 to over 6000 by end of 2010 and there is a plethora of patent claims with backlog at the US Patent and Trademark Office (USPTO). One of the problems is an inadequate patent classification system and lack of differentiation between the term "nanotechnology", which is used to search patent databases and nanobiotechnology. Various types of patents covered include: nanomaterial, nanostructure, nanofiber, nanowire, nanoparticle, fullerene, quantum dot, nanotube, dendrimer, or nanocrystal. Patents are not classified according to areas of application relevant to healthcare.

The USPTO has created a preliminary classification for nanotechnology, designated as Class 977 Nanotechnology Cross-Reference Art Collection, and its purpose is described on its website (http://www.uspto.gov/web/patents/biochempharm/crossref.htm). It is the first step in a multiphase nanotechnology classification project and will serve to facilitate the searching of prior art related to nanotechnology, function as a collection of issued US patents and published pre-grant patent applications relating to nanotechnology across the technology centers and assist in the development of an expanded, more comprehensive, nanotechnology cross-reference art collection classification schedule. It is important to note that this digest should not be construed as an exhaustive collection of all patent documents that pertain to nanotechnology. Nanoparticles have been patented for diagnostic use as well as combined diagnostic and therapeutic use.

Quantum Dot Patents Relevant to Healthcare Applications

Most of the patents about QDs relevant to healthcare are owned by Life Technologies, which acquired Quantum Dot Corporation 2005. Life Technologies owns or has licensed over 160 QD patents or international patent applications currently under examination. The most important of these is QdotTM, which were originally developed at Lawrence Berkeley National Laboratory, and the University of Melbourne in Australia and licensed to Quantum Dot Corporation. Qdot nanocrystals enable powerful new approaches to genetic analysis, drug discovery, and clinical diagnostics.

In 2008, Life Technologies sued Evident Technologies for allegedly infringing the three QD patent and in 2009, the latter filed for Chap. 11 bankruptcy. The three patents at issue in the case were US Patent Nos. 6,423,551; 6,699,723; and 6,927,069. All three patents cover nanocrystal probe technology for biological applications and were issued to the University of California, which exclusively licensed the patents to Invitrogen (now part of Life Technologies) and its two subsidiaries, Quantum Dot and Molecular Probes. Evident Technologies currently develops quantum dot semiconductor nanocrystals for thermoelectric applications.

Challenges and Future of Nanobiotechnology Patents

Over the past decade, universities and companies have been engaged in an intense race to patent their nanotechnology inventions, seeking a source of future licensing revenue and control of an emerging technology, which has led to overlapping patent rights in nanotechnology. According to one estimate, approximately 20% of nanotechnology patents are owned by universities, a disproportionately large number considering that universities typically hold about 1-2% of the patents issued in the US each year (Mouttet 2006). Patent overlap can partially be attributed to the complex nature of nanotechnology itself and to the fact that much of the field is the result of cumulative innovation, where innovations are built on many previous innovations. Because multiple patents from competing groups may cover each incremental innovation to some degree, a large number of overlapping patents is inevitable as complex technologies become commercialized. Nanotechnology is fundamentally a multidisciplinary field that overlaps a wide range of scientific and technical disciplines: materials science, biotechnology, synthetic chemistry, electrical engineering, and physical chemistry. There is some confusion about the validity and enforceability of numerous issued patents and reforms are urgently needed at the USPTO to address problems about poor patent quality and questionable examination practices. A robust patent system is needed for the development of competitive and commercially viable nanomedicine products.

One of the conclusions of a review of this topic is that robust patent system will aid nanomedicine companies that are striving to develop commercially viable products (Bawa 2007). Valid patents stimulate market growth and innovation, generate revenue, prevent unnecessary licensing and greatly reduce infringement lawsuits.

Legal Aspects of Nanobiotechnology

Like any other new technology, nanobiotechnology is likely to raise some legal issues. Legal aspects of nanobiotechnology in healthcare, particularly cell therapy and tissue engineering, are discussed in a separate article (Jain and Jain 2006). An early publication had already anticipated some of these issues (Fiedler and Reynolds 1994). The authors of this publication suggested that appropriate controls, in the form of regulations and legislation, must be tailored to fit the risk/benefit ratio of nanotechnology. Active measures in anticipation of development of technology should be considered as passive waiting for regulations to develop may allow unnecessary harm to society from unregulated technology. This will involve discussion of likely directions nanobiotechnology will take and preparation of flexible legislation to provide appropriate regulatory schemes even before the products arrive in the market place. Considering that these suggestions were made more than a decade ago and considerable advances and applications have taken place in nanobiotechnology, no legislation has been implemented yet to control nanobiotechnology. Regulatory authorities such as the FDA are just discussing the possible regulation of nanobiotechnology.

There is no law until now concerning nanotechnology. Because of safety concerns of exposure to nanoparticles in the environments and at workplace, as well as applications in human healthcare there is a risk of lawsuits in the future. Therefore, it would be necessary to use existing regulations about the use of drugs and therapies as a model. But this field of technology requires a specified ruling because many problems will arise in the future, which are not ruled until now and the safety of human being should be guaranteed as a primary aim, which could be achieved through an extensive legal regulation. As example serves the application of a nanorobot; there is no similar machine existing, neither with the same function nor the same aim. Considering a case would arise in which a surgeon uses a nanorobot, which is either afflicted with a technical problem or applied wrongly. The question followed by such an act would as usual contain the search after a person to hold liable and result in a products liability, a negligent employment of nanodevices or a personal responsibility. But to handle problems in such a new technical field with its specified terms and characteristics it is critical to achieve an optimal dialog between the technologists and legal experts using common terms.

Standards (see following section) will play an important role in nanotechnology law. They are needed for consistent measurement and characterization of various nanomaterials. Guidelines about nanotechnology do not exist yet, but would be very helpful for potential legal problems such as tort liability. To avoid or simplify possible lawsuits of or against consumers, patients or companies it would be desirable to require a declaration for nanoparticles, which does not exist yet. Anybody who gets in contact with nanoparticles should get fully informed about the possible effects and critical nature. Companies marketing nanoparticle-based products for healthcare should inform the consumers about potential safety issues.

Legal aspects of nanobiotechnology are complicated by interaction and combination with other new technologies. Cell/gene therapies have their own ethical and legal issues. For example, genetic modification of cells with products incorporating nanobiotechnology may raise issues combining those of nanoparticles and genetic modification.

Nanotechnology Standards

The first meeting of the American National Standards Institute (ANSI) Nanotechnology Standards Panel (NSP) was held in 2004 with participation from academia, government, industry and non-governmental with the aim of defining the needs and priorities of nanotechnology standards. In considering nanotechnology nomenclature and terminology, the Panel participants reached consensus on several important issues but there was debate about the more general use of the terms 'nanotechnology,' 'nanomaterial,' and 'nano' generally. Some felt that keeping the definitions broad allowed the most relevant topics within this area and is in accordance with the spirit of the National Nanotechnology Initiative definition. Others preferred to narrow such terms more substantially, and where possible, draw distinctions in the names between artificial and naturally occurring nanomaterials, science and technology, among other issues. The group also addressed the need for future standards activity beyond terminology and nomenclature. The three broad classes identified were:

- 1. Measurement and metrology
- 2. Environmental, health, and safety guidelines. This is most relevant to nanobiotechnology and requires development of reference standards and testing methods for toxicity.
- 3. Processes and manufacturing

It appears the nanobiotechnology would require specific set of standards. None have been set so far. Apart from ANSI, there should be participation by the biopharmaceutical industry and academic researchers in nanobiotechnology. Organizations interested in participants are invited to contact ANSI-NSP at www.ansi.org/surveybank.

Preclinical Testing of Nanometerials for Biological Applications

Nanotechnology Characterization Laboratory (NCL) at Science Applications International Corporation (Frederick, Maryland) provides services for preclinical testing of nanomaterials for biomedical applications as a free national resource available to investigators from academia, industry (domestic as well as foreign) and government. The aim of this initiative is to characterize nanoparticles using standardized methods, conduct structure activity relationships studies and facilitate regulatory review of nanoconstructs. NCL is a formal collaboration between the NCI, FDA and NIST of the US. NCL assay cascade includes physicochemical characterization of nanoparticles as well as in vitro and in vivo studies. Adequate immunological characterization is considered difficult without comprehensive physicochemical characterization. Immunotoxicity of nanoparticles is determined by the size, charge, hydrophobicity and targeting. Even slight differences in a nanoparticle's properties can greatly influence its interaction with the immune system. Biocompatibility depends on surface charge, which is important for protein binding and uptake by the reticuloendothelial system (RES). PEGylation of nanoparticle surface, i.e. coating with polyethylene glycol (PEG), prevents uptake by the RES. Because there are no formal regulatory guidelines for immunotoxicity assessment, proper characterization of nanoparticles is difficult. NCL works with investigators to find solutions for some of these problems.

FDA Regulation of Nanobiotechnology Products

The FDA regulates a wide range of products, including foods, cosmetics, drugs, devices, and veterinary products, some of which may utilize nanotechnology or contain nanomaterials. The FDA has not established its own formal definition, though the agency participated in the development of the National Nanotechnology Initiative (NNI) definition of nanotechnology (see Chap. 1). Using that definition, nanotechnology relevant to the FDA might include research and technology development that both satisfies the NNI definition and relates to a product regulated by FDA. A review has discussed the drugs and medical devices approved by the FDA to date with observations about the emerging trends (Bobo et al. 2016). To date 51 medical products reportedly comprised of nanomaterials have already been approved by the FDA for prescription use in humans and 71 are in clinical trials. Examples of FDA-approved nanotechnology based drugs are shown in Table 18.1.

The first generation of nanomedicines (liposomal preparations) were approved more than a decade ago before a real awareness existed about several issues related to safety concerns of nanomaterials, and with a demonstrable relative success, in terms of their clinical safety assessment and safe use in the cancer. However, nanomaterials such as phospholipids or biodegradable/bioerodible polymers, are of a completely different nature from other anticipated materials that will be produced in the future from the research pipeline. Carbon nanotubes, quantum dots and other nonbiodegradable and potentially harmful materials should be given different and closer attention, looking at their toxicological potential impact in several different applications. By the same standards and in the new context, already existing nanopharmaceuticals, when administered for the same or new therapeutic indications making use of different administration routes (e.g. pulmonary), should not be waived of a full assessment of their differential potential toxicology impact, particularly in the proinflammatory area (Gaspar 2007).

Name	Company	Particle size	Full PMA	Animal studies	Human studies	Claimed benefit relevant to nanotechnology
Emend (aprepitant)	Merck & Co	<1000 nm	Yes	Yes	Phase II/III	Improved bioavailability and reduced food effect
Rapamune (sirolimus)	Wyeth	<1000 nm	No	No	Phase III	Improved solubility and reduction of effective dose
Estrasorb	Novavax	?	No	?	Phase III	Transdermal delivery
TriCor®145 fenofibrate	Abbott	<1000 nm	No	No	Phase III	Improved bioavailability and reduced food effect
Doxil® doxirubicin	ALZA	100 nm	No	?	Phase III	Improved bioavailability, cellular penetration, and accumulation at target site
Abraxane (paclitaxel)	Abraxix/ AstraZeneca	130 nm	No	Yes	Phase III	Improved solubility and elimination of toxicity of solvents
Megace® (megestrol)	Par Pharma	<1000 nm	No	No	Phase III (stopped)	Improved bioavailability

Table 18.1 FDA-approved nanotechnology based drugs

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The FDA approval is essential for clinical applications of new technologies and substantial regulatory problems may be encountered in the approval of nanotechnology-based products. Some of the previously approved products with particles in the nanosize range were not considered to be nanotechnology products and were subject to the same testing requirements as all other products reviewed by the agency. But some of the novel platforms being developed, such as the multifunctional dendrimers, may require a multifaceted approach toward their review and evaluation. There is every expectation that some novel products utilizing nanotechnology will be combination products (i.e. drug-device, drug-biologic, or device-biologic) and will likely undergo a relevant review process. To ensure that nanotechnology products are regulated in a coordinated fashion across all product types, the FDA has established a NanoTechnology Interest Group on which all FDA centers and offices that report to the Office of the Commissioner participate. Centers have established multidisciplinary working groups to share information and help coordinate the review for the various product types. The groups are charged with identifying and defining the scientific and regulatory challenges in the various review disciplines and to propose a path forward. However, the appropriate review divisions will conduct the review of nanotechnology applications submitted to FDA.

The Working Group on Nanotechnology has discussed the need for a central resource to acquire basic safety data such as biodistribution, pharmacokinetics, efficacy, and toxicity for nanoparticles and other macromolecules. Information on FDA and its regulation of nanotechnology products can be viewed at the FDA web site (http://www.fda.gov/). Some of the questions that FDA considers internally are:

- What are the standard tools used to characterize nanoparticle properties?
- How to determine the short- and long-term stability of nanomaterials in various environments?
- What are the critical physical and chemical properties of nanomaterials including residual solvents, impurities and excipients and how do these affect product quality and performance?
- What are the critical steps in the scale-up and manufacturing process of nanotechnology products?
- What is the residence time of nanoparticles in body tissues, their clearance from the body, and their effects on cell and tissue function?
- Are current methods used for measuring drug levels in blood and tissues adequate for assessing nanoparticle levels?
- What methods would identify the nature, quantity and extent of nanoparticle release in the environment and what would be the impact of this on other species?

While the significant impact of nanotechnology and its applications is expected to be in the future, FDA has already approved many products such as imaging agents and nanoparticle ingredients in sunscreens. There are also cosmetics currently on the market that claim to contain nanoparticles. However, cosmetics do not undergo premarket approval, as do drugs and devices. Finally, there are products on the market that are reformulated to contain nanoparticles of previously approved products to improve product performance. The position of the FDA not to require labels indicating that products contain nanomaterials has been controversial for some advocacy groups. Some of the existing cosmetic labeling requirements have been examined in the context of recent calls by advocacy groups for special labels for cosmetics containing nanoscale materials (Monica 2008). Although the FDA has made a serious attempt to address cosmetic nano-labeling issues, a more rigorous analysis of some nano-labeling arguments is required.

While sponsors of nanotechnology products will be subject to the same testing requirements as for non-nanotechnology products, there likely will be certain challenges prior to commercialization. Specifically, there will need to be an understanding of the physical and chemical parameters that are crucial to product performance. Additionally, appropriate test methods and specifications to control the product or the manufacturing processes may need to be developed.

Finally, because much of the data currently available on nanotechnology products results from pilot batches produced in universities or small laboratories, there is very little known about what might be the challenges of scale-up to mass production. While testing during the investigational phase of the product may be conducted with pilot batches, bridging the investigational data to cover the scaled-up batches that will be commercialized may pose challenges for some of the novel nanotechnology formulations. However, these challenges are not considered to be insurmountable.

FDA and Nanotechnology-Based Medical Devices

Medical Devices are handled by the Center for Devices and Radiological Health. There is no available evidence that any of the three currently approved medical devices containing nanoparticles had any additional pre-market safety or efficacy review, whether nano-specific or not. Two of these devices, NanOss and Vitoss, are to be used as filler in damaged bone, providing a framework to support new bone growth, and then be absorbed into the body. TiMesh is classified as a bone fixation device. It appears that all were permitted to go straight to market based on the sponsors' 510(k) claims that the products performed essentially the same function as devices using traditionally engineered materials have done for years. The regulatory documents for NanOss Bone Void Filler are representative of this group. Angstrom Medica filed its Rule 510(k) PreMarket Notification in 2005, describing a device made of calcium phosphate preformed pellets intended for gentle packing into bony voids or gaps not intrinsic to the stability of the structure. The sponsor claimed that NanOss is substantially equivalent in indications and design principles to several devices on the market prior to 1976. The device utilizes nanocrystalline processing, which are translucent and uniform in density and strength. FDA's approval letter for this device makes no reference whatever to nanotechnology. The documents supporting approval of the 510(k) application for the other bone void filler, Vitoss, mention a canine study showing that 80% of the Vitoss scaffold of nanoparticles was reabsorbed within 12 weeks. This study seems to have identified a novel property - faster reabsorption - that the sponsor attributed to the use of nanoparticles. Still, FDA accepted the claim that the product was substantially equivalent to bone void fillers that had been approved before, without considering the possibility that it might present new risks.

NanOss and TiMesh were considered Class II medical devices, and therefore could have been subject to special conditions. None were imposed by FDA. Unlike drugs, therefore, it appears that medical devices utilizing nanotechnology have not been subject to additional testing to establish that the new nano-products are safe and effective. The assumption that nanotechnology devices are substantially equivalent to products made of traditional materials and marketed prior to 1976 is scientifically unproven.

FDA's Nanotechnology Task Force

The FDA has an internal Nanotechnology Task Force, which is charged with the task of determining regulatory approaches that encourage the continued development of innovative, safe and effective FDA-regulated products that use nanotechnology materials (http://www.fda.gov/scienceresearch/specialtopics/nanotechnology/ucm 309672.htm). The FDA internal task force on nanotechnology's report was published in 2007. The summary of the report is as follows:

The report addresses scientific issues as distinct from regulatory policy issues in recognition of the important role of the science in developing regulatory policies in this area, rapid growth of the field of nanotechnology, and the evolving state of scientific knowledge relating to this field. Rapid developments in the field mean that attention to the emerging science is needed to enable the agency to predict and prepare for the types of products FDA may see in the future.

A general finding of the report is that nanoscale materials present regulatory challenges like those posed by products using other emerging technologies. However, these challenges may be magnified both because nanotechnology can be used in, or to make, any FDA-regulated product, and because, at this scale, properties of a material relevant to the safety and (as applicable) effectiveness of FDA-regulated products might change repeatedly as size changes to nanoscale and varies within the nanoscale range. In addition, the emerging and uncertain nature of the science and potential for rapid development of applications for FDA-regulated products highlights the need for timely development of a transparent, consistent, and predictable regulatory pathway.

The Task Force's initial recommendations relating to scientific issues focus on improving scientific knowledge of nanotechnology to help ensure the agency's regulatory effectiveness, particularly for products not subject to premarket authorization requirements. The report also addresses the need to evaluate whether the tools available to describe and evaluate nanoscale materials are sufficient, and the development of additional tools where necessary.

The Task Force also assessed the agency's regulatory authorities to meet any unique challenges that may be presented by FDA-regulated products containing nanoscale materials. This assessment focused on such broad questions as whether FDA can identify products containing nanoscale materials, the scope of FDA's authorities to evaluate the safety and effectiveness of such products, whether FDA should require or permit products to be labeled as containing nanoscale materials, and whether the use of nanoscale materials in FDA-regulated products raises any issues under the National Environmental Policy Act.

The Task Force concluded that the agency's authorities are generally comprehensive for products subject to premarket authorization requirements, such as drugs, biological products, devices, and food and color additives, and that these authorities give FDA the ability to obtain detailed scientific information needed to review the safety and, as appropriate, effectiveness of products. For products that are not subject to premarket authorization requirements, such as dietary supplements, cosmetics, and food ingredients that are generally recognized as safe (GRAS), manufacturers are generally not required to submit data to FDA prior to marketing, and the agency's oversight capacity is less comprehensive.

The Task Force has made various recommendations to address regulatory challenges that may be presented by products that use nanotechnology, especially regarding products not subject to premarket authorization requirements, considering the evolving state of the science in this area. Several recommendations deal with requesting data and other information about effects of nanoscale materials on safety and, as appropriate, effectiveness of products. Other recommendations suggest that FDA provide guidance to manufacturers about when the use of nanoscale ingredients may require submission of additional data, change the product's regulatory status or pathway, or merit taking additional or special steps to address potential safety or product quality issues. The Task Force also recommends seeking public input on the adequacy of FDA's policies and procedures for products that combine drugs, biological products, and/or devices containing nanoscale materials to serve multiple uses, such as both a diagnostic and a therapeutic intended use. The Task Force also recommends encouraging manufacturers to communicate with the agency early in the development process for products using nanoscale materials, particularly about such highly integrated combination products.

The guidance that the Task Force is recommending would give affected manufacturers and other interested parties timely information about FDA's expectations, so as to foster predictability in the agency's regulatory processes, thereby enabling innovation and enhancing transparency, while protecting the public health.

In 2011, FDA announced that it is issuing a draft guidance on considering whether an FDA-regulated product contains nanomaterials or otherwise involves the use of nanotechnology. FDA's issuance of this guidance is a first step toward providing regulatory clarity on FDA's approach to nanotechnology. Over time, the agency plans to issue more specific recommendations tailored to specific products or classes of products. These actions are consistent with the 2007 FDA Nanotechnology Task Force's science and policy recommendations to the Commissioner.

FDA Collaboration with Agencies/Organizations Relevant to Nanotechnology

With the advent of nanotechnology, the regulation of many products will involve more than one Center, for example a "drug" delivery "device". In these cases, the assignment of regulatory lead is the responsibility of the Office of Combination Products. To facilitate the regulation of nanotechnology products, the Agency has formed a NanoTechnology Interest Group (NTIG), which is made up of representatives from all the Centers. The NTIG meets quarterly to ensure there is effective communication between the Centers. Most of the Centers also have working groups that establish the network between their different components. There are also a wide range of products involving nanotechnologies, which are regulated by other federal agencies. The breadth of products regulated by FDA and the other agencies is shown in below.

The only viable approach to providing the public with innovative and beneficial novel therapies is to maintain an open dialogue with the developers of such products. As such, the FDA has partnered with NIST and NCI. However, this partnership does not create a "fast track" through the back door to product approval. It is intended to create a straight track, or an efficient and direct track through the front door.

By working together (FDA, academia and industry) during the early stages of product development and evaluation, the appropriate test methodologies can be identified to make sure that the correct tests are done at the outset. These early discussions also are critical because the most efficient and predictive testing is done on the final commercial form of the product. If the right questions can be asked early, then the process can move forward. Additionally, if some of the test methods used can be standardized, then many of the regulatory hurdles may be overcome.

Within FDA, the Office of Science and Health Coordination (OC/OSHC), coordinates regular discussions on nanotechnology among the major experts from every organizational entity within the Agency. Additionally the Centers within FDA, e.g. Drugs and Medical Devices, have organized similar regular discussion groups. The purpose of these meetings is to share experiences with the review of the products, insure that each Center is aware of product guidance that may be developing elsewhere within the Agency, and generally educate staff and policy makers about nanotechnology. Safety issues are identified and studied.

In a similar manner, FDA coordinates knowledge and policy with the other US Government agencies as a member of the Nanoscale Science and Engineering Technology (NSET) Subcommittee of the National Science and Technology Council (NSTC) Committee on Technology. Also, FDA and NIOSH co-chair the NSET Working Group on Nanomaterials Environmental and Health Implications (NEHI) to define new test methods/protocols to define safety of these products. Finally, FDA is a direct contributor to the evaluations of the toxicity of materials supported by the NIEHS and the National Toxicology Program (NTP).

The National Institute of Standards and Technology, the FDA, and the National Cancer Institute have established the Nanotechnology Characterization Laboratory to perform preclinical efficacy and toxicity testing of nanoscale materials.

Regulation of Nanotechnology in the European Union

The current impression is that the European Union (EU) will adopt a cautious approach to regulation of nanotechnology. Like in the US and elsewhere, there is no existing regulatory framework for nanotechnology in the EU. Some fear that Registration, Evaluation, Authorization, and restriction of Chemicals (REACH), the new EU's chemical policy, may be used as a source of reference for the regulation of nanotechnology, which might imply a qualified shift of the burden of proof for safety, from the authorities to the manufacturer. Product liability law is less likely to play a preponderant role, at least at the EU level (as opposed to within the individual Member States) because the EU's harmonization in this field of practice is limited. An overview of current and future EU regulation of nanotechnology, with some comparisons between the EU and US regulatory frameworks, has been published (Geert van Calster 2006).

The scope of Nanotechnology-based medicinal products for human use reflects current thinking and initiatives taken by the European Medicines Agency (EMEA) following recent development of nanotechnology-based medicinal products. Nanotechnology is an emerging scientific research field with wide applicability and, in the context of medical science, is expected to contribute in developing a more proactive paradigm for the diagnosis and therapy of disease. Medicinal products containing nanoparticles have already been authorized both in EU and the US under existing regulatory frameworks.

Although nanosizing does not necessarily imply novelty, it is expected that nanotechnology will yield innovative products. Such products could span the regulatory boundaries between medicinal products and medical devices, challenging current criteria for classification and evaluation. Appropriate expertise will need to be mobilized for the evaluation of the quality, safety, efficacy and risk management of nanomedicinal products and the need for new or updated guidelines will be reviewed in the light of accumulated experience. EMEA has created the Innovation Task Force (ITF) to ensure EMEA-wide coordination of scientific and regulatory competence in the field of emerging therapies and technologies, including nanotechnologies, and to provide a forum for early dialogue with applicants on regulatory, scientific or other issues that may arise from the development.

Safety Recommendations of the Royal Society of UK

The Royal Society of UK has issued a report "Nanoscience and nanotechnologies: opportunities and uncertainties" (http://www.nanotec.org.uk/report/summary.pdf), contains a section on the safety issues of nanotechnology. This study is the first of its kind and responses are expected from organizations within the UK as well as from other countries. Some comments and recommendations in the report are:

- Most nanotechnologies pose no new risks to health and almost all the concerns relate to the potential impacts of manufactured nanoparticles and nanotubes that are free rather than fixed to or within a material.
- It is very unlikely that new manufactured nanoparticles could be introduced into humans in doses sufficient to cause the health effects that have been associated with nanoparticles in polluted air.
- Until more is known about the environmental impacts of nanoparticles and nanotubes, the release of manufactured nanoparticles into the environment should be avoided as far as possible.
- The chemicals in the form of nanoparticles or nanotubes should be treated as new substances under the existing "Notification of New Substances (NONS)" regulations and in the "Registration, Evaluation, Authorization, and Restriction of Chemicals".
- Overall, given the appropriate regulation and research along the lines just indicated, there is no need for the moratorium, which some have advocated on the laboratory or the commercial production of manufactured nanomaterials.

European Commission and Safety of Nanocosmetics

The European Commission has requested the Scientific Committee on Consumer Products (SCCP) to prepare an opinion on "Safety of Nanomaterials in Cosmetic Products". The preliminary version of the opinion can be found online (http://ec.europa.eu/health/ph_risk/committees/04_sccp/docs/sccp_o_099.pdf). The results obtained with nanosized delivery systems were not consistent. The following list of potential properties was considered:

- Nanomaterials constituents (such as lipids or surfactants) may act as penetration enhancers by penetrating individually into the stratum corneum (after particle disruption on skin surface) and subsequently altering the intercellular lipid lamellae within this skin layer.
- Nanomaterials may serve as a depot for sustained release of dermally active compounds.
- Nanomaterials may serve as a rate-limiting membrane barrier for the modulation of systemic absorption, hence providing a controlled transdermal delivery system.

TiO2 used as a mineral UV-filter in sunscreen cosmetic product does not penetrate through the stratum corneum of healthy skin. It poses no local or systemic risk to human health from cutaneous exposure (Borm et al. 2006, Gamer et al. 2006). Little information is available concerning other nanoparticles. Current investigations of nanoparticle penetration into the skin using static imaging technology are unable to detect small fractions of nanoparticles reaching the dermis, vascular bed of the dermis, and hence, the blood stream. However, that if the administered dose of nanoparticles is very large, as for instance could be the case for TiO2 in sunscreens, a possible minute uptake of nanoparticles may be of relevance. A specific feature of nanoparticles is that not only the dose to the intake organ needs to be considered but also the dose in secondary target organs resulting fromnanoparticle biokinetic distribution. In addition, nanoparticles may affect more cell types than larger particles because of use of endocytotic and non-endocytotic pathways.

Although cosmetic products are meant to be used on normal skin, it is known that they also are applied on non-healthy skin where the barrier properties of may be impaired. There is no published information yet available on the potential penetration of nanomaterials through atopic or sunburnt human skin. The possible uptake of nanosized materials from cosmetics via inhalation has also been considered. The SCCP adopted a preliminary report on the risk assessment of nanomaterials in 2007. The report provides a review of the applicability of currently available risk assessment methods to nanomaterials in cosmetic products, recommends a general approach to assess the health risks of nanomaterials in cosmetic products and identifies data and methodological gaps where further research and development is needed.

References

- Allhoff F, et al. Nanoethics: the ethical and social implications of nanotechnology. New York: Wiley; 2007.
- Allhoff F, Lin P, Moore D. What is nanotechnology and why does it matter?: From science to ethics. Chichester: Wiley-Blackwell; 2010.
- Bawa R. Patents and nanomedicine. Nanomedicine. 2007;2:351-74.
- Bobo D, Robinson IJ, et al. Nanoparticle-based medicines: a review of FDA-approved materials and clinical trials to date. Pharm Res. 2016;33:2373–87.
- Borm PJ, Robbins D, Haubold S, et al. The potential risks of nanomaterials: a review carried out for ECETOC. Part Fibre Toxicol. 2006;3:11.
- Dupuy JP. Some pitfalls in the philosophical foundations of nanoethics. J Med Philos. 2007; 32:237-61.
- Fiedler FA, Reynolds GH. Legal problems of nanotechnology: an overview. South Calif Interdisciplinary Law J. Winter 1994.
- Gamer AO, Leibold E, van Ravenzwaay B. The in vitro absorption of microfine zinc oxide and titanium dioxide through porcine skin. Toxicol In Vitro. 2006;20:301–7.
- Gaspar R. Regulatory issues surrounding nanomedicines: setting the scene for the next generation of nanopharmaceuticals. Nanomedicine. 2007;2:143–7.
- van Calster G. Regulating nanotechnology in the European union. Nanotechnol Law Bus. 2006; 3:359–72.
- Gordijn B. Nanoethics: from utopian dreams and apocalyptic nightmares towards a more balanced view. Sci Eng Ethics. 2005;11:521–33.
- Jain KK, Jain V. Impact of nanotechnology on healthcare. Nanotechnol Law Bus. 2006;3:411-8.
- Monica JC. FDA labeling of cosmetics containing nanoscale materials. Nanotechnol Law Bus. 2008;5:63–72.
- Mouttet B. Nanotechnology and U.S. Patents: A Statistical Analysis. Nanotechnol Law Bus. 2006; 3:309–16.
- Parr D. Will nanotechnology make the world a better place? Trends Biotechnol. 2005;23:395-8.
- Resnik DB, Tinkle SS. Ethics in nanomedicine. Nanomedicine. 2007;2:345-50.

Chapter 19 Research and Future of Nanomedicine

Introduction

Research is an important activity in nanobiotechnology both in the academic and commercial sectors. Major portion of the research activity is in the commercial sector and is focused on translation into clinical applications as the number of products in the market is still limited. Two important segments of research in the commercial sector are nanodiagnostics and nanoparticle-based drug delivery. Whereas most of the academic research in the US is funded by government agencies, research in the commercial sector is funded by venture capital and other private sources. Research activities at various companies involved in nanobiotechnology are described. There are numerous collaborations between the academia and the industry and many discoveries made in universities are commercialized by the companies.

Nanobiotechnology Research in the Academic Centers

Almost every university and academic research organization is involved in research on nanobiotechnology. Since it is a relatively new area, most of the established scientists come from backgrounds such as physics, chemistry, engineering etc. The younger generation of scientists is receiving training and get involved in research at the start of their careers in nanotechnology. Some of the noncommercial institutes, where research is conducted in nanobiotechnology are shown in Table 19.1.

Center/program	Parent Institutes	Areas of interest
Applied NanoBioscience Center at Biodesign Institute	State University of Arizona (Tempe, AZ)	Nanoscale processing technologies for improving molecular diagnostics
Australian Institute for	University of	Cell and tissue engineering
Bioengineering and	Queensland	Systems biotechnology
Nanotechnology	(Brisbane, Australia)	Biomolecular nanotechnology
Biomedical Engineering Center	Industrial Technology Research Institute (Taiwan)	In vivo nanodevices, biomimetic sensing, nanobiolabeling/diagnosis
Bio-molecular Engineering Group	University of Missouri (Columbia, MO)	Engineered membrane protein channels used to make single molecule biosensors
BioSecurity and NanoSciences Laboratory	Lawrence Livermore National Laboratory (Livermore, CA)	Nanoscience to detect even the single smallest molecule of harmful substances
Birck Nanotechnology Center	Purdue University (West Lafayette, IN).	Nanocantilever biosensors for detection of microorganisms and use of bacteria for delivery of nanoparticles into the cell
Center for Nanomedicine, Sanford-Burnham Medical Research Institute	University of California (Santa Barbara, CA)	Nanoparticles that target tumors and bind to their blood vessels to destroy them
California Nanosystems Institute	UCLA (Los Angeles, CA)	Developing nanomedicine
Carolina Center of Cancer Nanotechnology Excellence	University of North Carolina (Chapel Hill, NC)	Self-assembling nanoparticles for imaging and therapy of cancer
Center for Bio/Molecular Science and Engineering	US Naval Research Laboratory (Washington, DC)	FRET-derived structure of a quantum dot-protein bioconjugate nanoassembly
Center for Functional Nanomaterials	Brookhaven National Laboratory (Upton, NY)	Study of interaction of nanomaterials with biosystems at level of single molecules
Center for Molecular Imaging Research	Massachusetts General Hospital (Boston, MA)	Nanoparticles for in vivo sensing and imaging of molecular events
Center for Nanotechnology	Wake Forest University (Winston-Salem, NC)	Controlling cellular function through nanoscale engineering, e.g., insertion of complex nanostructures into human monocytes
Center for Nanotechnology	University of Washington (Seattle, WA)	Bionanotechnology for cancer diagnostics and therapeutics
Center for Nanotechnology	NASA Ames Research Center (Moffett Field, CA)	Carbon nanotubes and nanowires for biological sensing
Center for Photonics and OptoElectronic Materials	Princeton University (Princeton, NJ)	Interphase of nanotechnology and biological systems

 Table 19.1
 Academic institutes/laboratories involved in nanobiotechnology

	Table 19.1 (con	tinued)
Center/program	Parent Institutes	Areas of interest
Cornell NanoScale Science & Technology Facility	Cornell University (Ithaca, NY)	Biosensors, drug delivery systems, microarrays
Centre for Nanoscale Science & Technology	Queen's University (Belfast, Ireland)	Nanostructured materials as templates for tissue engineering
Center for Nanoscience & Nanotechnology	Georgia Institute of Technology (Atlanta, GA)	Nanodevicies and nanosensors for biotechnology
Clinatec (a clinic specializing in nanotechnology-based treatment)	University of Grenoble (France)/Minatec	Nanoneurosurgey of degenerative neurological disorders
FIRST (Frontiers in Research, Space and Time)	Swiss Federal Inst of Technol (Zurich, Switzerland)	AFM as a nanolithography tool
Heath Group	California Institute of Technology (Pasadena, CA)	Nanobiology: Nanolab combines several assays on a cm ² silicon chip resembling a miniature cell farm with rows of cells
IMTEK – Institute of Microsystem Technology	University of Freiburg, (Freiburg, Germany)	Nanoparticles for biosensors
INSERM	Paris, France	Nanodetection, drug delivery
Institute of NanoScience and Engineering	University of Pittsburgh (Pittsburgh, PA)	Nanotubes for molecular diagnostics and nanocarpet to detect and destroy bacteria
Institute for Nanotechnology	Northwestern University (Evanston, IL)	Nanoparticles and biosensors; nano- bar-code for detection of proteins; nanofibers for neuroregeneration
Institute of Microtechnology	University of Neuchatel, Switzerland	Biological applications of nanotechnology
Institute of Micro- and Nanotechnology	Technical University of Denmark, Denmark	Study of nanoscale structures with in situ scanning tunneling microscopy
Institute of Physical Chemistry	National Centre for Scientific Research (Athens, Greece)	Polymer-based nanosponges, nanotubes, drug delivery
Interdisciplinary Nanoscience Center (iNANO)	University of Aarhus, Denmark	Polyplexes for delivery of bioactive agents: plasmid DNA and siRNA
Kavli Nanoscience Institute	California Institute of Technology (Pasadena, CA)	Nanoproteomics: single-molecule nanomechanical mass spectrometry
Laboratory for Micro- and Nanotechnology	Paul Scherrer Institute (Villigen, Switzerland)	Nanopore membranes, biosensors and artificial noses
Laboratory for Photonics and Nanostructures	CNRS (Marcoussis, France)	Separation methods for DNA sequencing Protein analysis and on-chip detection Microfluidic systems for cell sorting.
		(continued)

Table 19.1 (continued)

Center/program	Parent Institutes	Areas of interest
Lerner Research Institute	The Cleveland Clinic	Nanometer-scale tissue engineering,
	(Cleveland, OH)	diagnostics, nanosensors for surgery
London Center for Nanotechnology	University College (London, UK)	Use of nanotechnology to develop low cost diagnostics and drug-delivery systems, and personalized medicine
MacDiarmid Institute, BioNanotechnology Network	University of Canterbury (Christchurch, New Zealand)	Development of biochip for AFM imaging Biosensors by splicing polymers with QDs
Michigan Nanotechnology Institute	University of Michigan (Ann Arbor, MI)	Nanoemulsions as antimicrobial agents Dendrimers for drug delivery in cancer Magnetic nanoparticle MRI agents Dendritic polymer-based nanosensors
Micro and Nano Biosystems Laboratory	Boston University (Boston, MA)	Application of nanotechnology to tissue engineering and cell/drug encapsulation
NanoApplications Center	Oak Ridge National Laboratory (Oak Ridge, TN)	Nanostructured devices for controlled gene expression and Nano-enabled FILMskin (bionic): Flexible Integrated Lightweight Multifunctional skin
Nanotechnology Research Institute	University of Ulster (Jordanstown, UK)	In vivo nanobiosensors
National Center for Competence in Research Nanoscale Science	Biozentrum, University of Basel (Basel, Switzerland)	To bring nanotechnology from the bench to the patient by developing new tools
National Center for Nanoscience and Technology	Institute of High Energy Physics, Chinese Academy of Sciences, Beijing, China	Biomedical effects of nanomaterials and nanosafety
Nanobioengineering Laboratory	National University of Singapore (Singapore)	Nanohydroxyapatite/chitosan as resorbable bone paste
NanoBiomolecular Engineering Group	University of California (Berkeley, CA)	BioCOM cantilever chip for cancer diagnosis, DNA-based self-assembly/ replication of inorganic nanostructures, and electrophoretic separation microchip
Nano-Mechanical Technology Lab	Massachusetts Institute of Technology (Cambridge, MA)	Studyof changes in human cells for research projects on infectious diseases like malaria and sickle cell anemia, and cancers of the liver and pancreas
Nanomedicine Development Center	Emory University/ Medical College of Georgia, Atlanta	Focus on DNA damage repair by protein complexes

 Table 19.1 (continued)

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Center/program	Parent Institutes	Areas of interest
NanoRobotics Lab	Carnegie Mellon University (Pittsburgh, PA)	Nano-enabled imaging capsule to look inside the small intestine
NanoRobotics Laboratory	École Polytechnique de Montréal, Canada	Magnetic resonance targeting for guiding nanobots to targets in vivo
NanoBioTechnology Initiative	Ohio University (Athens, OH)	Diagnosis/treatment: cancer and diabetes
Nanoscale Research Team	University of California (Davis, CA)	Artificial cell membrane to study single protein interaction with cell membrane
Nanoscale Science Research Group: Biomedical Research	University of North Carolina (Chapel Hill, NC)	Cystic fibrosis Fibrin and blood clotting Gene therapy and viruses Bacterial motility Molecular motors
Nano-Science Center	University of Copenhagen (Copenhagen, Denmark)	Boron carbide nanoparticles for boron neutron capture therapy of cancer
Nano-Bio Research Center	Korean Institute of Science and Technology	Collaboration with Purdue University, USA for use of nanobiotechnology to integrate diagnostics and therapeutics
NanoSystems Biology	California Institute of Technology (Pasadena, CA)	Nanowire biosensors for early detection of cancer biomarkers
Nanosystems Laboratory	University of Washington (Seattle, WA)	Nanoprobes based on thin film technology for rapid and cheap sequencing DNA
Nantional Institute of Nanotechnology of Canada	University of Alberta (Edmonton, Canada)	X-ray scattering beamline to determine the size of biomolecules on nanoscale
Pharmaceutical Bioengineering & Nanotechnology Group	University of London (London, UK)	Bridging the gap between nanomaterials engineering and pharmaceutical science to develop nanomedicines
Purdue Nanomedicine Development Center	Purdue University (West Lafayette, IN).	NIH supported center for research on phi29 nanomotor for potential use in the diagnosis and treatment of diseases
Richard E. Smalley Institute for Nanoscale Science & Technology	Rice University (Houston, Texas)	Carbon nanotechnology Improved delivery of bioactive molecules, nanoscale sensory systems, biochips
Roukes Group	California Institute of Technology (Pasadena, CA)	Nanotechnology for neurophysiology Nanodevices for molecular biosensing
Sandia National Laboratories (Albuquerque, NM)	Dept of Energy, US Government	Nanodevices: biosensors to detect biological agents

Table 19.1 (continued)

Center/program	Parent Institutes	Areas of interest
Siteman Center of Cancer Nanotechnology Excellence	Washington University School of Medicine (St. Louis, MO)	Molecular imaging using nanoparticle tags and MRI, combined with therapy
Swiss Nanoscience Institute	University of Basel, Switzerland	Rapid and sensitive detection of disease- and treatment-relevant genes Toxicity of nanoparticles
USC Nanocenter	University of South Carolina (Columbia, SC)	Nanomedicine as well as social and ethical implications of nanotechnology
Winship Cancer Institute	Emory University (Atlanta, GA)	Cancer nanotechnology: nanoparticles for molecular and cellular imaging
Yale Institute for Nanoscience & Quantum Engineering	Yale University (New Haven, CT)	Smart nanoparticles: a new class of nanomaterials with properties that mimic biological vectors like bacteria and viruses, for vaccine delivery

Table 19.1 (continued)

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Clinical Trials of Nanomedicines

The approval of drugs for human use by the FDA through CDER is a time-consuming and expensive process, and approval rates of clinical trials are low. Advances in nanotechnology are being applied in the development of novel therapeutics that may address some of the shortcomings of conventional small molecule drugs and may facilitate the realization of personalized medicine. Appealingly, nanoparticle drug candidates often represent multiplexed formulations (e.g. drug, targeting moiety, and nanoparticle scaffold material). By tailoring the chemistry and identity of variable nanoparticle constituents, it is possible to achieve targeted delivery, reduce side effects, and prepare formulations of unstable (e.g. siRNA) and/or highly toxic drugs. However, these benefits also lead to new challenges in all aspects of regulated drug development and testing. CALAA-01 from Calando Pharmaceuticals, which is now taken over by Arrowhead Research Corp, was the first targeted siRNA nanoparticle drug administered to humans. Certainly, more are following the lead of CALAA-01 and each will present its own unique challenges.

Clinical trials of nanobiotechnology-based therapeutics number >250 and more than half of these are for cancer. The most frequest product involved is nab-paclitaxel (Abraxane) an already approved product in new combinations for different types of cancer. Clinical trials of nanodiagnostics and imaging using nanomaterilas are described in Chap. 4. Selected clinical trials of nanotechnology-based therapies are listed in Table 19.2.

Ladie 19.	Table 19.2 Cumical utals of nanolecrinology-based unerapies	aseu unerapies	
Product/method	Indication	Sponsor/identifier	Status
Anti-EGFR-immunoliposomes loaded with doxorubicin	Advanced triple negative EGFR positive breast cancer	Swiss Group for Clinical Cancer Research/NCT02833766	Phase II
BIND-014 (Docetaxel NPs) for IV injection	Advanced solid cancer Metastatic cancer	BIND Biosciences/ NCT01300533	Phase I completed
Carboplatin and paclitaxel albumin-stabilized NP formulation before surgery	Locally advanced or inflammatory triple negative breast cancer	City of Hope Medical Center, California/NCT01525966	Phase II
Cyclodextrin NP eyedrops to deliver drugs to the posterior part of the eye	Diabetic macular edema	King Saud Univ, Saudi Arabia/ NCT01523314	Phase II in 2012
Derma Vir, synthetic pathogen-like nanomedicine, which contains plasmid DNA expressing 15 HIV antigens, is targeted to Langerhans cells by topical administration with DermaPrep (Lisziewicz et al. 2012)	Immunization of HIV-1 infected treatment-naïve patients	Genetic Immunity/ NCT00712530	Phase II
Docetaxel polymeric micelle	Recurrent/metastatic head and neck squamous cell carcinoma	Samyang Biopharmaceuticals Corporation/NCT02639858	Phase II
FUS1-nanoparticles and erlotinib	Stage IV lung cancer	Genprex Inc/NCT01455389	Phase II
MRI/US fusion imaging and biopsy in combination with nanoparticle directed focal therapy	Refractory head and neck cancer	Nanospectra Biosciences Inc/ NCT02680535	Phase I
Nab-paclitaxel (paclitaxel albumin-stabilized NP formulation)/carboplatin followed by chemoradiation	Recurrent squamous cell cancer of the head and neck	University of Chicago/ NCT01847326	Phase II
Nab-paclitaxel, cisplatin, and cetuximab plus radiation therapy	Stage III or IV head and neck cancer	Univ Texas Southwest Med Ctr/ NCT00851877	Phase II
Nab-paclitaxel, doxorubicin, cyclophosphamide, and pegfilgrastim with or without bevacizumab	Inflammatory or locally advanced breast cancer	Southwest Oncology Group/ NCT00856492	Phase II
Nanoliposomal CPT-11	Recurrent high-grade gliomas	University of California, San Francisco/NCT00734682	Phase I completed
			(continued)

Table 19.2 Clinical trials of nanotechnology-based therapies

	Table 19.2 (continued)		
Product/method	Indication	Sponsor/identifier	Status
NANOM FIM: Plasmonic Nanophotothermic Therapy of Atherosclerosis	Coronary atherosclerosis with angina	Ural State Medical Academy, Russia/NCT01270139	Phase II completed Kharlamov et al. (2015)
NBTXR3 (X-ray nanomedicine) injection into the tumor + radiation	Adult soft tissue sarcoma	Nanobiotix	Phase I completed
NK105, a paclitaxel-incorporating micellar NP, compared to paclitaxel	Progression-free survival in recurrent breast cancer	Nippon Kayaku Co Ltd., Japan/ NCT01644890	Phase III
RSV-F protein NP vaccine plus licensed influenza vaccine co-administration	Respiratory syncytial virus (RSV)	Novavax/NCT01709019	Phase I completed
SNAPIST-III: nanoparticle paclitaxel (Abraxane®) administered via intracoronary catheter immediately following PTCA/stenting	Prevention of in-stent restenosis	Celgene/NCT00124943	Randomized phase I/II completed
TKM 080301 (lipid NPs containing siRNA against the PLK1 gene product) by hepatic intra-arterial administration	Colorectal, pancreas, gastric, breast, ovarian and esophageal cancers with hepatic metastases	Arbutus Biopharma Corporation/NCT02191878	Phase I completed in 2012
XIENCE Prime TM and XIENCE Nano TM everolimus- eluting coronary stent	Show safety and efficacy of stents in chronic total coronary occlusion	Abbott Vascular/NCT01435031	Prospective, multicenter, single-arm completed
© Jain PharmaBiotech Abbreviations: <i>NP</i> nanoparticle, <i>Nab-paclitaxel</i> paclitaxel albumin-stabilized NP formulation (Abraxane®), <i>PEI</i> polyethylenimine, <i>PICN</i> Paclitaxel injection concentrate for nanodispersion, <i>PTCA</i> percutaneous transluminal coronary angioplasty, <i>RONDEL</i> TM RNA/oligonucleotide nanoparticle delivery, <i>siRNA</i> small interfering RNA.	l albumin-stabilized NP formulation (A luminal coronary angioplasty, <i>RONDE</i>	Abraxane®), <i>PEI</i> polyethylenimine, L TM RNA/oligonucleotide nanopart	<i>PICN</i> Paclitaxel injection icle delivery, <i>siRNA</i> small

Table 10.2 (continued)

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Future of Nanomedicine

Disease and other disturbances of function are caused largely by damage at the molecular and cellular level but current surgical tools are large and crude. Even a fine scalpel is a weapon more suited to tear and injure than heal and cure. It would make more sense to operate at the cell level to correct the cause of disease, rather than remove large lesions resulting from disturbances at cell level.

Nanotechnology-based approaches can be used to remove obstructions in the circulatory system, kill cancer cells, or take over the function of subcellular organelles. Instead of transplanting artificial hearts, a surgeon of the future would be transplanting artificial mitochondrion.

Nanotechnology will also provide devices to examine tissue in minute detail. Biosensors that are smaller than a cell would give us an inside look at cellular function. Tissues could be analyzed down to the molecular level, giving a completely detailed "snapshot" of cellular, subcellular and molecular activities. Such a detailed diagnosis would guide the appropriate treatment.

It is expected that within the next few years, we will have a better understanding of how to coat or chemically alter nanoparticles to reduce their toxicity to the body, which will allow us to broaden their use for disease diagnosis and for drug delivery. Biomedical applications are some of the earliest. The first clinical applications in cancer therapy will expand.

Support for Nanobiotechnology by US Government Agencies

Nanomedicine Initiative of NIH

The National Institutes of Health (NIH) started a nanomedicine initiative on in 2004 by soliciting comments from the scientific community to help shape the research aimed at developing new tools to improve human health. The initiative, which is still ongoing, is a broad program that seeks to catalog molecules and understand molecular pathways and networks. Nanomedicine is one of several initiatives that make up NIH's roadmap, a long-term plan for improving and accelerating biomedical research. This is a program oriented towards addressing biological issues of health and clinical applications in a context of the overall mission of the NIH.

Unlike many research projects, NIH did not predetermine specific areas of study. Instead, it called for proposals aimed at helping to fulfill the project's goals. To start with there were debates to find the best way to proceed with the nanomedicine initiative. Much of the initial research took place at a few Nanomedicine Development Centers established by the initiative. The number of nanomedicine centers has increased over the years. Some examples of areas of study that have been funded by the NIH are:

- Probing of molecular events inside cells on biologically relevant time scales that may be on the order of milliseconds or microseconds or even nanoseconds.
- To design systems to engineer within living cells.
- To ensure the biocompatibility of some nanodevices in humans and develop devices that may eventually reduce the cost of health care.

US Federal Funding for Nanobiotechnology

The US National Nanotechnology Initiative (NNI) was signed into a law in 2010 and authorized \$3.7 billion over the following 4 years for the program. The bill also required the creation of research centers, education and training efforts, research into the societal and ethical consequences of nanotechnology, and efforts to transfer technology into the marketplace. Some of the recommendations based on findings of Triennial Review of the NNI that are relevant to nanomedicine include the following (Committee on Triennial Review of the National Nanotechnology Initiative 2016):

- The NIH should assess what emerging medical applications, in addition to cancer diagnostics and treatment, rely on engineered nanomaterials. NIH should expand the Nanotechnology Characterization Laboratory (NCL) to address nanomaterials being developed for these emerging medical applications.
- The National Institute for Occupational Safety and Health, the National Institute of Standards and Technology, and the Environmental Protection Agency should join with the Consumer Product Safety Commission and the National Institute of Environmental Health Sciences to support development of centralized nanobio-technological characterization facilities, at the NCL or elsewhere, to serve as trusted sources of information on potential environmental, health, and safety implications of nanomaterials.
- The NIH should lead the development of a roadmap, in collaboration with the nanomedicine industry, to identify technical barriers to scaling up the manufacture of nanomedicines, as well as areas in which research is needed to overcome those barriers.

NCI Alliance for Nanotechnology in Cancer

One of the most important applications of nanotechnology will be in cancer. In 2004, the National Cancer Institute (NCI) launched a \$144-million, 5-year plan to apply nanoscale technology for research and treatment of cancer. This brought together researchers, clinicians and public as well as private organizations to translate cancer-related nanotechnology research for the benefit of the patient. NIH/NCI

Nanotechnology Cancer Plan of 2015 includes a section on "Commercialization of nano-products for cancer and manufacturing challenges of nano-products" (http:// nano.cancer.gov/about/plan/).

Formation of the NCI Alliance for Nanotechnology in Cancer has brought together researchers, clinicians and organizations to develop and translate cancerrelated nano research into clinical practice. The alliance has created nano-research centers within existing public facilities and a laboratory for preclinical testing that will help boost regulatory review and translation of nanomaterials and devices into the clinical realm. More detailed information on the NCI Alliance for Nanotechnology in Cancer is available on the web site (http://nano.cancer.gov). The alliance is designed as one of the first steps in crafting a Cancer Nanotechnology Plan, which will include milestones to measure success over two time periods. Within the first 3 years, the plan calls for accelerating projects promising for near-term clinical application. After 3 years, the plan will focus on solutions to more difficult technological and biological problems that could affect detection and treatment. The goals of the alliance are:

- Rapidly advance new nanotechnology discoveries into cancer-relevant applications in clinical practice.
- Aid nanoparticle characterization and standardization of characterization methods to enable technology transfer from university laboratories to companies that bring these technologies to patients.
- Develop the next generation of cancer researchers in nanotechnology.

Translation of Nanotechnology in Cancer consortium was established in 2011 to bring together alliance-funded research centers, pharmaceutical and biotechnology companies, and patient advocacy groups to promote collaboration between academia and industry and share knowledge about best practices in translating nanotechnology from the laboratory to the marketplace. The consortium has formed a working group on nanomedicines to develop clinical protocols for testing them in patients and to address limitations specific to nanomedicine.

Nanotechnology Characterization Laboratory

To accelerate the transition of basic nanobiotechnology research into clinical applications, NCI established the Nanotechnology Characterization Laboratory (NCL), which is a collaboration of the NCI, the National Institute of Standards and Technology, and the FDA. NCL is working to provide an "analytical cascade for nanomaterial characterization." NCL facilitates clinical development and regulatory review of nanomaterials for cancer clinical trials; identifies and characterizes critical parameters related to nanomaterial absorption, distribution, metabolism, and excretion and toxicity profiles; and examines multicomponent/combinatorial aspects. NCL also facilitates academic and industrial-based knowledge sharing of nanomaterial performance data and behavior resulting from preclinical testing.

Centers of Cancer Nanotechnology Excellence

Centers of Cancer Nanotechnology Excellence (CCNE) with multi-disciplinary teams are the main venue for the discovery and tool development toward the application of nanotechnology to clinical oncology. CCNE teams are focused on integrated technology solutions and the aggressive development of these solutions from preclinical to clinical application. CCNEs are designed to enable multidisciplinary team research by linking physical scientists, engineers and technologists working at the nanoscale with cancer biologists and oncologists specializing in the diagnosis, prevention and treatment of cancer. The centers with their locations at academic institutions in the US are:

- Center of Cancer Nanotechnology Excellence for Translational Diagnostics at Stanford University
- Center for Multiple Myeloma Nanotherapy at Washington University
- MSKCC-Cornell Center for Translation of Cancer Nanomedicine at Memorial Sloan Kettering and Cornell University
- Nanosystems Biology Cancer Center at California Institute of Technology and University of California, Los Angeles
- Nucleic Acid-Based Nanoconstructs for the Treatment of Cancer at Northwestern University

Innovative Research in Cancer Nanotechnology

The Innovative Research in Cancer Nanotechnology (IRCN) engage in directed, product-focused research that aims to translate cutting-edge science and technology into the next generation of diagnostic and therapeutic tools. These platforms serve as the core technologies for a wide array of specific applications that will ultimately benefit cancer patients.

IRCNs are designed to enable multi-disciplinary team research and transformative discoveries in basic and preclinical cancer research. The proposed individual, circumscribed research projects are expected to address major barriers and fundamental questions in cancer biology, diagnosis, prevention and treatment of the disease using innovative nanotechnology solutions. To advance such new nanotechnology discoveries, the platform projects take advantage of the collaborative environment of the Alliance network. The awarded programs are listed below:

- Mechanical drugs: harnessing cancer aggressiveness to overcome its resistance/ Masimo Corporation
- Nanoscale metal-organic frameworks for light triggered and X-ray induced photodynamic therapy of head and neck cancers/University of Chicago
- Optimizing RNA nanoparticle's size and shape for enhancing cancer targeting and treatment/Ohio State University and University of Kentucky
- Stroma breaking theranostic nanoparticles for targeted pancreatic cancer therapy/Emory University

- Targeted core shell nanogels for triple negative breast cancer/University of North Carolina at Chapel Hill
- The rodent eye as a non-invasive window for understanding cancer nanotherapeutics/University of California, Davis
- Thermoresponsive NanoVelcro CTC purification system for prostate cancer profiling/University of California, Los Angeles and Cedars-Sinai Medical Center
- Treatment of glioblastoma using chain-like nanoparticles/Case Western Reserve University
- UCLA Multifunctional mesoporous silica nanoparticle platform for treatment of pancreas cancer/University of California, Los Angeles

Nanomedicine Center for Nucleoprotein Machines

In 2006, the NIH awarded Georgia Institute of Technology, Emory University and Medical College of Georgia a grant to partner on the Nanomedicine Center for Nucleoprotein Machines. The new center will initially focus on understanding how the body repairs damage to DNA, a problem that lies at the heart of many diseases and illnesses. As cells replicate, mistakes are created in the DNA that, if not repaired, cause defects that lead to illness. DNA breakage can also occur from ionizing radiation, which is found in the environment, cosmic rays, radon gas and even the soil, as well as in our bodies, primarily from potassium and carbon. Learning how protein complexes repair DNA damage could be the key to understanding structure-function relationships in the cell nucleus' protein machines, called nucleoprotein machines that synthesize, modify and repair DNA and RNA. This could someday be used to reverse genetic defects, cure disease or delay aging. By studying the way natural machines are engineered by the body, researchers will develop the general principles that will enable engineering of artificial machines that could carry out these processes for therapeutic purposes, e.g. to fix genetic defects. The center received over \$6 million from the NIH over the following 5 years, and approximately \$3 million from the Georgia Research Alliance, a public-private partnership of Georgia universities, businesses and government created to build the state's technology industry.

Global Enterprise for Micro-mechanics and Molecular Medicine

It is an international collaboration to use nanotechnology tools for global health and medical research. The members include the National University of Singapore and Institut Pasteur of France. The collaboration, called GEM4 or Global Enterprise for Micro-Mechanics and Molecular Medicine, represents an ambitious effort to apply global sourcing principles to research at the intersection of engineering and life sciences. It will use tools like AFM, laser tweezers, and nanoscale plate stretchers to study changes in human cells such as in sickle cell anemia and for research projects on infectious diseases like malaria. Further information can be obtained from web site: http://www.gem4.org/.

- Joint research projects
- Education and training
- Sharing of resources
- Communication and dissemination

Nano2Life will contribute to ensure the development of nanobiotech devices, material and services in agreement with international social and ethical standards and according to the needs of European industry. The network started operation in 2004 and has integrated over 170 researchers from 12 countries since then.

Nanomedicine in Europe

NANO2LIFE

NANO2LIFE (http://cordis.europa.eu/result/rcn/49721_en.html) was the first European Network of Excellence supported by the European Commission under the 6th Framework Program (FP6). These endeavours were undertaken to keep Europe as a competitive partner to USA and Asia. Its objective is to merge existing European expertise and knowledge in the field of nanobiotechnology to keep Europe as a competitive partner and to make it a leader in nanobiotechnology transfer. NANO2LIFE aims at setting the basis for a virtual European Nanobiotech Institute, focused on the understanding of the nanoscale interface between biological and non-biological entities, and its possible application in complex and integrated novel sensor technologies for health care, pharmaceuticals, environment, security, food safety, etc.

To accomplish its goals, NANO2LIFE had >200 scientists involved in a multifacetted joint program of activity (JPA) aiming at:

- Creating the first technological roadmap for nanobiotechnology
- Identifying the key bottlenecks that need to be overcome in nanobiotechnology
- Founding the first European ethical, legal and social aspects board (ELSA) in the field of nanobiotechnology
- Implementing a scientific program focused on 12 strategic research areas, considered as key areas for the future development of innovative nanobiodevices
- Constituting a durable and long lasting integration of the network partner resources
- Supporting mobility among the members in sharing expertise and scientific equipment
- Training the young scientists in complementary disciplines required in nanobiotechnology.

Multimedia supported activities were provided through education and awareness of the scientific and industrial community outside of NANO2LIFE. Information was given to the public about the impact of nanobiotech on industry and society. More than 200 researchers were regularly involved in NANO2LIFE as well as ~30 associate partners from industry and academia within Europe and outside Europe.

European Technology Platform on NanoMedicine

European Technology Platform on NanoMedicine, which is an industry-led consortium that is bringing together the key European stakeholders in the sector and is supported by the European Commission (www.etp-nanomedicine.eu). In 2005 it delivered a common vision of this technologically and structurally multi-faceted area, and defined the most important objectives in this Strategic Research Agenda (SRA) that addresses the member states of the European Union (EU), its candidate countries and associated states to the EU Framework Programs for research and technological development, as well as the European Commission itself. Its main aim is to put forward a sound basis for decision making processes for policy makers and funding agencies, providing an overview of needs and challenges, existing technologies and future opportunities in nanomedicine. The SRA also takes into consideration education and training, ethical requirements, benefit/risk assessment, public acceptance, regulatory framework and intellectual property issues, thus representing a possible reference document for regulatory bodies. The proposed disease oriented priority setting of this SRA is based on several parameters such as mortality rate, the level of suffering that an illness imposes on a patient, the burden put on society, the prevalence of the disease and the impact that nanotechnology might have to diagnose and overcome certain illnesses. The scientific and technical approach is horizontal and exploits the benefits of interdisciplinarity and convergence of relevant technologies via breakthrough developments in the areas of diagnosis, targeted delivery systems, and regenerative medicine. The effective implementation of the SRA is expected to provide a major step forward in patient oriented affordable healthcare.

European Union's "Horizon 2020"

"Horizon 2020" is the biggest EU Research and Innovation program ever with $\sim \notin 80$ billion (\$83 billion) of funding available over 7 years (2014–2020) in addition to the private investment (http://ec.europa.eu/programmes/horizon2020/). It promises more breakthroughs, discoveries and world-firsts by taking great ideas from the lab to the market. To ensure the safe development and application of nanotechnologies, Horizon 2020 aims to advance scientific knowledge of the potential impact of

nanotechnologies on health or on the environment, and to provide tools for risk assessment and management along the entire life cycle. Expected impact is:

- Supporting European competitiveness through accelerated market uptake of nano-enabled products.
- Improvement in existing manufacturing processes and industrial productivity. It clearly articulates a set of goals that addresses the challenge of scale-up for the generation of nanomedicines.
- Promoting safe-by-design approaches and contributing towards the framework of EU nanosafety and regulatory strategies (including standardization)
- Providing significant long term societal benefits in terms of improved health care and improved quality of life

European Nanomedicine Characterisation Laboratory

European Nanomedicine Characterisation Laboratory (www.euncl.eu/), funded by Horizon 2020, was established in 2015 to provide critical infrastructure and characterization services that are needed for emerging nanomedicines ready for translation and clinical trials. Its mission is:

- To provide a trans-disciplinary testing infrastructure covering a comprehensive set of preclinical characterization assays (physical, chemical, in vitro and in vivo) enabling researchers to study the biodistribution, metabolism, pharmacokinetics, safety profiles and immunological effects of nanomedicines.
- To promote the use of standard operating procedures, benchmark materials, and quality management for the preclinical characterization of nanomedicines.
- To promote inter-sectorial and inter-disciplinary communication among key drivers of innovation, especially between developers and regulatory agencies.

References

- Committee on Triennial Review of the National Nanotechnology Initiative. Report. Washington, DC; NAS, National Academies Press; 2016.
- Kharlamov AN, Tyurnina AE, Veselova VS, et al. Silica-gold nanoparticles for atheroprotective management of plaques: results of the NANOM-FIM trial. Nanoscale. 2015;7:8003–15.
- Lisziewicz J, Bakare N, Calarota SA, et al. Single DermaVir immunization: dose-dependent expansion of precursor/memory T cells against all HIV antigens in HIV-1 infected individuals. PLoS One. 2012;7(5):e35416.

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